

Preclinical Evaluation of ^{18}F -JNJ41510417 as a Radioligand for PET Imaging of Phosphodiesterase-10A in the Brain

Sofie Celen¹, Michel Koole², Meri De Angelis³, Ivan Sannen¹, Satish K. Chitneni¹, Jesus Alcazar³, Stefanie Dedeurwaerdere⁴, Dieder Moechars⁴, Mark Schmidt⁴, Alfons Verbruggen¹, Xavier Langlois⁴, Koen Van Laere², José Ignacio Andrés³, and Guy Bormans¹

¹Laboratory for Radiopharmacy, Faculty of Pharmaceutical Sciences, K.U. Leuven, Leuven, Belgium; ²Department of Nuclear Medicine, K.U. Leuven, Leuven, Belgium; ³Johnson and Johnson Pharmaceutical Research and Development, Toledo, Spain; and ⁴Johnson and Johnson Pharmaceutical Research and Development, Beerse, Belgium

Phosphodiesterases are enzymes that inactivate the intracellular second messengers 3',5'-cyclic adenosine-monophosphate and/or cyclic guanosine-monophosphate. Of all 11 known phosphodiesterase families, phosphodiesterase-10A (PDE10A) has the most restricted distribution, with high expression in the striatum. PDE10A inhibitors are pursued as drugs for treatment of neuropsychiatric disorders. We have synthesized and evaluated ^{18}F -JNJ41510417 as a selective and high-affinity radioligand for in vivo brain imaging of PDE10A using PET. **Methods:** The biodistribution of ^{18}F -JNJ41510417 was evaluated in rats. Rat plasma and perfused brain homogenates were analyzed by high-performance liquid chromatography to quantify radiometabolites. Dynamic small-animal PET was performed in rats and in wild-type and PDE10A knock-out mice and compared with ex vivo autoradiography. Blocking and displacement experiments were performed using the nonradioactive analog and other selective PDE10A inhibitors. **Results:** Tissue distribution studies showed predominant hepatobiliary excretion, sufficient brain uptake (0.56 ± 0.00 percentage injected dose at 2 min after tracer injection), and continuous accumulation of the tracer in the striatum over time; rapid wash-out of nonspecific binding from other brain regions was observed. Polar radiometabolites were detected in plasma and brain tissue. Dynamic small-animal PET showed continuous tracer accumulation in the striatum, with rapid decline in the cortex and cerebellum. Pretreatment and chase experiments with PDE10A inhibitors showed that the tracer binding to PDE10A was specific and reversible. Imaging in PDE10A knock-out and wild-type mice further confirmed that binding in the striatum was specific for PDE10A. **Conclusion:** Experiments in rats and PDE10A knock-out mice indicate that ^{18}F -JNJ41510417 binds specifically and reversibly to PDE10A in the striatum, suggesting that this new fluorinated quinoline derivative is a promising candidate for in vivo imaging of PDE10A using PET.

Key Words: ^{18}F ; PET; PDE10A; brain imaging

J Nucl Med 2010; 51:1584–1591

DOI: 10.2967/jnumed.110.077040

Received Mar. 9, 2010; revision accepted Jul. 14, 2010.

For correspondence contact: Guy Bormans, Laboratory for Radiopharmacy, Faculty of Pharmaceutical Sciences, K.U. Leuven, Herestraat 49, B-3000 Leuven, Belgium.

E-mail: guy.bormans@pharm.kuleuven.be

COPYRIGHT © 2010 by the Society of Nuclear Medicine, Inc.

Phosphodiesterase-10A (PDE10A) belongs to a family of cyclic nucleotide phosphodiesterases, enzymes that hydrolyze adenosine and/or guanosine 3',5'-cyclic monophosphates (cAMP and cGMP, respectively). These cyclic nucleotides play an important role as second messengers in the central nervous system, serving to regulate a wide variety of neuronal functions. The human genome encodes 21 phosphodiesterase genes that are categorized into 11 distinct families. The PDE10A enzyme is the single member of the PDE10 family (1). Of all known phosphodiesterase families, PDE10A has the most restricted distribution, with high expression in the brain and testes only (2,3). In the brain, PDE10A messenger RNA and protein are highly abundant in the medium spiny neurons of the striatum, the principal input site of the basal ganglia which is involved in the regulation of motor, appetitive, and cognitive processes (3,4). Studies using papaverine (a relatively selective PDE10A inhibitor with a half-maximal inhibitory concentration of 36 nM) and behavioral experiments with PDE10A knock-out (KO) mice have indicated that PDE10A inhibition results in activation of the medium spiny neurons (5–7). These findings suggest that PDE10A inhibitors may be a novel therapeutic approach to the treatment of diseases characterized by a reduced activity of these neurons, such as schizophrenia, Huntington's disease, Parkinson's disease, obsessive-compulsive disorder, and addiction (1,8–10). Noninvasive imaging of PDE10A using PET would allow the distribution of this enzyme to be studied in vivo in these diseases. Furthermore, noninvasive imaging would be useful for the clinical development of PDE10A inhibitors, by giving direct insight into the relationship between enzyme activity and administered dose of the candidate drug (11–14). A first attempt to visualize PDE10A has recently been made by Tu et al. (15), who successfully radiolabeled the relatively selective PDE10A inhibitor papaverine with ^{11}C . Although ^{11}C -papaverine showed selective PDE10A binding in vitro, it failed in vivo because of rapid washout of the tracer from the striatum, as was observed in rat biodistribution studies and small-animal PET brain imaging in monkeys (15).

