



Center of pressure control for balance maintenance during lateral waist-pull perturbations in older adults

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ABSTRACT

When balance is disturbed, location of the center of pressure (COP) contributes to a person's ability to recover from a perturbation. This study investigated COP control prior to first step lift-off (FSLO) during lateral perturbations in older non-fallers and fallers. 38 non-fallers and 16 fallers received lateral waist-pulls at 5 different intensities. Crossover stepping responses at the intensity level where the largest number of subjects responded with crossover steps were analyzed. Whole-body center of mass (COM) and COP positions in the medio-lateral (ML) direction with respect to the base of support (BOS), and COP velocity were calculated. An inverted pendulum model was used to define the BOS stability boundary at FSLO, which was also adjusted using the COP position at FSLO (functional boundary). No significant differences were found in the COP velocities between fallers and non-fallers ($p > .093$). However, the COP positions for fallers were located significantly more medial at FSLO ($p \leq .01$), resulting in a significantly reduced functional boundary. Although the stability margins, measures of stability based on the BOS, were significantly larger than zero for fallers ($p \leq .004$), they were not significantly different from zero for the functional boundary, i.e., reaching the functional stability limit. Fallers had reduced functional limits of stability in the ML direction, which would predispose them to more precarious stability conditions than non-fallers. This could be a cause for taking more steps than non-fallers for balance recovery as we observed. The functional boundary estimation may be a more sensitive marker of balance instability than the BOS boundary.

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1. Introduction

Falls are the leading cause of serious injuries in older people due to age-related declines in balance control (Nevitt et al., 1989; Tinetti et al., 1988). An impaired ability to control lateral balance is an important aspect of balance problems contributing to falls (Maki and McIlroy, 2006; Rogers and Mille, 2003). A directional vulnerability to falling sideways among older individuals has been supported by a previous prospective study (Hilliard et al., 2008), recent experimental findings on multi-directional protective stepping (Mille et al., 2013), and an observational surveillance study of real-life falls (Robinovitch et al., 2013).

In order to effectively recover balance when standing stability is perturbed, protective steps must be appropriately timed and adjusted to arrest the motion of the whole-body center of mass (COM) (Mille et al., 2013). Older adults are much more likely than younger adults to take multiple balance recovery steps (Luchies

et al., 1994; Maki et al., 2000; Mille et al., 2013, 2005), where an inability to recover lateral balance with a single step is predictive of future falls (Hilliard et al., 2008). Moreover, younger adults more often use a side step maneuver with the limb that is passively loaded by the lateral perturbation, whereas older adults more frequently use crossover steps with the passively unloaded limb (Mille et al., 2013, 2005). While crossover stepping with the passively unloaded leg facilitates the onset of stepping, it increases the potential for inter-limb collisions and subsequent falls (Maki et al., 2000; Mille et al., 2005). Thus, balance recovery steps for older adults appear to be less efficient using multiple steps and less effective with more inter-limb collisions using crossover strategies.

While protective stepping parameters after first step lift-off (FSLO), such as step count and step type, could be used as measures of dynamic balance function, they do not fully capture the evolving state of balance stability represented by the COM-base of support (BOS) relationship. For example, the location of the center of pressure (COP) prior to FSLO contributes to a person's ability to recover balance from a perturbation. When standing balance is disturbed, acceleration (or deceleration) of the COM is directly related to the distance between the COP and COM (Winter et al., 1998). Since the BOS provides a possible area for COP movement, the BOS boundaries have been considered as stability limits within which balance is maintained by

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rapidly moving the COP to keep the COM from going outside the BOS (Hof et al., 2005; Pai et al., 1998; Winter, 1995). Therefore, how “fast” and how “far” the COP moves with respect to the BOS prior to FSLO is importantly involved with dynamic balance control.

