

A numerical solver for a nonlinear Fokker–Planck equation representation of neuronal network dynamics

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ABSTRACT

To describe the collective behavior of large ensembles of neurons in neuronal network, a kinetic theory description was developed in [15,14], where a *macroscopic* representation of the network dynamics was directly derived from the *microscopic* dynamics of individual neurons, which are modeled by conductance-based, linear, integrate-and-fire point neurons. A diffusion approximation then led to a nonlinear Fokker–Planck equation for the probability density function of neuronal membrane potentials and synaptic conductances. In this work, we propose a deterministic numerical scheme for a Fokker–Planck model of an excitatory-only network. Our numerical solver allows us to obtain the time evolution of probability distribution functions, and thus, the evolution of all possible macroscopic quantities that are given by suitable moments of the probability density function. We show that this deterministic scheme is capable of capturing the bistability of stationary states observed in Monte Carlo simulations. Moreover, the transient behavior of the firing rates computed from the Fokker–Planck equation is analyzed in this bistable situation, where a bifurcation scenario, of asynchronous convergence towards stationary states, periodic synchronous solutions or damped oscillatory convergence towards stationary states, can be uncovered by increasing the strength of the excitatory coupling. Finally, the computation of moments of the probability distribution allows us to validate the applicability of a moment closure assumption used in [15] to further simplify the kinetic theory.

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1. Introduction

As large-scale neuronal networks models in computational neuroscience become more common [52,56,54,31,44,26], the need to develop efficient methods and effective representations for simulating and analyzing the dynamics of large-scale networks becomes urgent. The multitude of spatial and temporal scales of brain phenomena presents a challenge for model simulation and reduction. While the modularity of brain regions motivates simplification via spatial coarse-graining, irregular temporal fluctuations in the neuronal membrane potentials and the synaptic inputs [53,49,4,48] suggest time-scales for temporal coarse-graining. Various theoretical approaches, based on spatial and temporal coarse-graining assumptions, have led to the development of dimensionally-reduced descriptions of the network dynamics through examining a probabilistic representation of the network dynamics and deriving an evolution equation governing a probability density function (pdf) [28,58,1,55,20,6,41,9,22,40,39,37,38,24,21]. In this work, we propose an efficient numerical scheme for the simulation of a nonlinear Fokker–Planck equation representation for neuronal network dynamics.

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The starting point for our description of neuronal network dynamics is a system of ordinary differential equations (ODEs) for a network of recurrently coupled, single compartment, conductance-based, linear integrate-and-fire (LIF) point neurons. In this work, we restrict the discussion to all-to-all coupled, excitatory neuronal networks. We consider the following dynamical system governing the temporal evolution of the membrane potential V_i and the excitatory conductance $G_i \geq 0$ of the i th neuron in a pool \mathcal{P}_E of N excitatory neurons,

$$\tau \frac{dV_i}{dt} = -(V_i - V_R) - G_i(V_i - V_E) \quad (1)$$

$$\sigma_E \frac{dG_i}{dt} = -G_i + \sum_{\mu} f_E \delta(t - t_{\mu}^i) + \frac{S_{EE}}{N_E} \sum_{j \in \mathcal{P}_E} \sum_{\mu} p_{j\mu}^E \delta(t - t_{\mu}^j) \quad (2)$$

where V_E is the (excitatory) reversal potential, τ is a typical leak (i.e., relaxation) time for the membrane potential, and σ_E is the decay time constant of the excitatory conductance. To complete the LIF dynamical system, whenever a membrane potential, V_i , reaches the spiking threshold (V_T), the spike time is recorded and V_i is immediately set to the reset potential V_R . We set the absolute refractory period to zero.

The first sum in Eq. (2) is due to incoming spikes (i.e., spikes from neurons external to the network): t_{μ}^i is the time of the μ th incoming spike received by the i th neuron. We model each incoming spike train with independent realizations of a Poisson process with rate $v_{0E}(t)$. The second sum in Eq. (2) describes the recurrent interaction with the other neurons in the pool via neuronal action potentials, i.e., t_{μ}^j is the time of the μ th spike of the j th neuron. The parameter S_{EE} describes the strength of network excitatory couplings. The factor of N_E provides the overall normalization of the coupling strength. $p_{j\mu}^E$ is the probability of synaptic release after the arrival of each spike. We model each synaptic release as a Bernoulli process, with probability equal to $p = N_E/N$, that is, $p_{j\mu}^E = 1$ with probability p ; and 0, otherwise.

Following [15,14], by assuming that the spike trains contributing to the second sum in Eq. (2) to be Poisson, the collective behavior of this network can be described in terms of a partial differential equation (PDE) for the time evolution of the probability density function (pdf), $\rho(t, v, g)$, of finding a neuron with a potential $v \in [V_R, V_T]$ and conductance $g \geq 0$ at time $t \geq 0$. A diffusive approximation, by assuming that f_E and S_{EE}/N_E to be small, then leads to the following Fokker–Planck equation [14]:

$$\partial_t \rho = \partial_v \left\{ \left[\left(\frac{v - V_R}{\tau} \right) + g \left(\frac{v - V_E}{\tau} \right) \right] \rho \right\} + \partial_g \left\{ \frac{1}{\sigma_E} (g - \bar{g}_E(t)) \rho + \frac{\sigma_g^2(t)}{\sigma_E} \partial_g \rho \right\} \quad (3)$$

which can be rewritten as a continuity equation

$$\partial_t \rho(t, v, g) + \partial_v J_V(t, v, g) + \partial_g J_G(t, v, g) = 0$$

where the fluxes are

$$J_V(t, v, g) = \left[\left(\frac{V_R - v}{\tau} \right) + g \left(\frac{V_E - v}{\tau} \right) \right] \rho(t, v, g)$$

and

$$J_G(t, v, g) = \frac{1}{\sigma_E} (\bar{g}_E(t) - g) \rho(t, v, g) - \frac{\sigma_g^2(t)}{\sigma_E} \partial_g \rho(t, v, g).$$

The effective drift and effective diffusivity in the conductance variable are given by:

$$\bar{g}_E(t) = f_E v_{0E}(t) + S_{EE} m_E(t) \quad \text{and} \quad \sigma_g^2(t) = \frac{1}{2\sigma_E} \left(f_E^2 v_{0E}(t) + \frac{S_{EE}^2}{N_E} m_E(t) \right)$$

and are dependent on $m_E(t)$, the firing rate per neuron, averaged over the network. The firing rate is the probability per unit time that a neuron at time t crosses the voltage threshold value V_T , and thus, can be computed as the probability flux at V_T , regardless of the value of the conductance, g ,

$$m_E(t) = \int_0^{\infty} J_V(t, V_T, g) dg. \quad (4)$$

All neurons arriving at the threshold voltage V_T emit a spike and we assume that they instantaneously relax to their rest value V_R . Therefore, we need to supply boundary conditions for the PDE consistent with the evolution of a pdf for the trajectories of the ODE system (1) and (2) with a reset boundary condition in the membrane potential variable:

$$J_V(t, V_T, g) = J_V(t, V_R, g) \quad \text{for all } g \in [0, \infty) \quad (5)$$

$$J_G(t, v, 0) = J_G(t, v, \infty) = 0 \quad \text{for all } v \in [V_R, V_T] \quad (6)$$

That is, the flux of spiking neurons at the threshold voltage re-enters instantaneously through the reset voltage (5) and that no neuron can have negative conductances or a non-decaying conductance distribution at large conductance values (6). We point out that the g -boundary condition (6) can be rewritten as $\rho(t, v, 0) = 0$ and $\rho(t, v, g) \rightarrow 0$ for all $v \in [V_R, V_T]$ as $g \rightarrow \infty$. Let

us also remark that the ν -boundary condition (5) on the threshold voltage implies that $\rho(t, V_T, g) = \rho(t, V_R, g) = 0$ for $0 \leq g \leq g_T$ with the critical conductance determined by $V_T - V_R = g_T(V_E - V_T)$ since for excitatory neurons we have $V_R < V_T < V_E$. For $g \geq g_T$, the boundary condition (5) imposes a relation between $\rho(t, V_T, g)$ and $\rho(t, V_R, g)$. Let us finally mention that this kinetic model (3) generalizes other Fokker–Planck equations derived from some current-based LIF neuronal networks where one considers only the evolution of the voltage (see, for instance, [9,8,32]).