The aim of this work was to synthesize and evaluate a specific and selective radioligand for imaging of PDE10A in the living brain using PET. Initial *in vitro* PDE10A inhibition studies, performed by Johnson & Johnson Pharmaceutical Research and Development, identified the quinoline JNJ41510417 as a potent PDE10A inhibitor. JNJ41510417 is a structure derived from the chemical series that includes PF-2545920 (Fig. 1, also known as MP-10), a compound developed by Pfizer (16–18). *In vitro* studies demonstrated that JNJ41510417 is selective for PDE10A (>1,000-fold over PDE2A, PDE3A, PDE4D3, PDE5A3, PDE7A, PDE8A1, PDE9A, PDE6, and PDE1B1) and has a half-maximal inhibitory concentration of 0.5 nM for rat PDE10A (Johnson & Johnson, unpublished data, 2009). In general, passive diffusion across the cerebral endothelium is considered to be possible for molecules with medium lipophilicity (logarithm of octanol/buffer_{pH7.4} distribution coefficient [$\log D_{7.4}$], 0.9–3.5), a molecular mass less than 600 Da, and a low capacity to form hydrogen bonds (19,20). JNJ41510417 is a small molecule with a molecular mass of 424, a low polar surface area of 0.53 nm² (53 Å²) (21,22), a measured $\log D_{7.4}$ of 4.7, and a plasma protein binding of 99.5% (both in humans and in rats) (Johnson & Johnson, unpublished data, 2009). Despite its rather high lipophilicity and plasma protein binding, JNJ41510417 seems to be potent, with an *in vivo* occupancy (median effective dose) of 0.48 mg/kg (Johnson & Johnson, unpublished data, 2009). Because of these characteristics, JNJ41510417 was radiolabeled with ¹⁸F (Fig. 1) and evaluated as a potential PET ligand to visualize PDE10A activity *in vivo*. This article reports the *in vivo* evaluation of ¹⁸F-JNJ41510417 in rats and PDE10A KO mice. The synthesis of the precursor and authentic reference material and the radiochemistry will be published in detail elsewhere.

MATERIALS AND METHODS

General

High-performance liquid chromatography (HPLC) analysis was performed on a LaChrom Elite HPLC system (Hitachi) connected to an ultraviolet spectrometer set at 254 nm. For the analysis of radiolabeled compounds, the HPLC eluate (after passage through the ultraviolet detector) was led over a 7.62-cm (3-in.) NaI(Tl) scintillation detector connected to a single-channel analyzer (GABI box; Raytest). Quantification of radioactivity measure-

ments in biodistribution studies and *in vivo* stability analyses was performed using an automated γ -counter equipped with a 7.62-cm (3-in.) NaI(Tl) well crystal coupled to a multichannel analyzer (1480 Wizard; Wallac). The results were corrected for background radiation and physical decay during counting.

Animals were housed in individually ventilated cages in a thermoregulated (~22°C), humidity-controlled facility under a 12 h–12 h light–dark cycle, with access to food and water *ad libitum*. All animal experiments were conducted according to the Belgian code of practice for the care and use of animals, after approval from the university ethics committee for animals.

Biodistribution Studies

The biodistribution study of ¹⁸F-JNJ41510417 was performed in healthy male Wistar rats (body weight, 270–340 g) at 2, 30, and 60 min after injection ($n = 3$ /time point). Anesthetized rats (2.5% isoflurane in O₂ at a flow rate of 1 L/min) were injected with about 1.1 MBq of the tracer via a tail vein and sacrificed by decapitation at the specified times points. Blood and major organs were collected in tared tubes and weighed. The radioactivity in blood, organs, and other body parts was counted using an automated γ -counter. For the calculation of total radioactivity in blood, blood mass was assumed to be 7% of the body mass.

Plasma Radiometabolite Analysis

After intravenous administration of about 59 MBq of ¹⁸F-JNJ41510417 via a tail vein of anesthetized rats (2.5% isoflurane in O₂ at a flow rate of 1 L/min), blood was collected via the contralateral tail vein at 2, 30, and 60 min after injection (from the same animal) in lithium heparin-containing tubes (4.5-mL lithium heparin PST tubes, BD Vacutainer; BD) and stored on ice. Next, the blood was centrifuged for 10 min at 3,000 rpm to separate the plasma. Plasma (0.1 mL) was spiked with 10 μ g of authentic JNJ41510417 and 10 μ g of JNJ41797444. Plasma was then analyzed with HPLC (Chromolith C₁₈, 3 \times 100 mm; Merck) eluted with gradient mixtures of 0.05 M sodium acetate (pH 5.5) (A) and CH₃CN (B) (0–4 min: isocratic 0% B and flow rate of 0.5 mL/min; 4–14 min: linear gradient 0% B to 90% B and flow rate of 1 mL/min; and 14–17 min: isocratic 90% B and flow rate of 1 mL/min). After passing through an inline ultraviolet detector (254 nm), the HPLC eluate was collected as 1-mL fractions. The radioactivity in all fractions was measured using an automated γ -counter.

Perfused Brain Radiometabolite Analysis

For each studied time point, 2 rats were injected with about 37 MBq of ¹⁸F-JNJ41510417. At 30 or 60 min after injection, the rats were sacrificed by an overdose of pentobarbital (200 mg/kg intraperitoneally; Nembutal [CEVA Santé Animale]). The rats were perfused by injection of saline into the right ventricle until the liver turned pale. The brain was isolated; the cerebrum and cer-

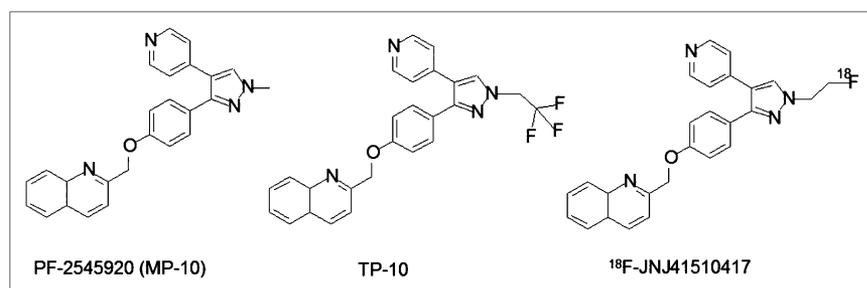


FIGURE 1. Chemical structure of PF-2545920 (MP-10; Pfizer), TP-10, and ¹⁸F-JNJ41510417, a potential PET ligand for *in vivo* imaging of PDE10A in brain.

ebellum were separated and homogenized in 3 and 2 mL of CH₃CN, respectively, for about 2 min. A volume of 1 mL of this homogenate was diluted with an equal volume of water, and 1 mL of the supernatant was filtered through a 0.22- μ m filter (Millipore). About 0.5 mL of the filtrate was diluted with 0.1 mL of water and spiked with 10 μ g of authentic JNJ41510417 and 10 μ g of JNJ41797444. A volume of 0.5 mL of the homogenate extracts was injected onto an HPLC system, consisting of an analytical XBridge column (C₁₈, 5 μ M, 3 \times 100 mm; Waters) eluted with a mixture of 0.05 M sodium acetate (pH 5.5) and CH₃CN (65:35 v/v) at a flow rate of 0.8 mL/min. The HPLC eluate was collected as 1-mL fractions after passing through the ultraviolet detector (254 nm), and radioactivity in the fractions was measured using an automated γ -counter.

