

PET Assessment of Myocardial Perfusion Reserve Inversely Correlates with Intravascular Ultrasound Findings in Angiographically Normal Cardiac Transplant Recipients

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Cardiac allograft vasculopathy (CAV) is the major determinant of long-term survival after heart transplantation. We aimed to evaluate the efficacy of PET as a noninvasive way to assess the early stages of CAV. **Methods:** Twenty-seven consecutive patients (20 men and 7 women; mean age \pm SD, 46 ± 12 y) who had normal results on coronary angiography and normal left ventricular systolic function (ejection fraction $\geq 60\%$) were enrolled at 2.5 ± 2.1 y after transplantation. Myocardial blood flow (MBF) was assessed using dynamic ^{13}N -ammonia PET at rest and during adenosine-induced hyperemia, and myocardial perfusion reserve (MPR) was calculated as the ratio of hyperemic MBF to resting MBF. Regional ^{13}N -ammonia PET was assessed using a 5-point scoring system. The intravascular ultrasound (IVUS) measurements for the extent of intimal hyperplasia, including plaque volume index (calculated as [total plaque volume/total vessel volume] $\times 100\%$) and maximum area of stenosis, were compared with MPR by linear regression analysis. **Results:** In 27 angiographically normal cardiac transplant recipients, MBF at rest and during adenosine stress and MPR of the left anterior descending artery distribution correlated strongly with the other 2 coronary artery distribution territories ($r \geq 0.97$, $P < 0.0001$). Summed stress score and summed difference score showed a moderate inverse correlation with MPR ($r = -0.41$ and -0.49 , respectively; $P < 0.05$) but not with IVUS measurements. MPR correlated inversely with plaque volume index ($r = -0.40$, $P < 0.05$) but not with maximal luminal stenosis as assessed by IVUS. In addition, MPR and IVUS measurements gradually inversely changed after heart transplantation (all $P < 0.05$). **Conclusion:** This study confirms that CAV is a progressive process, diffusely involving the epicardial and microvascular coronary system. Plaque burden as determined by IVUS agrees well with MPR as assessed by PET in recipients with normal

coronary angiography results. This finding suggests that dynamic ^{13}N -ammonia PET is clinically feasible for the early detection of CAV and can be used as a reliable marker of disease progression.

Key Words: cardiac allograft vasculopathy; transplantation; positron emission tomography; myocardial perfusion quantification

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Cardiac allograft vasculopathy (CAV) is one of the leading causes of late mortality after heart transplantation (1,2). Early CAV is clinically silent, and ischemia is usually not evident until the disease is far advanced. The traditional annual coronary angiogram for surveillance is of limited value because CAV is characterized by diffuse concentric intimal thickening of both epicardial and intramyocardial arteries and may thus be overlooked on a coronary angiogram. Intravascular ultrasound (IVUS) has been proposed to be the most sensitive method for diagnosis of early CAV (3–8). However, the invasiveness and the physical bulkiness of IVUS catheters make the widespread application of IVUS in the detection of CAV difficult (2–5).

Stress myocardial perfusion images, including SPECT and PET, have been recognized as key diagnostic methods to evaluate coronary artery disease (9–12). Stress myocardial SPECT, in comparison with invasive coronary angiography, frequently underestimates the extent and severity of CAV (8,13–16). Recently, PET has come to be considered the noninvasive gold standard. By quantification of the absolute myocardial blood flow (MBF) during stress and rest, the myocardial perfusion reserve (MPR) can be deduced to

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represent the epicardial arteries or microvascular dysfunction (17–20). Several studies involving patients with progressive coronary artery disease (21–23), idiopathic cardiomyopathies (24), and hypertrophic cardiomyopathies (25) have suggested the prognostic value of quantitative PET. However, for cardiac transplantation recipients, MPR measured by PET has been tested in only a few studies (26,27). A few previous studies have yielded conflicting results in Doppler-derived coronary flow reserve and morphologic change in CAV (28–34). In addition, the impact of MPR by dynamic PET on the prediction of graft failure is still inconclusive. Therefore, we sought to compare myocardial perfusion and MPR assessed by dynamic adenosine ^{13}N -ammonia PET and coronary morphologic changes measured by IVUS in angiographically normal cardiac transplant recipients, to test the value in detecting early stages of CAV.

