

# Ectoenzyme switches the surface of magnetic nanoparticles for selective binding of cancer cells



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## ABSTRACT

Enzymatic switch, such as phosphorylation and dephosphorylation of proteins, is the most important mechanism for cellular signal transductions. Inspired by Nature and encouraged by our recent unexpected observation of the dephosphorylation of D-tyrosine phosphate-contain small peptides, we modify the surface of magnetic nanoparticles (MNP) with D-tyrosine phosphate that is a substrate of alkaline phosphatase (ALP). Our studies find that ALP is able to remove the phosphate groups from the magnetic nanoparticles. Most importantly, placental alkaline phosphatase (ALPP), an ectoenzyme that locates on cell surface with catalytic domains outside the plasma membrane and is overexpressed on many cancer cells, dephosphorylate the D-tyrosine phosphates on the surface of the magnetic nanoparticle and enable the magnetic nanoparticles to adhere selectively to the cancer cells, such as HeLa cells. Unlikely commonly used antibodies, the selectivity of the magnetic nanoparticles to cancer cells originates from the enzymatic reaction catalyzed by ALPP. The use of enzymatic reaction to modulate the surface of various nanostructures may lead to a general method to broadly target cancer cells without relying on specific ligand–receptor interactions (e.g., antibodies). This work, thus, illustrates a fundamentally new concept to allow cells to actively engineer the surface of colloids materials, such as magnetic nanoparticles, for various applications.

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## 1. Introduction

The intersection of nanotechnology and molecular cell biology, over the last decade, has developed into an emerging research area: nanobiotechnology. As a versatile functional colloid material, magnetic nanoparticles offer controlled size, ability to be manipulated externally, and enhancement of contrast in magnetic resonance imaging (MRI) [1–13]. Consequently, magnetic nanoparticles have already been explored for many applications in biology and medicine [14–24], including protein purification [25,26], bacteria capture and inhibition [27,28], drug delivery [29,30], band gap materials [31,32], and medical imaging [33–35]. In order to make magnetic nanoparticles to be biofunctional, one of most common strategy is to attach antibodies to magnetic nanoparticles to target cell specifically [36,37]. Despite its effectiveness, this approach relies on the tight ligand–receptor binding, which becomes ineffective when the receptors on the cells mutate and no longer bind to the ligand on the nanoparticles. This generic drawback of ligand–receptor interactions highlights the need of a new approach to use nanoparticles to target the cell without rely-

ing on tight and specific ligand–receptor binding. Recently, we unexpectedly observed that alkaline phosphatase (ALP) catalytically removes the phosphate group from the D-tyrosine phosphate residue of a D-peptide at (almost) the same rate as that from the corresponding L-peptide [38]. The insensitivity of ALP to stereochemistry of its substrates lead to another surprise that placental alkaline phosphatase (ALPP), an ectoenzyme located on cell surface with catalytic domains outside the plasma membrane and overexpressed on HeLa cells, results in the formation a hydrogel/nanonet on the cancer cell surface, thus selectively inhibit the cancer cells [39,40]. These results indicate that ALPP on cancer cells may dephosphorylate D-peptides on magnetic nanoparticles, thus allowing the nanoparticles to interact with cancer cells selectively.

Based on the above rationale, we simply decorate magnetic nanoparticles with D-tyrosine phosphates to be a new type of substrate (MNP\_pY) of phosphatases. We find that ALP is able to dephosphorylate the D-tyrosine phosphates on the magnetic nanoparticles. Moreover, ALPP overexpressed on the surface of cancer cells [41,42] catalytically dephosphorylate the phosphate-bearing magnetic nanoparticles to form tyrosine coated magnetic nanoparticles (MNP\_Y) that adhere to the cancer cells. On the contrary, HS-5 cells, a stromal cell that has low level expression of ALPP [43], fail to trigger the adherence of the magnetic nanoparticles to HS-5

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cells. Moreover, MNP\_Y adheres to neither HeLa cells nor HS-5 cells, suggesting that the enzymatic switch of the surface of the magnetic nanoparticles is responsible for the selective binding of the magnetic nanoparticles to the cancer cells (see Scheme 1). This result represents a fundamentally new approach for selectively targeting cancer cells because it relies on enzymatic reaction near the cell surface rather than on a specific ligand–receptor interaction. The use of the ectoenzyme on cells to actively engineer the surface of nanoparticles, thus, provides a new opportunity to design the applications of nanoparticles, based on the spatiotemporal distribution of a specific enzyme, for disease diagnosis and treatment.