In addition to the COM–BOS relationship, balance would not be maintained if the COM has a sufficiently large horizontal velocity (Brown et al., 1999; McIlroy and Maki, 1996; Pai and Patton, 1997; Pai et al., 1998). Thus, dynamic balance stability has been quantified based on the position–velocity relationship between the COM and BOS (Carty et al., 2011; Hof et al., 2005; Pai and Patton, 1997; Pai et al., 1998), where an analysis applied to the frontal plane showed that older adults used a conservative strategy by stepping well before their stability limit was reached (Patton et al., 2006).

While these models used the BOS boundaries as limits of COP control, it has been shown that the functional limit of the BOS (FBOS), defined as the effectively utilized area for COP movement, is decreased with aging (Fujimoto et al., 2013; King et al., 1994). Such a reduced FBOS would limit an individual's ability to maintain balance because the COP–COM distance is proportional to the COM acceleration (Winter et al., 1998), which is important for regulating the momentum induced by perturbations as described earlier. A reduced area used for COP movement could predispose older individuals to a precarious condition for maintaining balance stability.

To further address these issues, the objective of this study was to investigate the COP control prior to and at FSLO during cross-over protective stepping in response to lateral perturbations of standing balance in older non-fallers and fallers. COP velocity prior to FSLO and COP position at FSLO were calculated to assess the COP control. An inverted pendulum model was used to define the

BOS lateral stability boundary at FSLO, which was also adjusted using the COP position at FSLO (functional boundary). We hypothesized that fallers would demonstrate a reduced functional boundary with a slower COP velocity than non-fallers.

2. Methods

2.1. Subjects

Thirty-eight healthy, community dwelling older adults [non-fallers: 19 men/19 women; age: 74.1 (SD 7.5) years; height: 1.67 (SD 0.09) m; body mass: 76.2 (SD 14.2) kg], and 16 healthy older adults with a history of falls [fallers: 6 men/10 women; age: 72.9 (SD 4.6) years; height: 1.67 (SD 0.11) m; body mass: 80.0 (SD 19.2) kg] participated in this study. Any individual who fell one or more times in the year prior to testing was categorized as a faller (Lord et al., 1999). A fall was defined as “coming to rest unintentionally on the ground or lower level, not as a result of a major intrinsic event (such as stroke) or overwhelming hazard” (Tinetti et al., 1988). Participants were medically examined by a physician to assess exclusion criteria including: (1) cognitive impairment (Folstein Mini Mental Score < 24); (2) sedative use; (3) non-ambulatory; (4) any clinically significant functional impairment related to musculoskeletal, neurological, cardiopulmonary, metabolic or other general medical problems; (5) participation in any regular vigorous or muscle strengthening exercise regimen; and (6) Centers for Epidemiological Studies Depression Survey score > 16. All participants provided written, informed consent prior to participation, and the study was approved by the Institutional Review Board at the University of Maryland School of Medicine and the Baltimore Veteran's Administration Medical Center.

2.2. Data collection

Participants received a total of 60 randomly applied, position-controlled, motor-driven waist-pull lateral perturbations at five different intensities (Levels 1–5) in the left and right directions (L and R pulls). The system has been previously described (Pidcoe and Rogers, 1998) and used in prior studies (Hilliard et al., 2008; Mille et al., 2013, 2005; Young et al., 2013; Yungher et al., 2012). Participants wore a waist belt to which cables were attached and through which the perturbations were applied. Six trials were conducted for each intensity and direction (2 directions × 5 intensities × 6 repetitions). The order in which the trials were presented was randomized to minimize anticipation and sequence learning effects. Participants stood in a self-selected, comfortable standing position at the start of each trial with each foot on a separate force platform (AMTI, Newton, MA, USA). The foot locations were traced onto the platform surface to ensure consistent initial foot placement over the trials. Participants were instructed to “relax and react naturally to prevent themselves from falling.”

