

**WORKSHOP PRESENTATION**

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# Pressure gradient measurement using phase contrast (PC)-MRI in stenotic phantom models: Towards noninvasive quantification of fractional flow reserve in the coronary arteries

Zixin Deng<sup>1,2\*</sup>, Sang Eun Lee<sup>3</sup>, Zhaoyang Fan<sup>1</sup>, Christopher T Nguyen<sup>1</sup>, Qi Yang<sup>1</sup>, Xiaoming Bi<sup>4</sup>, Byoung Wook Choi<sup>5</sup>, Daniel S Berman<sup>1</sup>, Hyuk-Jae Chang<sup>3</sup>, Debiao Li<sup>1,2</sup>

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## Background

Fractional flow reserve (FFR) is an invasive diagnostic tool to evaluate the functional significance of an intermediate coronary stenosis by quantifying the pressure gradient ( $\Delta P$ ) across that stenosis [1]. Noninvasive  $\Delta P$  measurement ( $\Delta P_{MR}$ ) using phase-contrast (PC)-MRI in conjunction with Navier-Stokes (NS) equations has been attempted in large to medium size vessels [2-4], and recently been applied to smaller coronary arteries [5]. However, the measurement accuracy awaits systematic validation given that the small, tortuous, and moving caliber in the coronary artery, particularly when a stenosis exists, may elicit errors in flow velocity quantification by PC-MRI. This study aimed to investigate the feasibility of deriving  $\Delta P_{MR}$  in small caliber stenotic phantom models at various diameters and its correlation with measured  $\Delta P$  values via a pressure transducer ( $\Delta P_{PT}$ ).

## Methods

11 small caliber phantom models ranging from 0%-85% area stenosis, with a reference diameter of 4.8 mm, were individually connected to a flow pump (gadolinium-doped water, constant volume velocity = 250 mL/min) while 2D cross-sectional PC-MRI images were acquired. Contiguous slices (10-20) were consecutively collected across each narrowing (fig. 1a/b). Imaging parameters were: FA = 15°; TE/TR = ~4.0/70 ms; in-plane spatial resolution = ~0.55 × 0.55 mm<sup>2</sup>; slice thickness = 3.2 mm;  $V_{enc} = z$  (40-260 cm/s) and x, y (40-80 cm/s), depending

on the degree of narrowing. Eddy-current correction was done offline followed by NS calculations [6]. Repeat scans were performed in 7/11 phantom models and reproducibility was assessed by calculating the intra-class correlation coefficient (ICC) and Bland-Altman plots. Immediately following the PC-MRI scans, pressure was measured using an arterial catheter connected to a pressure transducer at ~1.5 cm before and ~3 cm after the maximum narrowing of the phantom models.

