



ORIGINAL ARTICLE

Dosimetric effect of different isocenter for nasopharyngeal carcinoma with volumetric modulated arc therapy

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Abstract

Objective: The purpose of this study was to analyze the dosimetric effect of different isocenters with volumetric modulated arc therapy for nasopharyngeal carcinoma (NPC).

Methods: A total of 20 NPC patients who had received radiotherapy were re-planned by the volumetric modulated arc therapy plan. Three volumetric modulated arc therapy plans with different isocenters were generated for each patient: the first plan using the center of PGT_{V_{nx}} as the isocenter (AP-V), the second plan using the center of PGT_{V_{nd}} as the isocenter (BP-V), and the third plan using the center of PTV₂ as the isocenter (CP-V). The conformity and homogeneity indexes of the target, dose-volume histogram of organs at risk, normal tissue, volume of dose, and monitor units were compared for the three plans.

Results: AP-V provided a significantly lower maximum dose for the optic nerves and optic chiasm; lower mean dose for the eyeballs; lower absolute volume >10 Gy, absolute volume >20 Gy, and absolute volume >30 Gy; and fewer monitor units than BP-V and CP-V. BP-V and CP-V provided a significantly lower absolute volume >50 Gy than AP-V. In the conformity indexes of PGT_{V_{nd}} and PTV₂, BP-V and CP-V were significantly better than in AP-V. In the homogeneity index of PTV₂, BP-V and CP-V were significantly better than in AP-V. In general, there is no significant difference between BP-V and CP-V.

Conclusions: All three plans achieved the clinical demands. AP-V decreased the volumes of absolute volume >10 Gy, absolute volume >20 Gy, and absolute volume >30 Gy, whereas BP-V and CP-V decreased the volume of absolute volume >50 Gy. In terms of organs at risk, AP-V offered better protection of the optic nerves, optic chiasm, and eyeballs for NPC than BP-V and CP-V. Most importantly, AP-V enhanced the utilization of the monitor units. For this reason, we propose that the radiotherapy technician put the location position in the PGT_{V_{nx}} center during simulation of the NPC patients. We further propose that the isocenter be moved to the geometric center of PGT_{V_{nx}} if the NPC patient plan has higher dosimeter requirements for the optic nerves, optic chiasm, or eyeballs.

KEYWORDS

dosimetric comparison, isocenter, nasopharyngeal carcinoma, volumetric modulated arc therapy

1 | INTRODUCTION

Nasopharyngeal carcinoma (NPC) represents approximately 0.7% of all tumors, and is distinctly endemic in Southeast Asia.^{1,2} Because of its

anatomical characteristics, biological properties, and radiosensitivity, radiation therapy has been the mainstay treatment modality for non-metastatic NPC patients. Volumetric modulated arc therapy (VMAT) is currently widely used in the treatment of patients with NPC because of

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TABLE 1 T, N, and M stages of 20 patients

Stage	N0	N1	N2	N3	M0	M1	Sum
T1	0	0	1	1	2	0	2
T2	0	0	3	1	4	0	4
T3	1	1	5	2	9	0	9
T4	0	3	1	1	5	0	5
Sum	1	4	10	5	20	0	20

the dosimetric advantage over intensity-modulated radiation therapy (IMRT), as well as its lower radiotherapy time (RT).^{3–8} Because the current RT technology is mainly the isocentric irradiation technique, the position of the isocenter is very important. There are numerous literature reports regarding the dosimetric effects of errors of the isocenter on a variety of cancers with VMAT or IMRT.^{9–15} To our knowledge, no data are available on the dosimetric impact of different isocenters for NPC patients regardless of VMAT or IMRT status. Therefore, the present study aimed to elucidate the dosimetric effects of different isocenters for NPC with VMAT.

2 | METHODS

2.1 | Patients

A total of 20 non-metastatic NPC patients who had received VMAT treatment between April 2018 and July 2018 in Zhejiang Cancer Hospital were re-planned for our study. The study population included 15 men and five women, and the median age was 53 years (range 38–79 years). T1, T2, T3, and T4 had two, four, nine, and five patients, respectively, according to International Union Against Cancer 2010. The data of the tumor stages are shown in Table 1. This study was approved by the institutional review board of Zhejiang Cancer Hospital, and all the patients provided voluntary informed consent to participate in the study.