Radiometabolite Analysis of Rat Blood, Plasma, and Perfused Brain Homogenate After In Vitro Incubation with ¹⁸F-JNJ41510417

Rat blood, plasma, and homogenated perfused brain were incubated with about 7.4 MBq of ¹⁸F-JNJ41510417 at 37°C. After 60 min of incubation, the samples were cooled on ice. Blood and brain homogenate samples were processed and analyzed onto reversed-phase HPLC as described earlier in the previous two sections of this article.

Small-Animal PET Studies

Imaging experiments were performed on a Focus 220 microPET scanner (Concorde Microsystems) using male Wistar rats and wild-type (WT) and PDE10A KO mice. During all scan sessions, animals were kept under gas anesthesia (2.5% isoflurane in O₂ at a flow rate of 1 L/min). Dynamic 120-min scans were acquired in list mode. Acquisition data were Fourier rebinned in 31 time frames (4 \times 15 s, 4 \times 1 min, 5 \times 3 min, 8 \times 5 min, and 10 \times 6 min) and reconstructed with filtered backprojection. A summed image (frames 1–31) of the reconstructed data was spatially normalized to a ¹¹C-raclopride template of the rat brain in Paxinos coordinates created in-house (23). The affine transformation was then used to normalize all time frames of the dynamic dataset to allow automated and symmetric volume-of-interest analyses. Time–activity curves were generated for the striatum, cerebral visual and retrosplenial cortex, and cerebellum for each individual scan, using PMOD software (version 3.1;

PMOD Technologies Ltd.). The radioactivity concentration in the different brain regions was expressed as standardized uptake value (SUV) as a function of time after injection of the radiotracer by normalization for body weight of the animal and injected dose. Because PDE10A is expressed at a low level in the cerebellum (3), (striatum – cerebellum)/cerebellum (S/C-1) ratios were calculated for the transient equilibrium phase (32–75 min after tracer injection). These ratios were determined in order to provide the relative difference in tracer uptake between cerebellum and striatum and to have a preliminary approximation of binding potential values for the striatum.

Anesthetized rats (2.5% isoflurane in O₂ at a flow rate of 1 L/min) were injected with about 37–74 MBq of a high-specific-activity formulation of ¹⁸F-JNJ41510417 via the tail vein. For pretreatment and displacement experiments, JNJ41510417, MP-10, and TP-10 were dissolved and administered in a vehicle containing 10% dimethylsulfoxide and 20% (2-hydroxypropyl)- β -cyclodextrine. MP-10 and TP-10 (chemical structure in Fig. 1) are specific PDE10A inhibitors, with subnanomolar potency (1,16,24). Pretreatment studies were performed by subcutaneous administration at approximately 60 min before radiotracer injection. A displacement study was performed by intravenous injection at 60 min after radiotracer injection. Rats were pretreated with authentic JNJ41510417 (self-blocking, 2.5 mg/kg, *n* = 1), TP-10 (5 mg/kg, *n* = 1), and several doses of MP-10 (0.5, 1, and 5 mg/kg, *n* = 2 per dose). Doses and time of pretreatment were based on the results obtained by the study of Schmidt et al. (24). A washout period of at least 4 d was maintained between different pretreatment studies. Also, 2 PDE10A KO mice and 1 WT mouse (J&J PRD, Neuroscience) were injected with 13 MBq of ¹⁸F-JNJ41510417 via the tail vein and were scanned dynamically for 60 min using small-animal PET.

Ex Vivo Autoradiography in WT and PDE10A KO Mice

After the small-animal PET scan, the mice were sacrificed, brain was removed, and cerebrum was separated from cerebellum and rapidly frozen in 2-methylbutane (–40°C). Frontal sections (30 μ m) from the cerebrum were obtained using a cryotome (Shandon cryotome FSE; Thermo Fisher), mounted on adhesive microscope slides (Superfrost Plus; Thermo Fisher Scientific), and exposed to a phosphor storage screen film (super-resolution screen;

TABLE 1. Biodistribution of ¹⁸F-JNJ41510417 in Normal Rats at 2, 30, and 60 Minutes After Tracer Injection

Body part	Percentage of injected dose*		
	2 min	30 min	60 min
Urine	0.1 \pm 0.0	0.2 \pm 0.0	0.9 \pm 0.2
Kidneys	6.9 \pm 0.5	1.8 \pm 0.1	1.3 \pm 0.1
Liver	41.1 \pm 2.4	52.3 \pm 4.6	42.6 \pm 2.3
Spleen + Pancreas	1.9 \pm 0.1	0.6 \pm 0.1	0.4 \pm 0.0
Lungs	2.4 \pm 0.1	0.4 \pm 0.0	0.3 \pm 0.0
Heart	0.9 \pm 0.1	0.2 \pm 0.0	0.2 \pm 0.0
Stomach	1.7 \pm 0.3	5.1 \pm 2.0	13.7 \pm 1.4
Intestines	9.4 \pm 0.6	10.8 \pm 4.9	12.5 \pm 2.5
Cerebrum	0.447 \pm 0.009	0.266 \pm 0.003	0.257 \pm 0.007
Cerebellum	0.101 \pm 0.015	0.035 \pm 0.003	0.031 \pm 0.002
Blood	4.0 \pm 0.3	2.0 \pm 0.2	2.1 \pm 0.2
Remainder	32.8 \pm 2.4	26.4 \pm 1.5	26.0 \pm 1.3

*Calculated as counts per minute in organ/total counts per minute recovered. Data are expressed as mean \pm SD; *n* = 3 per time point.

Perkin Elmer) for about 24 h. The screens were read using a Cyclone Plus system (Perkin Elmer) and analyzed using Optiquant software (Perkin Elmer). The results are expressed as digital light units/mm², normalized for body weight of the animal and injected dose ($[\text{DLU}/\text{mm}^2] \times [\text{body weight}/\text{injected dose}]$).