MATERIALS AND METHODS

Between January 2007 and May 2009, 27 consecutive recipients (20 men and 7 women; mean age \pm SD, 46 ± 12 y) who had normal coronary angiography findings (7,8) and normal left ventricular systolic function (ejection fraction $\geq 60\%$) were enrolled at 2.5 ± 2.1 y (range, 1–9.5 y) after cardiac transplantation. For each recipient, PET and echocardiography were performed within 1 mo of the invasive coronary angiography and IVUS examination. The protocol was approved by the institutional review board, and written informed consent was obtained from each patient before enrollment.

IVUS

After the diagnostic coronary angiography, 5,000 U of intravenous heparin were administered and a 6-F guiding catheter was inserted in the left main coronary artery. The IVUS catheter (Atlantis SR Pro 2.5F, 40-MHz; Boston Scientific) was advanced so that the IVUS transducer was positioned at the distal left anterior descending coronary artery (LAD). The motorized IVUS transducer was pulled back at a constant rate of 1 mm/s along the length (≥ 50 mm) of the vessel to the ostium of the left main coronary artery. Two experienced readers, who did not know the PET findings, were responsible for analyzing the IVUS records using the resident software (Galax system; Boston Scientific). The plaque volume index was quantitatively measured according to the method of Pethig et al. (30), with slight modifications (7,8). In brief, serial cross-sectional areas (in mm^2) of lumen and vessel, defined as the areas within the intimal border and within the external elastic membrane, respectively, were determined every 2 mm along the entire length assessed. The plaque area was defined as the vessel minus the lumen. The percentage of area stenosis was then calculated as $(\text{plaque area}/\text{vessel}) \times 100\%$. The luminal, vessel, and plaque volumes (in mm^3) of each segment were calculated as cross-sectional areas (lumen, vessel, and plaque areas) \times segment length of 2 mm. Total volumes of lumen, vessel, and plaque were obtained by adding the measurements of all vascular segments. A plaque volume index, defined as $(\text{total plaque volume}/\text{total vessel volume}) \times 100$, was used to normalize the individual variations in the vessel and in the vessel length as assessed by IVUS.

TABLE 1. Baseline Characteristics of Study Population ($n = 27$)

Characteristic	Data
Recipient age (y)	
Mean \pm SD	46 ± 12
Range	22–67
Male sex (n)	20 (74%)
Posttransplant years	
Mean \pm SD	2.5 ± 2.1
Range	1–9.5
Hypertension (n)	5 (19%)
Diabetes mellitus (n)	8 (30%)
Hyperlipidemia/statin (n)	5 (19%)
Pretransplant diagnosis (n)	
Coronary artery disease	10 (37%)
Dilated cardiomyopathy	15 (56%)
Myocarditis	2 (7%)

PET

^{13}N -ammonia PET was performed at rest and during adenosine stress at a standard rate (0.14 mg/min/kg of body weight) over 6 min, as previously reported (35). Individual patients received a 740- to 925-MBq injection of ^{13}N -ammonia into a peripheral vein over 30 s by a volumetric pump. Images were acquired in 2-dimensional mode on an Advance PET scanner (GE Healthcare), within a field of view between 14.45 and 15.7 cm. The optimal imaging position was determined on a 2-min short transmission scan with an external ^{68}Ge source. Dynamic emission scans were obtained using a standard protocol consisting of 12×10 -s, 4×15 -s, 4×30 -s, and 3×300 -s frames and a matrix of 128×128 , followed by reconstruction using ordered-subset expectation maximization. Transmission scanning for photon attenuation correction was performed with an external ^{68}Ge source. The PET datasets were moved to a Xeleris workstation (GE Healthcare) by DICOM transfer. For review, the images were resliced in short-axis and vertical and horizontal long-axis orientations.