2.2 | Volume definition and dose prescription

As described previously, the gross tumor volume of the nasopharynx (GTV_{nx}) includes the primary tumor and metastatic retropharyngeal lymph nodes.¹⁶ Metastatic cervical lymph nodes are defined as the gross tumor volume of the involved cervical lymph nodes (GTV_{nd}). The high-risk clinical target volume CTV₁ includes the GTV_{nx} and GTV_{nd} with a margin of 5–10 mm, entire nasopharynx, inferior two-thirds of the sphenoid sinus, anterior third of the clivus, pterygoid fossae, posterior third of the nasal cavity and maxillary sinuses, parapharyngeal space, retropharyngeal nodes, and drainage of the upper neck. The low-risk clinical target volume CTV₂ encompasses the CTV₁ with a margin of 3–5 mm, lower neck, and supraclavicular lymphatic drainage region. The planning target volume (PTV) is defined as the area 3–5 mm outside of CTV or GTV. The dose prescribed was as follows: 70 Gy to PGTV_{nx} and PGTV_{nd}, 60 Gy to PTV₁, and 54 Gy to PTV₂ (The PGTV is defined as the area 3 mm outside of GTV. The PTV is defined as the area

3–5 mm outside of CTV. So PGTV_{nx} is defined as the area 3 mm outside of GTV_{nx}, PGTV_{nd} is defined as the area 3 mm outside of GTV_{nd}, PTV₁ is defined as the area 3–5 mm outside of CTV₁, PTV₂ is defined as the area 3–5 mm outside of CTV₂). The total doses of PGTV_{nx}, PGTV_{nd}, PTV₁, and PTV₂ were given in 33 fractions. All patients were irradiated with one fraction daily, 5 days per week. In the study, organs at risk (OARs) mainly included the brainstem, spinal cord, lenses, eyeballs, optic nerves, optic chiasm, temporal lobes, and parotid glands.

2.3 | Choosing the isocenter position

We usually moved the isocenter to the geometric center of the target volume if the location position was not suitable for the plan. There were four target volumes for NPC patients. Of these, the highest dose targets were PGTV_{nx} and PGTV_{nd}, and the lowest dose target was PTV₂. Thus, three isocenters were generated for each patient: the first using the geometric center of PGTV_{nx} as the isocenter (AP), the second using the geometric center of PGTV_{nd} as the isocenter (BP), and the third using the geometric center of PTV₂ as the isocenter (CP). Therefore, each patient had three different VMAT plans with different isocenters: the first plan using the geometric center of PGTV_{nx} as the isocenter (AP-V), the second plan using the geometric center of PGTV_{nd} as the isocenter (BP-V), and the third plan using the geometric center of PTV₂ as the isocenter (CP-V). The positions of the isocenters are shown in Figure 1.

2.4 | Planning design

A trilogy machine model was used in the study. We adopted RayArc of Raystation Planning System 4.5.1 (Raysearch Laboratories AB, Stockholm, Sweden) to design all VMAT plans. The multi-leaf collimator (MLC) of the Varian Trilogy machine has 40 pairs of blades. The MLC thickness of the middle 20 pairs of blades is 0.5 cm. There are 10 pairs of MLC blades on each side and the MLC thickness is 1 cm. All patients finished the 33 fractions RT simultaneously with an integrated boost technique. Photon beams of 6 MV were applied to all three plans. Each plan had two full arcs of a clockwise rotation from 182° to 178°, and counterclockwise rotation from 178° to 182°. The gantry interval was set as 4° between each control point in our planning to optimize the calculation time and accuracy of treatment planning. There were 180 control points for each plan. The collimator angle was 10° considering the tongue-and-groove effect.³ The dose grid resolution was set to 0.25 × 0.25 × 0.25 cm for all plans, considering the accuracy of calculation and a computed tomography image slice thickness of 0.25 cm.

The dose constraints for each target and OARs of all plans were as follows: the prescribed dose of each target should cover 95% of the target volume. In addition, it was necessary to evaluate the three-dimensional dose distribution. The brainstem maximum point dose (D_{max}) <54 Gy, spinal cord D_{max} <40 Gy, lenses D_{max} <6 Gy, eyeballs mean point dose (D_{mean}) <30 Gy, optic nerves and optic chiasm D_{max} <54 Gy, temporal lobes V_{65Gy} <1cc, and parotid glands V_{30Gy} <50% results are shown in Table 2. In the plan design, the OARs functions and weights were identical in the three plans of each patient;