RESULTS

Biodistribution Studies

Table 1 shows the percentage injected dose (%ID) at 2, 30, and 60 min after injection of the radiotracer. At 2 min after injection of the tracer, about 4.0% of the injected dose was present in the blood and cleared to 2.1% by 60 min after injection. The total brain uptake of the tracer at 2 min after injection was 0.56%. At 60 min after tracer injection, 55% of the injected dose was present in the liver and intestines, whereas urinary excretion of the tracer was minimal (2.2 %ID at 60 min after injection).

Table 2 presents the SUVs for the studied brain regions and blood. At 2 min after tracer injection, the radioactivity concentration in the striatum was highest of all brain regions. The striatum was the only brain region in which the tracer concentration increased as a function of time after injection. At 2 min after injection of the tracer, the striatum-to-cerebellum ratio was about 1.3, and this ratio increased to 7.0 by 60 min after injection. Striatum-to-cortex and striatum-to-hippocampus ratios were also 5.8 or more at 60 min after tracer injection.

Radiometabolite Analysis of ¹⁸F-JNJ41510417 in Plasma of Rats

Figure 2A shows the reconstructed radiochromatograms from rat plasma analysis at 2, 30, and 60 min after tracer injection, with the peak corresponding to intact ¹⁸F-JNJ41510417 eluting with a retention time of approximately 13 min. The small peak eluting just before (retention time, ~11 min) the intact tracer was identified as ¹⁸F-JNJ41797444 (Fig. 2B). Unidentified polar radiometabolite(s) eluting around 2 min were also detected in the brain (see

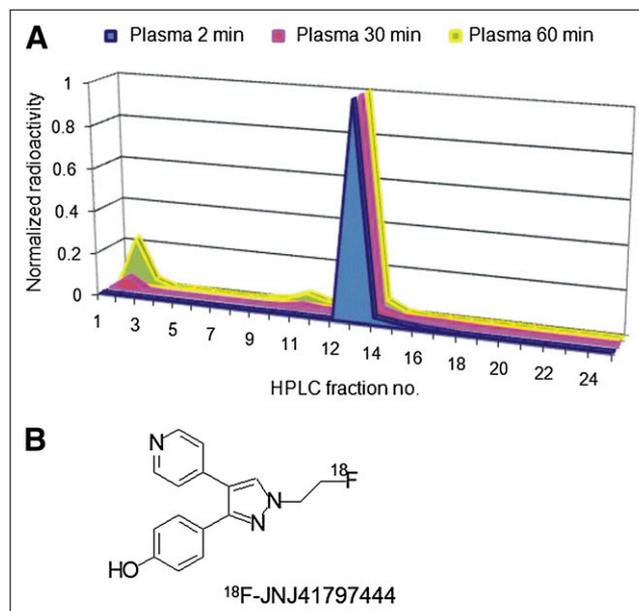


FIGURE 2. (A) Reconstructed radiochromatograms of rat plasma analysis at 2 (blue), 30 (pink), and 60 (yellow) min after injection of ¹⁸F-JNJ41510417. (B) Chemical structure of radiometabolite ¹⁸F-JNJ41797444. Retention time was approximately 11 min in radiochromatogram (A). no. = number.

below). An overview of the results from the plasma radiometabolite analysis is presented in Table 3. At 2 min after injection of the radiotracer, almost all the recovered radioactivity in plasma was in the form of intact tracer. At 30 min after tracer injection, 11% of polar metabolites were found in plasma, and this amount increased to 27% at 60 min after injection. No apolar metabolites were detected. The recovery of the HPLC and Chromolith column-injected radioactivity was 89% ($n = 2$).

Radiometabolite Analysis of ¹⁸F-JNJ41510417 in Perfused Cerebrum and Cerebellum of Rats

An overview of the results from the perfused rat brain radiometabolite analysis is presented in Table 4. The fraction of polar radiometabolites detected in the cerebellum was higher than that in the cerebrum. At 30 min after tracer injection, about 95% of the recovered radioactivity was present as intact tracer in the cerebrum; in the cerebellum, this recovered fraction was approximately 90%. After 60 min, the amount of intact tracer in the cerebrum

TABLE 2. ¹⁸F-JNJ41510417 Concentration in Different Brain Regions and Blood at 2, 30, and 60 Minutes After Tracer Injection

Body part	SUV*		
	2 min	30 min	60 min
Striatum	1.6 ± 0.0	1.7 ± 0.0	2.6 ± 0.0
Hippocampus	0.8 ± 0.0	0.4 ± 0.0	0.4 ± 0.0
Cortex	1.2 ± 0.0	0.5 ± 0.0	0.5 ± 0.0
Rest of cerebrum	1.0 ± 0.0	0.5 ± 0.0	0.6 ± 0.0
Cerebellum	1.2 ± 0.0	0.4 ± 0.0	0.4 ± 0.0
Blood	0.6 ± 0.0	0.3 ± 0.0	0.3 ± 0.0

*Calculated as (radioactivity in counts per minute in organ/weight of the organ in grams)/(total counts recovered/body weight in grams).

Data are expressed as mean ± SD; $n = 3$ per time point.

TABLE 3. Relative Percentages of Intact Tracer and Radiometabolites in Rat Plasma at 2, 30, and 60 Minutes After Injection of ¹⁸F-JNJ41510417

%	Mean ± SD ($n = 2$)		
	2 min	30 min	60 min
Polar metabolite(s)	0.9 ± 0.4	11.3 ± 4.8	26.8 ± 3.7
Intact tracer	99.1 ± 0.4	88.7 ± 4.8	73.2 ± 3.7

TABLE 4. Relative Percentages of Intact Tracer and Radiometabolites in Perfused Rat Cerebrum and Cerebellum at 30 and 60 Minutes After Injection of ^{18}F -JNJ41510417

%	30 min after tracer injection		60 min after tracer injection	
	Cerebrum	Cerebellum	Cerebrum	Cerebellum
Polar metabolite(s)	4.8 ± 2.0	9.7 ± 3.5	14.4 ± 0.6	25.8 ± 4.3
Intact tracer	95.2 ± 2.0	90.3 ± 3.5	85.6 ± 0.6	74.2 ± 4.2

Data are presented as mean ± SD ($n = 2$).

decreased to approximately 86%; in the cerebellum, this fraction was about 74%. The recovery of the HPLC and XBridge column–injected radioactivity was 79% ($n = 2$).

