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# Modulation of synaptic potentials and cell excitability by dendritic $K_{IR}$ and $K_{AS}$ channels in nucleus accumbens medium spiny neurons: A computational study

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The nucleus accumbens (NAc), a critical structure of the brain reward circuit, is implicated in normal goal-directed behaviour and learning as well as pathological conditions like schizophrenia and addiction. Its major cellular substrates, the medium spiny (MS) neurons, possess a wide variety of dendritic active conductances that may modulate the excitatory post synaptic potentials (EPSPs) and cell excitability. We examine this issue using a biophysically detailed 189-compartment stylized model of the NAc MS neuron, incorporating all the known active conductances. We find that, of all the active channels, inward rectifying  $K^+$  ( $K_{IR}$ ) channels play the primary role in modulating the resting membrane potential (RMP) and EPSPs in the down-state of the neuron. Reduction in the conductance of  $K_{IR}$  channels evokes facilitatory effects on EPSPs accompanied by rises in local input resistance and membrane time constant. At depolarized membrane potentials closer to up-state levels, the slowly inactivating A-type potassium channel ( $K_{AS}$ ) conductance also plays a strong role in determining synaptic potential parameters and cell excitability. We discuss the implications of our results for the regulation of accumbal MS neuron biophysics and synaptic integration by intrinsic factors and extrinsic agents such as dopamine.

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## 1. Introduction

The nucleus accumbens (NAc), which predominantly constitutes the ventral striatum, acts as an interface between the limbic and extrapyramidal motor systems (Mogenson *et al.* 1980; Meredith and Totterdell 1999; Cooper 2002). It integrates motivational inputs related to emotional salience and contextual constraints from limbic structures such as ventral hippocampus and basolateral amygdale, on the one hand, and executive/motor inputs from medial prefrontal cortex, on the other (Mogenson 1987; Goto and O'Donnell

2002; Goto and Grace 2008). These glutamatergic inputs are modulated by dopaminergic inputs from ventral tegmental area (Yang and Mogenson 1984; Goto and Grace 2005a, b) that signal the reward stimuli (Kalivas and Nakamura 1999; Schultz 1998; Brady and O'Donnell 2004; Nicola *et al.* 2004). The integrated output is sent back to the cortex via ventral pallidum and medial thalamus (O'Donnell and Grace 1995) in order to generate appropriate responses in goal-directed behaviour. In addition to the normal goal-directed behaviour, the NAc is also believed to be involved in pathological conditions such as schizophrenia and drug

**Keywords.** Computational model; excitatory post synaptic potential (EPSP); inward rectifying  $K^+$  ( $K_{IR}$ ) channel; medium spiny neurons; nucleus accumbens slowly inactivating A-type potassium channel ( $K_{AS}$ ); spiking

Abbreviations used: AMPA, alpha-amino-3-hydroxy-5-methyl-4-isoxazole propionic acid; DA, dopamine; D1R, D1 receptor; D2R, D2 receptor; EPSPs, excitatory post synaptic potentials; GABA, gamma amino butyric acid; ISI, interspike interval;  $K_{IR}$ , inward rectifying potassium; MS, medium spiny; NAc, nucleus accumbens; NMDA, *N*-methyl-D-aspartate; RMP, resting membrane potential;  $K_{AS}$ , slowly inactivating A-type potassium

addiction, where the normal brain reward circuit is distorted (O'Donnell and Grace 1998; Grace 2000; Cooper 2002; Wolf 2002; Carlezon and Thomas 2009).

The inputs to the NAc are integrated at the level of single neurons, the medium spiny (MS) neurons, which constitute the primary neurons of the NAc (O'Donnell and Grace 1995; French and Totterdell 2002; French and Totterdell 2003; McGinty and Grace 2009) and respond to the changes in reward-related behaviour and learning (Schultz *et al.* 2003; Carelli 2004). Studies using *in vitro* slices and *in vivo* anesthetized preparations have shown that these neurons display a two-state behaviour of the membrane potential in which the neurons remain preferentially in either a hyperpolarized down-state ( $\sim -86$  mV) or a depolarized up-state ( $\sim -55$  mV), depending on its inputs (O'Donnell and Grace 1993, 1995) as well as the presence of ionic currents (Nisenbaum and Wilson 1995; Wilson and Kawaguchi 1996; Cooper and White 2000; Nicola *et al.* 2000, 2004). Majority of the dopaminergic inputs to the MS neurons are located at the dendritic shafts and spines that also receive extensive glutamatergic excitatory inputs from the cortex or hippocampus (Smith and Bolam 1990; Meredith *et al.* 2008). The close proximity of these inputs has been suggested as a cellular mechanism that mediates reward-related learning in striatum (Reynolds *et al.* 2001).

In central neurons, dendritic active conductances are known to influence the input–output properties of the neuron including synaptic integration, neuronal excitability and synaptic plasticity (Magee *et al.* 1998). When activated, the currents through these channels can alter the amplitude and time course of the synaptic potentials (Reyes 2001). Moreover, voltage-gated channels alter the local input resistance and membrane time constant, which in turn influence both spatial and temporal summation of EPSPs (Johnston *et al.* 1996). For example, the hyperpolarization-activated cation ( $I_h$ ) currents present in the dendrites of neocortical L5 and hippocampal pyramidal neurons act to reduce the overall neuronal excitability.  $I_h$  channels, being partially activated at rest, contribute to the resting potential of these cells and reduce their input resistance (Reyes 2001), resulting in EPSPs of smaller amplitude and faster decay (shorter duration) (Magee 1998; Williams and Stuart 2000; Migliore and Shepherd 2002; Biel *et al.* 2009). An active channel with an I-V curve bearing a resemblance to that of the  $I_h$  channel is also present in NAc MS neurons (the  $K_{IR}$  channel), in addition to a wide variety of other active channels that might potentially influence their input–output behaviour. These channels include voltage-dependent fast and persistent  $Na^+$  channels (NaF and NaP), fast and slow A-type  $K^+$  channels ( $K_{AF}$  and  $K_{AS}$ ), and different types of  $Ca^{2+}$  (CaN, CaQ, CaR, CaT and L-type  $Ca_v1.2$  and  $Ca_v1.3$ ) as well as the small- and large-conductance  $Ca^{2+}$ -dependent  $K^+$  channels ( $SKK_{Ca}$  and  $BKK_{Ca}$ ) (Wolf *et al.* 2005). It is believed that the intrinsic properties of these neurons can be

modulated and, thereby, neuronal excitability, by extrinsic factors such as dopamine that forms a major neuromodulator in the NAc (Nicola *et al.* 2000).

While some information is available about the conductances instrumental in maintaining the up- and down-states of the neuron (Wolf *et al.* 2001; Nicola *et al.* 2004), experimental studies on the roles of this wide array of active channels on EPSP propagation and synaptic integration have not been carried out in NAc MS neurons. Computational models provide a useful means of formulating experimentally testable predictions about the input–output behaviour of the neuron. Investigations on the role of  $K_{IR}$  channels in determining the membrane electrical properties in neostriatal neurons have been carried out in a previous computational work (Wilson 1992, 1993) that used a reduced model of the neuron with just two conductances – the  $K_{IR}$  and leak conductances. These studies indicated that  $K_{IR}$  plays a dominant role in modulating the electrical behaviour of the neuron in the down-state. However, as indicated earlier, as recent studies have shown that striatal neurons possess a wide range of nonlinear active channels and a biophysically more detailed model of the neuron incorporating all these channels is currently available in the literature (Wolf *et al.* 2005, Steephen and Manchanda 2009), we wished to investigate in detail (i) whether  $K_{IR}$  conductance continues to play a dominant role in the down-state even in the presence of the other non-linear active conductances in the neuron and (ii) whether any of the other channels plays a role in modulating the EPSPs in NAc MS neurons in the down-state as well as in the depolarized membrane potentials of the neuron. We find that, in the down-state, while the contribution from most channels is absent or negligibly small, dendritic  $K_{IR}$  channels do contribute significantly to this modulation even in the presence of other active conductances. However, at depolarized membrane potentials brought about by the blocking of  $K_{IR}$  conductance,  $K_{AS}$  channels secondarily modulate the somatic EPSPs. As it is expected that at increasingly depolarized potentials the  $K_{AS}$  conductance would play a progressively significant role compared with  $K_{IR}$ , we have also delineated the influence of  $K_{AS}$  on EPSPs at relatively depolarized membrane potentials and also on the spiking behaviour of the neuron during the up-state.

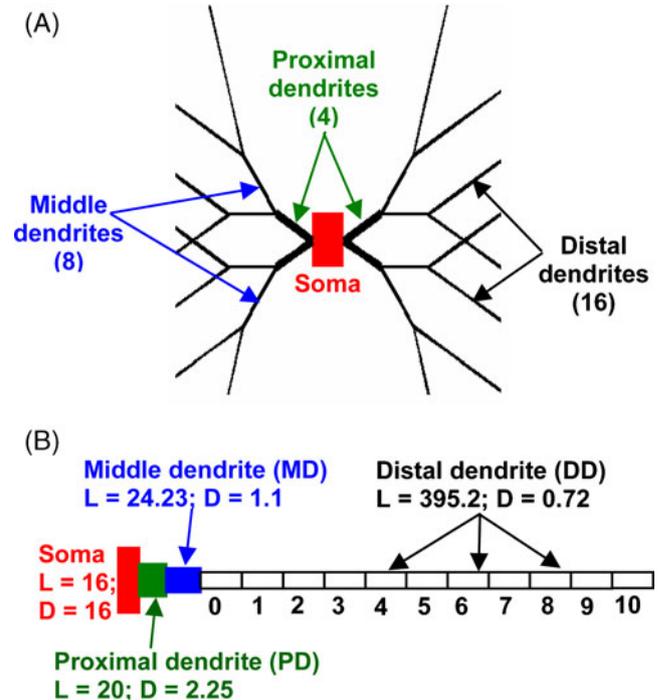
A further motivation for exploring the effects of the  $K_{IR}$  conductance on MS neuron biophysics stems from the reports that this conductance is a major target of modulation by neurotransmitters such as dopamine, the direction of modulation being dependent on the type of dopamine receptors present in these neurons. Therefore, we investigated the effects of varying the conductance of  $K_{IR}$  channels on down-state EPSPs and the possible mechanisms underlying these effects. We find that reduction in  $K_{IR}$  conductance results in depolarization of the RMP and enhancement of the amplitude and temporal indices of the EPSP.

Analogous to the results reported by Wilson (1992), we find that these effects are accompanied by the changes in electrical properties of the cell membrane that appear to be responsible for the observed effects. The similarities in the I-V curves of  $K_{IR}$  channels in MS neurons and  $I_h$  channels in pyramidal neurons prompted us to the conjecture that the some of the effects due to  $I_h$  channels on pyramidal neuron biophysics, such as normalization of synaptic potentials at the soma, might be mirrored in MS neurons through  $K_{IR}$  channels. We find that  $K_{IR}$  conductance contribute to the normalization of synaptic potentials in NAc MS neurons. We discuss our findings in relation to MS neuron membrane biophysics as well as the neuron functioning with respect to synaptic input processing. Portions of this work have appeared in abstract form (John and Manchanda 2009).