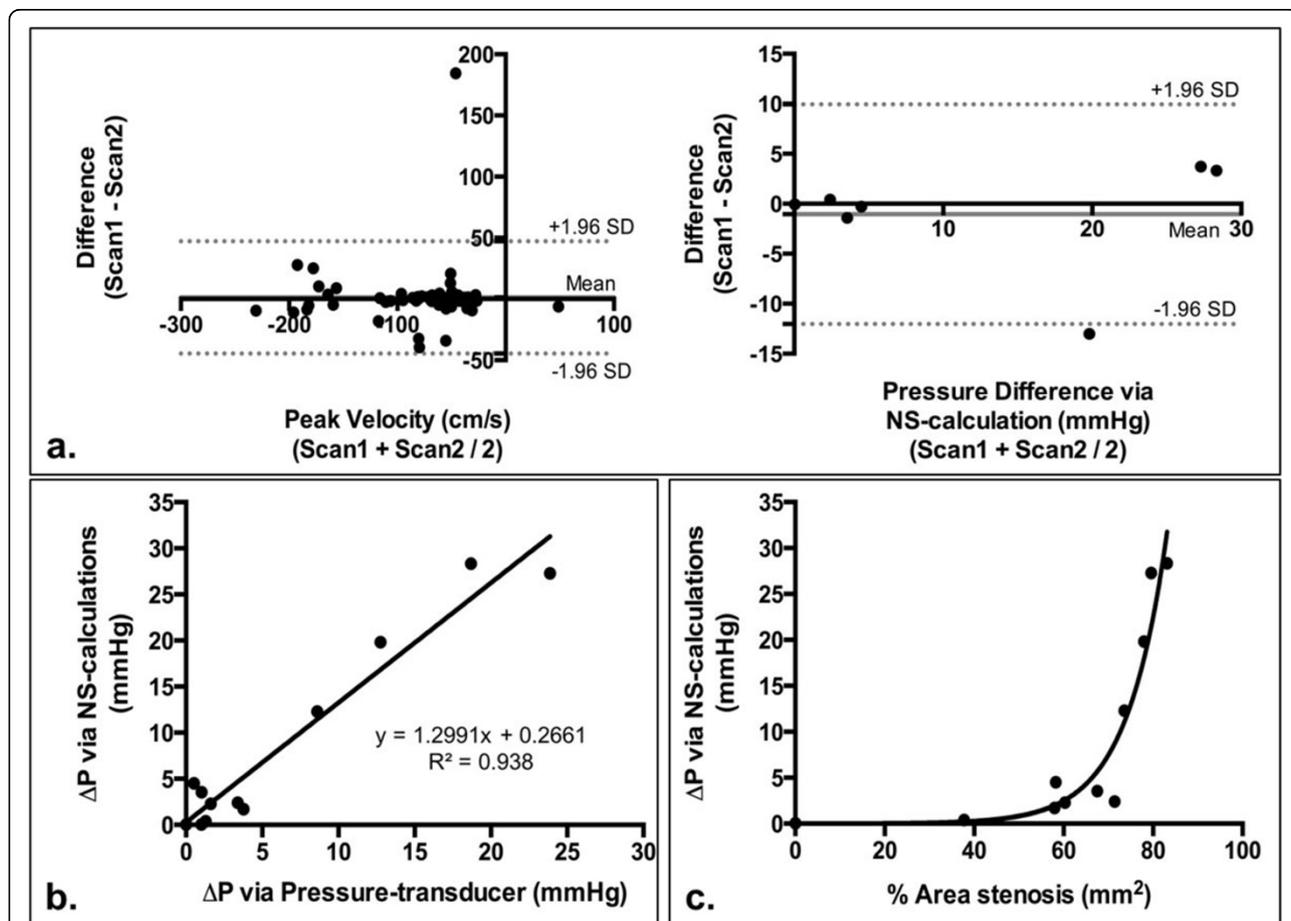
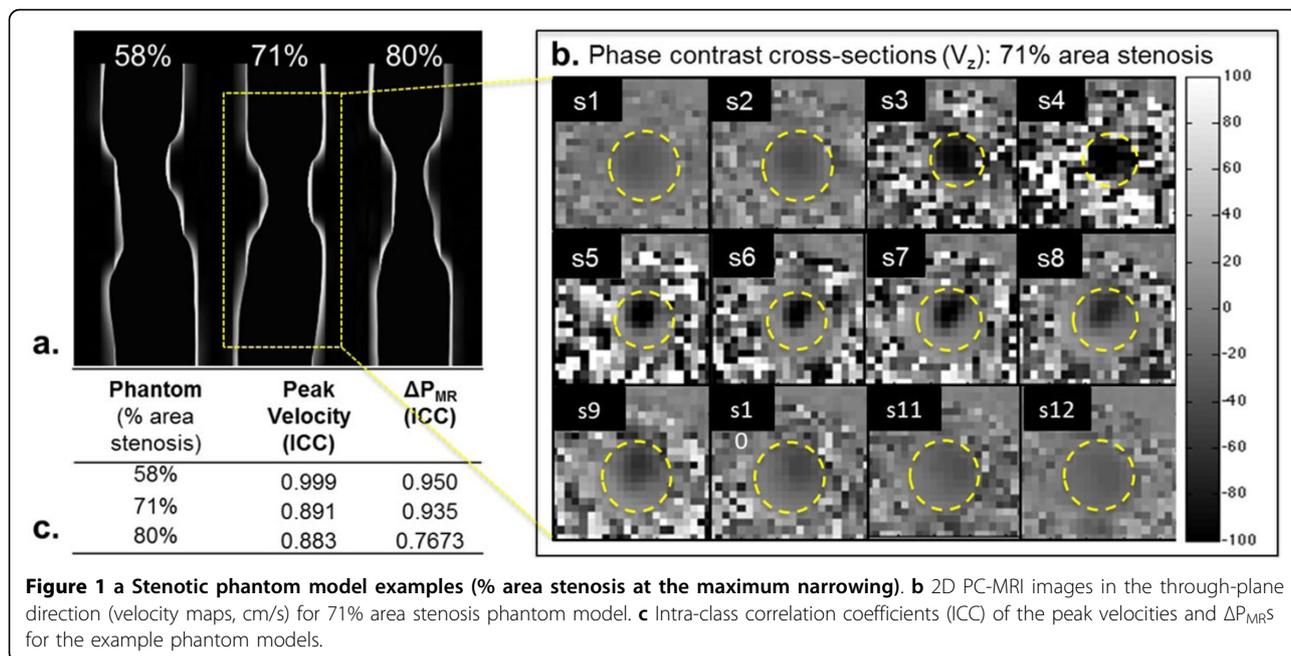
## Results

