

# Accuracy of PET for Diagnosis of Solid Pulmonary Lesions with $^{18}\text{F}$ -FDG Uptake Below the Standardized Uptake Value of 2.5

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Benign and malignant pulmonary lesions usually are differentiated by  $^{18}\text{F}$ -FDG PET with a semiquantitative  $^{18}\text{F}$ -FDG standardized uptake value (SUV) of 2.5. However, the frequency of malignancies with an SUV of <2.5 is significant, and pulmonary nodules with low  $^{18}\text{F}$ -FDG uptake often present diagnostic challenges. **Methods:** Among 360 consecutive patients who underwent  $^{18}\text{F}$ -FDG PET to evaluate pulmonary nodules found on CT, we retrospectively analyzed 43 who had solid pulmonary lesions (excluding lesions with ground-glass opacity, infiltration, or benign calcification) with an SUV of <2.5. The uptake of  $^{18}\text{F}$ -FDG was graded by a visual method (absent, faint, moderate, or intense) and 2 semiquantitative methods (SUV and contrast ratio [CR]). Final classification was based on histopathologic findings or at least 6 mo of clinical follow-up. **Results:** We found 16 malignant (diameter, 8–32 mm) and 27 benign (7–36 mm) lesions. When faint visual uptake was the cutoff for positive  $^{18}\text{F}$ -FDG PET results, the receiver-operating-characteristic (ROC) analysis correctly identified all 16 malignancies and yielded false-positive results for 10 of 27 benign lesions. Sensitivity was 100%, specificity was 63%, and the positive and negative predictive values were 62% and 100%, respectively. When an SUV of 1.59 was the cutoff for positive  $^{18}\text{F}$ -FDG PET results, the ROC analysis revealed 81% sensitivity, 85% specificity, and positive and negative predictive values of 77% and 89%, respectively. At a cutoff for positive  $^{18}\text{F}$ -FDG PET results of a CR of 0.29, the ROC analysis revealed 75% sensitivity, 82% specificity, and positive and negative predictive values of 71% and 85%, respectively. The areas under the curve in ROC analyses did not differ significantly among the 3 analyses (visual, 0.84; SUV, 0.81; and CR, 0.82). Analyses of intra- and interobserver variabilities indicated that visual and SUV analyses were quite reproducible, whereas CR analysis was poorly reproducible. **Conclusion:** These results suggested that for solid pulmonary lesions with low  $^{18}\text{F}$ -FDG uptake, semiquantitative approaches do not improve the accuracy of  $^{18}\text{F}$ -FDG PET over that obtained with visual analysis. Pulmonary

lesions with visually absent uptake indicate that the probability of malignancies is very low. In contrast, the probability of malignancy in any visually evident lesion is about 60%.

**Key Words:** lung cancer; PET;  $^{18}\text{F}$ -FDG; pulmonary nodules; CT  
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**P**ET has been used widely with  $^{18}\text{F}$ -FDG to differentiate malignant from benign pulmonary lesions. The intensity of  $^{18}\text{F}$ -FDG uptake by malignant tumors is influenced by various factors, including biologic nature and lesion size. Relatively large, rapidly growing, and metabolically active lesions are usually obvious on  $^{18}\text{F}$ -FDG PET. In contrast, slowly growing, well-differentiated, or small lesions exhibit little or no accumulation (1). A ground-glass appearance on CT typically represents bronchioalveolar carcinoma with either negative or very low  $^{18}\text{F}$ -FDG uptake (2). However,  $^{18}\text{F}$ -FDG uptake in solid malignant nodules also can be absent or low, thus providing diagnostic challenges.