## 2. Methods

In this study, data from published models (Wolf *et al.* 2005; Stephen and Manchanda 2009) were used to build a 189-compartment stylized model of the NAc MS neuron using the NEURON simulation platform (Carnevale and Hines 2006). The radially symmetric model included a soma and 4 proximal dendrites, each of which bifurcate twice to form 8 middle dendrites and 16 distal dendrites (figure 1A). Spatial discretization using the d-lambda rule (d-lambda value=0.15) resulted in a single compartment for the soma and each of the proximal and middle dendrites and 11 compartments for the long distal dendrites (figure 1B). Spines were not explicitly modelled but taken into account electrically by modifying the lengths and diameters of the dendrites, using published results, especially in the densely spine-laden middle and distal dendrites, to account for the additional membrane area attributable to the spines (Wolf *et al.* 2005). Being a radially symmetric model, the recordings in this study have been reported from one representative dendrite, responses in the other dendrites being identical.

The model incorporated all the 14 channels known to be present in these neurons. The parameters, except for the time constant of activation of  $K_{IR}$  channels, for modelling the different channels were taken directly from Wolf *et al.* (2005). These parameters were obtained from a recent computational study (Stephen and Manchanda 2009), in which the values were derived from rat neurons instead of the non-mammalian *aplysia* neurons as in Wolf *et al.* (2005). Hodgkin-Huxley formulations were used to model the sodium and potassium currents, the level of inactivation in each channel being adjusted using a variable whose value was set to match published data (Wolf *et al.* 2005). The reversal potentials of sodium and potassium channels were taken as +50 mV and -90 mV, respectively. The calcium ( $Ca^{2+}$ ) currents (N-, Q-, R- and T-types, as well as L-type  $Ca_v1.2$  and  $Ca_v1.3$ ) were modelled using the



**Figure 1.** The NAc MS neuron model. (A) Detailed view of the radially symmetric model developed in NEURON showing the soma and the different dendrites. (B) Compartmentalization of soma and the dendrites in a dendritic branch. Soma and each of the proximal (PD) and middle (MD) dendrites have only one compartment whereas each of the distal dendrites (DD) has 11 compartments (0, 1...10). L and D stand for length and diameter in  $\mu\text{m}$  respectively.

Goldman-Hodgkin-Katz (GHK) current equation because of the extremely low intracellular concentration of  $Ca^{2+}$ . The intracellular and extracellular concentrations of  $Ca^{2+}$  ions were 0.001 mM and 5 mM, respectively. The currents through the  $Ca^{2+}$  channels in the model contributed to two different intracellular pools of  $Ca^{2+}$ . One pool, to which N-, Q- and R-type  $Ca^{2+}$  channels contributed, controlled the  $Ca^{2+}$ -dependent  $K^+$  ( $K_{Ca}$ ) channels, whereas the second pool, to which the other  $Ca^{2+}$  channels (T- and L-types) contributed, was only used in the determination of  $[Ca^{2+}]_i$  and did not regulate the activity of other membrane channels directly. All the simulations were performed with the cell's operating temperature set to 35°C. Standard values of membrane capacitance ( $1 \mu\text{F}/\text{cm}^2$ ) and axial resistance ( $100 \Omega\text{-cm}$ ) were used. The leak conductance was modelled using the passive channel from NEURON's library with a maximum conductance,  $\hat{g}_{pas} = 11.5 \times 10^{-6} \text{ S}/\text{cm}^2$  and reversal potential,  $E_{rev} = -70 \text{ mV}$ .

EPSPs in NAc neurons have been found to be mediated by the activation of both *N*-methyl-D-aspartate (NMDA) and non-NMDA ( $\alpha$ -amino-3-hydroxy-5-methyl-4-isoxazole

propionic acid; AMPA) receptors (Uchimura *et al.* 1989b; Meredith and Totterdell 1999; Nicola *et al.* 2000; Taverna *et al.* 2004; Carlezon and Thomas 2009). Therefore, the EPSP in our model was generated by a co-localized NMDA-AMPA synapse, modelled using the published data (Wolf *et al.* 2005). The voltage-dependent  $Mg^{2+}$  block in NMDA conductance was taken into account while modelling the conductance. 10% of the NMDA and 0.5% of the AMPA currents contributed to  $Ca^{2+}$  influx in the pool with which  $K_{Ca}$  channels were not associated.

In the studies involving spatiotemporally distributed synaptic inputs, an array of excitatory and inhibitory synapses (a total of 168 synapses) were distributed as per the data obtained from Wolf *et al.* (2005). The excitatory synapses were glutamatergic (NMDA and AMPA) in nature with the reversal potentials set to 0 mV, whereas the inhibitory synapses were gamma amino butyric acid (GABA)-ergic in nature with a reversal potential of -60 mV. The excitatory synapses were placed on the dendrites only, 1 in each of the 4 primary dendrites, 2 in each of the 8 middle dendrites and 4 in each of the 16 distal dendrites. Out of the 84 GABA-ergic synapses, 16 were placed at the soma, 3 in each of the primary and middle dendrites and 2 in each of the distal dendrites. The procedure for applying temporally dispersed, random inputs to the spatially distributed synapses was adopted from literature (Stephen and Manchanda 2009). Each of the excitatory or inhibitory synapses received an independent, probabilistic spike train that was generated with NEURON using the following algorithm. Initially a spike train with a constant interspike interval (ISI) was generated at the required frequency (3 Hz for down-state and 7.5 Hz for up-state). Then, each spike in the train was shifted in time, the amount of shift randomly chosen from a Gaussian distribution with mean=0 and standard deviation 0.25 times the ISI. Finally, the whole of the resulting spike train was once again shifted in time randomly by a value between 0 and the ISI. This entire process was repeated for each of the 168 synapses so as to provide completely random inputs to the different synapses. The NMDA and AMPA conductances at a particular excitatory synapse received identical input trains. As the synaptic drive is modelled as a train of spikes randomized for the arrival time, we performed 30 trials for each study involving synaptic drive to calculate the mean and standard deviation of the data. We performed the Student's *t*-test (paired or independent, as appropriate) in order to statistically compare the relevant sets of data.

The model was validated using data obtained from the literature. For example, the membrane potential responses of the model to somatic current injections (both depolarizing and hyperpolarizing) were nearly identical to those obtained from the published computational model (figure 1D in Wolf *et al.* 2005). Comparison of the temporal characteristics of the EPSPs generated from our model showed similarities

with those recorded experimentally (Higashi *et al.* 1989; Pawlak and Kerr 2008). The amplitude of the EPSP in our model was found to be contributed mainly by the AMPARs, as observed experimentally in striatal MS neurons (Pawlak and Kerr 2008). For the synaptic drive case, as the inputs are probabilistic in nature, in order to achieve a robust comparison, we applied the synaptic input train used by Wolf *et al.* (2005) to our model and to the model of Wolf *et al.* (2005) obtained from ModelDB. We found that our model was able to replicate the responses of the Wolf *et al.* model, showing that the model operates identically as in Wolf *et al.* (2005). These similarities of the signals generated in our model with the experimental and computational responses of NAc MS neurons reported in the literature enabled us to place confidence in our model.

The simulations were initiated after a delay of 1000 ms to ensure that the cell had stabilized to a baseline resting potential from which the measurements could be made. In the simulations to study the influence of  $K_{IR}$  conductance on subthreshold down-state synaptic inputs (sections 3.2 and 3.3), the depolarization of the resting membrane potential (RMP) of the cell following the modulation of  $K_{IR}$  channel conductance was compensated to restore the RMP to its control level (-87.7 mV). This was done by injecting steady hyperpolarizing or depolarizing currents into each compartment of the model cell during the entire duration of the simulation depending on whether the cell was depolarized or hyperpolarized, respectively, following modulation of  $K_{IR}$  conductance. The membrane potential compensating currents were obtained from voltage clamp simulations performed to clamp the membrane potential in each compartment to  $\sim -87.7$  mV under resting conditions when the  $K_{IR}$  conductance in the model was varied. The parameters of the EPSP compared include its peak amplitude, half width, rise time and decay time. Half width was taken as the time between 50% of the amplitude in the rising and falling phases of the EPSP, rise time as the time taken to rise from 10% to 90% of the EPSP amplitude in the rising phase and decay time as the time taken to fall from 90% to 10% of the EPSP amplitude in the falling phase of the EPSP.

The active conductances were modified in the dendrites only, leaving the somatic conductances unchanged. This was done because the excitatory inputs to the MS neurons terminate at the numerous spines that are positioned on the dendrites of the neuron (Carter *et al.* 2007), while the somata being aspiny (Meredith *et al.* 1992; Meredith and Totterdell 1999) do not receive any significant amount of excitatory input (Meredith *et al.* 2008). Moreover, 94% of the dopaminergic inputs that are capable of modulating the active conductances and excitatory inputs in MS neurons (Nicola *et al.* 2000) contact the dendritic shafts and spines of the neuron (Smith and Bolam 1990; Meredith *et al.* 2008), making the

dendrites the primary target for modulation of ionic conductances in computational studies of this kind.

### 3. Results

#### 3.1 Effects of dendritic active conductances on EPSPs

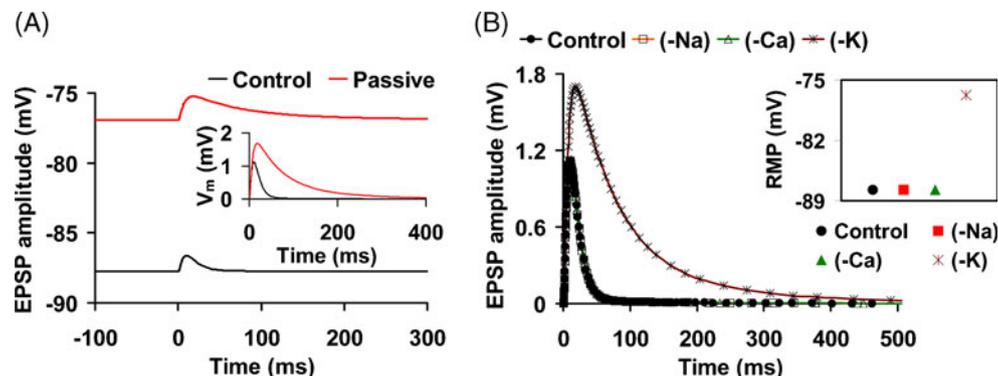
In order to investigate the effects of active conductances in shaping EPSPs, the EPSP was generated at the middle of the distal dendrite (DD5) and recorded at the soma (henceforth, 'EPSP'). The EPSP in the presence of all dendritic active conductances (henceforth, 'control') was compared with the EPSP in their absence (henceforth, 'passive model'). The results are shown in figure 2A (inset showing the EPSPs overlaid for ease of comparison). Blocking active conductances had two main effects: (i) depolarization of RMP of the cell and (ii) changes in EPSP amplitude and kinetics. The RMP of the cell ( $-87.7$  mV in the control) was depolarized to  $-76.9$  mV in the passive model (figure 2A). As seen in the inset, the absence of dendritic active conductances visibly altered EPSP parameters, its amplitude increasing by 50% and half width by 243%. Overall, thus, it appears that active conductances serve to hyperpolarize the cell membrane and to diminish the amplitude of EPSP while narrowing its time course.