Most studies of the behavior of neuronal networks as described by (1) and (2) through a kinetic theory [14,47,15,13,45,35,36] have approached the computational simulation of this neuronal ensemble through direct Monte-Carlo simulations of the stochastic differential system (see also [50,43], for details of the numerical schemes). Based on this Fokker–Planck equation, further dimensional reduction was obtained by a moment closure method [14] and then analyzed both numerically and theoretically [46,30].

The direct simulation of the $(2 + 1)$ -dimensional nonlinear Fokker–Planck equation (3) for a neuronal network has not been tackled thus far. Furthermore, our simulation has several advantages over direct Monte-Carlo simulations due to the results being deterministic (for instance, the accurate resolution of transients and the possibility of obtaining all macroscopic quantities of interest directly from suitable moments of the pdf, $\rho(t, \nu, g)$). A similar strategy was adopted for obtaining highly accurate resolution of the charged particle transport in semiconductors (see [16,17,12] and references therein). One of the possible drawbacks of the deterministic simulation of the Fokker–Planck equation (3) is its computational cost. However, if one wants to resolve (1) and (2) by direct Monte-Carlo simulation and obtain good statistics for distribution functions and for both dynamical transients and stationary states, the number of different realizations needed can be large, thus making the direct deterministic simulation of (3) competitive with the Monte-Carlo approach. We will comment on computational costs in Section 3.

The main objectives of this work are then: to propose a highly accurate finite differences scheme for the solutions of the Fokker–Planck equation (3), to cross-validate it against direct Monte-Carlo simulations, to analyze its performance, and to study numerically the transients of the ensemble dynamics showing the appearance of synchronous and asynchronous solutions. Concerning deterministic methods for related kinetic models, we are only aware of the results in [5]. There the authors proposed a deterministic scheme to directly solve an integro-differential equation for a model system that included refractory effect, that is, the spiking neurons went into a refractory state which could also be described by another kinetic integro-differential equation. The authors also proposed two deterministic methods: One based on a direct upwind first-order discretization of the advection derivatives together with an implicit time-stepping; the other based on splitting methods to decrease the computational time, though some time-steps are done implicitly.

In our deterministic scheme for the Fokker–Planck equation (3), we approximate the advection derivatives in voltage by finite-differences WENO (weighted essentially non-oscillatory) methods developed in [51,27] for nonlinear systems of conservation laws. Since the voltage variable does not have diffusion terms (second derivatives in the voltage), a high-order method is important for the accuracy and stability for the cases where sharp fronts in the voltage develop. Both the advection and the diffusion term in the conductance variable are approximated together, as is usually done in drift–diffusion equations for semiconductors or in granular media models [11]; keeping good stability properties of the g -discretization leads to an approximation scheme known as the Chang–Cooper method. Both approximations are assembled in an ODE system which is solved by explicit third-order Runge–Kutta methods as in [51]. The accurate approximation of the ν and g derivatives allows us to use explicit time integrators with a fairly moderate CFL condition. The derivation of this scheme follows similar ideas as in work done in Boltzmann–Poisson kinetic systems for semiconductors [16,17,12]. Also, splitting schemes were developed for plasmas and semiconductor modelling [19,18], which may be applied to the present situation for further computational savings.

After cross-validating our numerical results by direct comparisons to Monte-Carlo simulations, we focus on simulating two phenomena commonly observed in neuronal network models. We first examine the appearance of bistability. Bi- and multi-stable networks have been used in models of short term working memory [57], of oculomotor integrators [29], of visual perception [34] and of neuronal populations involved in decision making [3]. We then examine a model that exhibits periodic solutions even when driven with inputs that are steady in time. Periodic or oscillatory solutions have been used to model synchronous behavior and oscillations observed during cortical processing (for instance, [23,25]). Various studies have examined how oscillatory solutions may arise in networks (see, for instance, [1,9,8,10] and references therein). With our Fokker–Planck solver, we examine the transients as we increased the connectivity strength as we keep the strength of the time-steady input fixed. We observe a transition from asynchronous behavior (signified by convergence towards stationary states) to synchronous behavior (signified by periodic solutions) and back to asynchronous behavior. Finally, one advantage of the full deterministic simulation of the Eq. (3) is that we can compute accurately the evolution of the macroscopic moments of the pdf and their form in stationary states. Using these solutions, we validate the moment closure assumptions as proposed in [14].

Let us finally comment that the well-posedness of the Cauchy problem for Eq. (3) with the boundary conditions (5) and (6) has not been studied analytically yet, to the best of our knowledge. Furthermore, it is a difficult mathematical problem since it is not clear how to obtain good estimates on the flux of spiking neurons going over the threshold voltage. As a consequence, we do not know how to estimate analytically the firing rate of the neuron population (4) which is the source of nonlinearity. For this reason, a numerical analysis of the proposed algorithm remains an open issue.

The paper is structured as follows. In Section 2, we present a derivation of the deterministic scheme and compare its results to direct Monte-Carlo simulations. Section 3 details the simulation results obtained for the bistability issue, the

transients synchronous versus asynchronous behavior and the validation of moment closures. We offer concluding remarks in Section 4.

2. Numerical scheme for the kinetic equation

Our deterministic scheme for the Fokker–Planck equation (3) is based on a fifth order WENO-finite differences approximation for the advection part in the voltage variable and an “upwind” scheme mixed with a “ θ -scheme”, known as the Chang–Cooper method, for the advection and the diffusion term in the conductance variable. The evolution in time is done by means of a TVD third-order Runge–Kutta method. Both finite differences schemes (WENO and Chang–Cooper methods) produce very accuracy and stable approximations of derivatives on v and g and allow us to use explicit TVD third-order Runge–Kutta method with a fairly moderate CFL condition.

To discretize the Fokker–Planck equation, we rewrite (3) as follows:

$$\partial_t \rho(t, v, g) = -\partial_v J_V(t, v, g) + \frac{\sigma_g^2(t)}{\sigma_E} \partial_g \left\{ M(g) \partial_g \left(\frac{\rho(t, v, g)}{M(g)} \right) \right\} \quad (7)$$

where

$$M(g) = \exp \left\{ -\frac{|g - \bar{g}_E(t)|^2}{2\sigma_g^2(t)} \right\}.$$

and consider uniform meshes in v and g :

$$\begin{aligned} v_i &= V_R + i \Delta v \quad i = 0, \dots, N_v \\ g_j &= j \Delta g \quad j = 0, \dots, N_g \end{aligned}$$

where $\Delta v = \frac{V_T - V_R}{N_v}$ and $\Delta g = \frac{g_{\max}}{N_g}$. The maximum value of the conductance g_{\max} is adjusted in the numerical experiments in such a way that for all $t, v, \rho(t, v, g) \approx 0$ for $g \geq g_{\max}$. The approximations to the point values of the solution $\rho(t^n, v_i, g_j)$ (denoted by ρ_{ij}^n) are obtained with a dimension by dimension approximation to the derivatives on v and g .

Let us finally comment that although there are many numerical methods developed for classical Fokker–Planck equations, see for instance [2] where Hermite polynomial expansions are used, they do not adapt well to our situation. The main difficulty being that the diffusion term only acts on one of the two variables, as is the case for kinetic Fokker–Planck equations, see [7] for instance.