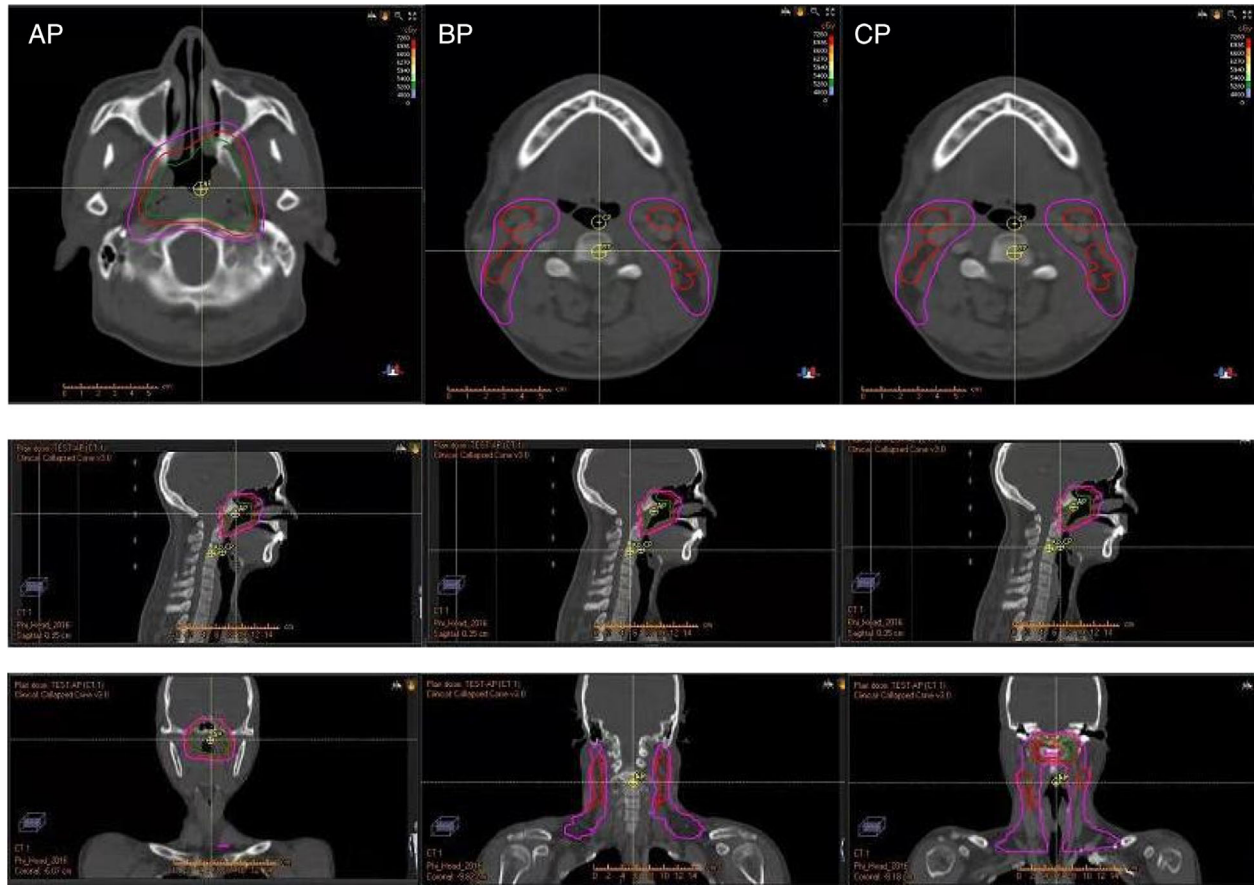


FIGURE 1 Isocenter positions of AP, BP, and CP with transverse, sagittal, and coronal planes. AP, the geometric center of target PGTV_{nx}; BP, the geometric center of target PGTV_{nd}; CP, the geometric center of target PTV₂

TABLE 2 Planning objectives for target volumes and organs at risk

Targets	Maximum dose PGTV _{nx} , PGTV _{nd}	
	<110% prescribed dose	
Targets	Coverage PGTV _{nx} , PGTV _{nd} , PTV ₁ , PTV ₂	
	D _{95%} ≥ prescribed dose	
OAR	Brainstem	D _{max} <54 Gy
	Spinal cord	D _{max} <40 Gy
	Lenses	D _{max} <6 Gy
	Eyeballs	D _{mean} <30 Gy
	Optic nerves	D _{max} <54 Gy
	Optic chiasm	D _{max} <54 Gy
	Temporal lobes	V _{65Gy} <1cc
	Parotid glands	V _{30Gy} <50%

D_{max}, maximum dose; D_{mean}, mean dose; OAR, organ at risk.

the functions and weights for the targets were slightly different to meet the clinical requirements of the target volumes.