In order to ascertain which set(s) of conductances present in MS neurons were mainly responsible for this modulation, the  $Na^+$ ,  $Ca^{2+}$  and  $K^+$  conductances were blocked serially in the control model (figure 2B). The broad finding was that blocking of  $Na^+$  and  $Ca^{2+}$  conductances (labelled '(-Na)' and '(-Ca)' respectively) had no effect on the RMP

(figure 2B inset) nor did they produce any appreciable changes in EPSP parameters (figure 2B). In contrast, the absence of dendritic  $K^+$  conductances (labelled '(-K)') depolarized the RMP of the cell to  $-76.8$  mV and affected the EPSP markedly, in the same direction as in the passive model. While the EPSP amplitude was boosted by nearly identical amounts as in the passive model (52%), the half width increased to a somewhat greater extent than in the passive model (266%). These observations indicate that  $K^+$  conductances are the key regulators of the RMP of the cell as well as the efficacy of excitatory synaptic inputs in NAc MS neurons.

By blocking the different dendritic  $K^+$  conductances individually, we next investigated whether some of the dendritic  $K^+$  conductances ( $K_A$ ,  $K_{IR}$  and  $K_{Ca}$ ) contribute more prominently than the others in determining the EPSP parameters. The results of these maneuvers, displayed in figure 3A–D, showed that the absence of  $K_{Ca}$  conductance (labelled '(-KCa)') had no appreciable effect on RMP (figure 3B) and EPSP amplitude and half width (figures 3C and D, respectively), and that the absence of  $K_A$  conductance (labelled '(-KA)') affected RMP and EPSP parameters only marginally (0.1 mV depolarization in RMP, 4% increase in EPSP amplitude and 1% increase in EPSP half width). In contrast, blockade of dendritic  $K_{IR}$  conductance (labelled '(-KIR)') depolarized the cell markedly (by 7.2 mV) and resulted in large percentage changes in EPSP parameters (amplitude augmented by 34% and half width by 118%). Thus, among the  $K^+$  conductances,  $K_{IR}$  appears to exert the dominant influence on RMP and on somatic EPSPs.

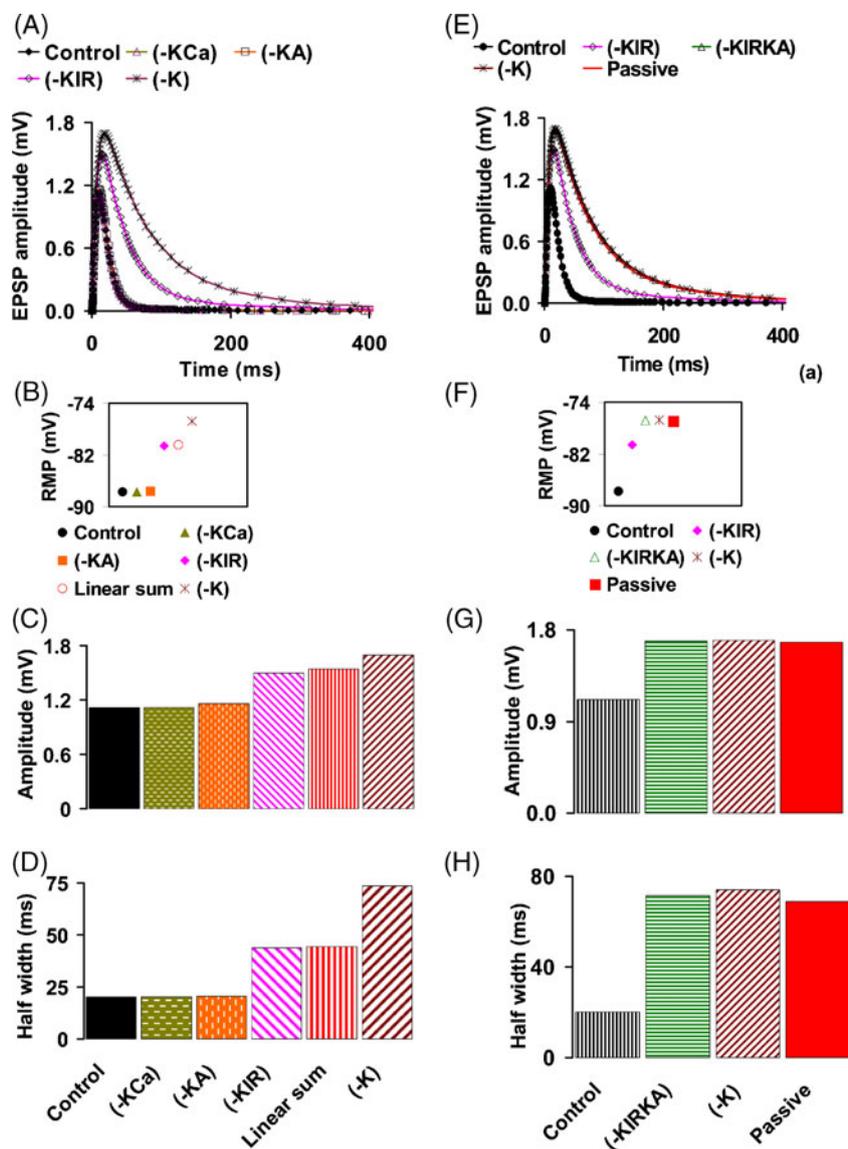
Although the  $K_{IR}$  conductance emerges as the principal determinant of EPSP indices, the changes induced by block



**Figure 2.** Active conductances, in particular  $K^+$  conductances, modulate RMP of the cell and also the amplitude and kinetics of somatic EPSPs. (A) EPSPs from the model with active and passive dendrites showing depolarization of RMP in the passive model (labelled 'Passive') compared to the control (labelled 'Control'). The inset shows the EPSPs overlaid for the ease of comparison of their parameters. EPSP amplitude and half width were augmented upon blocking the active conductances. (B) EPSPs on blocking  $Na^+$  [(-Na); unfilled squares]  $Ca^{2+}$  [(-Ca); unfilled triangles] and  $K^+$  conductances [(-K); asterisks] compared with the control (filled circles). The inset shows the RMP of the cell corresponding to the EPSPs in (B) showing depolarization of RMP upon blocking  $K^+$  conductances. The amplitude and half width of the EPSP were unaffected following the block of  $Na^+$  and  $Ca^{2+}$  conductances, but were augmented when  $K^+$  conductances were blocked in the model.

of  $K_{IR}$  were markedly lower than those induced by block of all  $K^+$  channels together (compare the bars with forward and backward slanting lines in figures 3C and D), which in turn

was similar to those in the passive model. Furthermore, the changes in EPSP parameters following block of all the  $K^+$  conductances together were different from the



**Figure 3.**  $K_{IR}$  conductance markedly affects the RMP and somatic EPSP parameters in the down-state of NAc MS neurons while  $K_A$  conductance contributes only secondarily to these changes when blocked along with  $K_{IR}$  conductance. (A) EPSPs on blocking individual  $K^+$  conductances. Blocking of the  $K_{Ca}$  (unfilled triangles) and  $K_A$  (unfilled squares) conductances individually did not produce any notable changes in the EPSP parameters, whereas blockade of  $K_{IR}$  conductance alone (unfilled diamonds) changed the RMP and EPSP parameters remarkably. (B) RMP of the cell corresponding to EPSPs in (A). EPSP amplitude (C) and half width (D) were enhanced upon blocking  $K_{IR}$  (bars with forward slanting lines) and remained more or less unchanged on blocking other  $K^+$  conductances individually (bars with horizontal and vertical dotted lines). Note that the linear sum of the changes in EPSP parameters due to block of  $K^+$  conductances individually (bars with vertical lines) was not equal to the changes observed when all the potassium conductances were blocked together (bars with backward slanting lines). (E) EPSPs when  $K_A$  and  $K_{IR}$  conductances are blocked simultaneously (unfilled triangles), upon blocking all  $K^+$  conductances (asterisks) and in passive model (plain line) compared with the control (filled circles) as well as  $K_{IR}$  blocked (unfilled diamonds) conditions. (F) RMP of the cell corresponding to EPSPs in (C). Upon simultaneous blocking of  $K_A$  and  $K_{IR}$  conductances (bars with horizontal lines) the EPSP amplitude (G) and half width (H) rose from the control (bars with vertical lines) and these changes were approximately equal to those when all  $K^+$  conductances were blocked simultaneously (bars with backward slanting lines) and also in passive model (filled bars).

linear sum of changes (labelled ‘Linear sum’) due to block of  $K^+$  conductances individually (compare the bars with backward slanting lines and vertical lines in figures 3C and D). It was, therefore, speculated that along with  $K_{IR}$  conductance, some other active conductance(s) might secondarily be playing a role in altering the EPSPs, ensuing from the primary changes induced by  $K_{IR}$ .

In order to investigate this idea, each of the different active conductances was blocked in the model in combination with  $K_{IR}$  conductance. In this case too, none of the  $Na^+$  and  $Ca^{2+}$  conductances nor the  $K_{Ca}$  conductance had any discernable influence on RMP and EPSP parameters (data not shown). However, as shown in figure 3E–H, when  $K_A$  and  $K_{IR}$  conductances were blocked simultaneously (labelled ‘(–KAKIR)’), the changes in the RMP (figure 3F) and EPSP parameters (figures 3G and H) were roughly equal to the changes resulting from simultaneous block of all the  $K^+$  conductances. This implies that even though the individual contribution of  $K_A$  channels to RMP and to EPSP indices is negligible,  $K_A$  conductance also influences these parameters in combination with  $K_{IR}$ . We analysed this situation and found that due to the depolarization in the RMP brought about primarily by the block of  $K_{IR}$  conductance, the cell is driven into the voltage range of activation of  $K_A$  channels, evoking an outward current that diminishes the amplitude and temporal characteristics of the EPSP. Blocking  $K_A$  channels along with  $K_{IR}$  raises the amplitude and time course of the EPSP and causes the depolarization of the RMP as well.

As observed above, depolarization induced by blocking of  $K_{IR}$  can entrain other active conductances (principally the  $K_A$ ) which secondarily affect the EPSPs. Because of the non-linear interactions between the several active channels present in the model, there could conceivably be secondary effects on the EPSPs such as those mediated by  $K_A$  channels, as indicated by figure 3E–H. Therefore, in order to isolate the effects of  $K_{IR}$  and minimize as far as possible the effects of other conductances, we restored the membrane potential to the resting level (–87.7 mV) by injecting suitable hyperpolarizing or depolarizing currents into the model. Such protocols have previously been adopted in studies aimed at isolating the effects of a single conductance out of the many present in a neuron (e.g. Magee (1998) for the case of the  $I_h$  conductance known to regulate the resting potential and influence EPSP parameters in hippocampal pyramidal neurons). The EPSPs in three conditions – (i) control, (ii) RMP unrestored and (iii) RMP restored conditions – were recorded and are shown in figure 4A. We found that the direction of changes in EPSP parameters (amplitude, half width, rise time and decay time) was similar in both RMP unrestored and restored conditions, but the extent of changes was enhanced when RMP was restored (figure 4B–E). We found that this is due to the reduction in the activation of outward  $K_A$  currents when the

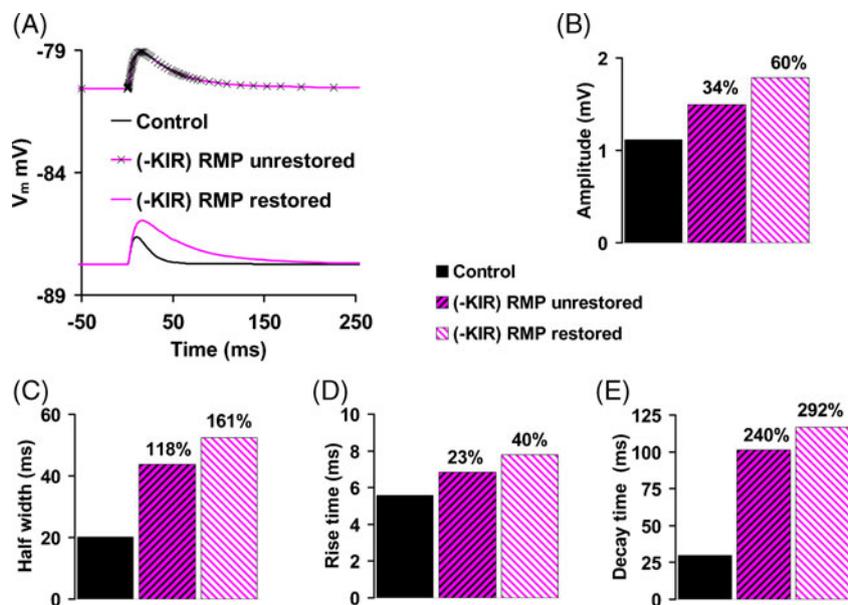
membrane potential was restored. The percentage increases in the different EPSP parameters from the control under RMP unrestored and restored conditions are provided in figure 4B–E. The figures also show that the enhancement in the half width of the EPSP from the control upon blocking of  $K_{IR}$  is mainly due to the enhancement in decay time (292% under RMP restored conditions), the increase in rise time being comparatively minor (40% under RMP restored conditions).