2.1. WENO-scheme

The advection term of Eq. (7) in the voltage variable is approximated using a fifth order conservative finite difference WENO scheme [51,27]. The weighted essentially non-oscillatory scheme was originally developed for hyperbolic conservation laws. These finite difference methods combine the high accuracy for the smooth parts of the evolution together with a nice treatment of possible steep fronts by locally weighting the best stencils. We remark that here, the flux in the voltage is completely linear and thus, this choice of finite differences approximation is just a simple high-order choice which adapts itself, when the need arises, to the nonlinear effect in the g variable and its possible transmission to the voltage variable through the drift $J_V(t, v, g)$. We give a summary of the WENO method below for the sake of completeness. The variable g is fixed and we consider the approximation in the v variable:

$$\partial_v \underbrace{(a(v_i, g_j) \rho(t_n, v_i, g_j))}_{J_V(t_n, v_i, g_j)} \approx \frac{1}{\Delta v} (\hat{h}_{i+1/2} - \hat{h}_{i-1/2}) \quad (8)$$

where $a(v_i, g_j) = \left(\frac{V_R - v_i}{\tau} \right) + g_j \left(\frac{V_E - v_i}{\tau} \right)$. To explain the WENO scheme, here we assume that $a(v_i, g_j) > 0$, without loss of generality (otherwise the procedure would just be mirror symmetric with respect to $i + 1/2$ when computing $\hat{h}_{i+1/2}$). We denote

$$h_i = a(v_i, g_j) \rho(t_n, v_i, g_j), \quad i = -2, -1, \dots, N_v + 2 \quad (9)$$

where j and n are all fixed. We obtain the numerical flux by

$$\hat{h}_{i+1/2} = \omega_1 \hat{h}_{i+1/2}^{(1)} + \omega_2 \hat{h}_{i+1/2}^{(2)} + \omega_3 \hat{h}_{i+1/2}^{(3)}$$

where $\hat{h}_{i+1/2}^{(m)}$ are the three third order fluxes on three different stencils given by

$$\begin{aligned} \hat{h}_{i+1/2}^{(1)} &= \frac{1}{3} h_{i-2} - \frac{7}{6} h_{i-1} + \frac{11}{6} h_i, \\ \hat{h}_{i+1/2}^{(2)} &= -\frac{1}{6} h_{i-1} + \frac{5}{6} h_i + \frac{1}{3} h_{i+1}, \\ \hat{h}_{i+1/2}^{(3)} &= \frac{1}{3} h_i + \frac{5}{6} h_{i+1} - \frac{1}{6} h_{i+2}, \end{aligned}$$

The nonlinear weights ω_m are given by

$$\omega_m = \frac{\tilde{\omega}_m}{\sum_{l=1}^3 \tilde{\omega}_l}, \quad \tilde{\omega}_l = \frac{\gamma_l}{(\varepsilon + \beta_l)^2},$$

with $\varepsilon = 10^{-6}$, the linear weights γ_l are given by

$$\gamma_1 = \frac{1}{10}, \quad \gamma_2 = \frac{3}{5}, \quad \gamma_3 = \frac{3}{10},$$

and the smoothness indicators β_l are given by

$$\begin{aligned} \beta_1 &= \frac{13}{12}(h_{i-2} - 2h_{i-1} + h_i)^2 + \frac{1}{4}(h_{i-2} - 4h_{i-1} + 3h_i)^2 \\ \beta_2 &= \frac{13}{12}(h_{i-1} - 2h_i + h_{i+1})^2 + \frac{1}{4}(h_{i-1} - h_{i+1})^2 \\ \beta_3 &= \frac{13}{12}(h_i - 2h_{i+1} + h_{i+2})^2 + \frac{1}{4}(3h_i - 4h_{i+1} + h_{i+2})^2. \end{aligned}$$

As usual with this kind of schemes, some ghost points are necessary to impose numerically the boundary conditions (5). This condition for the flux in v means that for every g if $a(t, V_T, g) < 0$ then $J_V(t, V_T, g) = 0$ and consequently $J_V(t, V_R, g) = 0$, otherwise $J_V(t, V_R, g) = J_V(t, V_T, g)$. Therefore, for n, j fixed, the values at the ghost points are defined as: if $a(t_n, V_T, g_j) < 0$ then $h_{-i} = 0$ and $h_{N_v+i} = 0$ for $i = 1, 2, 3$, otherwise if $a(t_n, V_T, g_j) \geq 0$ thus $h_{-i} = h_{N_v+1}$ and $h_{N_v+i} = h_{N_v+1}$ for $i = 1, 2, 3$, using the notation (9).

2.2. Chang–Cooper method

For the derivatives of the conductance variable in Eq. (7) we follow the Chang–Cooper method as considered in [11]. Originally, the Chang–Cooper method was designed to preserve the equilibrium state of the Fokker–Plank equation. This feature is important to get accurate behavior of the discretization scheme in g at long times. In fact, it ensures that the Maxwellian equilibria $M(g)$ are preserved for the discretized scheme in the absence of the external time dependent inputs and for homogeneous data in v . In the jargon of the numerical conservation law community, this property is known as “well-balanced.” Moreover, this scheme is also an entropy decay preserving method, i.e., it keeps the associated Liapunov functional (called entropy in statistical mechanics) decreasing in time for the semidiscrete scheme. As in the voltage variable we approximate the term of conductance using finite differences:

$$\partial_g \frac{\sigma_g^2(t_n)}{\sigma_E} \left\{ M(g_j) \partial_g \left(\frac{\rho(t_n, v_i, g_j)}{M(g_j)} \right) \right\} \approx \frac{F_{j+1/2} - F_{j-1/2}}{\Delta g} \quad (10)$$

where, for n and i fixed, the numerical flux is

$$F_{j+1/2} = \frac{\sigma_g^2(t_n)}{\sigma_E \Delta g} \tilde{M}_{j+1/2} \left(\frac{\rho_{j+1}}{M_{j+1}} - \frac{\rho_j}{M_j} \right)$$

and

$$\tilde{M}_{j+1/2} = \frac{M_j M_{j+1}}{M_{j+1} - M_j} (\ln(M_{j+1}) - \ln(M_j))$$

is a value between M_j and M_{j+1} . We have used the following notation: $M_j = M(g_j)$ and $\rho_j = \rho(t_n, v_i, g_j)$. After some computations, see [11] for details, $F_{j+1/2}$ can be rewritten as:

$$F_{j+1/2} = \frac{\sigma_g^2(t)}{\sigma_E \Delta g} (\rho_{j+1} - \rho_j) + \frac{\sigma_g^2(t) \omega}{\sigma_E \Delta g} (\theta \rho_j + (1 - \theta) \rho_{j+1}) \quad (11)$$

where $\omega = \ln(M_j/M_{j+1})$ and $\theta = \frac{1}{\omega} - \frac{1}{e^{\omega}-1}$. Now we observe, as we noted above, that (11) is an “upwind” scheme, mixed with a “ θ -scheme”. To conclude this description of the numerical approximation in g , we remark that the ghost flux for $j = -1$ and $j = N_g + 1$ are considered null, taking into account the boundary condition for g flux in (6). We finally remark that this method is only known to preserve the entropy decreasing property when an implicit-in-time discretization is used.

2.3. TVD third-order RK

The evolution in time is implemented by means of the third order TVD Runge–Kutta method as in [51]:

$$\begin{aligned}\rho^{(1)} &= \rho^n + \Delta t L(\rho^n, t^n) \\ \rho^{(2)} &= \frac{3}{4}\rho^n + \frac{1}{4}\rho^{(1)} + \frac{1}{4}\Delta t L(\rho^{(1)}, t^n + \Delta t) \\ \rho^{n+1} &= \frac{1}{3}\rho^n + \frac{2}{3}\rho^{(2)} + \frac{2}{3}\Delta t L\left(\rho^{(2)}, t^n + \frac{1}{2}\Delta t\right),\end{aligned}$$

where L is the approximation to the advection and diffusion terms given by adding (8) and (10):

$$L(\rho(t, g, v), t) \approx -\partial_v J_V(t, v, g) + \frac{\sigma_g^2(t)}{\sigma_E} \partial_g \left\{ M(g) \partial_g \left(\frac{\rho(t, v, g)}{M(g)} \right) \right\}$$

and Δt is the time step, which is conditioned on the following CFL restriction since an explicit scheme is considered:

$$\Delta t \leqslant CFL \min \left\{ \frac{\Delta v}{\max_{i,j} |a(v_i, g_j)|}, \frac{(\Delta g)^2}{\frac{\sigma_g^2(t_n)}{\sigma} + \Delta g \max_j |F_{j+1/2}|} \right\}$$

where we recall that $a(v, g) = \left(\frac{V_R - v}{\tau}\right) + g \left(\frac{V_E - v}{\tau}\right)$. Due to the accurate approximations of the WENO-scheme and the Chang-Cooper method of the fluxes, the CFL condition does not yield restrictive time-stepping.

Finally, since the system is nonlinear due to the firing rate:

$$m_E(t) = \int_0^\infty J_V(t, V_T, g) dg,$$

which need to be incorporated, in a self-consistent fashion, at each time step, we approximate m_E by the composite mid-point rule and re-inject it in the next step. In our simulations we consider as initial data the product of two different Maxwellian functions in g and v both normalized to be probability densities, i.e., unit numerical mass. For the bistable systems we proceed in a different way, as we explain below in Section 3.

3. Simulation results

Here we illustrate the use of our numerical Fokker–Planck solver first through simple test cases and then by examining the solutions to the following problems, produced by different choices of input forcing, v_{0E} : stationary case with a unique steady state, non-stationary solutions and a case exhibiting bistability. Finally, using our numerical solver we check the closure condition (12) in a variety of circumstances.