A standardized uptake value (SUV) of 2.5 generally has been used as a cutoff value for diagnosing pulmonary malignancies with  $^{18}\text{F}$ -FDG PET (3). However, 1 study indicated that the sensitivity of this SUV cutoff was lower than that of visual assessment (4). Some authors have recommended using visual evaluation rather than the SUV for small solitary pulmonary nodules (5), suggesting that the classical SUV criterion of 2.5 is inappropriate for diagnosing malignancies with low  $^{18}\text{F}$ -FDG uptake (4). Another study also indicated that the contrast ratio (CR), an index of relative tracer uptake of lesions versus background lung activity, is superior to the SUV for differentiating pulmonary malignancies (6). Thus, a reliable analytic method for discriminating lung lesions with low  $^{18}\text{F}$ -FDG uptake has not been established. Likewise, a relationship between the intensity of  $^{18}\text{F}$ -FDG uptake and a diagnosis of solid pulmonary lesions with low  $^{18}\text{F}$ -FDG uptake has not been confirmed.

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In the present study, we examined the characteristics of solid nodules or masses with an  $^{18}\text{F}$ -FDG SUV of  $<2.5$  and the diagnostic ability of  $^{18}\text{F}$ -FDG PET to differentiate benign from malignant lung diseases both visually and semiquantitatively.

## MATERIALS AND METHODS

### Patients

Patients were identified from a retrospective review of the PET center database at Tokyo Women's Medical University. Among 360 individuals who had a solitary pulmonary lesion and who presented between May 2003 and March 2005 (27 men; age [mean  $\pm$  SD],  $65 \pm 11$  y; range, 38–85 y), 43 fulfilled the following conditions for inclusion in the present study: chest CT scan available, solid nodules or masses seen on CT (excluding lesions with ground-glass appearance, infiltration, or typical benign calcification), a lesion  $^{18}\text{F}$ -FDG SUV of  $<2.5$ , and a definitive diagnosis (benign or malignant) determined by pathologic analysis or at least 6 mo of follow-up by chest radiograph or CT. A lesion that disappeared within the 6-mo follow-up period was classified as benign. We used SUVs from the original PET scan reports to select the study participants because we have routinely reported SUVs for visually detectable lesions as measured by the method used in this study. Two experienced radiologists independently reviewed all CT scans and measured maximum lesion diameters. Any disagreement was resolved by consensus. Prior malignancy and diabetes were not exclusion criteria, except for a fasting blood sugar concentration of higher than 200 mg/dL at the time of  $^{18}\text{F}$ -FDG PET.

In addition, we analyzed a selection of studies with original SUVs of  $<3.0$  to verify whether the optimal cutoff values would differ from those obtained in studies with SUVs of  $<2.5$ .

### $^{18}\text{F}$ -FDG PET

Patients fasted for at least 5 h before receiving an intravenous injection of  $^{18}\text{F}$ -FDG (3.7 MBq/kg of body weight). Approximately 60 min later, PET was undertaken by use of a dedicated full-ring lutetium oxyorthosilicate (LSO) scanner (ECAT ACCEL; Siemens) with a transaxial spatial resolution of 6.3 mm at full width at half maximum. Attenuation was corrected by standard transmission scanning with  $^{68}\text{Ge}$  sources. Transmission scans were acquired for 1 min and emission scans were acquired for 2 min per bed position in the 3-dimensional mode from the skull base to the midthigh level. Images were reconstructed by use of ordered-subset expectation maximization (OSEM) with 2 iterations and 8 subsets, a  $128 \times 128$  matrix, and postsMOOTHING with a gaussian filter.

### Data Analysis

The  $^{18}\text{F}$ -FDG PET scans were analyzed visually and semiquantitatively by 2 independent observers, who also performed the CT examinations and who were also unaware of the definitive diagnosis. Lesions on CT images were localized at the time of PET analysis. The intensity of  $^{18}\text{F}$ -FDG uptake by pulmonary lesions relative to the background activity in the uninvolved adjacent lung parenchyma and the mediastinum was assessed visually, and the intensity was scored with a 4-point scale (absent, faint, moderate, or intense) modified from a previously reported method (7) as follows: absent, not visible on the image display; faint, less intense than mediastinal blood-pool activity; moderate,

equal in intensity to mediastinal blood-pool activity; and intense, more intense than mediastinal blood-pool activity. Scans were analyzed semiquantitatively by use of the SUV and the CR (6) as indices of  $^{18}\text{F}$ -FDG uptake. Spheric regions of interest (ROIs) were placed over lesions visible on PET images, on simultaneously displayed axial, coronal, and sagittal tomograms. The ROIs of lesions that were invisible on PET images were located by use of the corresponding CT images. The highest activity within an ROI was measured, and the SUV was determined as the highest activity concentration per injected dose per body weight (kg) after correction for radioactive decay. The CR was determined by measuring the highest activity in the tumor ROI (T) and in the contralateral normal lung ROI (N) and was calculated as  $(T - N)/(T + N)$  for each lesion (6).