Earlier studies (Wilson 1992, 1993) suggest that while the  $K_{IR}$  conductance is a major determinant of the membrane potential and EPSP parameters in the down-state, in the up-state of the neuron, the  $K_A$  conductance, in particular  $K_{As}$ , might play a bigger part in shaping EPSPs (Nisenbaum *et al.* 1994, Mahon *et al.* 2000a, b). Therefore, we investigated the role played by the  $K_{As}$  conductance by measuring its effects on EPSPs generated at depolarized potentials akin to physiological up-state potentials ( $\sim -65$  mV, obtained by injecting depolarizing currents). Table 1 shows the percentage increase in the EPSP amplitude and half width when  $K_{IR}$  and  $K_{As}$  conductances were blocked individually in the resting (–87.7 mV) and at depolarized membrane potential (–65 mV). As is evident from table 1, in the down-state, the EPSP amplitude and half width increased by 64% and 160%, respectively, when  $K_{IR}$  was blocked, whereas the blocking of  $K_{As}$  had no effect on EPSP amplitude and produced only a 5% rise in the EPSP half width. However, when the membrane potential was depolarized to –65 mV, the contribution from  $K_{As}$  conductance was markedly boosted, EPSP amplitude increasing by 24% and half width by 191% when  $K_{As}$  conductance was blocked. In contrast, the blocking of  $K_{IR}$  increased the amplitude only by 7% and decreased half width by 26%. Thus, we find that while the  $K_{IR}$  conductance is the major determinant of membrane potential and EPSP parameters in the down-state, in the up-state, the  $K_{As}$  conductance plays a more prominent role in shaping the EPSPs.

The salient observations arising from a consideration of the above data are (i) that  $K_{IR}$  conductance in NAc MS neurons primarily, and significantly, influences the shaping of somatic EPSPs in the down-state and (ii) that progressive depolarization of the membrane potential could result in increasing influence of  $K_A$  conductance in shaping the somatic EPSPs. In the following section, we investigate the modulation of subthreshold synaptic inputs by the  $K_{IR}$  conductance in detail.

### 3.2 Effects of modulation of $K_{IR}$ conductance on EPSP properties

Physiologically, the conductance of  $K_{IR}$  channels is likely to be modulated by external factors such as dopamine, a major neurotransmitter carrying information about reward



**Figure 4.** Restoration of RMP during blocking of  $K_{IR}$  conductance further enhanced the EPSP parameters. (A) EPSPs in the control, RMP unrestored and RMP restored conditions. Blocking of  $K_{IR}$  conductance depolarized the membrane potential by 7.2 mV (light line with crosses) compared to the control (dark line). The direction of changes in EPSP parameters were preserved upon restoration of RMP. The changes in EPSP amplitude (B), half width (C), rise time (D) and decay time (E) upon blocking  $K_{IR}$  conductance under RMP unrestored conditions (bars with backward slanting lines) in the model compared to the control (filled bars) was enhanced further upon restoration of the RMP (bars with forward slanting lines).

conditions to the NAc (Uchimura *et al.* 1989a; Moyer *et al.* 2007). Therefore, we investigated the effects of varying the maximum conductance of  $K_{IR}$  channels ( $g_{max}(K_{IR})$ ) on somatic EPSP parameters as well as the probable mechanisms underlying these effects. Figure 5A shows the EPSPs generated from our model for different levels of  $g_{max}(K_{IR})$  under RMP unrestored conditions, while the inset shows the amplitude of the EPSPs after restoration of RMP. Figure 5A, as expected, shows that reduction in  $g_{max}(K_{IR})$  resulted in progressive depolarization of the RMP. As shown in the inset, reduction in  $g_{max}(K_{IR})$  enhanced the amplitude and temporal characteristics of the EPSP (also see Table 2). The simulations reported in the next three sections (3.3 to 3.5) were again done after restoring the

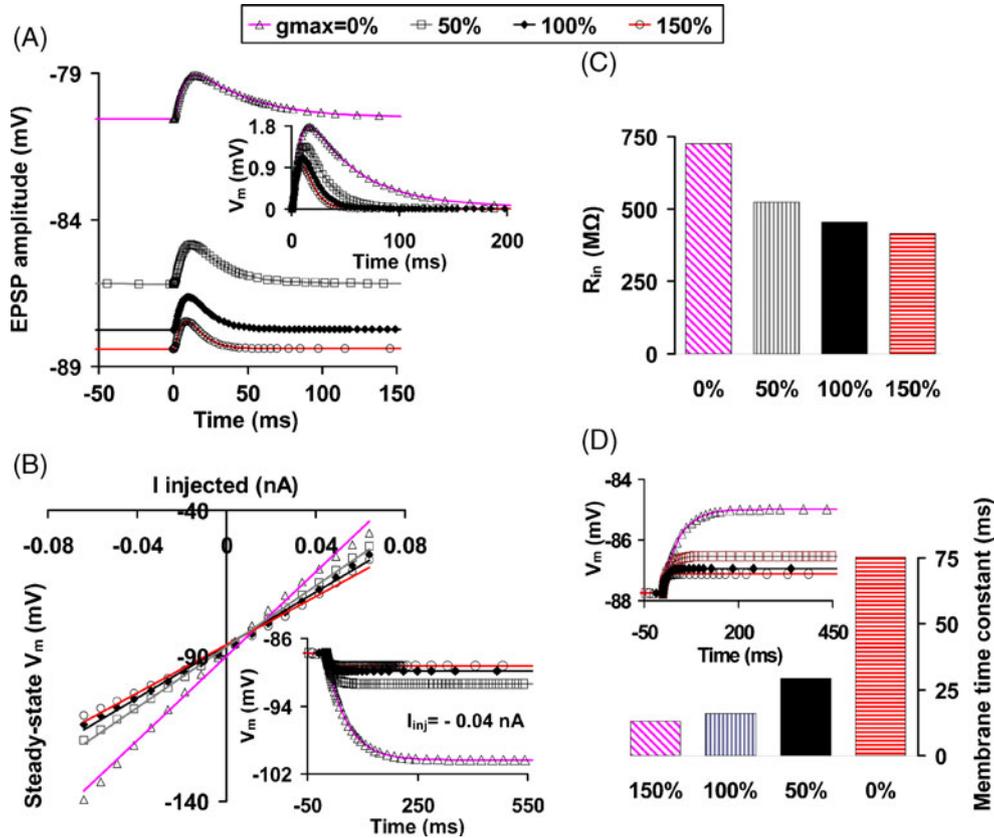
**Table 1.** Percentage increases in EPSP amplitude and half width at down-state ( $-87.7$  mV) and up-state ( $-65$  mV) membrane potentials when  $K_{IR}$  and  $K_{As}$  are blocked individually

V <sub>m</sub> (mV)	EPSP amplitude (mV)		EPSP half width (ms)	
	(-K <sub>IR</sub> )	(-K <sub>As</sub> )	(-K <sub>IR</sub> )	(-K <sub>As</sub> )
-87.7	64	0	160	5
-65	7	24	-26	191

RMP to isolate the effects due to  $K_{IR}$  conductance (see the section on methods).

### 3.3 Effects of modulation of $K_{IR}$ conductance on electrical properties of the cell membrane

The changes in EPSP parameters observed here could be attributed to the changes in the electrical properties of the cell membrane following the modulation of  $K_{IR}$  conductance. For instance, suppression of  $K_{IR}$  conductance is expected to lead to a rise in both the input resistance ( $R_{in}$ ) of the cell and its effective membrane time constant [ $\tau_m$ ; we have used the descriptor ‘effective’ here because of the presence of voltage gated channels in the dendrites (Koch *et al.* 1996), which endow an active component to electrical responses of the membrane even in the subthreshold region]. In order to analyse the mechanisms underlying the changes in EPSP parameters, we measured  $R_{in}$  and  $\tau_m$ .  $R_{in}$  was obtained from the slope of the I-V curve of the cell at different levels of  $g_{max}(K_{IR})$ . In order to plot the I-V curves, step currents were injected into the cell at the distal dendritic location (DD5). The currents injected ranged from  $-0.064$  to  $+0.064$  nA in 17 equal steps for a duration of 1500 ms (inset of figure 5B shows the response of the model to step current injection of  $-0.04$  nA under different  $g_{max}(K_{IR})$  conditions). The low amplitudes of



**Figure 5.** Changes in  $K_{IR}$  conductance modulate somatic EPSPs and electrical properties of the cell membrane. **(A)** EPSPs from our model under different levels of  $g_{max}(K_{IR})$  showing depolarization of RMP under reduced  $g_{max}(K_{IR})$  conditions. Inset shows the EPSPs under RMP restored conditions illustrating that their amplitude and time course enhanced with reduction in  $g_{max}(K_{IR})$ . **(B)** Plots of I-V curves from the model under different levels of  $g_{max}(K_{IR})$  fitted with best-fit straight lines to measure  $R_{in}$ , the slope of the I-V curves. The inset shows the response of the model to a hyperpolarizing current injection ( $-0.04$  nA for 1500 ms), both current injection and recording at DD5. **(C)** Reduction in  $g_{max}(K_{IR})$  raised the input resistance of the cell. **(D)** Effective  $\tau_m$  rose with reduction in  $K_{IR}$  conductance. The inset shows the somatic response of the model to a depolarizing somatic current injection ( $0.01$  nA for 1500 ms) under different levels of  $g_{max}(K_{IR})$ .

**Table 2.** Summary of the values of RMP, parameters of the somatic EPSP and membrane properties for different levels of  $g_{max}(K_{IR})$

Parameters	$g_{max}(K_{IR})=0\%$	$g_{max}(K_{IR})=50\%$	$g_{max}(K_{IR})=100\%$	$g_{max}(K_{IR})=150\%$
RMP (mV)	-80.56	-86.19	-87.74	-88.4
Amplitude (mV)	1.79	1.36	1.12	0.95
Half width (ms)	52.4	28.4	20.1	18.3
Rise time (ms)	7.8	6.1	5.6	4.9
Decay time (ms)	116.8	45.2	29.8	23.7
$R_{in}$ ( $M\Omega$ )	725	523	455	414
$\tau_m$ (ms)	75.2	29.3	16.1	13.1
Half attenuation distance ( $\mu m$ )	DD10	245	205	190
	DD5	160	127	118

the currents ensured that the changes in membrane potential were confined to ranges of linear behaviour. For each value of the current injected, the steady-state membrane potentials were recorded at the site of current injection and the data thus obtained were plotted and fitted with best-fit straight lines (figure 5B).