3.1. Test cases

We solve the set of Eqs. (1) and (2) with a modified second-order Runge–Kutta scheme [50] with a numerical time-step of 0.01 ms. In a few cases, runs with a numerical time-step of 0.001 ms were performed and no significant quantitative differences were observed. We note that Eqs. (1) and (2) are already written in reduced-dimensional units, in which only time has dimensions, in ms; see, for instance, [33]. We set the network pool size to be $N = 100,000$ neurons, each one connected to $N_E = 100$ neurons in the direct Monte-Carlo simulations. The parameters of the system are as follows: $\tau = 20$ ms, $\sigma_E = 3$ ms, $V_E = 14/3$, $V_T = 1$, $V_R = 0$ and we set equal the rest and reset potentials. We set $f_E = 10$ ms and $S_{EE} = 0.05$ for our comparison between the Monte-Carlo and Fokker–Planck solvers.

We compare our numerical Fokker–Planck solver to direct Monte Carlo simulations via the following examples, going from stationary to non-stationary cases.

Stationary case. Case A: We consider a network in which the rate of input Poisson process $v_{0E}(t) = A$ with constant $A \in [1000, 1500]$.

Fig. 1 compares the network firing rate versus mean $g_{imp} = f_E v_{0E}$ between the Monte-Carlo and the Fokker–Planck simulations. We observe very good agreement between the simulations. In Fig. 2 we compare the pdfs between the two simulations. We fix $A = 1400$ and we display marginal probability distribution functions ρ_v and ρ_g for the stationary solutions. Again we observe that the numerical results from the two solvers are in excellent agreement. We would like to point out that for the results from the deterministic Fokker–Planck simulations, the distribution functions ρ_v and ρ_g were obtained by numerical integrations of ρ , therefore we did not need to consider other, possibly simpler, derived Fokker–Planck systems (say, by assuming a closure hypothesis) for ρ_v or for ρ_g . The time evolution of these distribution functions is shown in Fig. 3, specifically, both at times 0.05. In our simulations we observe that ρ_g at time 0.05 has achieved steady state; however, at time 0.05, ρ_v has yet to achieve steady state (attained before $t = 0.1$).

Non stationary case. We also analyze cases where the rate of Poisson process is not constant in time. We consider the two following cases:

- *Case B:* The input Poisson process has a rate that depends on time continuously

$$v_{0E}(t) = A(1 + \epsilon \sin(\omega t))$$

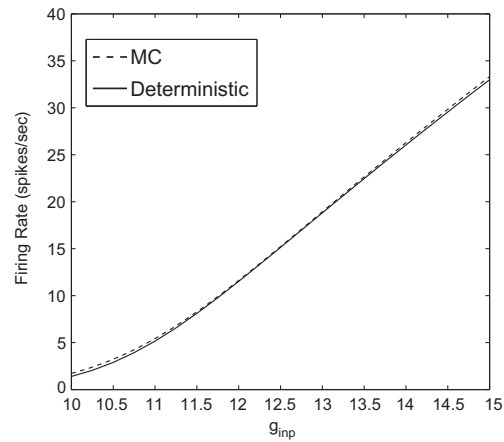


Fig. 1. Evolution in time of the firing rate for Case A. Comparison between Monte Carlo and deterministic simulations.

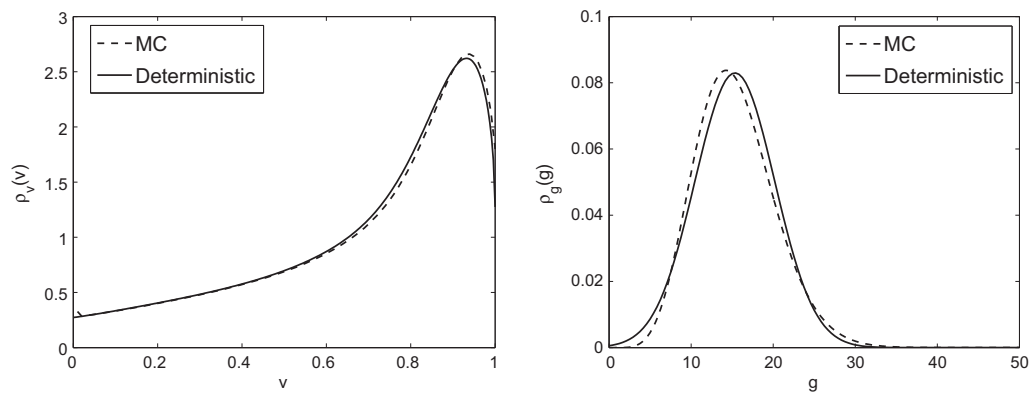


Fig. 2. Comparison between Monte Carlo and deterministic simulations for the stationary distribution functions ρ_v and ρ_g in the Case A with $A = 1400$.

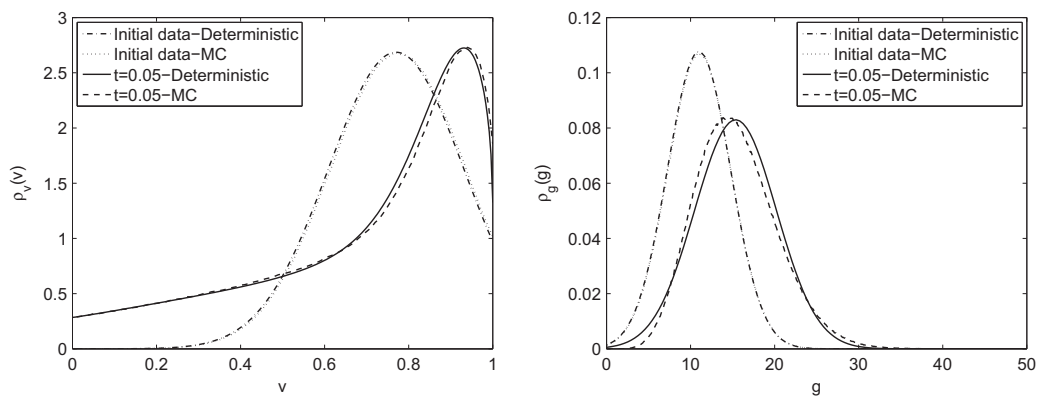


Fig. 3. Comparison between Monte Carlo and deterministic simulations for the evolution in time of the distribution functions ρ_v and ρ_g in Case A with $A = 1400$ in two different instants: $t = 0$ s and $t = 0.05$ s.

- B1 : $A = 1500$, $\epsilon = 300$, $\omega = 8\pi$
 B2 : $A = 1000$, $\epsilon = 200$, $\omega = 8\pi$
 B3 : $A = 1500$, $\epsilon = 300$, $\omega = 80\pi$

- **Case C:** The input Poisson process has a rate that has a discrete jump in time

$$v_{0E}(t) = A\theta(t - t_0) + B, \quad \theta \text{ being the Heaviside function}$$

$A = 500$, $B = 1000$, $t_0 = 1$.

Figs. 4–6 compare the time evolution of the firing rate for the *Case B* ($B1$, $B2$ and $B3$), whereas Fig. 7 shows the firing rate in the *Case C*. Comparing these figures we observe how the shape of the external input is reflected in the evolution of the firing rate.

We note that simulating accurately ensembles of 100,000 or more LIF neurons are often needed to get good statistics for the PDFs and for convergence of the instantaneous network firing rate. For instance, in the non-stationary cases (*Cases B* and *C*), to capture individual spikes, we need to run the LIF simulations at a time-step of 0.1 ms or less and to get good convergence of the firing rate, which, in all cases, took 20–50 times longer than solving the corresponding Fokker–Planck equation. Furthermore, the difference between the LIF simulations and the corresponding Fokker–Planck results is more pronounced in the cases where we are interested in the dynamical transients (for instance, in *Case C*), when a larger number of ensembles (and/or realizations) are needed for an accurate resolution of the pdfs.