Bland-Altman plots of peak velocities and  $\Delta P_{MR}$  are shown in fig. 2a. For velocity measurements, excellent correlation was seen in the through-plane peak velocities ( $V_z$ , ICC = 0.90) and lower in  $V_x$  (ICC = 0.57) and  $V_y$  (ICC = 0.58). For  $\Delta P_{MR}$ s, overall ICC = 0.87; When observed individually, higher correlation was seen at smaller stenosis degrees and weaker as stenosis increased (fig. 1b). This could be due to the increased velocity in larger stenosis, causing minor turbulence distal of the narrowing, thus, inconsistent velocity and  $\Delta P_{MR}$  between the two scans. Furthermore,  $\Delta P_{MR}$  and  $\Delta P_{PT}$  were highly correlated (fig. 2b). We also observed that as % area stenosis increased,  $\Delta P_{MR}$  also increased (fig. 2c).

## Conclusions

Preliminary results suggest that quantification of  $\Delta P_{MR}$  in a small caliber is feasible. Further technical improvements in higher in-plane and through-plane spatial resolutions and reduction of noise need to be employed, which could potentially help improve the accuracy of the  $\Delta P_{MR}$  calculations.

<sup>1</sup>Cedars Sinai Medical Center, Los Angeles, CA, USA  
Full list of author information is available at the end of the article



**Figure 2** a Bland-Altman plots of peak velocities at all cross-sectional slice from repeat PC-MRI scans and the derived  $\Delta P$  of the phantom models. Mean (bias) and 95% confidence internal limits are displayed. b Pressure measurement comparison between  $\Delta P$  calculated via NS-equations and  $\Delta P$  measured using pressure transducer. Excellent correlation ( $R^2 = 0.938$ ) was observed between the two techniques. c % area stenosis versus  $\Delta P_{MR}$  measurement. An exponential increase in  $\Delta P_{MR}$  was observed as % area stenosis increases.

#### Authors' details

<sup>1</sup>Cedars Sinai Medical Center, Los Angeles, CA, USA. <sup>2</sup>Bioengineering, University of California, Los Angeles, Los Angeles, CA, USA. <sup>3</sup>Severance Cardiovascular Hospital, Yonsei College of Medicine, Seoul, Korea (the Republic of). <sup>4</sup>MR R&D, Siemens Healthcare, Los Angeles, CA, USA. <sup>5</sup>Radiology, Research Institute of Radiological Science, Yonsei University College of Medicine, Seoul, Korea (the Republic of).

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#### References

1. Pijls, *et al: NEJM* 1996.
2. Bock, *et al: MRM* 2011.
3. Lum, *et al: RY* 2007.
4. Bley, *et al: RY* 2011.
5. Deng, *et al: ISMRM* 2014.
6. Yang, *et al: MRM* 1996.

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