PET Data Analysis

Regional ^{13}N -ammonia PET results were assessed using a 17-segment model and a semiquantitative scoring system of the severity and extent of the defect, as recommended by the American Heart Society of Nuclear Cardiology (9,36,37). Each segment was scored using a 5-point system based on the severity of tracer uptake (0 = normal, 1 = equivocal, 2 = moderate, 3 = severe, and 4 = apparent absence of tracer uptake). Summed scores were calculated from these segmental scores, including a summed rest score (the sum of the 17 segmental rest scores) and summed stress score (the sum of the 17 segmental stress scores). A summed difference score (the difference between summed stress and rest scores) was calculated. The extent of ischemia was expressed as the percentage of ischemic myocardium (summed difference score/ 68×100): $<2.5\%$ was considered nonischemic, $2.5\%–8\%$ was considered slight to moderate ischemia, and $\geq 8\%$ was considered extensive ischemia, as modified from Zellweger et al. (38). PET image interpretation according to these definitions was performed by 2 experienced readers who had no access to the IVUS records. Diverging interpretations were classified by consensus. Quantitative MBF at rest and during adenosine stress was determined using ^{13}N -ammonia PET. Previously validated compartmental modeling techniques were

TABLE 2. MBF and Myocardial Perfusion Ratio Using Dynamic PET

Parameter	LAD	LCX	RCA	Global
MBF (mL/min/g)				
Rest	0.94 ± 0.18 (0.55–1.32)	1.17 ± 0.23 (0.75–1.80)	0.98 ± 0.19 (0.51–1.39)	0.94 ± 0.18 (0.58–1.38)
Hyperemia	2.43 ± 0.62 (1.28–3.41)	2.71 ± 0.64 (1.51–4.11)	2.46 ± 0.70 (1.07–3.80)	2.30 ± 0.56 (1.16–3.42)
MPR	2.67 ± 0.90 (1.39–5.52)	2.41 ± 0.80 (1.26–4.53)	2.63 ± 1.22 (1.26–7.47)	2.54 ± 0.92 (1.39–5.51)

LCX = left circumflex artery; RCA = right coronary artery.
Values are mean ± SD, with range in parentheses. There are no statistically significant differences between groups.

applied to the time–activity curves to obtain regional estimates of MBF (mL/g/min) (39) using the PMOD software package (version 2.8; PMOD Technologies Ltd.) (23). MPR was calculated as the ratio of hyperemic to resting MBF, and values of 2.0 or more were considered normal (40).

Statistical Analysis

Data were expressed as mean ± SD. Comparisons were made using the Student test for continuous variables and χ^2 analysis for categorical variables. ANOVA was performed to detect any associations between 2 or more variables. IVUS measurements were compared with PET variables by linear regression analysis. All analyses were performed using STATA (release 10.0; StataCorp LP) statistical software. All statistical tests were 2-sided, and a *P* value of less than 0.05 was considered statistically significant.

RESULTS

A total of 27 cardiac transplant recipients with patent coronary angiograms were included in the study. Relevant baseline characteristics of the patients are reported in Table 1. All patients received standard immunosuppressive therapy as previously described (7,8,13–15). Based on concurrent endomyocardial biopsy findings, none had acute rejection of grade II or higher (according to the system of the International Society for Heart and Lung Transplantation) during the IVUS study (41).