3.2. Bistability

Bistability is typical of systems with strong excitatory feedback. Even in situations as in *Case A* above, there are circumstances, when the recurrent excitatory coupling is sufficiently strong, that exhibit two distinct steady state solutions (with different firing rates) for the same input forcing. For instance, let us consider an example with the following parameters: $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$ and $\sigma_E = 2$ ms. Fig. 8 shows bistability in the firing rate vs. input strength diagram. Here the two different branches have different firing rates and can be distinguished by the choice of initial data. To obtain this firing rate diagram we fit for an input of $f_E v_{0E} = 11$ as initial data the product of two different Maxwellian functions: one for the

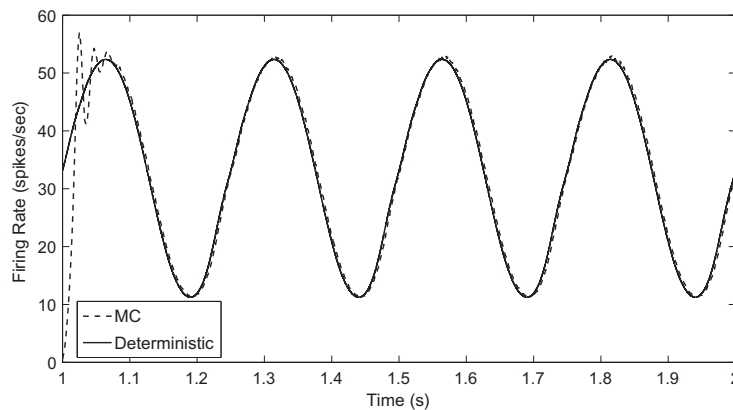


Fig. 4. Evolution in time of the firing rate for *Case B1*. Comparison between Monte Carlo and deterministic simulations.

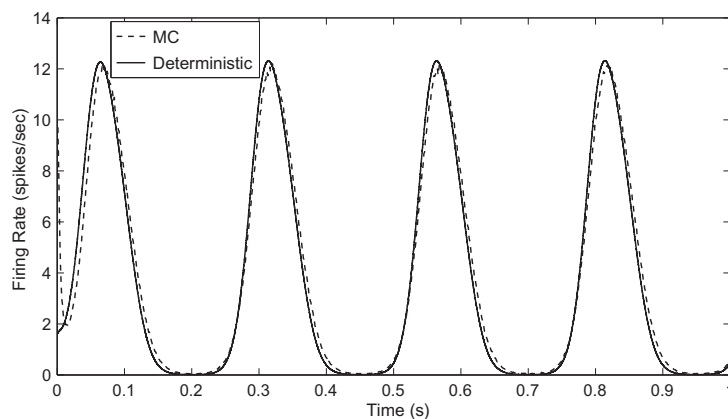


Fig. 5. Evolution in time of the firing rate for *Case B2*. Comparison between Monte Carlo and deterministic simulations.

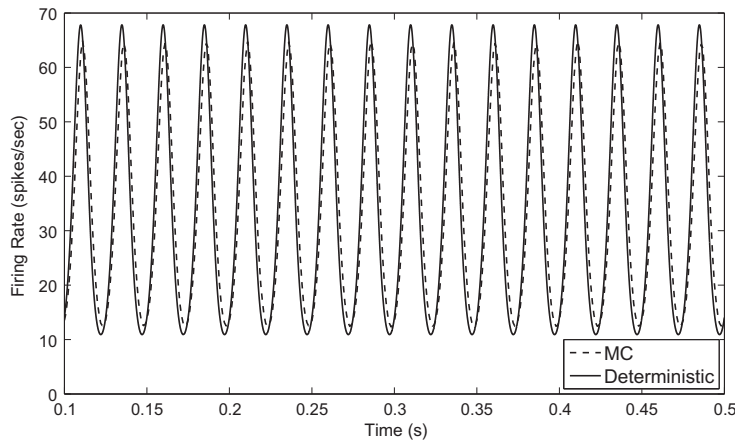


Fig. 6. Evolution in time of the firing rate for Case B3. Comparison between Monte Carlo and deterministic simulations.

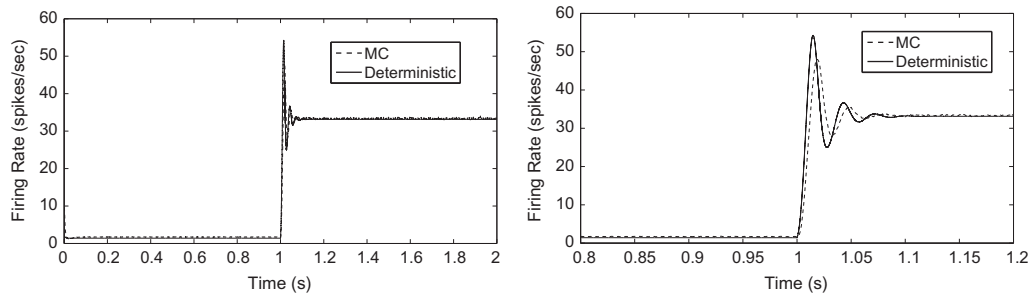


Fig. 7. Evolution in time of the firing rate for Case C. Comparison between Monte Carlo and deterministic simulations.

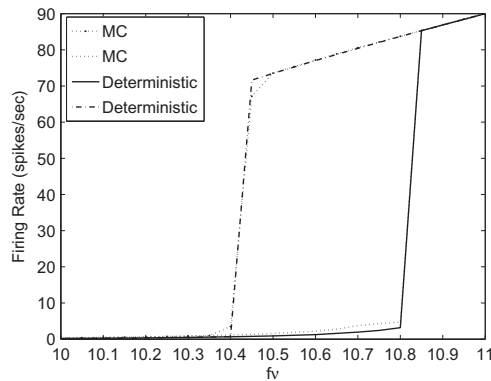


Fig. 8. Stationary firing branches in Case A where $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$ and $\sigma_E = 2$ ms. Comparison between Monte Carlo and deterministic simulations.

variable g and other one for the variable ν , each normalized to have unit numerical integral (since $\rho(\nu, g)$ is a probability distribution). Then the stationary solution of this problem is considered as initial data for the system with $f_{E\nu_{0E}} = 10.9$, whose stationary state is taken as initial data for the case $f_{E\nu_{0E}} = 10.8$ and so on, to obtain the firing rates of the top branch. However, to obtain the lower branch, it is not necessary to proceed in the same fashion, since this branch appears considering the same initial data for all the input $f_{E\nu_{0E}}$.

In Figs. 9 and 10, we display temporal evolution (of network firing rates) and the (eventual) steady-state pdf for $f_{E\nu_{0E}} = 10.8$ which is in the parameter regime exhibiting bistability. Fig. 9 shows the evolution of the firing rate and the stationary solution for the lower branch, whereas Fig. 10 shows the same for the upper branch. Note that we needed to start

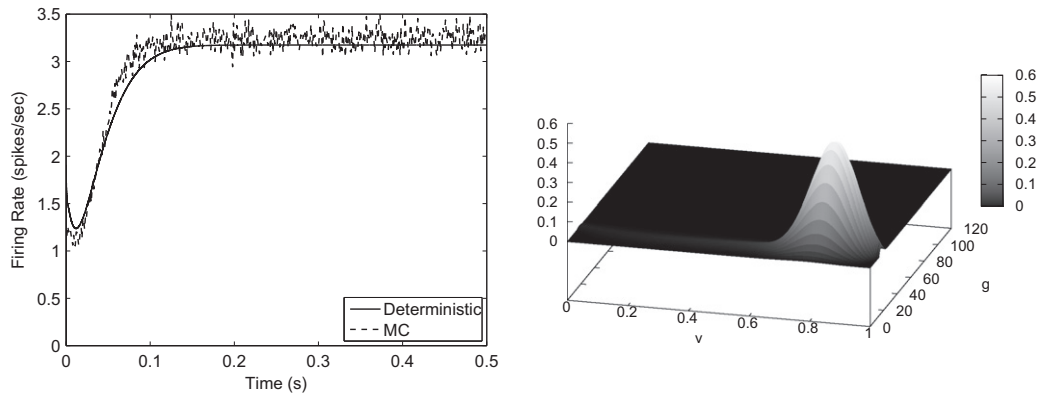


Fig. 9. Comparison between Monte Carlo and deterministic simulations for (left panel) the evolution in time of the firing rate and (right panel) deterministic stationary distribution function for the lower branch in Case A where $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$, $\sigma_E = 2$ ms and $f_E v_{OE} = 10.8$.