Radiometabolite Analysis of Rat Blood, Plasma, and Perfused Brain Homogenate After In Vitro Incubation with ^{18}F -JNJ41510417

^{18}F -JNJ41510417 was shown to be metabolically stable in rat whole blood, rat plasma, and rat brain homogenate in vitro. The fraction of polar metabolites observed after 60 min of incubation at 37°C was negligible (<2.2%).

Small-Animal PET

Baseline Scans. A high-intensity signal was observed in the striatum with only background radioactivity in cortical regions and the cerebellum (Fig. 3). High uptake was also present in the Harderian glands. After the high initial brain uptake, radioactivity cleared from the cortical regions and cerebellum, whereas the radiotracer activity increased in the striatum (Fig. 4A).

Pretreatment Blocking Studies. Pretreatment with the authentic reference material and with PDE10A inhibitors at a dose of 5 mg/kg injected subcutaneously at 60 min before tracer injection resulted in a significant decrease of the radioactivity concentration in the striatum. Figure 4B shows this decrease for MP-10 (5 mg/kg). At baseline, a maximum average S/C-1 ratio of 2.9 ($n = 2$) was reached at about 32 min after tracer injection, which stayed constant until about 75 min after injection (Table 5). Self-blocking at a dose of 2.5 mg/kg and pretreatment with TP-10 and MP-10 at a dose of 5 mg/kg resulted in a significant reduction of the S/C-1 ratios, from 2.9 at baseline to 1.4 or less after pretreatment (Table 5). Predosing of rats with MP-10 (1 mg/kg) reduced tracer uptake in the striatum by about 14% relative to the tracer uptake in the cerebellum. At a dose of 0.5 mg/kg, the decrease in tracer uptake was about 7%.

Displacement Study. One hour after injection of ^{18}F -JNJ41510417 (40.7 MBq), MP-10 was injected intravenously at a dose of 3 mg/kg in a rat. The intensity of the signal in the striatum significantly decreased after injection of the chase compound (Fig. 4D). ^{18}F -JNJ41510417 continuously accumulates in the striatum up to 60 min after tracer injection. After injection of the chase compound, the radioactivity decreased to the level of the cortex and cerebellum (Fig. 4C). Injection of the chase resulted in a significant reduction of the S/C-1 ratio from 2.9 before MP-10 injection to 1.0 after injection of the chase.

Small-Animal PET and Ex Vivo Autoradiography in PDE10A KO Mice. After injection of ^{18}F -JNJ41510417, only background radioactivity was observed in the brain of the PDE10A KO mice (Fig. 5, lower image). The WT mouse, on the other hand, showed clear brain uptake with a high radioactivity concentration in the striatum (Fig. 5, upper image). High uptake was also present in the Harderian glands. After an initial peak in all regions, radioactivity was washed out from the striatum of the KO mice and the cerebellum of KO and WT mice, whereas a continuous accumulation of ^{18}F -JNJ41510417 was observed in the striatum of the WT mouse (Fig. 5, graph).

Subsequent to the small-animal PET study, ex vivo autoradiography was performed (75 min after tracer injection) on cerebral coronal sections (Fig. 6). Analysis of the autoradiograms showed high tracer uptake in the striatum of the WT mouse. The binding to WT striatum was about 24 times higher than that to KO striatum. There was also some uptake in the cortex of the WT mouse brain, with a striatum-to-cortex ratio of about 14 and a WT cortex-to-KO cortex ratio of about 1.9 (Fig. 6, Table). The

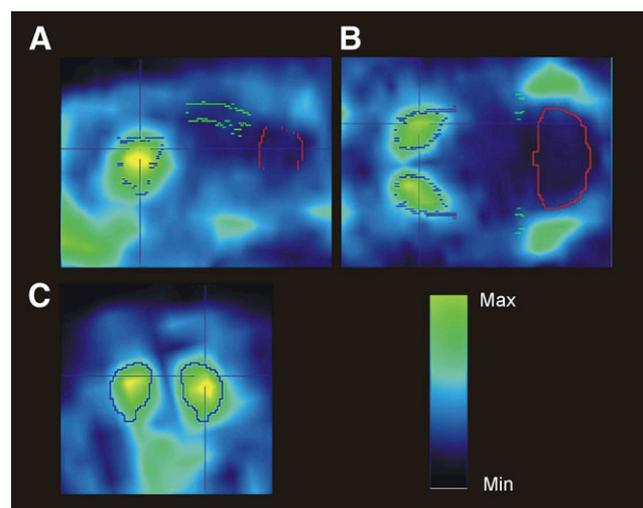


FIGURE 3. Sagittal (A), transversal (B), and coronal (C) sections of rat brain through striatum, cortex, and cerebellum. These are averaged images (60–120 min after tracer injection scaled on SUV 1) of a representative rat injected with 56 MBq of ^{18}F -JNJ41510417. Max = maximum; Min = minimum.

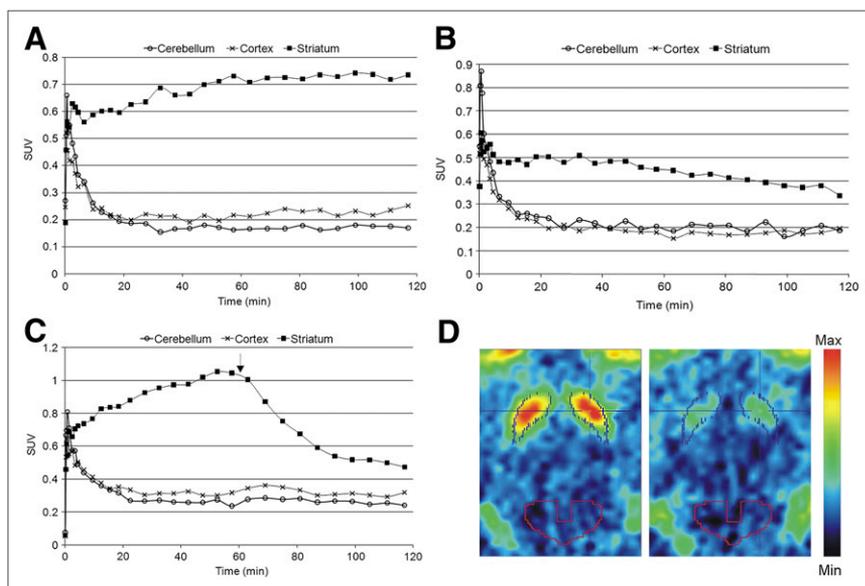


FIGURE 4. Small-animal PET time-activity curves for ^{18}F -41510417 in striatum, cortex, and cerebellum. (A) Untreated baseline scan. (B) Pretreatment experiment: MP-10, 5 mg/kg, was injected subcutaneously 60 min before tracer injection. (C) Chase experiment: MP-10, 3 mg/kg, was injected intravenously (arrow) 60 min after tracer injection. (D) Transversal images corresponding to the chase experiment: averaged image (40–60 min after tracer injection) before chase injection (left) and averaged image (96–120 min after tracer injection) after chase injection (right). Max = maximum; Min = minimum.