### Statistical Analysis

Data are expressed as mean  $\pm$  SD. Three datasets for the same lesion from 2 readers were averaged, and the mean values were used for further analyses. Receiver-operating-characteristic (ROC) curves for visual scores, the SUV, and the CR were derived and evaluated by comparing the areas under the curves. The sensitivity, specificity, and positive and negative predictive values of the 3 analyses were determined at the optimal cutoff values by use of the ROC curves. Unpaired *t* tests were used to examine normally distributed continuous variables, and  $\chi^2$  analyses were used to assess differences in frequencies. The intra- and interobserver variabilities of each method were determined by use of the Cohen  $\kappa$ -statistic for visual scores and the coefficient of variation (CV) for the SUV and the CR. The CV was calculated by dividing the SD by the mean of the 2 repeated measurements, and the root-mean-square values of these CVs represented the overall intra- and interobserver variabilities. A *P* value of  $<0.05$  was considered significant.

## RESULTS

### Malignant and Benign Lesions

Table 1 summarizes the clinical,  $^{18}\text{F}$ -FDG PET, and histologic findings for the 43 lesions. Sixteen (37%) were malignant, and 27 were benign. The maximum diameters did not differ significantly between malignant and benign lesions ( $15 \pm 6$  mm, with a range of 8–32 mm, and  $15 \pm 8$  mm, with a range of 7–36 mm, respectively). The prevalence of small lesions ( $\leq 10$  mm) also did not differ significantly between malignant and benign lesions (18.8% and 29.6%, respectively). All 16 malignancies were histologically confirmed primary lung cancers (13 adenocarcinomas, 1 squamous cell carcinoma, 1 small cell carcinoma, and 1 large cell carcinoma). The adenocarcinomas were classified as either well differentiated ( $n = 8$ ) or moderately differentiated ( $n = 5$ ), and the maximum diameter ranged from 10 to 32 mm ( $16.5 \pm 5.4$  mm). Seven of the 27 benign lesions also were confirmed by histologic analysis (2 hamartomas and 5 tuberculomas). For the remaining 20 benign lesions, the median duration of clinical follow-up for lesions that disappeared or decreased in size ( $n = 10$ ) was 15.5 mo (range, 3–21 mo), and for those with no change ( $n = 10$ ), this duration was 16 mo (range, 6–24 mo).