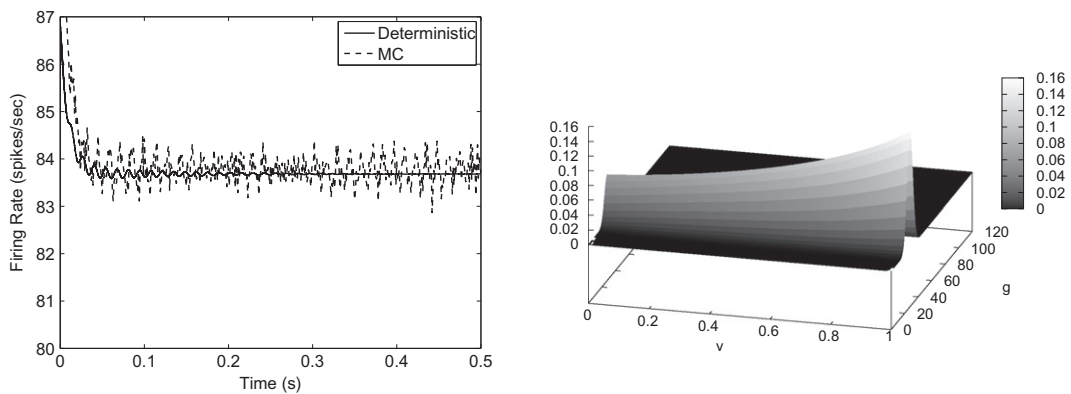


Fig. 10. Comparison between Monte Carlo and deterministic simulations for (left panel) the evolution in time of the firing rate and (right panel) deterministic stationary distribution function for the upper branch in Case A where $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$, $\sigma_E = 2$ ms and $f_E v_{OE} = 10.8$.

with initial data with high firing rates to access the upper branch. We also remark that there are damped, oscillatory transients in the latter case. Let us next turn to the development of oscillatory solutions.

3.3. Synchronous versus asynchronous solutions

In Fig. 11 we exhibit the firing rate for $f_E v_{OE} = 11$ where there is no bistability. (Thus any initial data will eventually approach the unique, high firing rate, steady state solution.) The damped oscillatory transients may be the signature of oscil-

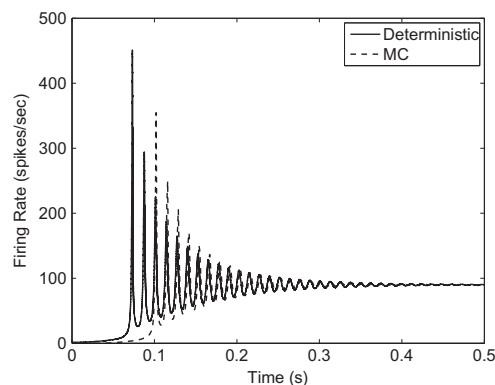


Fig. 11. Comparison between Monte Carlo and deterministic simulations for the evolution in time of the firing rate in Case A where $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$, $\sigma_E = 2$ ms and $f_E v_{OE} = 11$.

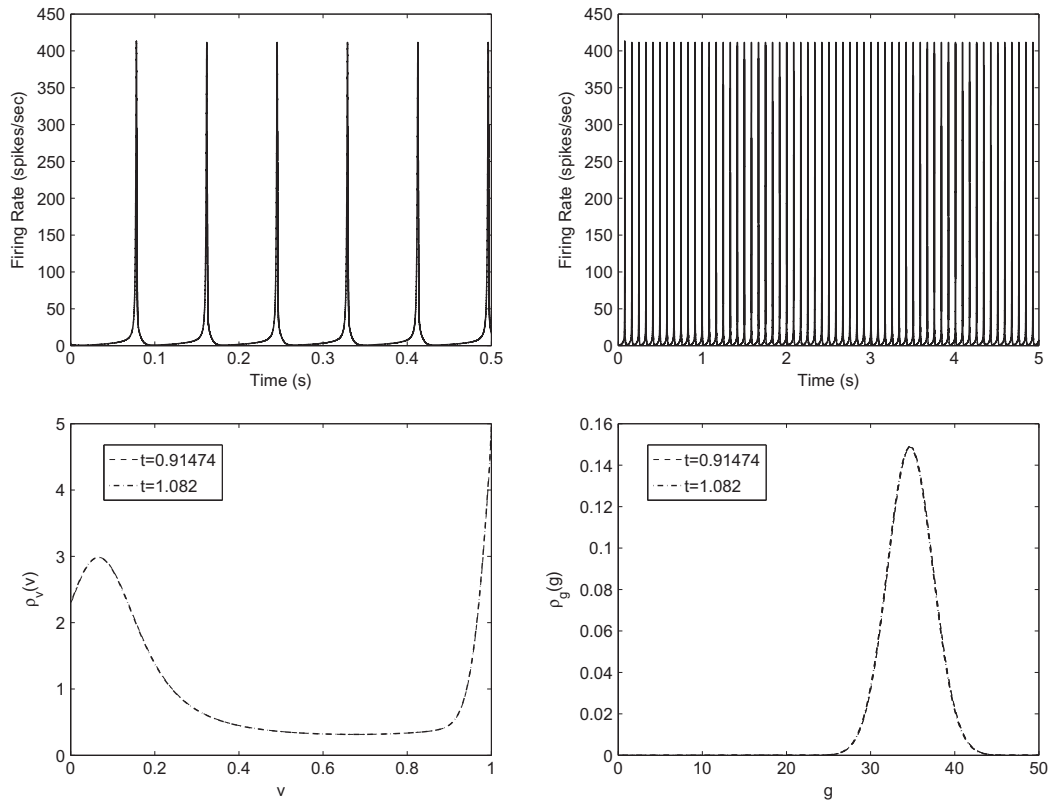


Fig. 12. For Case A with $S_{EE} = 0.15$, $N_E = 500$, $f_E = 0.002$ s and $f_{E^{V_{0E}}} = 12$ the evolution in time of the firing rate (top) and the distribution functions ρ_v (left bottom) and ρ_g (right bottom) in two different time: $t = 0.91474$ s and $t = 1.082$ s.

latory solutions that are nearby in parameter space. Therefore, let us now consider the following case, $S_{EE} = 0.15$, $N_E = 500$, $f_E = 0.002$ s and $f_{E^{V_{0E}}} = 12$, where firing rate is periodic in time; see Fig. 12. In fact, if we fix $N_E = 500$, $f_E = 0.002$ s and $f_{E^{V_{0E}}} = 12$ and vary S_{EE} , we obtain Fig. 13, which shows that there is a range in the excitatory coupling strength, S_{EE} , approximately, between 0.13 and 0.17 where periodic solutions appear (and outside of this interval oscillations do not happen). For small S_{EE} , solutions go quickly to the steady state but for slightly larger values over this interval ($S_{EE} \geq 0.17$), the solution reaches the steady state in an oscillatory way, starting with huge oscillations which vanish after some time.

In the case where $0.13 \leq S_{EE} \leq 0.17$ and periodic solutions appear, we also observe that maximum firing rate increases when S_{EE} is increased. Fig. 13 shows that the maximum value for $S_{EE} = 0.13$ is around 250 spikes/s, while for $S_{EE} = 0.14$ is around 350 spikes/s, for $S_{EE} = 0.16$ is less than 500 spikes/s and for $S_{EE} = 0.17$ is more than 500 spikes/s. At the same time, as we increase S_{EE} the frequency of oscillations increases also. However, eventually the oscillations damp out again and steady state solutions are obtained and asynchronous behavior is observed again (see last panel of Fig. 13).

We note that the same sequence of asynchronous and synchronous behavior is observed in the Monte Carlo simulations, i.e., an asynchronous convergence to stationary states at small values of S_{EE} ; periodic synchronous solutions at intermediate values of S_{EE} (with a decreasing period accompanied with an increase in the peak firing rates, as S_{EE} is increased); and finally, at high S_{EE} , to a damped oscillatory convergence towards a stationary states with high firing rates (≥ 100 spikes/s). However, while the same sequence is observed, the precise bifurcation values of S_{EE} are different. In fact, some of the Monte Carlo simulations show a sensitivity to initial conditions, even for statistically similar initial conditions (i.e., similar initial distributions of voltage and conductances), making a direct comparison difficult. Therefore, we are content with a qualitative comparison as we detailed above.