2.5 | Plan comparisons

The dosimetric comparison criteria of the plans are as follows:

1. Conformity index (CI): measurement of how conformal the dose distribution is along the target volume. Formula: $CI = TV_{PV} \times$

$TV_{PV} / (V_{PTV} \times V_{TV})$. Possible values for CI range from 0 to 1. A CI value closer to 1 indicates better dose conformity in the PTV (V_{TV} is the treatment volume of the prescribed isodose line, V_{PTV} is the volume of PTV, and TV_{PV} is the volume of PTV covered by the prescription dose).^{17,18}

2. Homogeneity index (HI): measurement of how uniform the dose distribution is in all four targets PGTV_{nx}, PGTV_{nd}, PTV₁, and PTV₂. Formula: $HI = D_{5\%} / D_{95\%}$. A higher HI indicates poorer homogeneity.^{3,19}
3. OAR: determination of D_{max} to serial organs, such as the brainstem, spinal cord, lenses, optic nerves, and optic chiasm; the mean dose of eyeballs, the absolute volume V_{60Gy} of temporal lobes, and the volume percentage V_{30Gy} of the parotid glands.
4. Normal tissue (NT) volume of dose: evaluation of absolute dose volume to the NT of V_{10Gy}, V_{20Gy}, V_{30Gy}, V_{40Gy}, and V_{50Gy} (which represent the absolute volume more than 10 Gy, 20 Gy, 30 Gy, 40 Gy, and 50 Gy, respectively).
5. Monitor units (MUs): comparison of the MUs for the three group plans of AP-V, BP-V, and CP-V. The delivery time was not included in the study, because two full arcs were used for all plans and the delivery time was almost identical for the three plans of each patient.

TABLE 3 Plan comparison for the CI and HI of PGTV_{nx}, PGTV_{nd}, PTV₁, and PTV₂

	AP-V	BP-V	CP-V	P-value		
				AP-V vs BP-V	AP-V vs CP-V	BP-V vs CP-V
CI-PGTV _{nx}	0.370 ± 0.0115	0.371 ± 0.118	0.374 ± 0.113	0.765	0.140	0.167
HI-PGTV _{nx}	1.057 ± 0.006	1.057 ± 0.006	1.056 ± 0.006	0.943	0.221	0.367
CI-PGTV _{nd}	0.321 ± 0.098	0.328 ± 0.102	0.330 ± 0.105	0.003	0.002	0.198
HI-PGTV _{nd}	1.051 ± 0.005	1.050 ± 0.006	1.050 ± 0.006	0.125	0.195	0.752
CI-PTV ₁	0.648 ± 0.155	0.648 ± 0.149	0.649 ± 0.143	0.204	0.079	0.538
HI-PTV ₁	1.178 ± 0.016	1.177 ± 0.018	1.178 ± 0.017	0.680	0.694	0.652
CI-PTV ₂	0.722 ± 0.031	0.738 ± 0.027	0.739 ± 0.032	0.000	0.000	0.538
HI-PTV ₂	1.336 ± 0.006	1.333 ± 0.007	1.332 ± 0.006	0.001	0.001	0.492

AP-V, the first plan using the center of PGTV_{nx} as the isocenter; BP-V, the second plan using the center of PGTV_{nd} as the isocenter; CI-, conformity index of; CP-V, the third plan using the center of PTV₂ as the isocenter; HI-, homogeneity index of; The target PGTV_{nx}, PGTV_{nd}, PTV₁, PTV₂ are defined in "2.2 Volume definition and dose prescription".

2.6 | Statistical analysis

Results are described as the mean ± standard deviation. The two-tailed Wilcoxon matched-pairs signed-rank sum test was carried out to analyze the difference between the three different isocenter plans in the CI and HI of the targets, D_{max}, D_{mean}, V_{60Gy}, and V_{30Gy} of the OARs; the NT absolute dose volumes of V_{10Gy}, V_{20Gy}, V_{30Gy}, V_{40Gy}, and V_{50Gy}; and the MUs. A two-tailed P-value <0.05 is considered statistically significant. All analyses were carried out using the statistical software SPSS 19.0 (IBM Corporation, Armonk, NY, USA).

3 | RESULTS

3.1 | Target CI and HI

For a paired comparison, the CIs of PGTV_{nd} and PTV₂ with BP-V and CP-V were found to be statistically significantly greater than that of AP-V. The HIs of PTV₂ with BP-V and CP-V were found to be statistically significantly smaller than that of AP-V. PGTV_{nx} and PTV₁ were found to have no statistically significant differences with the three groups in the CI and HI (Table 3).