uptake in the WT cortex could be partly due to partial-volume effects of the highly radioactive striatum.

DISCUSSION

The aim of this study was to evaluate a potential PET ligand for *in vivo* imaging of the PDE10A enzyme in the brain. From several MP-10 analogs, JNJ41510417 was selected as the most promising candidate. Therefore, this compound was radiolabeled and evaluated *in vivo* in rats and PDE10A KO mice. Rat biodistribution studies showed a significant accumulation of the tracer in the striatum over time, whereas there was a clear washout from the other studied brain regions (cerebellum, cortex, hippocampus) in accordance with the reported intracerebral distribution of PDE10A (2–4). The highest radioactivity concentration in the striatum was 2.6 (SUV, at 60 min after tracer injection;

Table 2), with a maximum striatum-to-cerebellum ratio of 7.0. Compared with other brain radioligands (e.g., ^{18}F -fallypride (25): SUV striatum at 60 min after injection, ~ 4 ; striatum-to-cerebellum ratio, ~ 42), the observed maximal brain concentration is low. In view of the rather high lipophilicity and associated high plasma protein binding of the tracer, the brain uptake is still surprisingly high, suggesting rapid dissociation of the protein-bound fraction on passage of the blood through the brain capillaries. The high plasma protein binding can, however, be a potential limitation of this radioligand because the plasma-free fraction may vary in disease conditions and is an important parameter in kinetic imaging analysis when the specific distribution volume needs to be determined. However, if further studies show that the simplified reference tissue model can be used for kinetic model analyses, normalization to the reference region will effectively correct for inter-subject variations in plasma-free fraction and thus avoid the need to measure this parameter.

Two polar radiometabolites of ^{18}F -JNJ41510417 have been detected in rat plasma. The minor metabolite ^{18}F -JNJ41797444, resulting from the cleavage of the ether bond and loss of the methyl-quinoline group, was not detected in the brain. The major polar metabolite, on the other hand, was detected in the cerebrum and cerebellum (Table 4). ^{18}F -JNJ41510417 probably undergoes oxidative metabolism, generating *N*-dealkylated ^{18}F -JNJ41510417. The polar radiometabolite eluting with the void volume likely is ^{18}F -fluoroethanol or its oxidation products ^{18}F -fluoroacetaldehyde or ^{18}F -fluoroacetic acid. Because ^{18}F -JNJ41510417 is stable *in vitro* in rat brain homogenates, its metabolism presumably occurs in the periphery. Polar radiometabolites entering the brain could complicate the quantification of PDE10A (26). The contribution of the radiometabolite to the brain signal is, however, relatively small and is not

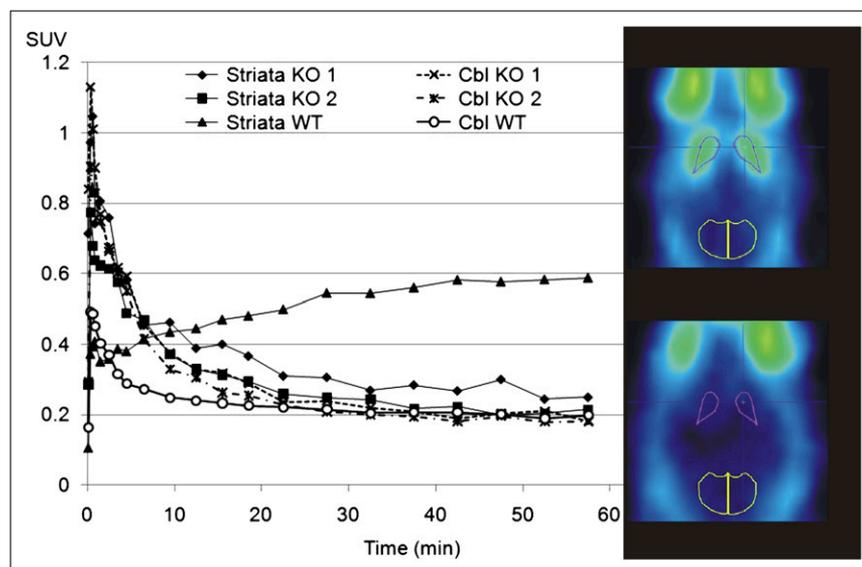
TABLE 5. Summary of Average S/C-1 Ratios

Experiment	Dose blocker (mg/kg)	S/C-1 ratio	% Reduction, compared with baseline*
Baseline ($n = 2$)		2.9	
Self-block ($n = 1$)	2.5	0.4	~ 86
TP-10 ($n = 1$)	5	0.5	~ 83
MP-10 ($n = 2$)	5	1.4	~ 52
	1	2.5	~ 14
	0.5	2.7	~ 7

*Calculation based on S/C-1 ratios.

Data were obtained from baseline small-animal PET imaging of ^{18}F -JNJ41510417 and from pretreatment self-blocking and blocking experiments with TP-10 and MP-10. S/C-1 ratios are averaged values from 32 min after tracer injection (when maximum is reached) until 75 min after tracer injection (when S/C-1 ratio starts decreasing). Data are expressed as mean when $n > 1$.