3.4. Validation of moment closure assumptions

Eq. (3) is a nonlinear $(2 + 1)$ dimensional problem and requires a numerical solver, one of which has been the subject of this paper. To simplify the mathematical representation further, one can project out the g variable by defining the conditional moments $\mu_n(v) = \int_0^\infty g^n \rho(g|v) dg$, for $n = 1, 2, \dots$ where $\rho(g|v)$ is the (conditional) pdf of g given v and can be computed from $\rho(t, v, g) = \rho(g|v)\rho_v(t, v)$. However, this will lead to a hierarchy of moment equations, where the dynamical equations for lower order moments depend on higher order moments. To close this hierarchy, in [42,14] the authors postulated a closure condition

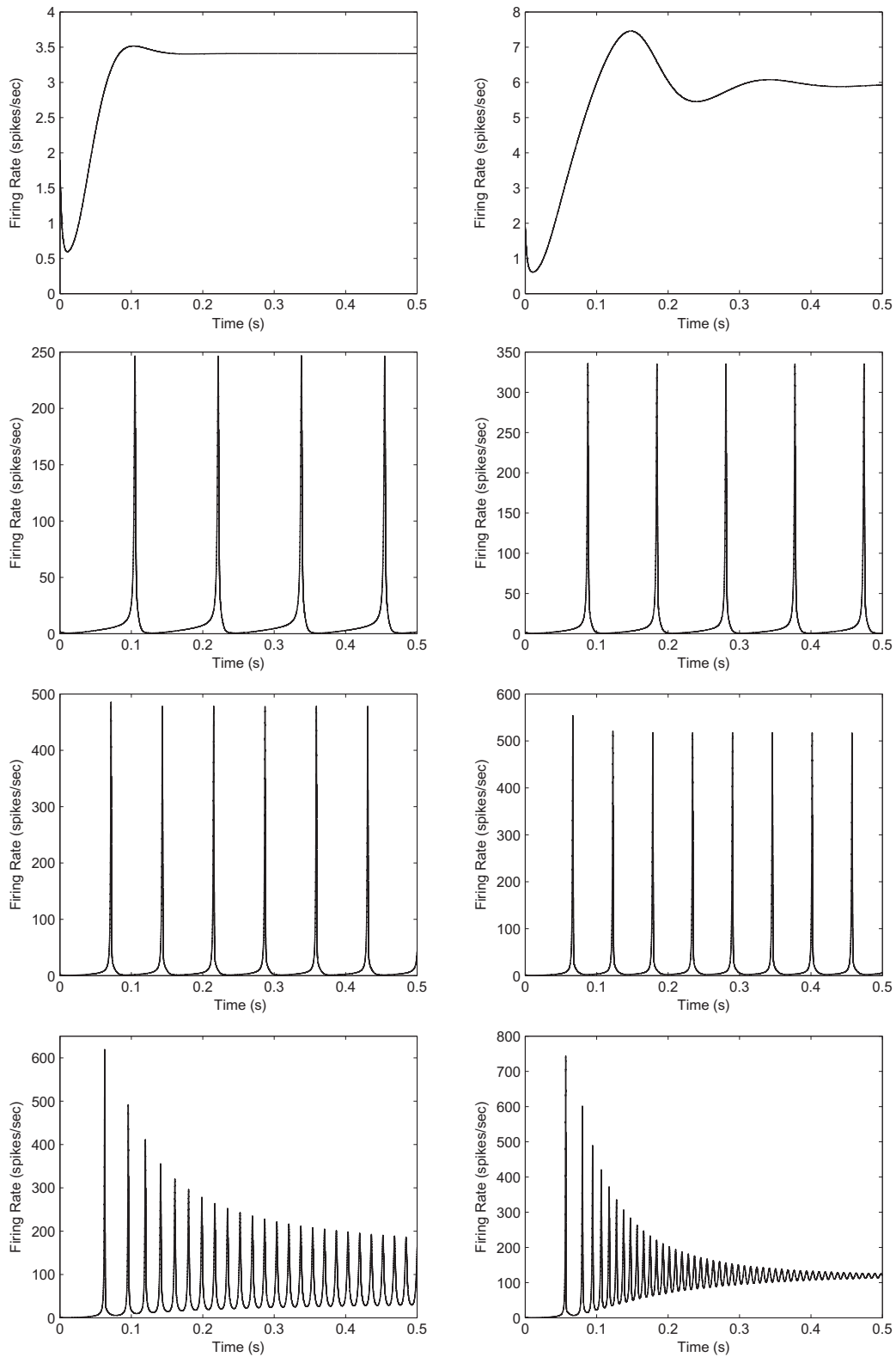


Fig. 13. Evolution in time of the firing rates for different values of S_{EE} for Case A with constant: $N_E = 500$, $f_E = 0.002$ s and $f_{EVOE} = 12$. From top to bottom and left to right: $S_{EE} = 0.1$, $S_{EE} = 0.12$, $S_{EE} = 0.13$, $S_{EE} = 0.14$, $S_{EE} = 0.16$, $S_{EE} = 0.17$, $S_{EE} = 0.18$ and $S_{EE} = 0.2$.

$$\Sigma^2(t, v) = \sigma_g^2(t) \quad (12)$$

for the conditional variance, $\Sigma^2(t, v) \equiv \mu_2(t, v) - \mu_1^2(t, v)$, and derived a system of two (1 + 1) dimensional PDEs for $\rho_v(t, v) = \int_0^\infty \rho(t, v, g) dg$ and $\mu_1(t, v)$:

$$\partial_t \rho_v(t, v) = \partial_v \left\{ \left[\left(\frac{v - V_R}{\tau} \right) + \mu_1(t, v) \left(\frac{v - V_E}{\tau} \right) \right] \rho_v(t, v) \right\} \quad (13)$$

$$\partial_t \mu_1(t, v) = -\frac{1}{\sigma_E} [\mu_1(t, v) - \bar{g}(t)] + \frac{\sigma_g^2(t)}{\rho_v(t, v)} \partial_v \left[\left(\frac{v - V_E}{\tau} \right) \rho_v(t, v) \right] + \left[\left(\frac{v - V_R}{\tau} \right) + \mu_1(t, v) \left(\frac{v - V_E}{\tau} \right) \right] \partial_v \mu_1(t, v). \quad (14)$$

With our numerical scheme we can validate the closure assumption $\Sigma^2(t, v) = \sigma_g^2(t)$ (12) since we can easily compute moments of the distribution function. Fig. 14 compares the conditional variance $\Sigma^2(t, v)$ with the variance $\sigma_g^2(t)$ for different