**TABLE 1**  
Clinical, Scintigraphic, and Histologic Findings

Lesion	Size on CT (mm)	Location	Intensity of $^{18}\text{F}$ -FDG uptake determined by:			Pathologic or FU findings	FU period (mo)
			Visual analysis	SUV	CR		
1	13	RML	Faint	1.25	0.16	Adenoca (well)	—
2	14	LUL	Faint	1.61	0.37	Adenoca (well)	—
3	15	RUL	Moderate	2.08	0.49	Adenoca (well)	—
4	16	LLL	Faint	1.69	0.21	Adenoca (well)	—
5	17	LLL	Faint	1.92	0.48	Adenoca (well)	—
6	20	RLL	Moderate	1.64	0.45	Adenoca (well)	—
7	20	RLL	Moderate	2.18	0.29	Adenoca (well)	—
8	32	RUL	Moderate	2.29	0.39	Adenoca (well)	—
9	10	LUL	Moderate	1.51	0.36	Adenoca (mod)	—
10	12	LLL	Faint	2.01	0.36	Adenoca (mod)	—
11	15	RLL	Moderate	2.20	0.39	Adenoca (mod)	—
12	15	LUL	Moderate	1.74	0.43	Adenoca (mod)	—
13	16	LLL	Faint	0.97	0.09	Adenoca (mod)	—
14	10	LLL	Faint	1.69	0.32	Squamous cell ca	—
15	8	RUL	Faint	1.60	0.18	Small cell ca	—
16	14	RLL	Faint	1.64	0.29	Large cell ca	—
17	12	LLL	Absent	1.52	0.16	Hamartoma	—
18	28	RML	Absent	0.90	0.03	Hamartoma	—
19	8	RUL	Absent	1.25	−0.02	Tuberculoma	—
20	8	RUL	Faint	2.11	0.28	Tuberculoma	—
21	12	RUL	Faint	0.69	−0.01	Tuberculoma	—
22	15	LUL	Moderate	1.88	0.42	Tuberculoma	—
23	25	RUL	Moderate	1.58	0.30	Tuberculoma	—
24	14	LLL	Absent	1.41	0.25	FU (disappearance)	3
25	15	LLL	Absent	1.05	0.17	FU (disappearance)	14
26	21	LUL	Absent	1.28	0.27	FU (disappearance)	17
27	9	RML	Absent	1.31	0.09	FU (decrease)	13
28	10	RLL	Faint	1.55	0.26	FU (decrease)	19
29	12	RML	Absent	0.65	−0.18	FU (decrease)	19
30	12	RML	Absent	0.81	0.00	FU (decrease)	20
31	15	LUL	Absent	1.13	0.37	FU (decrease)	21
32	15	RLL	Absent	1.59	0.24	FU (decrease)	13
33	33	LLL	Moderate	2.31	0.36	FU (decrease)	6
34	7	RLL	Faint	1.39	0.21	FU (no change)	13
35	9	RUL	Absent	1.22	0.13	FU (no change)	16
36	9	RLL	Absent	0.96	−0.02	FU (no change)	12
37	10	RML	Absent	1.27	0.15	FU (no change)	16
38	12	RUL	Faint	1.39	0.11	FU (no change)	21
39	15	RUL	Absent	1.05	−0.04	FU (no change)	24
40	15	RML	Absent	0.95	0.08	FU (no change)	21
41	16	RUL	Faint	1.95	0.31	FU (no change)	6
42	17	RUL	Faint	1.45	0.29	FU (no change)	12
43	36	RLL	Absent	1.51	0.17	FU (no change)	16

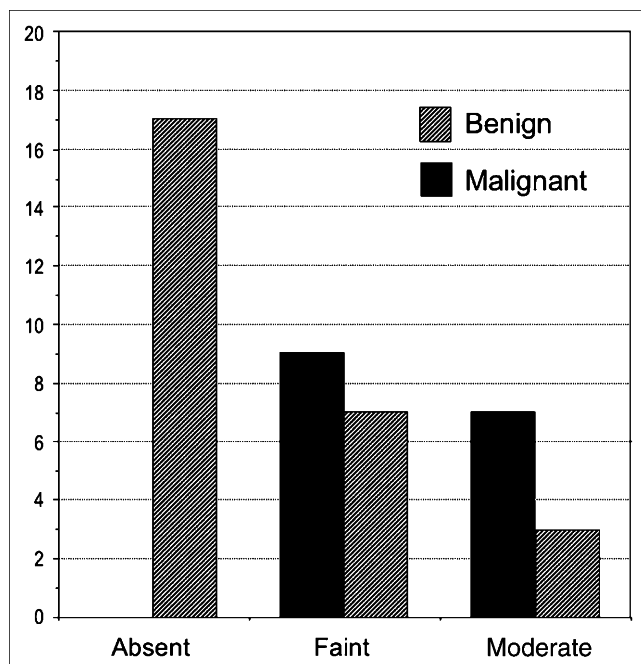
FU = follow-up; RML = right middle lung; adenoca = adenocarcinoma; well = well differentiated; —, no follow-up data; LUL = left upper lung; RUL = right upper lung; LLL = left lower lung; RLL = right lower lung; mod = moderately differentiated; ca = carcinoma.