IVUS and PET were successfully performed on all 27 patients, and no complications occurred. The mean and maximal plaque indices of LAD as assessed by IVUS were $27.82 \pm 12.33 \text{ mm}^3$ (range, 7.11–50.13 mm^3) and $44.57 \pm$

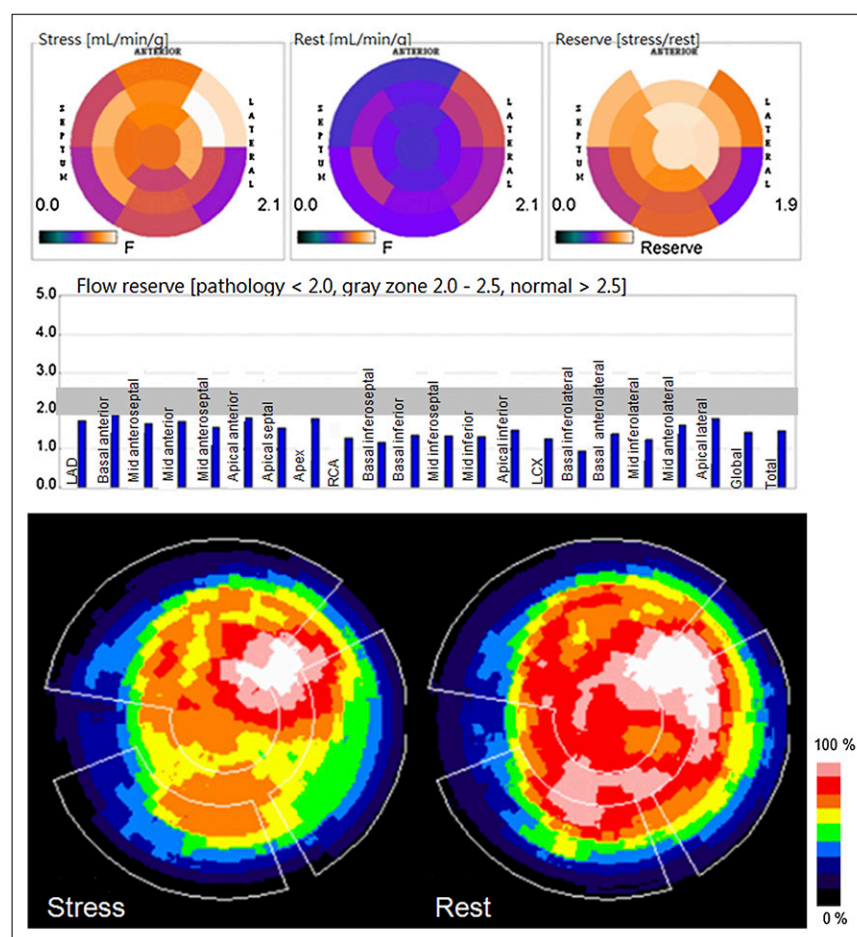


FIGURE 1. Quantitative and qualitative assessment by rest/adenosine stress ^{13}N -ammonia PET of 57-y-old man who had received orthotopic heart transplant 4 y previously. Polar maps and bar chart of absolute MBF in dynamic images (top) show regional perfusion heterogeneity, and qualitative static images normalized to individual left ventricular maximum (bottom) show significant reduction of stress flow, resulting in blunted flow reserve.