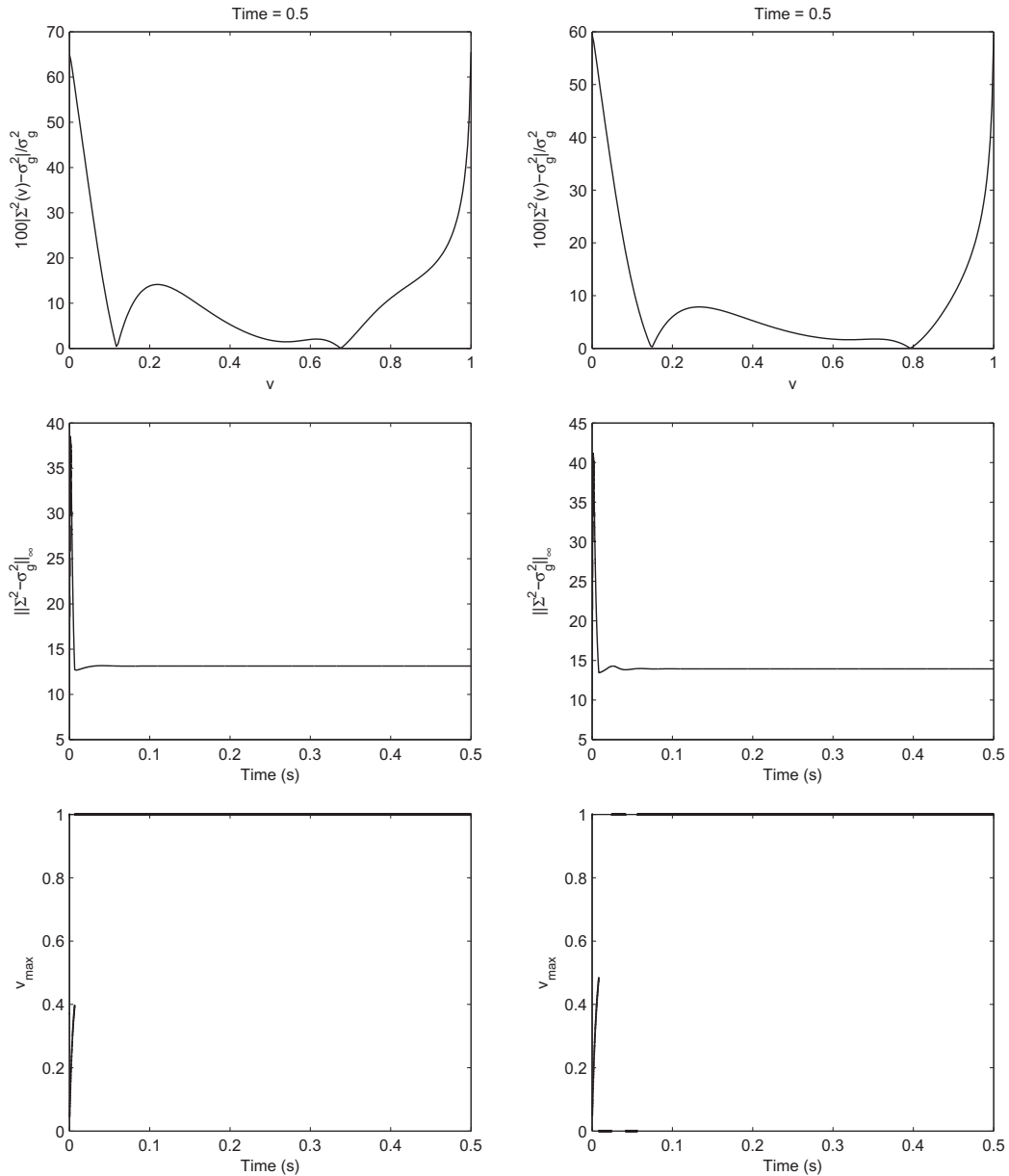


Fig. 14. For Case A validation of the closure (12). Left: $A = 1200$. Right: $A = 1400$. Top: Relative error (percent error) for the stationary solution, which was reached before 0.5 s. Middle: Evolution in time of the L_∞ -norm of $\Sigma^2(v) - \sigma_g^2$. Bottom: maximum value of v where $|\Sigma^2(v) - \sigma_g^2|$ reaches the value $\|\Sigma^2 - \sigma_g^2\|_\infty$.

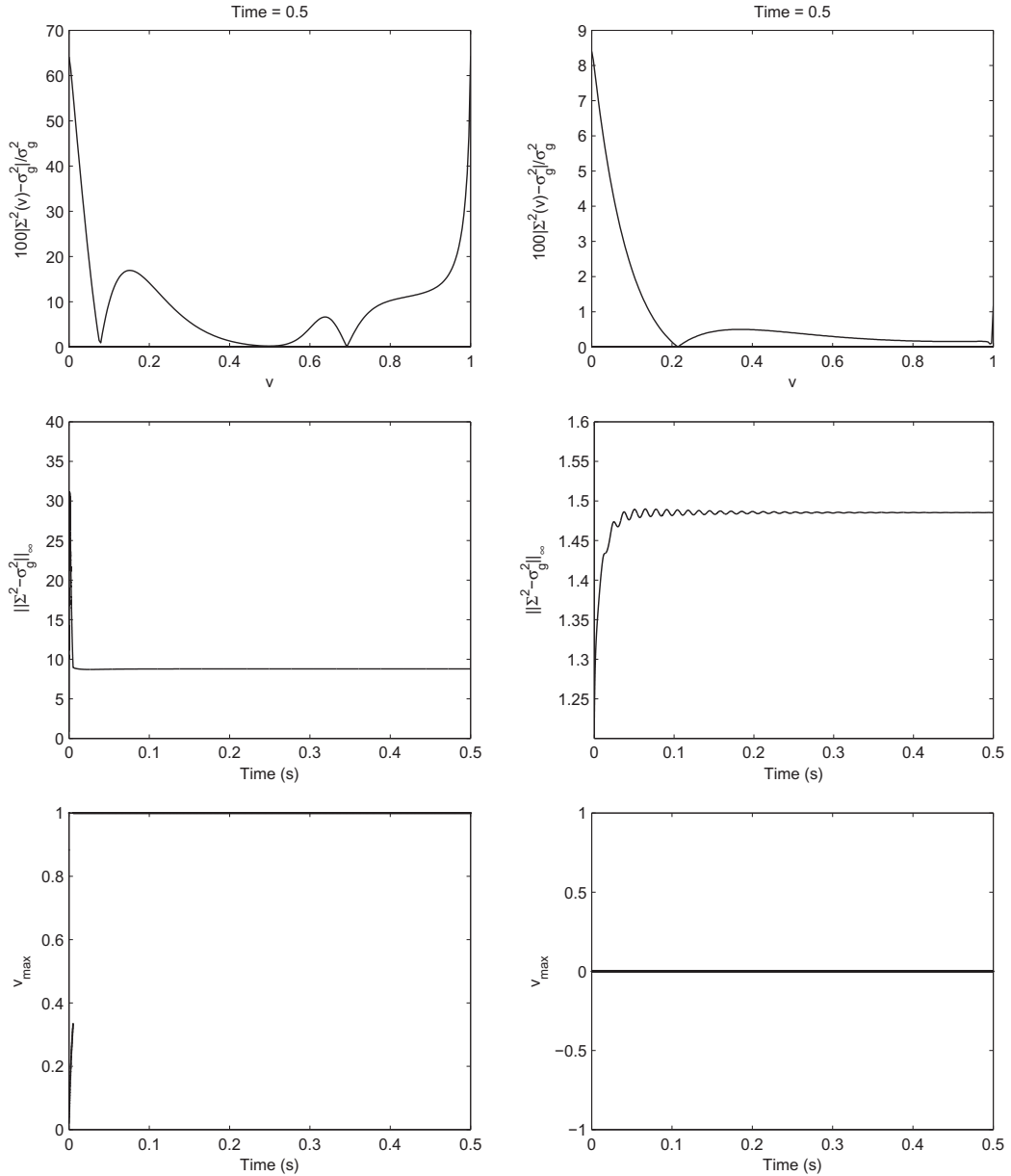


Fig. 15. For Case A where $f_E = 1/200$ s, $S_{EE} = 0.2$, $N_E = 200$, $\sigma_E = 2$ ms and $f_E v_{0E} = 10.8$ validation of the closure (12). Left: Lower branch. Right: Upper branch. Top: Relative error (percent error) for the stationary solution. Middle: Evolution in time of the L_∞ -norm of $\Sigma^2(v) - \sigma_g^2$. Bottom: Maximum value of v where $|\Sigma^2(v) - \sigma_g^2|$ reaches the value $\|\Sigma^2 - \sigma_g^2\|_\infty$.

values of A in Case A where unique, steady state solutions exist. We note that, in the steady state, the closure condition is satisfied, on average, away from the v -boundaries (the boundary presents the maximum percent relative error which is around 60%). More precisely, the maximum L_∞ difference of the two variances occurs at $v = 1$ (for all but the briefest of initial transients). In Fig. 15 we observe similar behavior in the case of where bistable solutions exist. Comparing both branches and the considered cases in Fig. 14, we realize that the percent relative error for the upper branch is the lowest, less than 9%. In general, we obtain that the closure assumption is reasonable for most values of v , away from the boundaries.

4. Conclusions

Our numerical Fokker–Planck solver is an efficient and accurate way of simulating the effective dynamics of a large-scale LIF neuronal network. This deterministic representation of the dynamics at the macroscopic level allows us to efficiently track the temporal evolution of the pdfs and to obtain any macroscopic quantities of the network dynamics. In this work,

we have validated our numerical scheme by comparing it with stochastic Monte Carlo simulations. We have also used our numerical solver to analyze a series of numerical examples. While a direct comparison between networks with physiological parameters and our numerical simulations is not technically feasible at this point, we have chosen to examine results from model networks with firing rates that are physiological realistic, i.e., with firing rates that range from a few spikes a second to a hundred spikes a second. In future work, we will extend our numerical scheme to networks with both excitatory and inhibitory couplings and to networks with spatial dependencies. This future project is not a direct nor obvious modification of the scheme developed in this paper: the boundary conditions in voltage are more complicated in cases where networks with both excitatory and inhibitory couplings; more variables (and thus more equations) are needed; the spatial dependence has to be clarified at the level of the Fokker–Planck equation, etc. Therefore, the work described in this paper is an essential step towards simulating realistic, large-scale neuronal network behavior.

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