As shown in figure 5C,  $R_{in}$  varied inversely with  $g_{max}(K_{IR})$ . Under control conditions  $R_{in}$  was 455 M $\Omega$  ( $R^2=0.99$ , the high value of  $R^2$  indicating that the cell membrane was passive and operating in the linear range) and rose to 725 M $\Omega$  ( $R^2=0.99$ ) in the absence of  $K_{IR}$  currents (also see table 2). This elevated  $R_{in}$  may underlie the enhancement of EPSP amplitude following the reduction in  $K_{IR}$  conductance.  $\tau_m$  was evaluated as the time taken to reach 84% of the steady-state somatic response of the model (inset of figure 5D) to a sufficiently long-duration step current injection at the soma (0.01 nA for 1500 ms). The index 84% was taken from the standard definition of membrane time constant at the point of current injection (in an infinite cable) as predicted by the solution of the cable equation (Johnston and Wu 1995).  $\tau_m$  also showed inverse relation with  $g_{max}(K_{IR})$ , absence of  $K_{IR}$  current resulting in  $\tau_m$  nearly 4.7-fold higher than the control (figure 5D; also see table 2). The augmentation of  $\tau_m$  appears to cause the slow rise and fall of the EPSP under reduced  $g_{max}(K_{IR})$  conditions.

### 3.4 Effects of modulation of $K_{IR}$ conductance on EPSP propagation and spatial electrical properties of the cell membrane

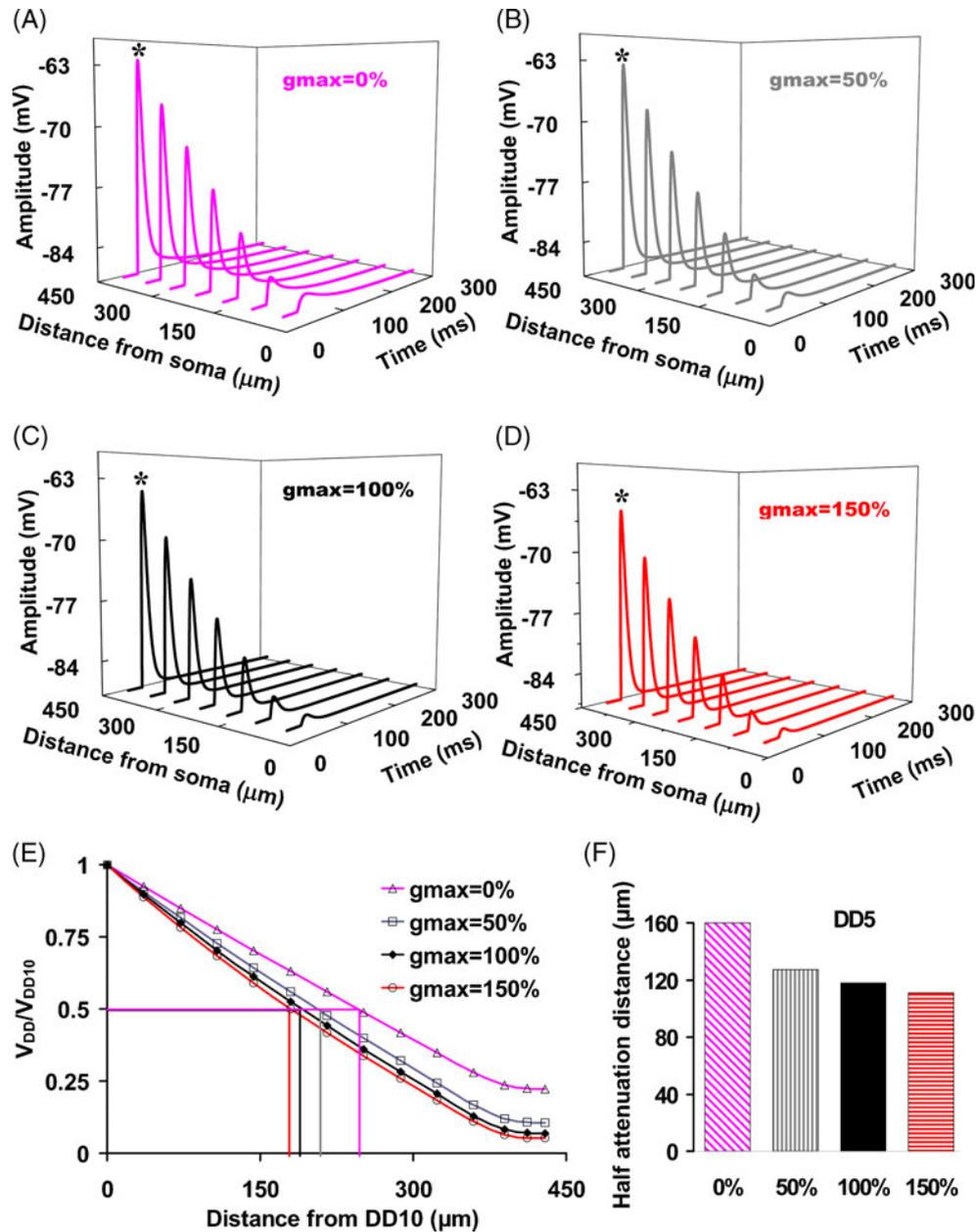
Figures 6A–D show the EPSPs generated at the distal end of the distal dendrite (DD10) and recorded at different locations along the length of the dendrite. We found that the amplitude of the local EPSP increases with reduction in  $g_{max}(K_{IR})$ . Additionally, for all levels of  $g_{max}(K_{IR})$ , the majority of the reduction in amplitude of the EPSP occurs in the distal dendrite (~90% at DD0) and only about 5–6% of the reduction occurs in its further propagation towards the soma. The enhancement in membrane resistance upon reduction of  $K_{IR}$  conductance might result in differences in the spatial electrical properties of the membrane. One such possibility is a change in the rate of voltage attenuation along the length of dendrite. This possibility was tested by injecting a sufficiently long-duration step current (0.01 nA for 1500 ms) at the tip of the distal dendrite (DD10). As a measure of spatial spread, we used the index of steady-state voltage attenuation, obtained by plotting the steady-state voltage reached in each dendritic location as a function of distance from the soma. In figure 6E, the steady-state voltage at each location is shown normalized with respect to that at the current injection site for different levels of  $g_{max}(K_{IR})$ . The half-attenuation distance, which is the

distance at which the voltage attenuation is 50%, varied inversely with  $g_{max}(K_{IR})$ , being 190  $\mu$ m under control conditions and rising to 245  $\mu$ m in the absence of  $K_{IR}$  conductance (indicated by lines in figure 6E and also table 2). Changing the site of current injection from DD10 to DD5 in order to reduce end effects (e.g. current reflection from the electrically sealed tip of the dendrite) also showed similar results (half-attenuation distance rising from 118  $\mu$ m in the control to 160  $\mu$ m under  $K_{IR}$  blocked conditions; figure 6F; also table 2).

Thus, we found that modulation of the amplitude and kinetics of subthreshold somatic EPSPs by the  $K_{IR}$  conductance were accompanied by the modulation of electrical properties of the cell membrane such as  $R_{in}$  and  $\tau_m$  and also the changes in the spatial electrical properties of the neuronal membrane, effects that are consistent with the electrotonic expansion of the dendrite earlier investigated (Wilson 1995).

### 3.5 Effect of $K_{IR}$ conductance on normalization of synaptic inputs at the soma

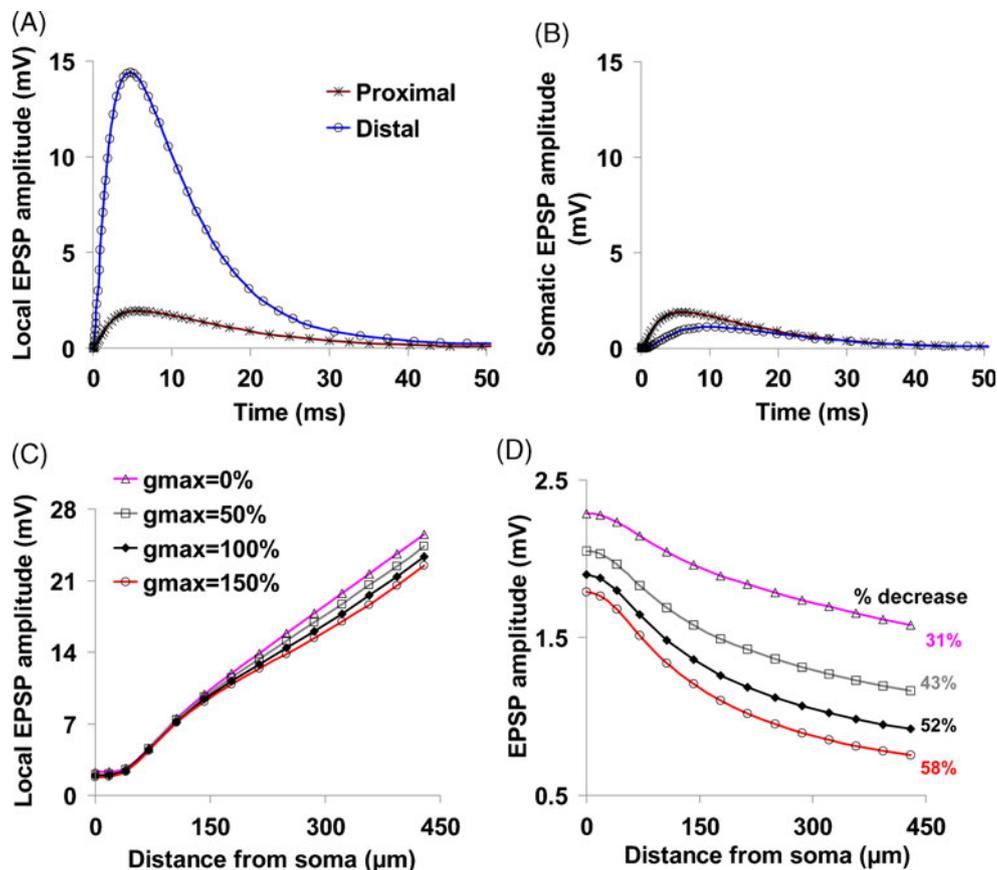
It has been found that in central neurons dendritic voltage-gated ion channels serve to counter the passive filtering of EPSPs as they propagate towards the soma, thereby assisting in the normalization of these inputs at the soma irrespective of the site of their generation (Magee and Cook 2000; Williams and Stuart 2003). We explored if EPSPs under control conditions undergo normalization in MS neurons. As  $K_{IR}$  is a major conductance affecting the EPSPs in the down-state of the neuron, we also investigated whether  $K_{IR}$  contributes to this normalization. Figures 7A and B show the local dendritic EPSPs and propagated somatic EPSPs, respectively, generated at distal (DD5; light trace with unfilled circles) and proximal (PD; dark trace with asterisks) dendritic locations. The local dendritic EPSP at the distal location was found to be 7.4 times larger than that at the proximal location, whereas somatic EPSPs propagated from distal and proximal locations were relatively similar in amplitude (with EPSP from proximal location being only 0.7 times larger than that from the distal location). The amplitude of the local dendritic EPSPs for different values of  $g_{max}(K_{IR})$  was plotted along the length of the dendrite (figure 7C). We find that, in the control conditions (filled diamonds), the amplitude of the local dendritic EPSP from distal location (DD10) increases more than 11-fold compared to that from the proximal location (PD). However, when these EPSPs are recorded at the soma (figure 7D), they show relatively similar amplitudes, only a 52% reduction in amplitude when the location of EPSP generation is moved from the proximal to the distal location. Furthermore, figure 7D shows that the extent of normalization was dependent on  $K_{IR}$  density, progressive reduction in  $g_{max}(K_{IR})$  leading to a progressive enhancement of amplitude