3.2 | OARs

All the doses for the OARs met the clinical demands. In comparison with BP-V and CP-V, AP-V performed statistically significantly better in sparing the optic nerves, optic chiasm, and eyeballs. The D_{max} of the AP-V L-optic nerve was reduced by 12.3% compared with BP-V, and 10.6% compared with CP-V. The D_{max} of the AP-V R-optic nerve was reduced by 7.8% compared with BP-V, and 7.0% compared with CP-V. The D_{max} of the AP-V optic chiasm was reduced by 15.2% compared with BP-V, and 13.9% compared with CP-V. The mean dose of the AP-V left eyeball was reduced by 6.8% compared with BP-V, and 4.9% compared with CP-V. The mean dose of the AP-V right eyeball was reduced by 8.3% compared with BP-V, and 7.8% compared with CP-V. There were no statistically significant differences between

BP-V and CP-V in terms of the D_{max} of the optic nerves, optic chiasm, and mean dose of the eyeballs. There were no statistically significant differences between the three groups in terms of the D_{max} of the brainstem, spinal cord, lenses, V_{60Gy} of the temporal lobes, and V_{30Gy} of the parotid glands (Table 4).

3.3 | NT dose volume and MUs

In the present study, we counted the absolute volume of NT with V_{10Gy}, V_{20Gy}, V_{30Gy}, V_{40Gy}, and V_{50Gy}. V_{10Gy} of AP-V was statistically significantly reduced by 3.7% with BP-V, and 3.0% with CP-V. V_{20Gy} of AP-V was statistically significantly reduced by 1.6% with BP-V, and 1.6% with CP-V. V_{30Gy} of AP-V was statistically significantly reduced by 1.4% with BP-V, and 1.9% with CP-V. However, V_{50Gy} of AP-V was statistically significantly increased by 1.4% with BP-V, and 1.9% with CP-V. V_{10Gy}, V_{20Gy}, V_{30Gy}, and V_{50Gy} were not statistically significantly different between BP-V and CP-V. V_{40Gy} was not statistically significant in the three groups. The MUs of AP-V were found to be statistically significantly reduced by 11.5% with BP-V, and 10.2% with CP-V (Table 5).

4 | DISCUSSION

The treatment of NPC has included CRT, 3D-CRT, IMRT, and VMAT. IMRT and VMAT are the main RT techniques for NPC patient treatment. For VMAT and IMRT, different settings in the plan design might cause dosimetry differences in the plans for a variety of cancers; these differences include the number of arcs,^{6,20,21} the spacing units of the gantry for VMAT,²² the angle of the collimator,²³ the calculation grid size,²⁴ and the photon energy.²⁵

The isocenter is very important, because RT usually uses an isocentric irradiation technique. The movement of the isocenter for the gamma knife is convenient, and more multi-isocenter irradiation technology is used. There are several studies regarding the dosimetric differences of different isocenters for the gamma knife.^{26,27} In addition,

TABLE 4 Dosimetric comparison for organs at risk between the first plan using the center of PGTV_{nx} as the isocenter, the second plan using the center of PGTV_{nd} as the isocenter, and the third plan using the center of PTV₂ as the isocenter

					P-value		
					AP-V vs BP-V	AP-V vs CP-V	BP-V vs CP-V
Brainstem	D _{max} (Gy)	53.79 ± 2.80	54.11 ± 2.38	53.41 ± 2.75	0.737	0.140	0.332
Spinal cord	D _{max} (Gy)	39.57 ± 0.76	39.48 ± 1.81	39.57 ± 1.89	0.681	0.305	0.444
L-eyes	D _{max} (Gy)	5.44 ± 0.66	5.39 ± 0.44	5.42 ± 0.54	0.255	0.322	0.940
R-eyes	D _{max} (Gy)	5.37 ± 0.72	5.43 ± 0.30	5.37 ± 0.49	0.559	0.287	0.268
L-eyeball	D _m (Gy)	5.07 ± 0.84	5.44 ± 0.60	5.33 ± 0.74	0.003	0.016	0.140
R-eyeball	D _m (Gy)	4.85 ± 0.54	5.29 ± 0.42	5.26 ± 0.45	0.000	0.002	0.380
L-optic nerve	D _{max} (Gy)	37.73 ± 15.47	43.03 ± 10.55	42.23 ± 12.90	0.004	0.003	0.808
R-optic nerve	D _{max} (Gy)	40.51 ± 12.54	43.96 ± 9.33	43.56 ± 10.86	0.010	0.044	0.911
Optic chiasm	D _{max} (Gy)	38.23 ± 16.23	45.11 ± 11.30	44.39 ± 12.38	0.000	0.006	0.550
L-temporal lobe	V _{60Gy} (cc)	0.66 ± 1.18	0.69 ± 1.33	0.64 ± 1.20	0.850	0.329	0.315
R-temporal lobe	V _{60Gy} (cc)	0.75 ± 0.94	0.78 ± 1.07	0.72 ± 1.00	0.693	0.340	0.368
L-parotid gland	V _{30Gy} (%)	45.81 ± 2.75	45.40 ± 2.88	45.04 ± 2.87	0.332	0.117	0.433
R-parotid gland	V _{30Gy} (%)	45.56 ± 2.43	45.77 ± 2.72	45.07 ± 2.36	0.490	0.156	0.135