Whole body motion was captured with a six-camera motion analysis system (Vicon 460, Oxford, UK). 28 reflective markers were placed according to Eames et al. with additional markers on the medial malleoli and 5th metatarsophalangeal (MP) joints (Eames et al., 1999). Three-dimensional marker trajectories were collected at 120 Hz and smoothed using a fourth-order Butterworth filter with a cut-off frequency of 8 Hz. Ground reaction forces (GRFs) were collected by two force platforms located under each foot at 600 Hz and filtered with a 10 Hz cut-off frequency (Hernandez et al., 2012; Maki et al., 1994).

2.3. Data analysis

Since crossover stepping is a common maneuver used by older adults to recover lateral balance (Maki and McIlroy, 2006; Mille et al., 2005), responses to the lateral waist-pulls at intensity Level 4, where the largest number of subjects responded with crossover steps (74% non-fallers (28/38) and 44% fallers (7/16) for L pulls, and 71% non-fallers (27/38) and 69% fallers (11/16) for R pulls), were

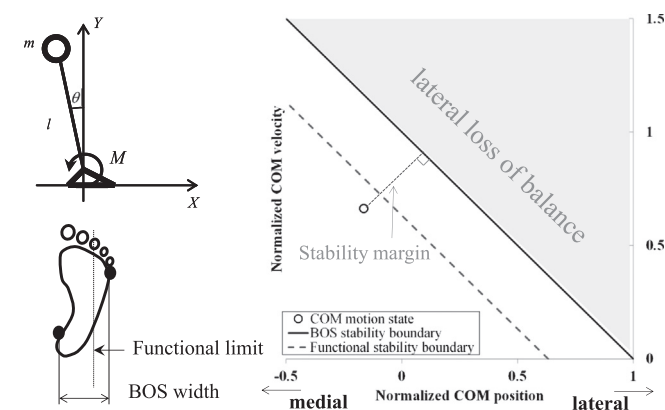


Fig. 1. A single-link-plus-foot inverted pendulum model in the frontal plane and lateral stability boundaries. X indicates the COM position in the medio-lateral direction. m , l and M are whole body mass, pendulum length (distance from the ankle to the COM), and ankle joint moment. The lateral stability boundaries were defined in two ways: one with the BOS width (BOS stability boundary), and the other adjusted with the COP position at FSLO, considering it as a functional limit for COP movement (functional stability boundary). Stability margins were calculated as the shortest distances from the experimental data to those stability boundaries.

Table 1

Subjects' age, height, weight and stance width. Data are presented as mean (SD). Stance width was calculated as the mean distance between the left and right lateral ankles and 5th MP joints in the ML direction prior to the onset of perturbation. No significant differences were found between non-fallers and fallers ($p \geq .087$).

COP velocities	L pull			R pull		
	Non-fallers	Fallers	p	Non-fallers	Fallers	p
# of subjects	15 Men/13 women	1 Man/6 Women		16 Men/11 Women	4 Men/7 Women	
Age [years]	72.8 (7.1)	71.7 (4.9)	.635	74.1 (7.3)	72.6 (4.6)	.450
Height [m]	1.67 (0.08)	1.62 (0.04)	.087	1.68 (0.08)	1.69 (0.12)	.807
Weight [kg]	76.6 (14.2)	73.9 (15.8)	.653	77.6 (14.2)	82.7 (20.9)	.388
Stance width [cm]	33.6 (4.5)	35.0 (3.4)	.460	34.2 (4.4)	36.4 (3.5)	.160

analyzed. Each set of L and R pulls consisted of 6 repeated trials, and the averages for those trials were used as representative values for each subject.

The whole-body COM was calculated as the weighted sum of 13 body segments, including head and neck, trunk, pelvis, 2 upper arms, 2 forearms with hands, 2 thighs, 2 shanks, and 2 feet (Eames et al., 1999). COM and combined COP positions in the medio-lateral (ML) directions at FSLO were referenced to the medial ankle and normalized to the BOS width. The BOS width was the ML distance between the medial ankle and 5th MP joint of the stance foot determined prior to the perturbation onset (Fig. 1). Peak and average COP velocities prior to FSLO were also calculated both before and after stance width normalization (Maki et al., 1994). FSLO timing was determined as the instant when the vertical GRF dropped to less than 10 N (Brauer et al., 2002). Step onset latency was calculated as the time between the perturbation onset and FSLO. Average COP velocity was the average over the time between the perturbation onset and FSLO.