**Figure 6.**  $K_{IR}$  conductance modulates local EPSPs and the spatial electrical properties of the cell membrane. (A–D) EPSPs generated at DD10 (indicated by asterisks) and recorded at different distances (DD10, DD8, DD6, DD4, DD2, DD0 and soma). See text for details. (E) The steady-state voltage at each location along the dendrite normalized to that at the site of current injection (DD10) plotted as a function of distance from the soma under different levels of  $g_{max}(K_{IR})$ . (F) Half-attenuation distance varied inversely with  $K_{IR}$  conductance when the site of current injection was at DD10 (marked using lines in (E)) and at DD5 (F) as well.

normalization at the soma. The percentage decrease in amplitude of propagated somatic EPSP from the distal location (DD10) compared with that from the proximal location (PD) was 31% with  $K_{IR}$  conductance blocked and it rose to 58% for  $g_{max}(K_{IR})$  set to 150%. This enhancement in the extent of amplitude normalization with reduction in  $g_{max}(K_{IR})$  could be

attributed to the increase in the amplitude of the local dendritic EPSPs at the distal locations when  $g_{max}(K_{IR})$  is reduced. These simulations show that normalization of EPSP amplitude at the soma does take place to a significant degree in our NAc MS neuron model, the extent of normalization being dependent on the level of  $K_{IR}$  conductance.



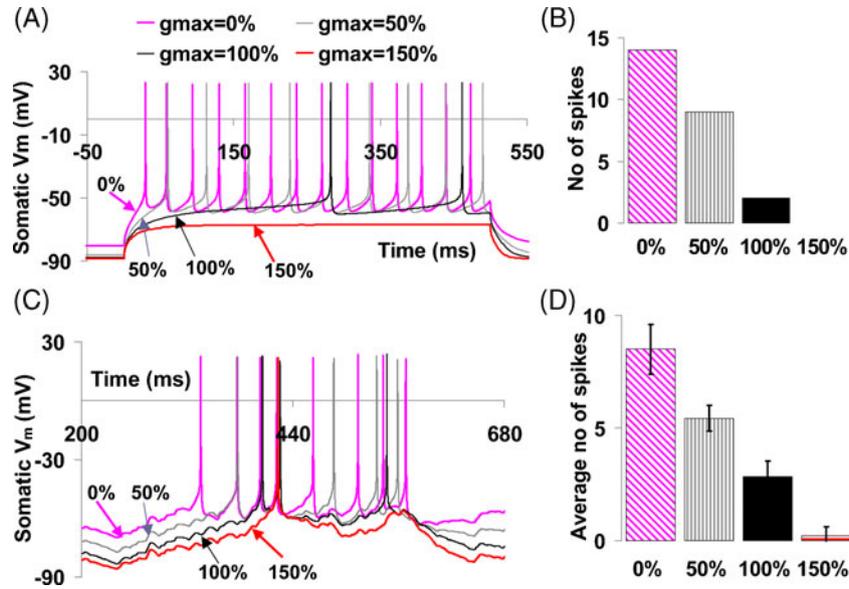
**Figure 7.**  $K_{IR}$  conductance contributes to normalization of amplitude of synaptic inputs at the soma. Local dendritic EPSPs (A) and propagated somatic EPSPs (B) generated at a proximal (PD; asterisks) and distal (DD5; unfilled circles) dendritic locations. Note the large amplitude changes in the local dendritic EPSPs from the two locations at different distances from the soma and similar amplitude of the propagated EPSPs at the soma. Peak amplitude of the local dendritic (C) and propagated somatic (D) EPSPs plotted against the distance from the soma for different levels of  $g_{max}(K_{IR})$ . Reduction in  $g_{max}(K_{IR})$  enhanced the amplitude of the local EPSPs at the distal dendritic locations while it also enhanced the extent of normalization of amplitude of synaptic inputs at the soma.

### 3.6 Effects of modulation of $K_{IR}$ conductance on cell excitability

The studies presented so far suggest that  $K_{IR}$  conductance affects the amplitude and time course of EPSPs in such a way that more effective summation should occur when  $g_{max}(K_{IR})$  is reduced. This, in turn, should lead to an increase in the excitability of the cell. To test this prediction, we need to allow the membrane potential to change beyond the limited window of  $V_m$  close to the hyperpolarized down-state potential explored above. Therefore, we next carried out studies in the absence of compensating current injection, allowing membrane potential to depolarize following the block of  $K_{IR}$ . We investigated, for different values of  $g_{max}(K_{IR})$ , the spiking behaviour of the cell following two kinds of stimulation: (i) injection of rectangular pulses of current at the soma and (ii) spatiotemporally distributed synaptic drive mimicking the physiological inputs.

In current injection studies a rectangular current pulse of amplitude 0.25 nA for 500 ms, which elicits two spikes in control conditions was injected into the soma of the model cell. As shown in figure 8A, when the conductance of the  $K_{IR}$  channel was elevated ( $g_{max}(K_{IR})=150\%$ ), the cell produced no spike, whereas the same current produced progressively increasing number of spikes when  $g_{max}(K_{IR})$  was reduced. Figure 8B summarizes this data showing that number of spikes increased with reduction in  $g_{max}(K_{IR})$ . Table 3 shows that the latency to the first spike increased with  $g_{max}(K_{IR})$ , thus indicating that  $K_{IR}$  conductance acts to increase the duration of the depolarizing ramp before firing the action potential, as also suggested by previous computational studies (Moyer *et al.* 2007; Steephen and Manchanda 2009).

Spatiotemporally distributed synaptic inputs at a mean frequency of 3 Hz per synapse for the down-state and 7.5 Hz per synapse for driving the cell to up-state as



**Figure 8.** Cell spiking enhances with reduction in  $K_{IR}$  conductance. (A) Response of the model to step current injections of 0.25 nA for 500 ms at the soma for different levels of  $g_{max}(K_{IR})$ . (B) Bar graph showing reduction in the number of spikes when  $g_{max}(K_{IR})$  is raised. (C) Response of the model to spatiotemporally distributed synaptic inputs of frequency 3 Hz in the down-state and 7.5 Hz to drive the cell to up-state for different values of  $g_{max}(K_{IR})$ . Note the depolarization in the down-state potential of the cell with decrease in  $g_{max}(K_{IR})$ . (D) The average number of spikes varies inversely with  $g_{max}(K_{IR})$ . Mean number of spikes for each  $g_{max}(K_{IR})$  value shown (0%, 50%, 100% and 150%) was significantly higher ( $P < 0.001$ ) than the next.

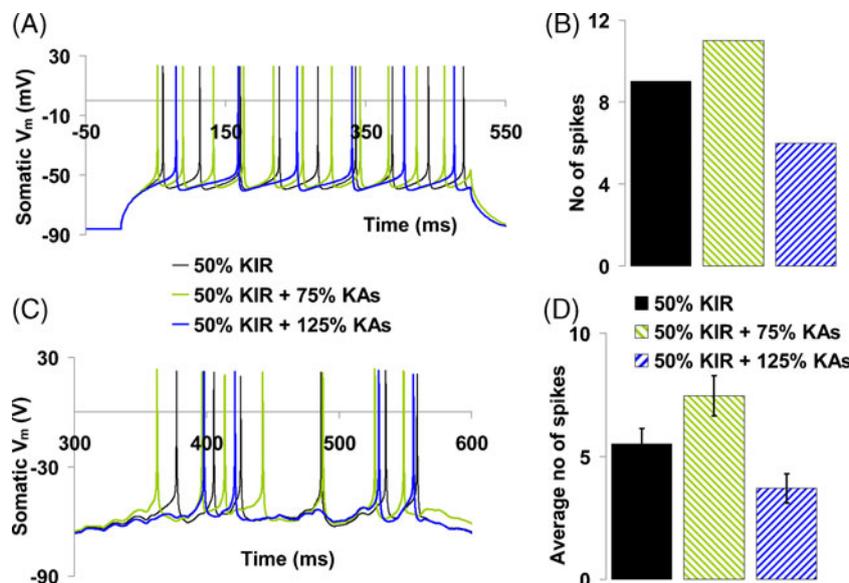
described in Steephen and Manchanda (2009) were applied to the model for different values of  $g_{max}(K_{IR})$ . The responses are shown in figure 8C. Note that the mean down-state potential in control conditions ( $-80$  mV) is  $\sim 7$  mV depolarized compared with the RMP without synaptic input ( $-87.7$  mV), essentially because of the net excitatory drive. As  $K_{IR}$  conductance was reduced, the down-state potential was further depolarized, whereas enhancement of  $K_{IR}$  conductance (to 150% of control) hyperpolarized the membrane potential by 3 mV. Moreover, cell excitability was enhanced with progressively greater number of spikes being generated as  $g_{max}(K_{IR})$  was progressively reduced. Figure 8D shows the average number of spikes (30 trials) for different levels of  $g_{max}(K_{IR})$ . We found that the average number of spikes increased with reduction in  $g_{max}(K_{IR})$  and the difference in means were statistically significant (paired  $t$  test;  $P < 0.001$ ). Table 3 shows that, as in the case of current injection study, the onset time for the first spike increased with  $g_{max}(K_{IR})$ . For the reduced  $g_{max}(K_{IR})$  and control conditions, the model generated spikes and the differences in means of the onset time of the first spike were found to be statistically significant using the paired  $t$ -test ( $P < 0.001$ ). However, in the case of enhanced  $g_{max}(K_{IR})$ , where the cell generated spikes very rarely, we performed independent  $t$ -tests to compare the differences in means and these were again found to be significantly different ( $P < 0.001$ ).