AP-V, the first plan using the center of PGTV_{nx} as the isocenter; BP-V, the second plan using the center of PGTV_{nd} as the isocenter; CP-V, the third plan using the center of PTV₂ as the isocenter; D_{max}, maximum dose; D_m, mean dose; L, left; R, right; V_{60Gy} (cc), absolute volume >60 Gy; V_{30Gy} (%), volume percentage >30 Gy. The target PGTV_{nx}, PGTV_{nd}, PTV₂ are defined in "2.2 Volume definition and dose prescription".

TABLE 5 Plan comparison for normal tissue, dose-volume histogram and monitor units

	AP-V	BP-V	CP-V	P-value		
				AP-V vs BP-V	AP-V vs CP-V	BP-V vs CP-V
V _{10Gy} (cc)	4622 ± 917	4800 ± 1031	4763 ± 991	0.001	0.000	0.108
V _{20Gy} (cc)	3403 ± 619	3460 ± 625	3458 ± 609	0.019	0.004	0.926
V _{30Gy} (cc)	2272 ± 414	2322 ± 414	2313 ± 423	0.011	0.025	0.601
V _{40Gy} (cc)	1416 ± 271	1418 ± 281	1409 ± 266	0.765	0.313	0.212
V _{50Gy} (cc)	876 ± 174	864 ± 177	860 ± 169	0.011	0.000	0.295
MUs	500 ± 36	565 ± 40	557 ± 46	0.000	0.000	0.467

AP-V, the first plan using the center of PGTV_{nx} as the isocenter; BP-V, the second plan using the center of PGTV_{nd} as the isocenter; CP-V, the third plan using the center of PTV₂ as the isocenter; MUs, monitor units; V_{10Gy} (cc), absolute volume >10 Gy; V_{20Gy} (cc), absolute volume >20 Gy; V_{30Gy} (cc), absolute volume >30 Gy; V_{40Gy} (cc), absolute volume >40 Gy; V_{50Gy} (cc), absolute volume >50 Gy.

there are reports of multi-isocenter technology of RT with a linear accelerator.^{28,29}

Linear accelerator RT currently uses the isocentric irradiation technique, which generally just has an isocenter for the treatment. In most hospitals globally, if multi-isocenter technology is used, the RT technician needs to enter the machine room to move the treatment bed. This is very inconvenient and increases the patient's irradiation time, which is not conducive to the stability of the patient's RT position.

Our comparative planning study first compared the dosimetric difference produced by different single isocenters for NPC with VMAT. However, no literature has reported the dosimetric difference of any cancer produced by different single isocenters, regardless of whether it is IMRT or VMAT. For the cancer of the chest and abdomen, there were generally only one or two target volumes, and the technician usually put the positioning point in the center of PTV₂ when located; the

difference between the isocenter positions of the two target areas was small. The dosimetric differences were also small. However, NPC generally had four target volumes, and the position of the nasopharynx and the neck was different. If the center of each target volume was used as the isocenter, the positions of the four isocenters were different. This might result in a dosimetric difference for the VMAT plans using the four different isocenters. Therefore, it would be meaningful to discuss the dosimetric difference resulting from the different isocenters of the VMAT plans for NPC.

In the present study, the AP-V showed its superiority in protecting the optic nerves, optic chiasm, and eyeballs compared with BP-V and CP-V. In the NT, AP-V also showed its superiority in V_{10Gy}, V_{20Gy}, and V_{30Gy}. The AP-V could also use fewer MUs to meet the clinical requirements. The first reason might be that the MLC of each control point would first open near the isocenter point when the treatment planning system received the VMAT plan.