A single-link-plus-foot inverted pendulum model was used to define the lateral stability boundary at FSLO, the beginning of the single-limb support phase (Fig. 1), using the following equation (Hof et al., 2005):

$$\tilde{X}_{SO} \leq 1 - \tilde{X}_{SO}$$

where \tilde{X}_{SO} and \tilde{X}_{SO} are normalized COM position and velocity at FSLO in the ML direction, defined as $\tilde{X}_{SO} = (X_{SO} - X_{ma})/L_w$, $\tilde{X}_{SO} = \dot{X}_{SO}/(L_w\omega_0)$ ($\omega_0 = \sqrt{g/L}$, L_w : BOS width, X_{ma} : medial ankle, L : pendulum length). In addition, since previous studies have shown that the area functionally used for COP movement is smaller than the BOS (Fujimoto et al., 2013; King et al., 1994), the lateral stability boundary was also determined based on the COP position at FSLO, considering it as a functional limit for COP movement (Fig. 1). Thus, the lateral stability boundaries were defined in two ways: one with the BOS (BOS boundary), and the other adjusted according to the functional limit (functional boundary). In each case, the stability margin was defined as the shortest distance from the experimental data to the respective

boundaries (Yang et al., 2009). A larger stability margin indicates that the COM motion state is within the stability limits.

An independent *t*-test was performed to examine between-group differences in the subject characteristics (age, height, weight, and initial stance width), step count, step onset latency, the ML COP velocities prior to FSLO, the COM position and velocity as well as COP position at FSLO, and the stability margins at FSLO. Since our previous study did not identify any differences in outcome measures between the perturbation directions (Young et al., 2013), no direct comparisons were made between the left and right perturbations. One sample *t*-tests were also performed to determine if the stability margin was significantly different from zero. Statistical analyses were performed using SPSS (Chicago, IL). Significance level was set at $\alpha = .05$.

3. Results

No significant differences were found in the age, height, weight, and initial stance width between fallers and non-fallers ($p > .087$, Table 1). Fallers took more recovery steps than non-fallers (L pull: 1.8 (SD 0.5) vs 2.5 (SD 0.9) steps, $p = .007$; R pull: 1.7 (SD 0.5) vs 2.9 (SD 1.3) steps, $p = .014$). Although not significant, fallers showed longer step onset latency than non-fallers (L pull: 333 (SD 102) ms vs. 385 (SD 113) ms, $p = .24$; R pull: 386 (SD 95) ms vs. 423 (SD 113) ms, $p = .32$). The COP relative to the medial ankle of the stance foot was initially displaced in the pull direction prior to FSLO and reached a plateau after FSLO (Fig. 2). COP velocity also reached a peak level prior to FSLO. The same trend was observed for fallers.

No significant differences were found in the peak or average COP velocities between the groups, regardless of the pull directions ($p > .093$, Table 2). However, the values of the COP positions at FSLO for fallers were up to 18% smaller than those for non-fallers for both pull directions (L pull: 0.64 (SD 0.07) vs 0.52 (SD 0.10), $p = .002$; R pull: 0.63 (SD 0.07) vs 0.56 (SD 0.06), $p = .01$, Fig. 3). This indicates that COP positions with respect to the stance side BOS for fallers were more medially located compared to non-fallers, which resulted in more medially located functional boundaries for fallers (Fig. 4). No significant differences were found for the COM positions and velocities at FSLO ($p > .457$, Fig. 4).