### Diagnostic Performance of Visual and Semiquantitative Analyses

The frequency distributions of visual uptake scores for benign and malignant lesions are shown in a histogram (Fig. 1). The ROC analysis revealed that when faintly enhanced uptake on visual assessment was taken as the cutoff for positive  $^{18}\text{F}$ -FDG PET results, the visual inspection yielded 100% sensitivity, 63% specificity, and positive and

negative predictive values of 62% and 100%, respectively. At this threshold, visual scores correctly identified 33 of 43 lesions (78%) with low  $^{18}\text{F}$ -FDG uptake (Table 2).

The median SUVs were 1.69 (range, 0.97–2.29) for malignant lesions and 1.31 (range, 0.65–2.31) for benign lesions. When an SUV of 1.59 was used as the cutoff for positive  $^{18}\text{F}$ -FDG PET results, the ROC analysis showed 81% sensitivity, 85% specificity, and positive and negative



**FIGURE 1.** Histogram of visual uptake scores for benign and malignant lesions.

predictive values of 77% and 89%, respectively. At this threshold, the SUV correctly identified 36 of 43 lesions (84%) with low  $^{18}\text{F}$ -FDG uptake (Table 2).

The median CRs were 0.36 (range, 0.09–0.49) for malignant lesions and 0.17 (range, –0.18 to 0.42) for benign lesions. At a cutoff for positive  $^{18}\text{F}$ -FDG PET results of a CR of 0.29, the ROC analysis showed 75% sensitivity, 82% specificity, and positive and negative predictive values of 71% and 85%, respectively. At this threshold, the CR correctly identified 34 of 43 lesions (79%) with low  $^{18}\text{F}$ -FDG uptake (Table 2).

The areas under the ROC curves, which represent overall diagnostic performance, did not differ significantly among

the 3 analytic methods (visual, 0.84; SUV, 0.81; and CR, 0.82) (Fig. 2).

A reanalysis of 49 studies (18 malignant and 31 benign) with original SUVs of  $<3.0$  showed that the optimal cutoff values for visual scores, the SUV, and the CR were faint, 1.59, and 0.29, respectively, values that were identical to those of studies with SUVs of  $<2.5$ .

### Intra- and Interobserver Reproducibilities

The Cohen  $\kappa$ -statistic for intra- and interobserver reproducibilities were 0.62 and 0.65, respectively, indicating good agreement with visual scores of pulmonary lesions with low  $^{18}\text{F}$ -FDG uptake. The root-mean-square values of the CVs for the intraobserver variability were 11% and 221% for the SUV and the CR, respectively, and those for the interobserver variability were 20% and 142%, respectively. These findings indicated that the SUV was quite reproducible whereas the CR was poorly reproducible with respect to the semiquantitative assessment of pulmonary lesions with low  $^{18}\text{F}$ -FDG uptake.