This makes it more likely that the plans would preferentially meet the critical organ and target requirements near the isocenter. Because most OARs of NPC were around the $PGTV_{nx}$, it could increase the utilization of MUs and protect the OARs around the $PGTV_{nx}$ better when the isocenter was in the center of $PGTV_{nx}$.

In this study, BP-V and CP-V showed no significant differences in CI, HI, dose of OARs, NT dose volume, and MUs, because the isocenter positions of BP-V and CP-V did not differ much. BP-V and CP-V were better in the CI and HI of PTV_2 , and the CI of $PGTV_{nd}$ compared with AP-V. In NT, BP-V and CP-V showed their superiority in V_{50Gy} . The possible reason was that the isocenter of CP-V was in the center of PTV_2 and the target dose of PTV_2 was 54 Gy. Because the MLC of each control point would first open near the isocenter point, CP-V had more advantages in the isodose of 50 Gy, and CI and HI of PTV_2 . For the same reason, BP-V had an advantage over CI of $PGTV_{nd}$. The isocenter position of BP-V and CP-V was so close that BP-V and CP-V had the same advantage compared with AP-V.

5 | CONCLUSIONS

The three plans all meet the clinical requirements. The MUs of the AP-V plans were significantly reduced by 11.5% with BP-V, and 10.2% with CP-V. In addition, the change in head contour is smaller than that of the neck during radiotherapy. Thus, the set-up error is smaller when the location position is in the geometric center of $PGTV_{nx}$ than in the geometric center of $PGTV_{nd}$ or PTV_2 . We propose that the RT technician put the location position in the geometric center of $PGTV_{nx}$ during location of the NPC patients. We further suggest that the isocenter be moved to the geometric center of $PGTV_{nx}$ if the NPC patient plan has higher dosimeter requirements for the optic nerves, optic chiasm, or eyeballs.