FIGURE 5. Small-animal PET transversal sections of WT (upper image) and PDE10A KO (lower image) mouse brain injected with ^{18}F -JNJ41510417 (summed images from 40 to 60 min after tracer injection). Regions of interest were drawn on areas corresponding to striatum and cerebellum to obtain time-activity curves of ^{18}F -JNJ41510417 in striatum and cerebellum of 2 PDE10A KO mice and 1 WT mouse. Cbl = cerebellum.



reflected in the in vivo time-activity curves of regions with low activity of PDE10A such as the cerebellum. The fraction of polar radiometabolites detected in cerebellum is comparable to that observed in plasma and higher than that observed in cerebrum. The latter can be explained by the large amount of specifically bound tracer in the striatum, thus enriching the total fraction of intact tracer in the cerebrum. Radiometabolite analysis of the cerebrum and cerebellum of PDE10A KO mice—thus in the absence of specific binding—showed that the fraction of radiometabolites in the cerebellum is identical to that of the cerebrum (results not shown). These findings, together with the fact

that PDE10A is expressed at a low level in the cerebellum, suggest that a reference tissue kinetic model (27) could be used for kinetic model analyses and estimation of binding potential values for the striatum. However, a validation of this model by sampling and measuring metabolite-corrected arterial input functions is needed to ascertain the validity of a reference tissue model and to determine whether even a simplified reference tissue model is appropriate. Because no skull uptake was observed in small-animal PET experiments, the tracer is probably not defluorinated in vivo in rats. Defluorination would result in binding of free ^{18}F -fluoride to bone and skull, resulting in inaccurate quantification of radiotracer binding in the brain due to partial-volume effects of the high amount of radioactivity in the skull. Species differences in susceptibility to radiodefluorination exist for many tracers. Although less extensive metabolism is generally expected in higher species (20), further in vivo evaluation in humans will be necessary to check the extent of defluorination.

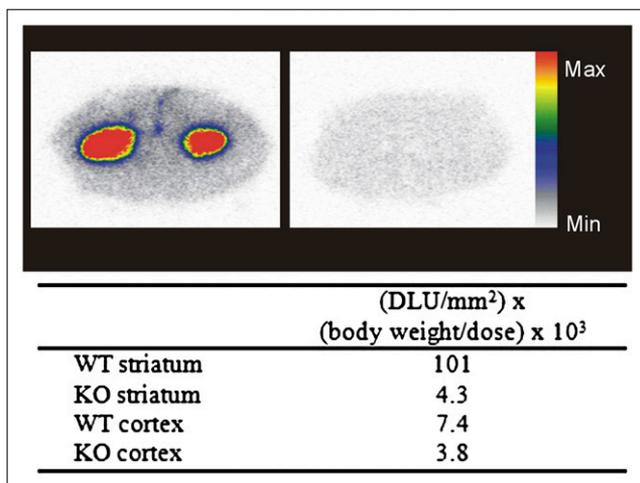


FIGURE 6. Ex vivo autoradiograms of coronal cerebral sections (30 μM) from WT mouse brain (left) and PDE10A KO mouse brain (right) 75 min after injection with ^{18}F -JNJ41510417. Binding is expressed as digital light units per mm^2 (DLU/ mm^2) for brain regions of interest. Values are corrected for injected dose and weight of animal. Max = maximum; Min = minimum.

Baseline small-animal PET studies in normal rats confirmed the results of the biodistribution studies. Time-activity curves showed increasing tracer accumulation in the striatum and clear washout from other brain regions. The tracer shows relatively slow kinetics, which may require longer acquisitions in clinical applications to obtain robust distribution volumes. Relatively high striatum-to-cerebellum ratios resulted in good signal-to-noise images in vivo. Self-blocking studies and blocking studies with the PDE10A-specific inhibitors TP-10 and MP-10 (1,16–18,24) showed a dose-dependent decrease of the in vivo binding of ^{18}F -JNJ41510417. A displacement experiment with MP-10 demonstrated that binding of ^{18}F -JNJ41510417 to PDE10A is reversible. The experiment using PDE10A KO and WT mice confirmed that ^{18}F -JNJ41510417 binds specifically to PDE10A in the striatum.

CONCLUSION

To our knowledge, this is the first report of a successful radioligand for in vivo imaging of the PDE10A enzyme using PET. Biodistribution studies and small-animal PET in rats and PDE10A KO mice demonstrated that ¹⁸F-JNJ41510417 shows reversible and specific binding to PDE10A in the striatum. Further clinical evaluation of this radioligand is warranted to investigate its potential use as a PDE10A PET ligand for human brain imaging.

ACKNOWLEDGMENTS

We thank Peter Vermaelen and Ann Van Santvoort from the Department of Nuclear Medicine (K.U. Leuven) for their assistance in the small-animal PET studies and Julie Cornelis (Laboratory for Radiopharmacy, K.U. Leuven) for her skillful help with the animal experiments. This research was funded by Johnson & Johnson Pharmaceutical Research and Development.