### 3.7 Effects of modulation of $K_{As}$ conductance in relation to $K_{IR}$ on cell excitability

In order to study the role of  $K_{As}$  in relation to  $K_{IR}$  in determining the spiking behaviour of the neuron in the up-state, we performed both current injection as well as synaptic input simulations after allowing the membrane to depolarize in response to a reduction in  $K_{IR}$  conductance. We chose a level of  $g_{max}(K_{IR})$  (50% of control) that depolarized the membrane by a moderate amount and evoked a significant level of spiking in response to either current injection (9 spikes for a somatic current injection of 0.25 nA for 500 ms) or increase in synaptic drive (6 spikes). In the current injection study, reduction of  $g_{max}(K_{IR})$  to 50% of its control level depolarized the resting membrane from  $-87.7$  mV to  $\sim -86$  mV. The

**Table 3.** Changes in onset time of the first spike with  $g_{max}(K_{IR})$

$g_{max}(K_{IR})$	Onset time of first spike (ms)	
	Current injection	Synaptic input (30 trials)
0%	29	$33 \pm 13$
50%	60	$70 \pm 27$
100%	282	$128 \pm 47$
150%	–	$237 \pm 50$



**Figure 9.**  $K_{AS}$  conductance also contributes to the increase in spiking behaviour of MS neurons. (A) Response of the model to current injection of 0.25 nA for 500 ms at the soma under conditions of concomitant changes in  $K_{IR}$  and  $K_{AS}$  conductances, when the  $K_{IR}$  conductance is reduced to 50% (thin black trace), when the  $K_{AS}$  conductance is additionally reduced to 75% (thick green trace) and to 125% (thick blue trace). (B) Bar graph showing the number of spikes generated when the  $K_{IR}$  conductance is reduced to 50% (filled bars) when the  $K_{AS}$  conductance is additionally reduced to 75% (forward slanting lines) and increased to 125% (backward slanting lines). (C) Response of the model to spatiotemporally distributed synaptic inputs under conditions described in (A). (D) Bar graph showing the number of spikes generated under the same conditions as in (B).

response for this level of  $g_{max}(K_{IR})$  is shown in figure 9A (thin black trace). Keeping  $g_{max}(K_{IR})$  at 50% we either increased or decreased the  $K_{AS}$  conductance to 75% and 125% of its control value and measured the corresponding responses. These are indicated respectively by the thick green and blue traces in figure 9A. Figure 9B shows the bar graph for the number of spikes when the  $K_{IR}$  conductance was reduced to 50% (filled bars) when the conductance of  $K_{AS}$  was additionally reduced to 75% (forward slanting lines) and when  $K_{AS}$  conductance is additionally increased to 125% (backward slanting lines). As is evident from figures 9A and B, suppression of the  $K_{AS}$  conductance resulted in a marked increase in the spiking frequency while elevation of  $K_{AS}$  had the opposite effect. A drop in  $K_{AS}$  conductance also elicited a reduction in the latency to the first spike, as demonstrated by the data in table 4.

In the case of synaptic drive, reducing  $g_{max}(K_{IR})$  to 50% depolarized membrane to  $-74$  mV at the basal level of spatiotemporally distributed synaptic activation (3 Hz, giving rise to the noisy down-state under synaptic drive visible in figure 9C). Figure 9C shows the spiking behaviour of the neuron for the following conditions:  $g_{max}(K_{IR})=50\%$  (thin black trace),  $K_{AS}$  conductance additionally reduced to 75% (thick green trace) and  $K_{AS}$  conductance additionally increased to 125% (thick blue trace). Figure 9D shows the bar graph for the number of spikes in each of these cases.

These figures indicate that, as in current injection study, reduction of  $K_{AS}$  conductance markedly increased the spiking frequency and reduced the latency to the first spike (table 4), while elevation of  $K_{AS}$  had the opposite effects. Each of these effects was statistically significant (paired  $t$ -test;  $P < 0.001$ ). Reduction or enhancement of  $K_{AS}$  conductance to different degrees resulted in effects in the expected direction and proportional to the extent of block or enhancement of the conductance. Taken together, these findings indicate that, unlike in the down-state, where  $K_{IR}$  is the primary controller of electrical behaviour of the neuron, at depolarized levels of membrane potential both  $K_{IR}$  and  $K_{AS}$  conductances affect the neuronal excitability to substantial degrees.

**Table 4.** Influence of varying  $K_{AS}$  conductance along with 50%  $g_{max}(K_{IR})$  on onset time of the first spike

$g_{max}(K_{AS})$	Onset time of first spike (ms)	
	Current injection	Synaptic input (30 trials)
100%	60	72±27
75%	52	53±16
125%	79	91±38

#### 4. Discussion

In this study we have shown that, first, dendritic active conductances are strong modulators of subthreshold excitatory synaptic inputs in NAc MS neurons and, second, among the conductances present in the neuron,  $K_{IR}$  conductance is the primary determinant of the RMP and somatic EPSPs in the down-state. The excitatory effects evoked in the cell following the reduction in  $K_{IR}$  conductance were accompanied by an increase in  $R_{in}$  and  $\tau_m$  as well as spatial electrical properties such as the half attenuation distance. Owing to the depolarization of the RMP evoked by the blockade of  $K_{IR}$ , the  $K_A$  conductance also affected the EPSPs secondarily. Our results suggest that  $K_{IR}$  and  $K_{As}$  channels in NAc MS neurons influence the modulation of temporal integration as well as the firing properties of the neuron, the membrane potential of their operation being different.

It may be noted that although the effects of  $K_{IR}$  and  $K_{As}$  in determining the membrane electrical properties in MS neurons have been investigated earlier, our findings extend previous studies in the field in several ways: (i) Computational studies done previously in striatal MS neuron investigating the role of  $K_{IR}$  channels in the modulation of membrane electrical properties (Wilson 1992,1993) used a reduced biophysical model of the neuron in which the only conductances present were the  $K_{IR}$  and leak conductances. While these studies demonstrated a marked effect of the  $K_{IR}$  conductance on generation and propagation of synaptic potentials, the question remained as to whether these effects would also occur in a physiologically more realistic model of an MS neuron equipped with its wide array of voltage-dependent active channels. The presence of a large number of nonlinear conductances makes it difficult to predict such effects analytically, and complex interactions between these mechanisms can sometimes lead to counter-intuitive outcomes (Williams and Stuart 2003; Samuelsson and Kotaleski 2007; Steephen and Manchanda 2009). We, therefore, used a biophysically detailed model of the NAc MS neuron, which has recently become available (Wolf *et al.* 2005), incorporating all the 14 active conductances known to be present in these neurons, to investigate the effects of these active conductances in modulating the subthreshold down-state synaptic inputs as well as excitability in the up-state. In a related context, the outcomes of our study are closer to the physiological situation also because we have used more realistic models of NMDA-AMPA synapses for the generation of EPSP rather than the generalized alpha synapse. (ii) Previous computational studies on the subject (Wilson 1992, 1993) excluded other active conductances from the model in order to isolate the effects due to  $K_{IR}$ . However, in our model we have taken a different approach, i.e. while we included all the known active

conductances, we isolated the effects due to  $K_{IR}$  by restoring the RMP electrically to its resting value ( $\sim -87.7$  mV), a maneuver that would ensure primarily the activation of  $K_{IR}$  conductance. Restoration of RMP in order to selectively study the effects of a single conductance, e.g. due to  $I_h$  currents in hippocampal pyramidal neurons, has been employed in previous studies also (Magee 1998). (iii) We have investigated the effects of the  $K_{IR}$  conductance on normalization of synaptic potentials as well as on the spiking behaviour of the neuron through current injection and synaptic input studies, effects that have not previously been explored. (iv) Finally, as the  $K_{As}$  conductance is suspected to play a major role in the up-state of the neuron, we investigated the role of  $K_{As}$  in relation to  $K_{IR}$  in modulating up-state EPSPs as well as spiking behaviour of the cell. We discuss below (i) the influence of  $K_{IR}$  and  $K_{As}$  channels on MS neuron membrane biophysics and (ii) the implications for MS neuron functioning in the context of synaptic input processing.

##### 4.1 Influence of $K_{IR}$ and $K_{As}$ on MS neuron membrane biophysics

$K_{IR}$  channels present in NAc MS neurons have been suggested to be crucial determinants of resting potential of the cell (Uchimura *et al.* 1989a; Uchimura and North 1990; Mermelstein *et al.* 1998). In other cell types such as cardiac cells and skeletal muscle cells, these channels provide large inward currents at membrane potentials more negative than the reversal potential of  $K^+$  ( $E_K = -90$  mV), thus preventing excessive hyperpolarization of the resting potential caused by the electrogenic  $Na^+$  pump. Additionally, in the event of small depolarizations they provide small outward currents, thus stabilizing the resting potential of the neuron at a hyperpolarized potential near to  $E_K$  (Kubo *et al.* 1993; Hille 2001). Depolarization of RMP following the reduction of  $K_{IR}$  conductance has been suggested to occur in NAc MS neurons (Uchimura *et al.* 1989a; Perez *et al.* 2006). Supporting this idea, our simulations show that  $K_{IR}$  currents act to maintain the RMP ( $\sim -88$  mV) in NAc MS neurons, their absence depolarizing the cell by about 7 mV. Dopamine-induced membrane potential changes ( $\sim 6$  mV) have been reported in literature apparently mediated by unidentified  $K^+$  channels active in the resting conditions of NAc MS neurons (Uchimura *et al.* 1986; Higashi *et al.* 1989; Uchimura and North 1990; Nicola *et al.* 2000).

Alterations in the magnitude of  $K_{IR}$  conductance are believed to have major impact on the response of MS neurons to excitatory inputs (Wilson and Kawaguchi 1996; Mermelstein *et al.* 1998).  $K_{IR}$  currents, comprising the major portion of the currents active in the down-state of the neuron (Nisenbaum and Wilson 1995), are found to be

critical in determining its input resistance in the quiescent state (Wilson and Kawaguchi 1996). The presence of these currents reduces the membrane resistance in MS neurons (North and Uchimura 1989), thus resisting attempts by excitatory synaptic inputs to depolarize the membrane potential (Wilson and Kawaguchi 1996) and resulting in low-amplitude EPSPs. In agreement with these predictions, our results showed that the suppression of  $K_{IR}$  conductance increased the amplitude of EPSPs that was accompanied by a rise in  $R_{in}$ . The depolarization of the RMP and enhancement of  $R_{in}$  would together facilitate the transition of the neuron from the down-state to the up-state. Additionally, a reduced  $K_{IR}$  conductance enhanced the membrane time constant ( $\tau_m = R_m C_m$ ) that might be due to the increase in membrane resistance. This in turn would result in a slower decay of the injected current, prolonging the time course of the EPSP that was manifested in our simulations. This augmentation of the amplitude as well as the time course of the EPSPs reaching the soma would facilitate enhanced temporal summation of these inputs at the soma, thus increasing the effectiveness of these inputs during synaptic integration and consequently, of the likelihood of cell firing.

$K_{IR}$  channels in MS neurons share certain important electrical characteristics with  $I_h$  channels present in the dendrites of hippocampal and neocortical pyramidal neurons. The currents through both the channels are activated by hyperpolarization, with hyperpolarization increasing the inward currents through them. Both currents are non-inactivating as well. Larger depolarization deactivates these currents, thus blocking them near the firing threshold (Mermelstein *et al.* 1998; Magee 1998). The presence of  $I_h$  channels modulates the resting potential, hyperpolarizing the RMP, and decreases the amplitude and duration of the EPSP in the pyramidal cell. Our study shows similar effects in NAc MS neurons mediated by  $K_{IR}$  channels, with hyperpolarization of the RMP and reduction in the amplitude and duration of EPSP in the presence of these channels.  $I_h$  channels are also found to suppress the subthreshold synaptic transmission and integration in pyramidal neurons as well as the dendritic excitability (Magee 1998). Previous studies have suggested that  $K_{IR}$  channels should modulate temporal summation and cell excitability (Wilson and Kawaguchi 1996; Uchimura *et al.* 1989a; Mermelstein *et al.* 1998). The suppression, and temporal compression, of the EPSPs in their presence has been suggested to impose a requirement for greater spatial and/or temporal coherence of excitatory inputs (Wilson and Kawaguchi 1996) to evoke firing in MS neurons (Nicola *et al.* 2004). Our results show that  $K_{IR}$  channels contribute to the modulation of cell excitability in NAc MS neurons. They were also found to participate in the normalization of amplitude of synaptic inputs at the soma, thus helping the neuron to compensate for the dendritic filtering of distal input

amplitude, thereby increasing their impact on somatic  $V_m$ . Thus, dendritic  $K_{IR}$  channels are likely to be strong modulators of the propagation and integration of down-state excitatory synaptic inputs in NAc MS neurons, through effects similar to those which  $I_h$  currents exert in the pyramidal neurons of the hippocampus and neocortex (Magee 1999, 2000; Williams and Stuart 2003).