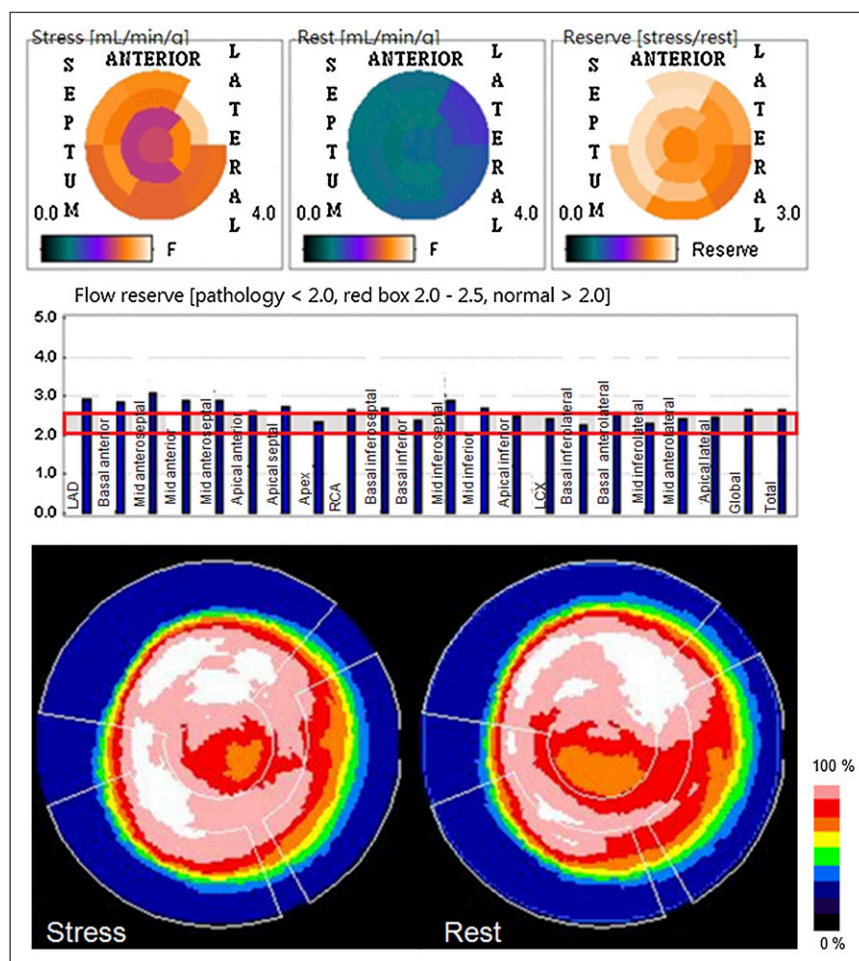


FIGURE 2. ^{13}N -ammonia PET study of 54-y-old man who had received orthotopic heart transplant 1 y previously shows normal flow reserve in dynamic images (top) and no significant perfusion heterogeneity in qualitative static images (bottom).

17.31 mm³ (range, 16.14–77.92 mm³), respectively. By semiquantitative PET analysis, the summed stress score, summed rest score, and summed difference score were 2.0 ± 2.3 (range, 0–10), 0.8 ± 0.7 (range, 0–2), and 1.2 ± 2.0 (range, 0–9), respectively. The distribution of patients based on the extent of ischemia was 20 (74%), 3 (11%), 3 (11%), and 1 (4%) for no ischemia, slight ischemia, moderate ischemia, and extensive ischemia, respectively. MBF at rest or during adenosine stress, and the MPR of the LAD distribution, correlated strongly between the other 2 coronary artery distribution territories ($r \geq 0.97$, $P < 0.0001$, Table 2), suggesting that CAV involved the 3 major coronary arteries to a similar degree. Representative images of quantitative and qualitative assessment by rest and adenosine stress ^{13}N -ammonia PET are shown in Figures 1 and 2.

There were moderate inverse correlations between summed stress score, summed difference score, and the MPR of the global myocardium ($r = -0.41$ and -0.49 , respectively; $P < 0.05$) but not IVUS parameters. There was no significant correlation between IVUS parameters and MBF at rest. In contrast, stress MBF and MPR correlated inversely with plaque volume index measured by IVUS (both $r = -0.40$ in LAD territory, whereas

$r = -0.46$ and -0.36 , respectively, in global myocardium; all $P < 0.05$) but not maximal luminal stenosis (Fig. 3). In the 20 cases regarded as nonischemic by semiquantitative PET analysis, a global myocardium MPR of 2 or more in 4 subjects (20%) was noted, suggesting diffuse coronary lesions with balanced ischemia.