Although not statistically significant, fallers demonstrated a similar or larger stability margin than non-fallers based on their BOS boundary (L pull: 0.38 (SD 0.19) vs 0.37 (SD 0.32), $p = 0.917$; R pull: 0.29 (SD 0.20) vs 0.34 (SD 0.31), $p = .543$), while the stability margins of fallers became smaller or similar to those of non-fallers when the functional boundary was used (L pull: 0.13 (SD 0.17) vs 0.03 (SD 0.29), $p = .288$; R pull: 0.03 (SD 0.18) vs 0.04 (SD 0.28), $p = .964$) (Fig. 5). In addition, while the functional stability margin was significantly different from zero for L pulls for non-fallers (0.13 (SD 0.17), $p = .001$), it was not significantly different from zero for R pulls for non-fallers (0.03 (SD 0.18), $p = .37$), or for both L and R pulls for fallers (0.03 (SD 0.29) and 0.04 (SD 0.28), $p > .68$).

4. Discussion

The objective of this study was to investigate COP control during medio-lateral crossover stepping in older non-fallers and fallers.

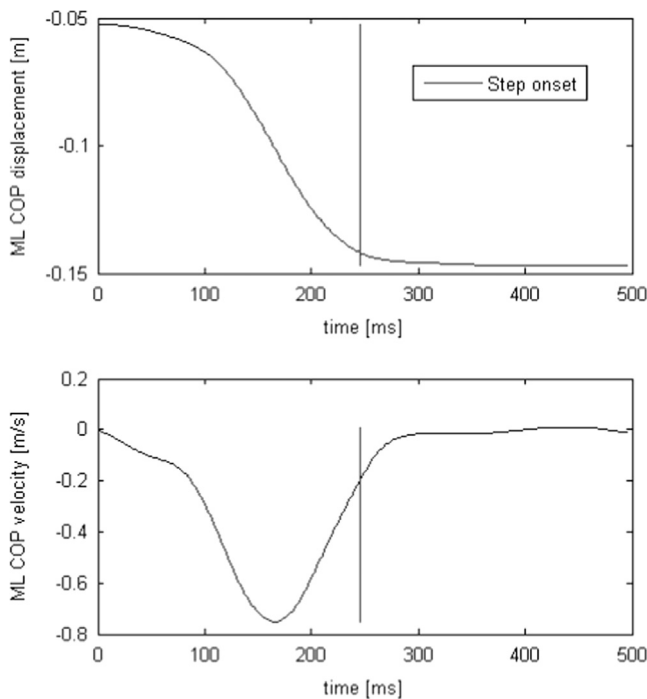


Fig. 2. Representative time-history plot of COP displacement relative to the medial ankle of the stance foot (Left) for L pull for non-fallers group. Negative is to the left. The same trend was seen in the faller group.

Table 2

Peak and average COP velocities prior to FSLO before and after normalization (Norm) by stance width. Data are presented as mean (SD). Pull direction is positive. No significant differences were found between non-fallers and fallers ($p > .093$).

COP velocities	L pull			R pull		
	Non-fallers	Fallers	<i>p</i>	Non-fallers	Fallers	<i>p</i>
Peak [m/s]	0.99 (0.20)	0.97 (0.33)	.873	0.86 (0.19)	0.89 (0.18)	.608
Norm Peak [/s]	2.95 (0.53)	2.75 (0.79)	.437	2.51 (0.45)	2.46 (0.49)	.782
Average [m/s]	0.42 (0.11)	0.37 (0.12)	.268	0.39 (0.10)	0.37 (0.11)	.685
Norm average [/s]	1.28 (0.31)	1.06 (0.28)	.093	1.15 (0.28)	1.04 (0.33)	.289

No significant differences were found in the COP velocities between the groups prior to FSLO. However, the COP positions for fallers were located significantly more medial at FSLO, suggesting that the area functionally used for COP movement was significantly reduced for fallers as was hypothesized. These results suggested that fallers might be predisposed to more precarious stability conditions than non-fallers because such a reduced area for COP movement would diminish the limits of lateral stability for COM control.