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REFERENCES

- Bray F, Ferlay J, Soerjomataram I, et al. Global Cancer Statistics 2018: gLOBOCAN Estimates of Incidence and Mortality Worldwide for 36 Cancers in 185 Countries. *CA Cancer J Clin*. 2018;68:394–424.
- Yu MC, Yuan JM. Epidemiology of nasopharyngeal carcinoma. *Semin Cancer Biol*. 2002;12:421–429.
- Lu SH, Cheng JCH, Kuo SH, et al. Volumetric modulated arc therapy for nasopharyngeal carcinoma: a dosimetric comparison with TomoTherapy and step-and-shoot IMRT. *Radiother Oncol*. 2012;3:324–330.
- Verbakel WF, Cuijpers JP, Hoffmans D, et al. Volumetric intensity-modulated arc therapy vs. conventional IMRT in head and neck cancer: a comparative planning and dosimetric study. *Int J Radiat Oncol Biol Phys*. 2009;74:252–259.
- White P, Chan KC, Cheng KW, et al. Volumetric intensity-modulated arc therapy vs conventional intensity-modulated radiation therapy in nasopharyngeal carcinoma: a dosimetric study. *J Radiat Res*. 2013;54:532–545.
- Ning ZH, Mu JM, Jin JX, et al. Single arc volumetric-modulated arc therapy is sufficient for nasopharyngeal carcinoma: a dosimetric comparison with dual arc VMAT and dynamic MLC and step-and-shoot intensity-modulated radiotherapy. *Radiat Oncol*. 2013;8:1–9.
- Lee TF, Chao PJ, Ting HM. Comparative analysis of SmartArc-based dual arc volumetric-modulated arc radiotherapy (VMAT) versus intensity-modulated radiotherapy (IMRT) for nasopharyngeal carcinoma. *J Appl Clin Med Phys*. 2011;12:158–174.
- Chen BB, Huang SM, Xiao WW, et al. Prospective matched study on comparison of volumetric-modulated arc therapy and intensity-modulated radiotherapy for nasopharyngeal carcinoma: dosimetry, delivery efficiency and outcomes. *J Cancer*. 2018;9:978–986.
- Delia C, Daniela A, Barbara AJF, et al. Set-up errors in head and neck cancer patients treated with intensity modulated radiation therapy: quantitative comparison between three-dimensional cone-beam CT and two-dimensional kilovoltage images. *Phys Med*. 2015;31:1015–1021.
- Cranmer-Sargison G. A treatment planning investigation into the dosimetric effects of systematic prostate patient rotational set-up errors. *Med Dosim*. 2008;33:199–205.
- Siebers JV, Keall PJ, Wu Q, et al. Effect of patient setup errors on simultaneously integrated boost head and neck IMRT treatment plans. *Int J Radiat Oncol Biol Phys*. 2005;63:422–433.
- Lee J, Kim JI, Ye SJ, et al. Dosimetric effects of roll rotational setup errors on lung stereotactic ablative radiotherapy using volumetric modulated arc therapy. *Br J Radiol*. 2015;88:20140862.
- Takemura A, Togawa K, Yokoi T, et al. Impact of pitch angle setup error and setup error correction on dose distribution in volumetric modulated arc therapy for prostate cancer. *Radiol Phys Technol*. 2016;9:178–186.
- Yan M, Lovelock D, Hunt M, et al. Measuring uncertainty in dose delivered to the cochlea due to setup error during external beam treatment of patients with cancer of the head and neck. *Med Phys*. 2013;40:121–124.
- Adamson J, Wu Q, Yan D. Dosimetric effect of intrafraction motion and residual setup error for Hypofractionated Prostate Intensity-Modulated Radiotherapy With Online Cone Beam computed tomography image guidance. *Int J Radiat Oncol Biol Phys*. 2011;80:453–461.
- Liu TX, Sun QQ, Chen J, et al. Neoadjuvant Chemotherapy with Fluorouracil plus Nedaplatin or Cisplatin for Locally Advanced Nasopharyngeal Carcinoma: a Retrospective Study. *J Cancer*. 2018;9:3676–3682.
- Lee FKH, Yip CWY, Cheung FCH, et al. Dosimetric difference amongst 3 techniques: tomoTherapy, sliding-window intensity-modulated radiotherapy (IMRT), and RapidArc radiotherapy in the treatment of late-stage nasopharyngeal carcinoma (NPC). *Med Dosim*. 2014;39:44–49.
- Wang JQ, Chen Z, Li WW, et al. A new strategy for volumetric-modulated arc therapy planning using AutoPlanning based multi-criteria optimization for nasopharyngeal carcinoma. *Radiat Oncol*. 2018;13:94–104.
- Weiss E, Siebers JV, Keall PJ. An analysis of 6-MV versus 18-MV photon energy plans for intensity-modulated radiation therapy (IMRT) of lung cancer. *Radiother Oncol*. 2007;82:55–62.
- Lee TF, Ting HM, Chao PJ, et al. Dual arc volumetric-modulated arc radiotherapy (VMAT) of nasopharyngeal carcinomas: a simultaneous integrated boost treatment plan comparison with intensity-modulated radiotherapies and single arc VMAT. *Clin Oncol*. 2012;24:196–207.
- Guckenberger M, Richter A, Krieger T, et al. Is a single arc sufficient in volumetric-modulated arc therapy (VMAT) for complex-shaped target volumes? *Radiother Oncol*. 2009;93:259–265.
- Murtaza G, Cora S, Khan EU. Validation of the relative insensitivity of volumetric-modulated arc therapy (VMAT) plan quality to gantry space resolution. *J Radiat Res*. 2017;58:579–590.

23. Pietro M, Luca C, Antonella F, et al. Collimator angle influence on dose distribution optimization for vertebral metastases using volumetric modulated arc therapy. *Med Phys*. 2010;37:4133–4137.
24. Srivastava SP, Cheng CW, Das IJ. The dosimetric and radiobiological impact of calculation grid size on head and neck IMRT. *Pract Radiat Oncol*. 2016;7:209–217.
25. Onal C, Arslan G, Dolek Y, et al. Dosimetric analysis of testicular doses in prostate intensity-modulated and volumetric-modulated arc radiation therapy at different energy levels. *Med Dosim*. 2016;41:310–314.
26. Morbidini GS, Chung CT, Alpert TE, et al. Doses greater than 85 Gy and two isocenters in Gamma Knife surgery for trigeminal neuralgia: updated results. *J Neuro Surg*. 2006;105:107–111.
27. Cho YB, Laperriere N, Hodaie M, et al. Hybrid isocenter technique for Gamma-Knife Perfexion treatment of trigeminal neuralgia. *Med Dosim*. 2016;41:271–276.
28. Boman E, Rossi M, Kapanen M. The robustness of dual isocenter VMAT radiation therapy for bilateral lymph node positive breast cancer. *Phys Med*. 2017;44:11–17.
29. Jin XC, Wu SX, Yu JY, et al. Technical and dosimetric considerations in multi-isocenter intensity modulated radiotherapy for nasopharyngeal carcinoma with small multileaf collimator. *Med Dosim*. 2009;34:9–15.

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