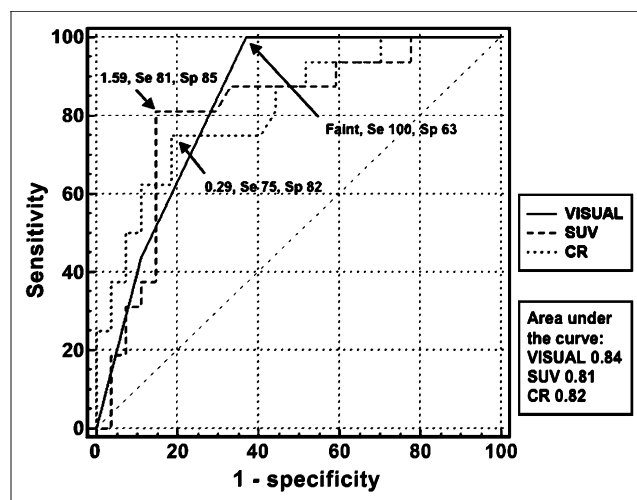
### DISCUSSION

One major finding of the present study was that visual and semiquantitative (SUV and CR) assessments can differentiate malignant from benign pulmonary lesions equally, a finding that is consistent with those of previous reports (3,4,8,9). The present study reconfirmed this fact for lesions with low  $^{18}\text{F}$ -FDG uptake (SUVs of  $<2.5$ ). Another key finding was that a solid pulmonary lesion with visually absent or very low tracer activity (SUVs of  $<1.59$  or CRs of  $<0.29$ ) on  $^{18}\text{F}$ -FDG PET images had a low probability (0%–15%) of malignancy. In contrast, the probability of malignancy was likely to be moderate (62%–77%) when tracer uptake was at least faintly visible or moderate (SUVs of  $\geq 1.59$  or CRs of  $\geq 0.29$ ).

Traditionally, lung lesions have been evaluated visually by comparison with the intensity of uptake in a lesion with

**TABLE 2**  
Diagnostic Accuracy of Visual Assessment, SUV, and CR  
in 43 Patients with Lesion  $^{18}\text{F}$ -FDG SUV of  $<2.5$

Criterion	No. of patients with following tumor diagnosis:		Sensitivity (%)	Specificity (%)
	Malignant	Benign		
Visual score				
At least faint	16	10	100	63
Absent	0	17		
SUV				
≥1.59	13	4	81	85
<1.59	3	23		
CR				
≥0.29	12	5	75	82
<0.29	4	22		
Total	16	27		



**FIGURE 2.** ROC curves for  $^{18}\text{F}$ -FDG PET results analyzed by visual assessment, SUV, and CR. Se = sensitivity (% true-positive rate); Sp = specificity (% true-negative rate).

normal mediastinal activity. That is, if the intensity of uptake is lower than that in the mediastinum, then the lesion is suspected to be benign (9). However, our findings suggested that any lesions visually detectable on  $^{18}\text{F}$ -FDG PET images should be considered carefully for the possibility of malignancy; other clinical (age, smoking history, or other cancer) and radiologic (spiculation, lesion location, and size) factors that influence the likelihood of malignancy also should be taken into consideration (10).

Among the various factors that influence the visibility and uptake of malignant tumors on  $^{18}\text{F}$ -FDG PET images, tissue differentiation of tumors is important (1). Most malignant pulmonary nodules with SUVs of  $<2.5$  are differentiated adenocarcinomas (4). The present study also showed that 81% of the malignant tumors were determined histologically to be differentiated adenocarcinomas. Lesion size is also an important factor (11). The contrast between a tumor and normal lung decreases as the size of the lesion decreases and may even disappear (12) because of partial-volume averaging effects attributable to the limited resolution of a PET scanner (13). The detection of nodules measuring less than 15 mm in diameter is slightly less sensitive than that for lesions larger than 15 mm (14). Correction of the SUV on the basis of lesion size determined from axial CT images may help to improve sensitivity without degrading specificity compared with the use of conventional SUV measurements (11). However, other studies have indicated that the recovery coefficient (measured activity in a lesion divided by true activity) depends not only on lesion size but also on object geometry (15,16). Thus, whether a simple correction of the SUV on the basis of lesion size actually can improve semiquantitative discrimination between benign and malignant pulmonary nodules with low  $^{18}\text{F}$ -FDG uptake remains to be determined.

Other important factors affecting the visibility of target lesions include scintillator type, image reconstruction methodology, and image noise. We used an LSO-based PET scanner, a 3-dimensional acquisition mode, and an OSEM reconstruction method after the administration of  $^{18}\text{F}$ -FDG at 3.7 MBq/kg. Compared with the dose used for a conventional bismuth germanate (BGO) scanner, the dose administered in the present study seems to be rather low. However, compared with a BGO scintillator, an LSO scintillator has a similar attenuation length but 4 times the light output and a decay time 7 times shorter. The coincidence time resolution of the scanner used in the present study (ECAT ACCEL) is substantially narrower (6 ns) than that of BGO-based scanners (10–12 ns). All of these factors are likely to improve the visibility of target lesions on  $^{18}\text{F}$ -FDG PET images because of an improvement in performance and a reduction in image noise accomplished by a limited administered dose.