## 2. Experimental methods

### 2.1. Materials and instruments

Iron oxide nanoparticles with amphiphilic polymer coating and a monolayer of oleic acid were purchased from the Ocean Nano-Tech company. Transmission electron microscope images were collected by using Morgagni 268 microscope. Confocal images were taken with the Leica TCS SP2 Spectral Confocal Microscope. The cells were counted by a hemacytometer.

### 2.2. Phosphate assay

We quantify the amount of phosphate on MNP\_pY with the purchased phosphate assay kit (colorimetric) (ab65622, abcam). First, we made the 0, 1, 2, 3, 4, 5 nmol of phosphate standard solutions, mixed 200  $\mu$ l these standard solutions and 30  $\mu$ l phosphate reagent for 30 min, and read the absorbance at 620 nm using a plate reader. Similarly, when quantifying the amount of phosphate on MNP\_pY, we followed the same protocol. After incubating 40  $\mu$ g MNP\_pY with 100  $\mu$ l dH<sub>2</sub>O or 100  $\mu$ l dH<sub>2</sub>O containing 30 U alkaline phosphatase (ALP) for 24 h, we centrifuged the nanoparticles and the solutions. We took 20  $\mu$ l treated solution out and adjusted the volume to 200  $\mu$ l with dH<sub>2</sub>O. With the treatment with 30  $\mu$ l phosphate reagent for 30 min at room temperature, we read the absorbance by using a plate reader.

### 2.3. Cell culture

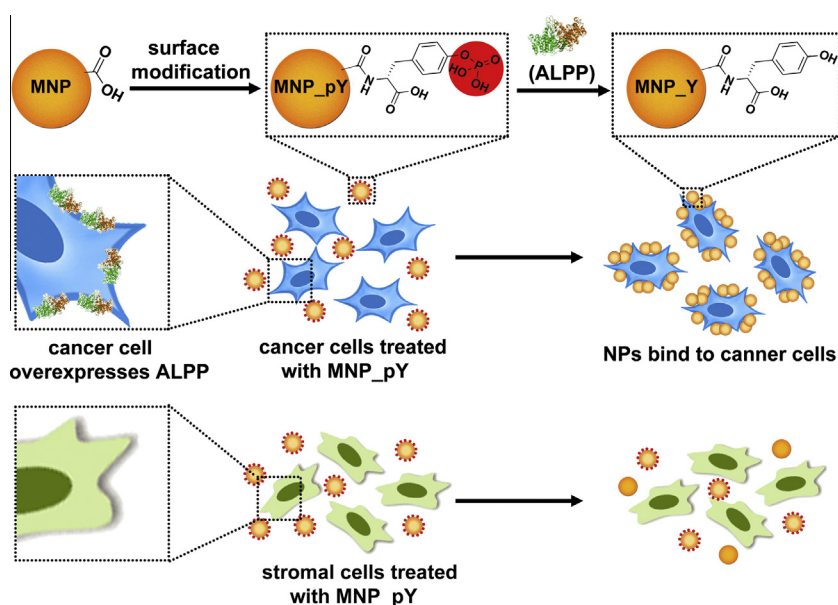
The HeLa-GFP and HS-5 cells were purchased from the American Type Culture Collection (ATCC, Manassas, VA, USA). Both of the cells were incubated in a fully humidified incubator containing 5% CO<sub>2</sub> at 37 °C with the growth medium, Dulbecco's Modified Eagle Medium (DMEM, Invitrogen Life Technologies, 10829-018) supplemented with 10% fetal bovine serum (FBS, Invitrogen Life Technologies, 10082-147), 100 U ml<sup>−1</sup> penicillin and 100  $\mu$ g ml<sup>−1</sup> streptomycin (Invitrogen Life Technologies, 15070-063).

### 2.4. Confocal microscopy

Initially,  $1.0 \times 10^6$  cells were seeded in 6 cm cell culture dish with 5 mL growth medium. The cells were allowed for 12 h to adhere on culture dish. New medium containing MNP\_pY, MNP\_Y, or MNP at the concentration of 40  $\mu$ g/mL was added into each dish after the old medium was removed. With 4 h of incubation, cells were washed with growth medium for 3 times and detached with 0.25% (w/v) Trypsin- 0.53 mM EDTA solution. As described in the main text, after harvesting all the cells, we separated extraction from supernatant by using one small magnet, rinsed the two cells for three times with growth medium, and then seeded them back onto the confocal dishes. 4 h later, the cells were rinsed for three times in PBS, and then kept in the PBS buffer for imaging.