REFERENCES

- Kehler J, Ritzén A, Rodriguez Greve D. The potential therapeutic use of phosphodiesterase 10 inhibitors. *Expert Opin Ther Patents*. 2007;17:147–158.
- Fujishige K, Kotera J, Omori K. Striatum- and testis-specific phosphodiesterase PDE10A: isolation and characterization of a rat PDE10A. *Eur J Biochem*. 1999;266:1118–1127.
- Seeger TF, Bartlett B, Coskran TM, et al. Immunohistochemical localization of PDE10A in the rat brain. *Brain Res*. 2003;985:113–126.
- Coskran TM, Morton DG, Menniti FS, et al. Immunohistochemical localization of phosphodiesterase 10A, PDE10A, in multiple mammalian species. *J Histochem Cytochem*. 2006;54:1205–1213.
- Siuciak JA, Chapin DS, Harms JF, et al. Inhibition of the striatum-enriched phosphodiesterase PDE10A: a novel approach to the treatment of psychosis. *Neuropharmacology*. 2006;51:386–396.
- Siuciak JA, McCarthy SA, Chapin DS, et al. Genetic deletion of the striatum-enriched phosphodiesterase PDE10A: evidence for altered striatal function. *Neuropharmacology*. 2006;51:374–385.
- Siuciak JA, McCarthy SA, Chapin DS, Martin AN, Harms JF, Schmidt CJ. Behavioral characterization of mice deficient in the phosphodiesterase-10A (PDE10A) enzyme on a C57/B16N congenic background. *Neuropharmacology*. 2008;54:417–427.
- Menniti FS, Chappie TA, Humphrey JM, Schmidt CJ. Phosphodiesterase 10A inhibitors: a novel approach to the treatment of the symptoms of schizophrenia. *Curr Opin Investig Drugs*. 2007;8:54–59.
- Menniti FS, Faraci WS, Schmidt CJ. Phosphodiesterases in the CNS: targets for drug development. *Nat Rev Drug Discov*. 2006;5:660–670.
- Halene TB, Siegel SJ. PDE10 inhibitors in psychiatry: future options for dementia, depression and schizophrenia? *Drug Discov Today*. 2007;12:870–878.
- Lee C-M, Farde L. Using positron emission tomography to facilitate CNS drug development. *Trends Pharmacol Sci*. 2006;27:310–316.
- Cunningham VJ, Parker CA, Rabiner EA, Gee AD, Gunn RN. PET studies in drug development: methodological considerations. *Drug Discov Today*. 2005;2:311–315.
- Passchier J, Gee A, Willemsen A, Vaalburg W, van Waarde A. Measuring drug-related receptor occupancy with positron emission tomography. *Methods*. 2002;27:278–286.
- Wong DF, Tauscher J, Gründer G. The role of imaging in proof of concept for CNS drug discovery and development. *Neuropsychopharmacol*. 2009;34:187–203.
- Tu Z, Xu J, Jones LA, Li S, Mach RH. Carbon-11 labeled papaverine as a PET tracer for imaging PDE10A: radiosynthesis, in vitro and in vivo evaluation. *Nucl Med Biol*. 2010;37:509–516.
- Verhoest PR, Chapin DS, Corman M, et al. Discovery of a novel class of phosphodiesterase 10A inhibitors and identification of clinical candidate 2-[4-(1-methyl-4-pyridin-4-yl-¹H-pyrazol-3-yl)-phenoxy]methyl]-quinoline (PF-2545920) for the treatment of schizophrenia. *J Med Chem*. 2009;52:5188–5196.
- Walker MA. Discovery of PDE10A inhibitor, PF-2545920. *Drug Discov Today*. 2010;15:79.
- Verhoest PR, Helal CJ, Hoover DJ, Humphrey JM, inventors; Pfizer Products, Inc., USA, assignee. Heteroaromatic quinoline compounds as phosphodiesterase inhibitors, their preparation, pharmaceutical compositions, and use in therapy. World patent WO 2006072828 A2. July 13, 2006.
- Waterhouse RN. Determination of lipophilicity and its use as a predictor of blood-brain barrier penetration of molecular imaging agents. *Mol Imaging Biol*. 2003;5:376–389.
- Pike VW. PET radiotracers: crossing the blood-brain barrier and surviving metabolism. *Trends Pharmacol Sci*. 2009;30:431–440.
- Ertl P, Rohde B, Selzer P. Fast calculation of molecular polar surface area directly from SMILES. Novartis Pharma AG, ChemInformatics, Basel, Switzerland. Available at: <http://www.daylight.com/meetings/emug00/Ertl/index.html>. Accessed July 27, 2010.
- Ertl P, Rohde B, Selzer P. Fast calculation of molecular polar surface area as a sum of fragment-based contributions and its application to the prediction of drug transport properties. *J Med Chem*. 2000;43:3714–3717.
- Casteels C, Vermaelen P, Nuyts J, et al. Construction and evaluation of multitracer small-animal PET probabilistic atlases for voxel-based functional mapping of the rat brain. *J Nucl Med*. 2006;47:1858–1866.
- Schmidt CJ, Chapin DS, Cianfrogna J, et al. Preclinical characterization of selective phosphodiesterase 10A inhibitors: a new therapeutic approach to the treatment of schizophrenia. *J Pharmacol Exp Ther*. 2008;325:681–690.
- Mukherjee J, Yang Z-Y, Das MK, Brown T. Fluorinated benzamide neuroleptics-III: development of (S)-N-[(1-allyl-2-pyrrolidinyl)methyl]-5-(3-[¹⁸F]fluoropropyl)-2,3-dimethoxybenzamide as an improved dopamine D-2 receptor tracer. *Nucl Med Biol*. 1995;22:283–296.
- Zoghbi SS, Shetty HU, Ichise M, et al. PET imaging of the dopamine transporter with ¹⁸F-FECNT: a polar radiometabolite confounds brain radioligand measurements. *J Nucl Med*. 2006;47:520–527.
- Ichise M, Liow JS, Lu JQ, et al. Linearized reference tissue parametric imaging methods: application to [¹¹C]DASB positron emission tomography studies of the serotonin transporter in human brain. *J Cereb Blood Flow Metab*. 2003;23:1096–1112.



The Journal of
NUCLEAR MEDICINE

Preclinical Evaluation of ^{18}F -JNJ41510417 as a Radioligand for PET Imaging of Phosphodiesterase-10A in the Brain

Sofie Celen, Michel Koole, Meri De Angelis, Ivan Sannen, Satish K. Chitneni, Jesus Alcazar, Stefanie Dedeurwaerdere, Dieder Moechars, Mark Schmidt, Alfons Verbruggen, Xavier Langlois, Koen Van Laere, José Ignacio Andrés and Guy Bormans

J Nucl Med. 2010;51:1584-1591.

Published online: September 16, 2010.

Doi: 10.2967/jnumed.110.077040

This article and updated information are available at:

<http://jnm.snmjournals.org/content/51/10/1584>

Information about reproducing figures, tables, or other portions of this article can be found online at:

<http://jnm.snmjournals.org/site/misc/permission.xhtml>

Information about subscriptions to JNM can be found at:

<http://jnm.snmjournals.org/site/subscriptions/online.xhtml>

The Journal of Nuclear Medicine is published monthly.
SNMMI | Society of Nuclear Medicine and Molecular Imaging
1850 Samuel Morse Drive, Reston, VA 20190.
(Print ISSN: 0161-5505, Online ISSN: 2159-662X)

© Copyright 2010 SNMMI; all rights reserved.

The logo for the Society of Nuclear Medicine and Molecular Imaging (SNMMI) features the letters 'S', 'N', 'M', and 'I' in a white, sans-serif font, each contained within a red square. The squares are arranged in a 2x2 grid.
SOCIETY OF
NUCLEAR MEDICINE
AND MOLECULAR IMAGING