One study has indicated that the CR is more sensitive than the SUV in diagnosing faintly positive pulmonary nodules when the classical SUV criterion of 2.5 is applied (4). However, the ROC curve analysis in the present study showed that these methods were identical in terms of overall diagnostic performance. Furthermore, the present

study also indicated that the inter- and intraobserver reproducibilities of CR measurements were quite poor. Factors that determine the reproducibility of CR measurements include the maximal SUVs of lesions and the contralateral pulmonary background (6). Because the lesion SUV was quite reproducible in the present study, key reasons for the poor CR reproducibility must have been related to the inconsistent pulmonary background SUV. Indeed, regional pulmonary SUVs differ significantly depending on the sampling location in the lung (17). In addition, the poor CR reproducibility might have been associated with the SDs of SUV measurements of the normal lung. When the tumor SUV was low and within the ranges of the present study, the value overlapped the reconstruction noise in the normal lung. Thus, the CR does not seem to have any advantage over the SUV in diagnosing malignant pulmonary nodules with low  $^{18}\text{F}$ -FDG uptake.

The present study has some limitations. During semiquantitative analysis with only a PET scanner, the ROI location that corresponded to the lesion site was impossible to determine only on PET images when the lesion was invisible. Thus, we selected a nearby location by using corresponding CT slices; this method would have produced some inaccuracies in SUV and CR measurements. This problem can be resolved by using a PET/CT scanner, because the ROI location can be determined easily by use of fused PET and CT images even when  $^{18}\text{F}$ -FDG uptake in lesions is negative. Another limitation may be that not only the SUV but also the visibility of target lesions is dependent on image reconstruction methodology and image noise (18). For example, PET/CT apparently improves the contrast-to-noise ratio of images over that of PET alone because of the noise reduction achieved with CT-based attenuation correction rather than  $^{68}\text{Ge}$ -based attenuation correction. CT-based attenuation correction produces a significantly higher SUV than attenuation correction based on germanium (19). Thus, the optimal cutoff thresholds for visual scores, the SUV, and the CR for differentiating benign from malignant lesions should be determined individually depending on the detector type (BGO, LSO, or germanium oxyorthosilicate), the reconstruction method (filtered backprojection or OSEM), and the scanner (PET or PET/CT). Finally, the present study was a retrospective analysis, and we did not use dual-time-point imaging, which can be potentially valuable in distinguishing benign from malignant lung nodules. One study has indicated that  $^{18}\text{F}$ -FDG activity in cancerous lesions increases whereas benign lung nodules remain relatively stable over time (20). The technique described here may help to improve the accuracy of characterizing lung nodules with  $^{18}\text{F}$ -FDG SUVs of less than 2.5 at the initial scan but requires further investigation.

## CONCLUSION

Our results suggest that the abilities of visual and semiquantitative methods to identify malignancies in solid pulmonary lesions with low  $^{18}\text{F}$ -FDG uptake are equal.

The probability of malignancy for pulmonary lesions with visually absent uptake is very low. In contrast, the probability of any visually obvious lesion being malignant is about 60%.