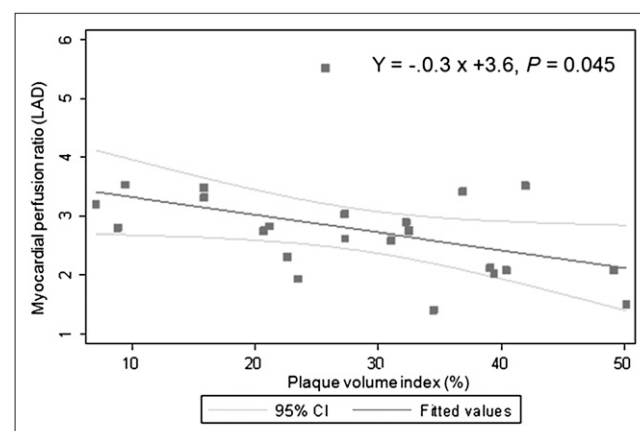


FIGURE 3. Correlation between myocardial perfusion ratio as assessed by PET and plaque volume index as measured by IVUS.

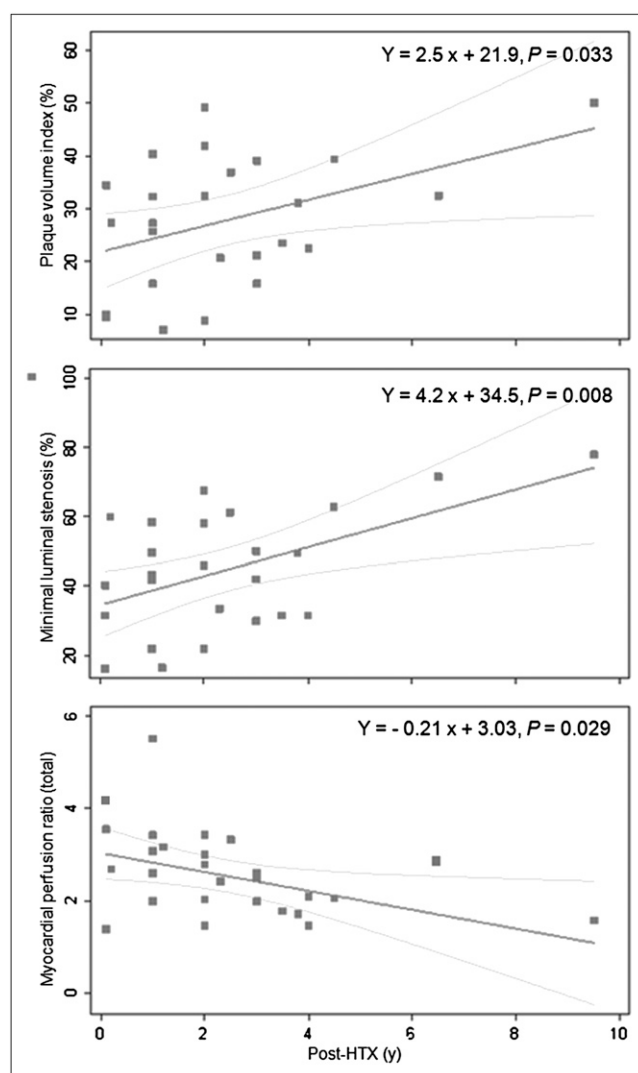


FIGURE 4. Correlations between plaque volume index (top), maximal luminal stenosis (middle), and myocardial perfusion ratio (bottom) and time after heart transplantation.

Furthermore, we compared the patient characteristics with the results of PET or IVUS. With the exception of posttransplantation time, no significant correlations were found between clinical characteristics (including pretransplantation diagnosis, diabetes mellitus, hypertension, hyperlipidemia, sex or age, or number of cardiac risk factors) and PET or IVUS parameters. Although the coronary angiograms showed patency for all subjects, the MPR of the LAD territory or global myocardium deteriorated, and IVUS parameters (both plaque volume index and maximal luminal stenoses) increased as the time after heart transplantation increased (all $P < 0.05$) (Fig. 4).