Fallers took more recovery steps than non-fallers, which is consistent with previous findings (Mille et al., 2013) and corroborated the use of multiple steps as a predictor of fall risk (Hilliard et al., 2008). Neither the peak nor average COP velocities differed between the groups, in agreement with a previous report of COP speed during induced ML sway (Maki et al., 1994). The COP velocity may reflect the amount of balancing activity that is needed to maintain a stable upright posture (Maki et al., 1994). Crossover stepping takes advantage of the passive unloading beneath the stepping limb in initiating the response unlike lateral side stepping that requires active unloading of the passively loaded leg (Mille et al., 2005). Such a reduction of active

postural movement for crossover steps might have contributed to the lack of difference in COP velocities between the groups.

The COP position for fallers was more medially located than that for non-fallers. This indicated that the area functionally used for COP movement in the ML direction was significantly reduced in fallers, which resulted in a significant reduction in the functional stability boundary. Although the BOS is the area within which the COP can possibly move, the area effectively used for COP movement, i.e., FBOS, to control the COM was limited. Age-related decreases in the FBOS have been previously reported in the AP direction (Fujimoto et al., 2013; King et al., 1994). The present results further indicated that the area used for COP movement can also be limited in the ML direction and reduced in older adults at greater risk for falls, thus constricting the limits of lateral stability. Since the range of the COP excursion needs to be greater than that of the COM to effectively reduce the momentum induced by perturbations, such a reduced area for COP movement would limit one's ability to maintain balance.

Because of this functional limitation, larger stability margins based on the BOS might not always mean that they are well within the stability limits as suggested previously for forward and lateral induced stepping (Pai et al., 1998; Patton et al., 2006; Rogers and Mille, 2003). In fact, although the stability margins for fallers were significantly different from zero for the BOS boundaries, they were not significantly different for the functional boundaries, i.e., reaching the functional stability limit. These results suggested that even when the COM motion state for fallers is located farther from the BOS boundary than for non-fallers, it is possible that they have approached their functional limit. Therefore, the functional boundary estimation may be a more sensitive marker of balance instability than the BOS boundary. In this regard, a previous study of lateral balance recovery reported that older fallers stepped well before they reached their stability limit during crossover steps (Patton et al., 2006). It is plausible that older adults at greater risk for falls adopt a more conservative strategy by preserving greater BOS stability margins. However, our results indicated that fallers might actually be predisposed to more precarious stability conditions than those estimated by the BOS boundaries because of the reduction in their functional limit for COP movement.

What caused such a reduction in the functional limit in fallers? An earlier step initiation time due to safety concerns has been

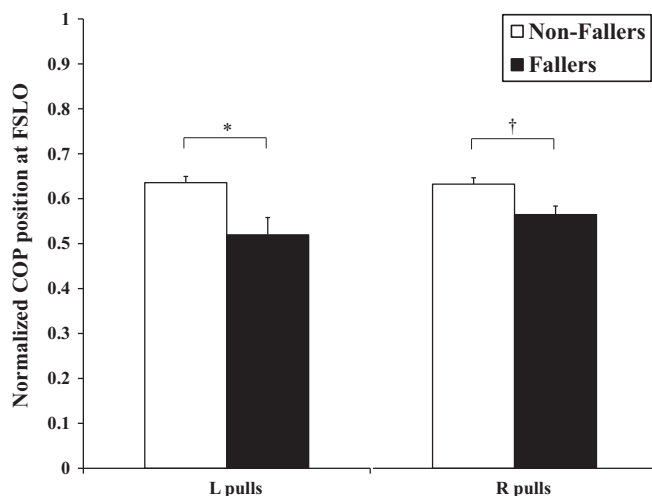


Fig. 3. Normalized COP positions at FSLO for non-fallers and fallers. Values and error bars are mean and SEM. (* $p=.002$, † $p=.01$).