The situation is likely to be different in the up-state, however, where  $K_{IR}$  channels are largely deactivated and  $K_{AS}$  channels more strongly activated. Our studies on the role of  $K_{AS}$  in shaping the EPSPs in the up-state indicate that when the membrane potential is depolarized (e.g. to  $-65$  mV), the contribution from  $K_{AS}$  significantly increases. The influence of  $K_{AS}$  will be exerted both on EPSPs generated during the up-state and on the spiking behaviour of the neuron. It may be noted that  $K_{AS}$  has also been shown to modulate MS neuron excitability in a use-dependent manner across individual up-states (at membrane potentials more depolarized than  $-65$  mV; Mahon *et al.* 2000b), but this effect is produced mainly by the slow inactivation of this channel, while the effects described here are attributable to the *activation* of the conductance. It may be noted that, in the up-state, the possibility cannot be ruled out that channels other than  $K_{IR}$  and  $K_{AS}$  (e.g.  $Ca^{2+}$  and  $Na^+$  channels) might also play their own, more subtle roles in regulating excitability. On the whole, it appears that while  $K_{IR}$  conductance plays a primary role in determining the electrical behaviour in the down-state and in regulating the transition from the down- to the up-state, in the up-state,  $K_{AS}$  also start to play a prominent role in determining the excitability of the neuron. It is worth noting that a recent study (Mahon *et al.* 2006) has shown that this two-state membrane potential behaviour could be an artifact of anesthesia as, in the anaesthetized awake animal, the cell spends most of its time at relatively depolarized membrane potentials ( $\sim -70$  mV). Thus, in the awake animal,  $K_{IR}$  and  $K_{AS}$  might act as equal determinants of the properties of incoming EPSPs and their efficiency at evoking spikes.

#### 4.2 Implications on MS neuron functioning

In the neurons that express them,  $K_{IR}$  channels are believed to play an important role in a variety of cellular functions especially in regulating  $K^+$  homeostasis, synaptic integration, neuronal firing and resting conductance (Wilson 1993; Mermelstein *et al.* 1998; Hille 2001; Perez *et al.* 2006). Our findings on the modulatory influence of  $K_{IR}$  channels on EPSPs in MS neurons indicate that neurotransmitters or modulators that are capable of varying the conductance of  $K_{IR}$  channels could affect synaptic integration and excitability in these neurons. One such example is dopamine, an important neuromodulator in striatum that is capable of

altering several voltage-dependent conductances including  $K_{IR}$  conductance, thus regulating the neuron's responsiveness to synaptic inputs (Wickens and Wilson 1998; Nicola *et al.* 2000; Gruber *et al.* 2003). Experimental studies have shown that dopamine (DA) induces hyperpolarization in NAc MS neurons by activation of D1 receptors (D1R) and depolarization through activation of D2 receptors (D2R) (Uchimura *et al.* 1986; Higashi *et al.* 1989; Uchimura and North 1990; Nicola *et al.* 2000; Perez *et al.* 2006). The dopamine-induced hyperpolarization was found to be accompanied by increase in  $K^+$  conductance and decrease in apparent input resistance, while the depolarization was accompanied by decrease in  $K^+$  conductance and increase in apparent input resistance (Uchimura *et al.* 1986). However, the type of  $K^+$  conductance mediating these effects remains to be uncovered and our results help to shed light on this question. The changes in  $R_{in}$  observed in our study are both in qualitative as well as quantitative agreement with experimental data. For instance, qualitatively, hyperpolarization of the cell (induced by increase of  $K_{IR}$  conductance) was associated with a drop in  $R_{in}$ , and depolarization (induced by reduction of  $K_{IR}$  conductance) with a rise in  $R_{in}$ . For quantitative analysis we compared the DA-induced percentage changes in  $R_{in}$  at the soma observed by Uchimura *et al.* (1986) with corresponding changes of  $R_{in}$  at the soma in our model. The hyperpolarization-linked reduction of  $R_{in}$  was ~20% in the experimental study [see figure 1A (b) in Uchimura *et al.* (1986)], and 22.5% in our model (data not shown), while depolarization-linked enhancement of  $R_{in}$  was ~50% in the experimental study [see figure 1A (c) in Uchimura *et al.* (1986)], and an identical 50% in our model. As the changes in membrane potential and  $R_{in}$  in our study are elicited by alterations of  $K_{IR}$  conductance, the close quantitative agreement strongly suggests that, among the various  $K^+$  channels present in the NAc MS neurons,  $K_{IR}$  channels are the most likely target of DA action, in agreement with the suggestion tentatively put forward by Uchimura *et al.* (1989a).

Our findings also appear to have implications for the dynamics of the networks in which NAc MS neurons are embedded. Experimental studies have shown that the excitability of MS neuron in the two regions of the NAc (core and shell) differs, shell neurons being less excitable than core neurons (O'Donnell and Grace 1993). One factor believed to contribute to this difference is the type of DA receptor (D1 and D2 receptors denoted as D1R and D2R, respectively) expressed in each region. Our results offer a plausible explanation for the observations on differential excitability. MS neurons with D1-like expressions have been correlated with the expression of substance P (SP) and are more concentrated in the shell region while neurons with

D2-like receptor expression are correlated with enkephalin (ENK) expression and constitute the larger fraction in the core region (Lu *et al.* 1998; Mermelstein *et al.* 1998; Nicola *et al.* 2000). D1R-mediated inhibitory synaptic responses observed in NAc MS neurons (Pennartz *et al.* 1992) may have occurred through the reduction, and D2R-mediated excitatory responses through the augmentation of  $K_{IR}$  conductance (Perez *et al.* 2006), respectively. Taken together, our findings allow us to speculate that in shell neurons DA acting mainly through D1Rs would raise the conductance of  $K_{IR}$  channel, depressing the EPSP amplitude and half width leading to reduction in temporal summation and excitability of the neuron while in core neurons activation of D2Rs would reduce the conductance of  $K_{IR}$  channels, resulting in the enhancement of EPSP parameters and, thereby, higher excitability of the neuron.

Experimental evidence suggests that both  $K_{IR}$  and  $K_{AS}$  conductances are modulated by DA concomitantly via the D1 and D2 receptors (Perez *et al.* 2006; Moyer *et al.* 2007), implying that, when DA acts on the accumbal MS neuron, both conductances might participate in mediating its effects. However, the ranges of membrane potential at which these conductances operate are different. This is because, as discussed above,  $K_{IR}$  dominates in the down-state, influencing the transitions to the up-state, while effects of  $K_{AS}$  on EPSPs and spiking are exerted in the up-state. Previous work in this area suggests that the  $K_{AS}$  conductance is not modulated through D1 receptors while activation of D2 receptors produces an increase in this conductance of up to 10% (Moyer *et al.* 2007). Since in our simulations increase in  $K_{AS}$  conductance decreases the cell excitability, our findings suggest that DA acting on  $K_{AS}$  via D2 would reduce the excitability of the MS neuron during the up-state. Such an effect has in fact been observed experimentally in an earlier work, where the application of D2R agonists was shown to suppress the up-state spiking frequency in rat accumbal neurons (Perez *et al.* 2006).

Since  $K_{IR}$  and  $K_{AS}$  are powerful modulators of EPSP properties, it is conceivable that sets of MS neurons expressing different densities of  $K_{IR}$  and  $K_{AS}$  conductances would display appreciably different excitabilities. As of now, there seems to be no information on variation of  $K_{IR}$  or  $K_{AS}$  density among different accumbal MS neurons. However, there exist two distinct regions of the NAc, the core and the shell, whose MS neurons show differences in the levels of inactivation expressed in the  $K_{IR}$  conductance, and these differences have been shown to result in different excitabilities (Mermelstein *et al.* 1998; Steephen and Manchanda 2009). This indicates that if differences in density of channel conductances, or in other important biophysical parameters, were to be expressed in distinct subsets of neurons within the NAc, separate accumbal input processing streams could arise that exhibit different excitabilities.

The question remains as to whether background noise present in electrophysiological recordings in MS neurons might mask the findings that we have reported when these are elicited experimentally. However, considering the magnitude of the changes observed in our study, it is probable that these changes will also be observed in experimental situations designed to test these ideas. For example, the percentage effects observed upon raising or diminishing the  $K_{IR}$  conductance on the salient parameters studies here (e.g. EPSP amplitude and time course, half attenuation distance, membrane time constant and input resistance) are appreciable, and should be readily observable in experimental recordings, at least in those cases where noise is not a major contaminant of the signals. As an example, the amplitude of the EPSP increased by between 25% and 60% when the conductance of  $K_{IR}$  was varied to different degrees. The level of noise observed in experimental recordings from NAc MS neurons (O'Donnell and Grace 1995, 1998; O'Donnell *et al.* 1999; O'Donnell 2003) is ~1–2 mV, which would conceivably confound the observation of effects in the case of signals of very low amplitude, but not of relatively high amplitude signals. However, in experimental studies, steps are usually taken to enhance the discrimination of signal from noise, for example, statistical analysis of effects over several trials, as well as signal conditioning and processing techniques that improve signal to noise ratio, strategies that can accentuate changes subtler than those observed in the present work.

## 5. Conclusion

Our study demonstrates that, in NAc Ms neurons, reduction in  $K_{IR}$  and  $K_{As}$  conductances results in a facilitatory influence, whereas their enhancement produces an inhibitory influence on EPSPs in the down-state and depolarized up-state, respectively, of the neuron. These effects should modulate synaptic integration in these neurons, which in turn, modulate their spiking behaviour, as verified in our study. The predictions made by this study are experimentally testable because our conclusions are based mainly on somatic data; and electrophysiological recordings, although technically challenging, are carried out by several groups from the somata of NAc MS neurons (Uchimura *et al.* 1989b; O'Donnell and Grace 1993; Perez *et al.* 2006). The strength of the predictions made by computational models of neurons depends strongly on the fidelity of the model with respect to the actual neuron. The results of the validation of responses from our model (see the methods section), built using knowledge currently available about NAc MS neurons from the experimental literature, place confidence in the reliability of our predictions. However, the accuracy of the model as well as the robustness of these predictions

may be enhanced by improvements in the model resulting from superior characterization of the channel parameters and their densities and distribution. For example, in our model, the value of  $[Ca^{2+}]_i$  at rest is high (1 mM) when compared with the experimental literature available for the resting  $[Ca^{2+}]_i$  in other neurons (~0.2–0.3 mM). This value was obtained from the original model by Wolf *et al.* (2005), which they adopted to match the experimental results from MS neurons. The value of  $[Ca^{2+}]_i$  in the model remains subject to revision in light of pertinent experimental evidence. Also, the fraction of receptor currents mediated by the individual ions may be calculated separately when data for the conductances of receptor channels for each of these ions is known differentially. This would yield an improvement over the approximation we adopted in our model, of estimating a fixed fraction of receptor currents as  $Ca^{2+}$  currents. Further improvements would result from using a model with real morphology instead of a stylized one.

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