## 3. Results and discuss

The synthesis of MNP\_pY is fast and straightforward. Starting from the well-established iron oxide nanoparticles (MNP) that are surface-functionalized with carboxylic acid groups (and are commercially available), we use N-hydroxysuccinimide (NHS) to activate the carboxylic acid groups on the nanoparticles for directly coupling them with D-tyrosine phosphate. Following three times rinsing by methanol and water, respectively, centrifugation separates the final MNP\_pY dispersed in water for use. Transmission electron microscopy (Fig. 1) confirms that, except an increased clustering on the TEM grids, there is little morphological change of the iron oxide nanoparticles before and after functionalization



**Scheme 1.** Ecto-enzyme transforms magnetic nanoparticles for selectively binding with cancer cells.

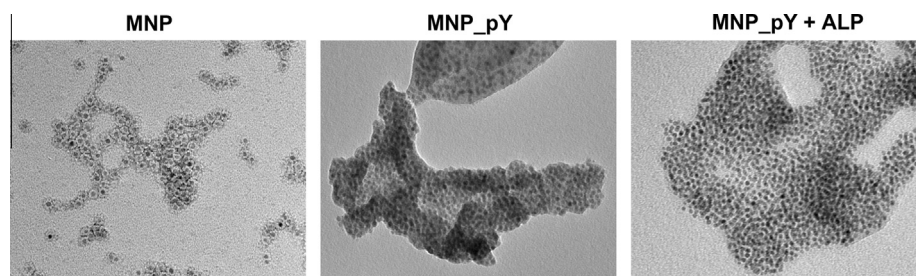
by D-tyrosine phosphates (Fig. 1). The nanoparticles MNP, coated with a layer of amphiphilic polymer and a layer of oleic acid, already cluster to form small aggregates that consist of the particles with a diameter of around 10 nm. Similarly, both MNP\_pY and MNP\_Y (which results from the treatment of MNP\_pY with ALP), also form aggregates of nanoparticles that still have well-defined iron oxide cores and amphiphilic coatings.

To determine the number of D-tyrosine phosphate molecules decorated on the surface of the MNP, we utilized the phosphate assay to quantify the amount of phosphate on MNP\_pY (Fig. 2). According to the phosphate standard curve (Fig. 2A), we can conclude that there are at least 34 nmol D-tyrosine phosphate molecules on the surface of 40  $\mu$ g MNP\_pY (Fig. 2B), considering that the treatment of MNP\_pY with ALP for 24 h unlikely remove all the phosphates from the nanoparticles. According to the manufacture data of the commercial iron oxide nanoparticles, there are 6.9 nmol particles of 1 mg iron oxide, which means 40  $\mu$ g MNP\_pY contains 0.28 nmol nanoparticles. Thus, this quantification of phosphate on MNP\_pY indicates that, on average, there are at least 124 D-tyrosine phosphate molecules on each MNP\_pY nanoparticles.

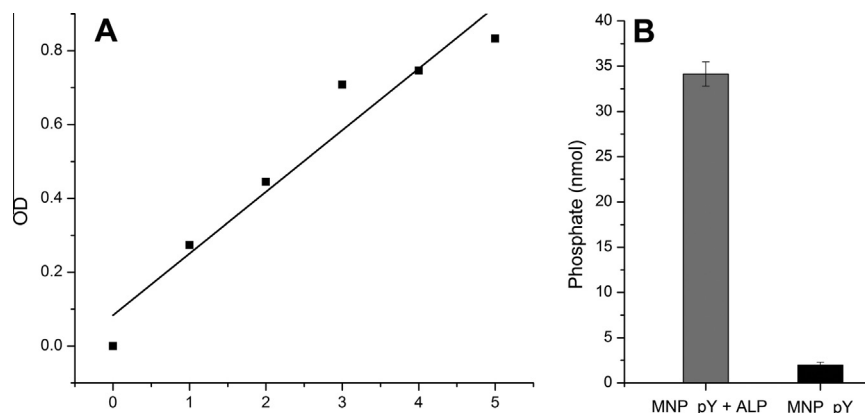
After determine the numbers of the D-tyrosine phosphates on the surface of the MNP, we incubated the nanoparticles and the relevant controls to prove the selective interaction between the nanoparticles and cancer cells. The procedure for testing the selective binding of these nanoparticles to cells is exceptionally simple. After seeding about  $1.0 \times 10^6$  HeLa-GFP or HS-5 cells per culture dish (6 cm) overnight,[44] we add MNP\_pY, MNP\_Y, or MNP (40  $\mu$ g/mL) to incubate the cells for 4 h. After removing the growth medium containing nanoparticles and rinsing the cells for three times, we use trypsin solution (0.25% (w/v) in 0.53 mM EDTA) to detach the cells. Following aspirating the cells to obtain the cell suspension by gently pipetting, we place a small magnet outside

the Eppendorf tube for 1 min to divide the cell suspension into two portions: supernatant and extraction. After the centrifugation and rinse of the supernatant or extraction, the pellets of cells are reseeded onto confocal petri dishes for imaging which acts as a way to verify the results of the interactions between nanoparticles and cells.