DISCUSSION

Because of the low sensitivity of coronary angiography, IVUS and Doppler-derived coronary flow reserve have been considered the standards in the diagnosis of CAV (1–3).

However, clinical application is limited because the procedure is invasive and time-consuming and requires highly trained medical personnel. The current study demonstrated that the vasodilation capacity and perfusion abnormalities detected by PET correlated well with the coronary morphologic changes in IVUS.

The main advantage of PET is its superior spatial resolution and the possibility of noninvasive assessment of absolute quantitative MBF, from which MPR can be calculated. The assessment of quantitative regional MBF and MPR with ^{13}N -ammonia PET has been well established. ^{13}N -ammonia dynamic PET blood flow measurements include integrated vasodilation capacity, endothelium-related vasomotor function, and epicardial conduit vessel function (42,43). MBF and MPR not only can provide important diagnostic and prognostic information (10–12,20–25) but also can be used as a surrogate endpoint to assess therapeutic response (44–48) and to guide interventions aimed at reducing cardiac risks or ischemic burden in subjects with native coronary artery disease (49).

CAV is a progressive process involving the epicardial and microvascular coronary systems. Conflicting results in IVUS- and Doppler-derived coronary flow reserve studies (7,8,28–34,50–52) suggest that the correlation between endothelial dysfunction and coronary changes is complex. Studies in the past have shown that dynamic PET provides information complementary to coronary anatomy. By using dipyridamole ^{13}N -ammonia PET, Preumont et al. (27) found that MBF reserve was impaired early after heart transplantation and restored within 1 y in heart transplant recipients free of allograft rejection and with normal coronary angiography findings. Allen-Auerbach et al. (26) found that the degree of vasodilatory capacity detected by PET is associated with morphologic indices of disease progression as assessed by IVUS at 1–2 y after transplantation. However, the sample sizes were rather small, and posttransplantation durations were short. Whether dynamic PET is enough to assess patients at risk of CAV remains to be determined.

Consistent with previous reports, our study confirmed that semiquantitative ^{13}N -ammonia PET is superior to invasive coronary angiography in the detection of CAV. Through the use of dynamic PET, an additional 20% of subjects who had normal semiquantitative PET results were found to have impaired coronary flow reserve. Moreover, the severity of the impairment inversely correlated with the coronary plaque burden as assessed by IVUS. This finding demonstrated the superiority of coronary flow reserve over perfusion scans alone, partly because CAV involves multiple vessels so that regional perfusion abnormalities could be masked by diffuse lesions with balanced ischemia on qualitative images. Therefore, dynamic ^{13}N -ammonia PET is a better, more reliable noninvasive tool for the detection of early CAV and disease progression. A preserved coronary flow reserve as assessed by dynamic PET may obviate

invasive coronary angiography and IVUS surveillance in transplant recipients.

The study had some limitations. First, the number of recipients included was small, and they were heterogeneous in coronary risk factors, donor age, immunosuppressive protocols, and history of myocardial rejections. Second, in this cross-section study, not all patients underwent IVUS immediately after transplantation; therefore, it is difficult to differentiate donor-transmitted coronary artery disease from CAV. In addition, there is not a clear MPR cutoff value to recognize more altered vessels, and the predictive value of ^{13}N -ammonia PET for long-term clinical outcome is not yet known. A large-scale prospective study of serial quantitative IVUS and PET measurements to assess the progression of CAV and to elucidate the prognostic value of quantitative PET in posttransplant recipients is needed.

CONCLUSION

Using noninvasive ^{13}N -ammonia PET, this study confirmed that CAV is a progressive and diffuse process involving the epicardial and microvascular coronary system. There is good agreement between plaque burden as determined by IVUS and MPR as assessed by PET in recipients with normal coronary angiography findings. The findings of this study suggest that quantitative measurement of myocardial flow using dynamic ^{13}N -ammonia PET is clinically feasible for the early detection of CAV and could be used as a reliable marker of disease progression.

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