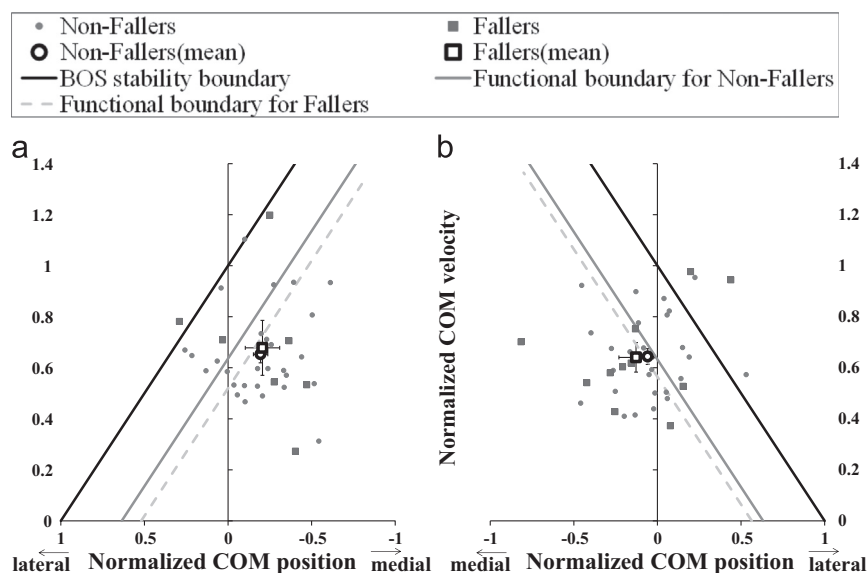


Fig. 4. Normalized COM velocity vs. normalized COM position at FSLO in the ML direction for non-fallers (♦) and fallers (■) for (a) L pull and (b) R pull. Mean for each group (◇ and □) are also indicated. Error bars are SEM. The solid line indicates the BOS stability boundary. The two dashed lines indicate the functional stability boundaries for non-fallers and fallers. Since the functional boundaries vary between subjects, the average for all subjects within the group was shown here.