## REFERENCES

1. Higashi K, Ueda Y, Yagishita M, et al. FDG PET measurement of the proliferative potential of non-small cell lung cancer. *J Nucl Med*. 2000;41:85–92.
2. Higashi K, Ueda Y, Seki H, et al. Fluorine-18-FDG PET imaging is negative in bronchioloalveolar lung carcinoma. *J Nucl Med*. 1998;39:1016–1020.
3. Al-Sugair A, Coleman RE. Applications of PET in lung cancer. *Semin Nucl Med*. 1998;28:303–319.
4. Nomori H, Watanabe K, Ohtsuka T, Naruke T, Suemasu K, Uno K. Visual and semiquantitative analyses for F-18 fluorodeoxyglucose PET scanning in pulmonary nodules 1 cm to 3 cm in size. *Ann Thorac Surg*. 2005;79:984–988.
5. Herder GJ, Golding RP, Hoekstra OS, et al. The performance of <sup>18</sup>F-fluorodeoxyglucose positron emission tomography in small solitary pulmonary nodules. *Eur J Nucl Med Mol Imaging*. 2004;31:1231–1236.
6. Nomori H, Watanabe K, Ohtsuka T, Naruke T, Suemasu K, Uno K. Evaluation of F-18 fluorodeoxyglucose (FDG) PET scanning for pulmonary nodules less than 3 cm in diameter, with special reference to the CT images. *Lung Cancer*. 2004;45:19–27.
7. Vansteenkiste JF, Stroobants SG, Dupont PJ, et al. FDG-PET scan in potentially operable non-small cell lung cancer: do anatomometabolic PET-CT fusion images improve the localisation of regional lymph node metastases? The Leuven Lung Cancer Group. *Eur J Nucl Med*. 1998;25:1495–1501.
8. Gould MK, Maclean CC, Kuschner WG, Rydzak CE, Owens DK. Accuracy of positron emission tomography for diagnosis of pulmonary nodules and mass lesions: a meta-analysis. *JAMA*. 2001;285:914–924.
9. Lowe VJ, Hoffman JM, DeLong DM, Patz EF, Coleman RE. Semiquantitative and visual analysis of FDG-PET images in pulmonary abnormalities. *J Nucl Med*. 1994;35:1771–1776.
10. Swensen SJ, Silverstein MD, Ilstrup DM, Schleck CD, Edell ES. The probability of malignancy in solitary pulmonary nodules: application to small radiologically indeterminate nodules. *Arch Intern Med*. 1997;157:849–855.
11. Hickeson M, Yun M, Matthies A, et al. Use of a corrected standardized uptake value based on the lesion size on CT permits accurate characterization of lung nodules on FDG-PET. *Eur J Nucl Med Mol Imaging*. 2002;29:1639–1647.
12. Weber W, Young C, Abdel-Dayem HM, et al. Assessment of pulmonary lesions with <sup>18</sup>F-fluorodeoxyglucose positron imaging using coincidence mode gamma cameras. *J Nucl Med*. 1999;40:574–578.
13. Bar-Shalom R, Valdivia AY, Blafox MD. PET imaging in oncology. *Semin Nucl Med*. 2000;30:150–185.
14. Dewan NA, Shehan CJ, Reeb SD, Gobar LS, Scott WJ, Ryschon K. Likelihood of malignancy in a solitary pulmonary nodule: comparison of Bayesian analysis and results of FDG-PET scan. *Chest*. 1997;112:416–422.
15. Hoffman EJ, Huang SC, Phelps ME. Quantitation in positron emission computed tomography: 1. Effect of object size. *J Comput Assist Tomogr*. 1979;3:299–308.
16. Kessler RM, Ellis JR Jr, Eden M. Analysis of emission tomographic scan data: limitations imposed by resolution and background. *J Comput Assist Tomogr*. 1984;8:514–522.
17. Miyauchi T, Wahl RL. Regional 2-[<sup>18</sup>F]fluoro-2-deoxy-D-glucose uptake varies in normal lung. *Eur J Nucl Med*. 1996;23:517–523.
18. Boellaard R, Krak NC, Hoekstra OS, Lammertsma AA. Effects of noise, image resolution, and ROI definition on the accuracy of standard uptake values: a simulation study. *J Nucl Med*. 2004;45:1519–1527.
19. Nakamoto Y, Osman M, Cohade C, et al. PET/CT: comparison of quantitative tracer uptake between germanium and CT transmission attenuation-corrected images. *J Nucl Med*. 2002;43:1137–1143.
20. Zhuang H, Pourdehnad M, Lambright ES, et al. Dual-time-point <sup>18</sup>F-FDG PET imaging for differentiating malignant from inflammatory processes. *J Nucl Med*. 2001;42:1412–1417.



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## Accuracy of PET for Diagnosis of Solid Pulmonary Lesions with $^{18}\text{F}$ -FDG Uptake Below the Standardized Uptake Value of 2.5

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