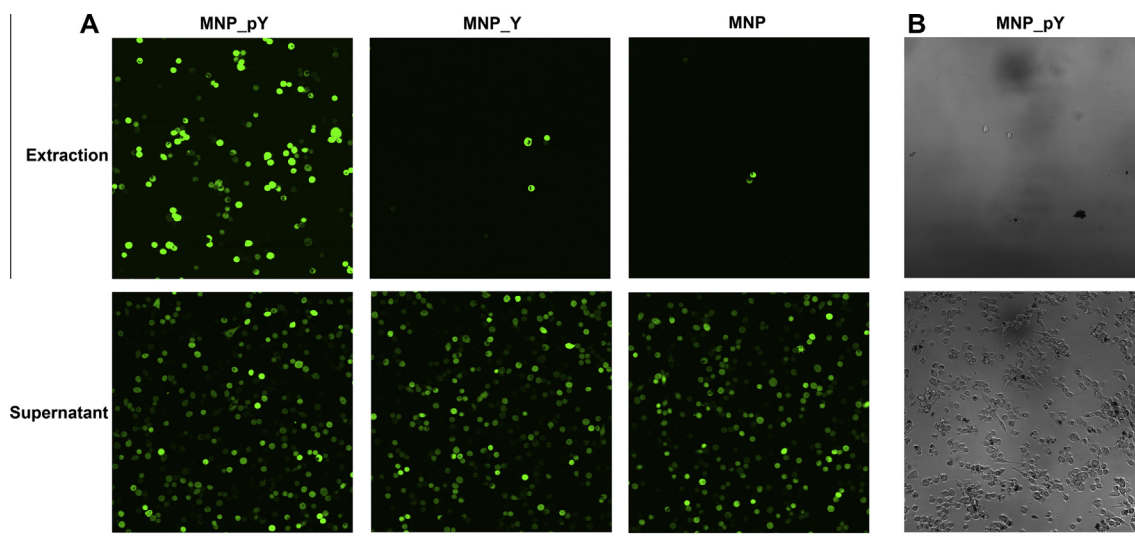
Figs. 3 and 4 show the results of the binding of HeLa-GFP cells (Figs. 3A and 4A) and HS-5 cells (Figs. 3B and 4B) treated with MNP\_pY, MNP\_Y, or MNP. As shown in Fig. 3A, after the treatment by MNP\_pY and the magnetic separation, around 40% HeLa-GFP cells (Fig. 4A) are extracted from all the cells with bright green fluorescence. Meanwhile, the bright field images also confirm that many magnetic nanoparticles (MNP\_Y) adhere on the surface of the cancer cells extracted by the magnet (Fig. 4C), which likely results from the dephosphorylation of D-tyrosine phosphates on the iron oxide nanoparticles by the overexpressed ALPP on the surface of cancer cells. To confirm that enzymatic dephosphorylation is responsible for the adhesion of the magnetic nanoparticles to the HeLa cells, we use MNP\_Y as a control and repeat the same experiment as that of MNP\_pY. After the treatment by MNP\_Y and magnetic separation, almost no cell (less than 4%, Fig. 4A) is observed from the extraction portion after reseeding, but the corresponding supernatant (i.e., from the sample treated by MNP\_Y) contains (almost) all the fluorescent (HeLa-GFP) cells (Fig. 3A). Agreeing with this observation, after the incubation of the cells with the control nanoparticles (MNP\_Y), the bright field images reveal that the nanoparticles hardly adhere on the surface of cancer cells (Fig. 4D). Another control iron oxide nanoparticle (MNP) shows the similar results to those of MNP\_Y when being treated with HeLa-GFP cells (Fig. 3A). Moreover, the incubation of MNP\_pY with HS-5 cells hardly results in HS-5 cells in the extraction portion, and there are almost no nanoparticles on the HS-5 cells in the supernatant (Fig. 3B). These results, together, confirm that MNP\_pYs, being