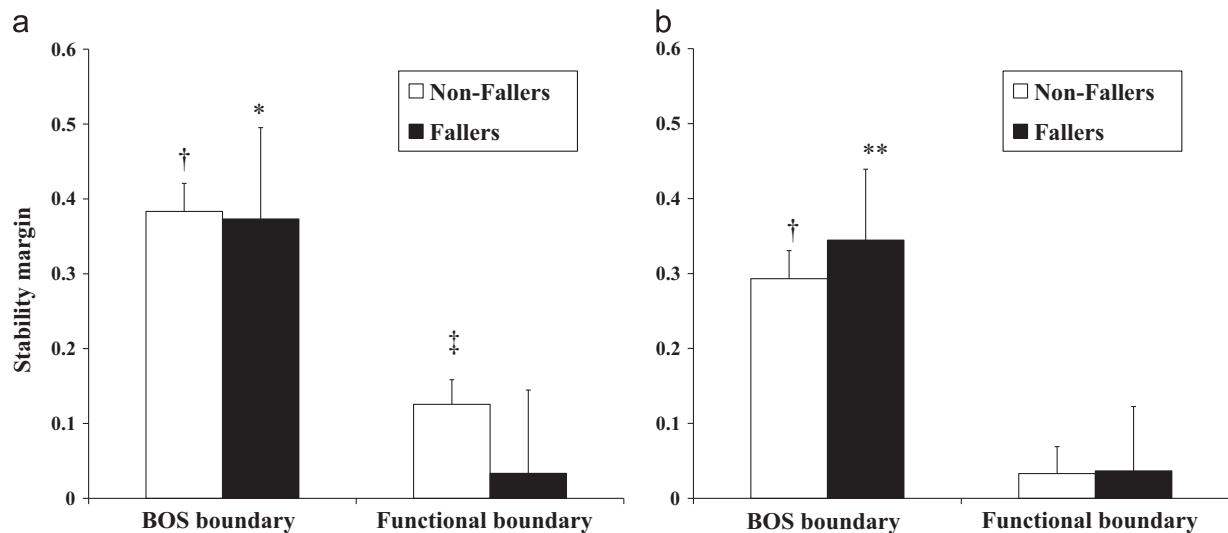


Fig. 5. Stability margins based on the BOS and functional stability boundaries for (a) L pull and (b) R pull. Values and error bars are mean and SEM. *, **, †, and ‡ indicate that the stability margin is significantly different from zero (* $p < .001$, ** $p = .004$, † $p = .011$, ‡ $p = .042$).

previously reported in older adults and fallers (Mille et al., 2013; Rogers et al., 2001). Such an earlier step initiation due to anxiety about falling could limit the COP movement before FSLO. However, in this study, the fallers showed a tendency to have a later step onset time than non-fallers. Therefore, it is unlikely that a later step onset contributed to the more medially located COP in fallers since a later step onset would result in a more laterally located COP imposed by the perturbation. From a motor control perspective, the reduced area for COP movement could be related to ankle or hip muscle performance capacity. Ankle invertor–evertor and hip abductor–adductor muscle torques contribute to the lateral COP movement (Rietdyk et al., 1999). A reduction in muscle strength or power related to the risk of falls could therefore have contributed to the functional stability differences between the groups. Furthermore, deterioration in foot plantar mechanoreception might also have contributed to the reduced area for COP movement. Previous studies have indicated an influential role for cutaneous sensation from the plantar surface of the foot in the control of balance, where impaired cutaneous sensation has been associated with impaired postural control and increased risk of falling (Lin et al., 2010; Lord et al., 1994; Maki et al., 1999; Perry, 2006; Perry et al., 2000, 2008). Diminished sensation could play a role in detecting the proximity of the COM to the stability boundaries of the BOS to maintain balance (Maki et al., 1999). Further investigation is needed to determine the relationship between neuromuscular and sensorimotor functions and COP control during lateral balance recovery responses.

Among the limitations of the study is the smaller number of subjects classified as fallers. However, the significant findings pertaining to a medially located COP position at FSLO for fallers would only likely be further strengthened with a larger sample size and increased statistical power. Another limitation is that we did not control for the number of recovery steps used by participants which could have influenced the results obtained by using combined single and multiple stepping trials. However, even when the same analyses involved only the multiple stepping trials it did not affect the findings, where the COP positions for fallers were located significantly more medial (non-fallers vs. fallers: 0.63 (SD 0.08) vs. 0.52 (SD 0.10), $p = .005$ (L pulls); 0.63 (SD 0.08) vs. 0.56 (SD 0.06), $p = .015$ (R pulls)). It should also be noted that the functional stability margin for non-fallers was significantly different from zero for L pulls, although it was not significantly different for R pulls, indicating asymmetries in dynamic balance stability.

Although such asymmetries in stability margins were not seen in fallers, the causes remain to be determined.

In conclusion, COP position with respect to the BOS at FSLO for fallers was found to be located more medial to that for non-fallers, indicating reduced functional limits of dynamic stability. This implies that even when fallers seem to use a more conservative strategy than non-fallers, ensuring a greater stability margin in relation to their BOS, the stability margin relative to the functional limit for COP movement could still be smaller. The functional limit might therefore provide more sensitive estimation of lateral stability. The reduced functional limits of stability for fallers would predispose them to more precarious stability conditions than non-fallers by limiting their ability to regulate COM momentum induced by perturbations. Consequently, this could be a biomechanical cause for lateral instability requiring older fallers to take more steps than non-fallers for balance recovery.

Conflict of interest statement

The authors have no conflicts of interest in relation to the work reported here.

Acknowledgments

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