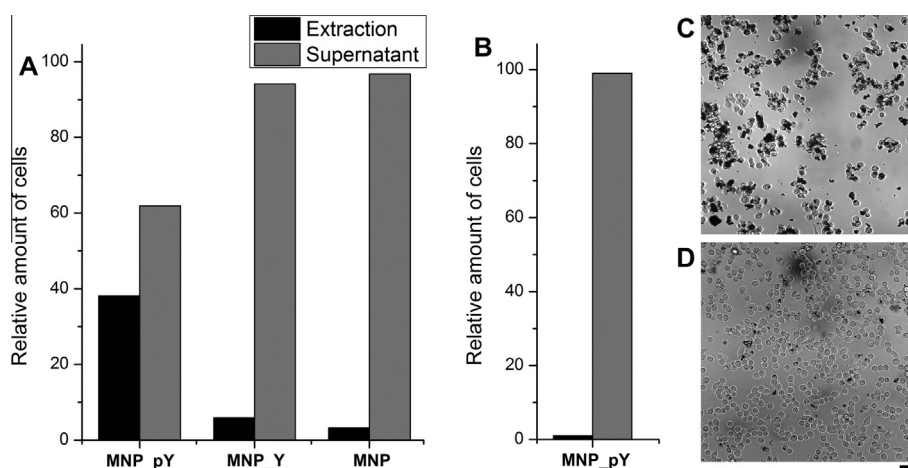
**Fig. 1.** Transmission electron microscope (TEM) images of iron oxide nanoparticles MNP (Left), MNP\_pY (Middle), and MNP\_pY + ALP (Right). The nanoparticles are dissolved in water at the concentration of 2000  $\mu$ g/mL (pH = 7.4). The scale bar is 20 nm.



**Fig. 2.** (A) Phosphate standard curve performed according to the phosphate assay (ab65622, abcam). (B) Average amount of the phosphates on 40  $\mu$ g MNP\_pY. Gray bar indicates amount of phosphates in MNP\_pY treated with ALP for 24 h; and black bar indicates amount of phosphates from the MNP\_pY treated with di H<sub>2</sub>O for 24 h.



**Fig. 3.** (A) The fluorescent images (×20 dry objective lens) of the extraction and supernatant portions of cells after adding MNP\_pY (Left), MNP\_Y (Middle), and MNP (Right) to HeLa-GFP cells. (B) The bright field images (×20 dry objective lens) of the extraction and supernatant portions of cells after adding MNP\_pY to HS-5 cells. Cells were incubated with the growth medium, Dulbecco's Modified Eagle Medium (DMEM), containing 40 µg/mL nanoparticles for 4 h (top: the cells extracted by magnet; bottom: the cells remained in supernatant). The initial number of cells is  $1.0 \times 10^6$  per 6 cm culture dish. The scale bar is 100 µm.



**Fig. 4.** (A) Relative amount of cells (%) in the extraction or supernatant of all the HeLa-GFP cells collected after the treatment by 40 µg/mL MNP\_pY, MNP\_Y, or MNP. (B) Relative amount of cells (%) in the extraction or supernatant of all the HS-5 cells collected after the treatment by 40 µg/mL MNP\_pY. The bright field microscope images (×20 dry objective lens) of HeLa-GFP cells after treated with (C) MNP\_pY and (D) MNP\_Y show the interaction between cells and nanoparticles. Cells were incubated with the growth medium, Dulbecco's Modified Eagle Medium, containing 40 µg/mL nanoparticles for 4 h. The initial number of cells is about  $1.0 \times 10^6$  per 6 cm culture dish. The scale bar is 100 µm.

catalytic dephosphorylated by the ectophosphatases overexpressed on the HeLa cells, selectively adhere to HeLa cells.

#### 4. Conclusion

In conclusion, this work, for the first time, demonstrates the use of enzymatic reaction from ectoenzymes (i.e., ALPP) to actively modulate the surface composition of magnetic nanoparticles for selectively binding to cancer cells without involving specific ligand–receptor interactions or the use of antibodies. The application of isoenzymes, such as ALPP, for selective enzymatic transformation and self-assembly [39,45], promises a fundamentally new way to control cell–materials interactions. Although the cells usually internalize nanoparticles, the decorating of the MNP by D-tyrosine phosphates or D-tyrosine promote the nanoparticles to reside on the surface of the cells, similar to the case of the D-peptide nanofibrils [39]. While the detailed mechanism of this intriguing observation warrants further investigation, this strategy

may find application for sorting or inhibiting cancer cells in a mixture of cells or co-culture, which is the on-going study of this research.

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