

Characterization of a $^{67}\text{Ga}/^{68}\text{Ga}$ Radiopharmaceutical for SPECT and PET of *MDR1* P-Glycoprotein Transport Activity In Vivo: Validation in Multidrug-Resistant Tumors and at the Blood–Brain Barrier

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Overexpression of multidrug resistance (*MDR1*) P-glycoprotein (Pgp) remains an important barrier to successful chemotherapy in cancer patients and impacts the pharmacokinetics of many important drugs, thus evoking a need to noninvasively interrogate Pgp transport activity in vivo. **Methods:** Cell tracer transport experiments as well as mouse biodistribution and microPET imaging studies were performed to characterize a nonmetabolized gallium(III) complex, gallium(III)-(bis(3-ethoxy-2-hydroxybenzylidene)-*N,N'*-bis(2,2-dimethyl-3-amino-propyl)ethylenediamine) (Ga-[3-ethoxy-ENBDMP])⁺, as a candidate SPECT (^{67}Ga) and generator-produced PET (^{68}Ga) radiopharmaceutical recognized by *MDR1* Pgp. **Results:** The ^{67}Ga -complex showed high membrane potential-dependent accumulation in drug-sensitive KB3-1 cells and modulator-reversible low accumulation in MDR KB8-5 cells. In KB8-5 cells, the median effective concentrations (EC₅₀) of MDR modulators LY335979, PSC 833, and cyclosporin A were 69 nmol/L, 1 $\mu\text{mol/L}$, and 3 $\mu\text{mol/L}$, respectively. Using a variety of cells stably expressing *MDR1* Pgp, multidrug resistance-associated proteins (*MRP1*–*MRP6*), or the breast cancer resistance protein (BCRP/MXR), the ^{67}Ga -complex was shown to be readily transported by *MDR1* Pgp and, to a much lesser extent, by *MRP1*, but not *MRP2*–*MRP6* or BCRP/MXR. In a nude mouse xenograft tumor model, the ^{67}Ga -complex produced a readily detected 3-fold difference between Pgp-expressing tumors and drug-sensitive tumors in the opposite flank. In *mdr1a/1b*(–/–) gene-deleted mice, the ^{67}Ga -complex showed 17-fold greater brain uptake and retention compared with wild-type mice with no net difference in blood pharmacokinetics, consistent with transport in vivo by Pgp expressed at the capillary blood–brain barrier. This could be readily observed with microPET using the ^{68}Ga -complex. Incidentally, wild-type mice showed heart-to-blood ratios of >100

by 1 h after injection and heart-to-liver ratios of 2.2 by 120 min.

Conclusion: Molecular imaging of the functional transport activity of *MDR1* Pgp with ($^{67}/^{68}\text{Ga}$ -[3-ethoxy-ENBDMP])⁺ may enable noninvasive SPECT/PET monitoring of the blood–brain barrier, chemotherapeutic regimens, and *MDR1* gene therapy protocols in vivo. These Pgp-directed properties of the radiopharmaceutical may also translate favorably to myocardial perfusion imaging.

Key Words: *MDR1* P-glycoprotein; multidrug resistance; blood–brain barrier; perfusion imaging; $^{67}\text{Ga}/^{68}\text{Ga}$ radiopharmaceutical

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One of the best-characterized pathways for chemotherapeutic failure in malignancy are transport-mediated multidrug resistance mechanisms due to overexpression of the adenosine triphosphate-binding-cassette (ABC) superfamily of transporters (1). Biochemical and clinical data implicate P-glycoprotein (Pgp; ABCB1), a 170-kDa plasma membrane protein product of the *MDR1* gene (1,2), the multidrug resistance-associated protein (*MRP1*; ABCC1), a related 190-kDa transporter protein (3,4), along with other selected members of the MRP subfamily (*MRP1*–*MRP9*; ABCC1–ABCC9) in drug resistance. Pgp confers resistance by reducing tumor cell content of a variety of structurally and functionally unrelated xenobiotics that are generally cationic through efflux transport, whereas MRPs (*MRP1*–*MRP3*) are thought to efflux transport conjugated or unconjugated generally anionic compounds as well as selected neutral hydrophobic chemotherapeutic agents. In addition, the breast cancer resistance protein (BCRP/MXR; ABCG2), an ABC “half transporter,” is also known to confer resistance to mitoxantrone and anthracyclines (5).

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MDR1 Pgp has been a target for cancer therapy on several fronts. First, reversal of multidrug resistance in tumor cells by nontoxic agents that block the transport activity of Pgp has been an important target for pharmaceutical development (1). When coadministered with a cytotoxic agent, these inhibitors, known as MDR modulators, enhance net accumulation of cytotoxic compounds within the tumor cells. Second, transgenic expression of the *MDR1* gene has been explored for hematopoietic cell protection in the context of cancer chemotherapy (6), wherein Pgp could protect hematopoietic progenitor cells from chemotherapy-induced myelotoxicity. In addition, *MDR1* Pgp and MRP transporters normally are present in a variety of tissues, including intestinal epithelium, choroid plexus epithelium, testes, kidney, liver, adrenal, placenta, as well as capillary endothelial cells of the blood–brain barrier (BBB) (4,7,8). Thus, ABC transporters impact the pharmacokinetics of many common pharmaceuticals, and Pgp modulation is currently under evaluation as a means to improve oral absorption, for example, of chemotherapeutics and HIV-1 protease inhibitors (9,10). Therefore, a noninvasive method for determining Pgp-mediated drug transport activity could be important in predicting oral absorptivity, pharmacokinetics, and penetration of MDR drugs into tumors, brain, germ cells, and the fetus.

In this regard, various SPECT radiopharmaceuticals, exemplified by ^{99m}Tc -sestamibi, ^{99m}Tc -tetrofosmin, ^{99m}Tc -furofosmin, ^{99m}Tc -Q-58, and ^{99m}Tc -COMIBI (^{99m}Tc -tricarboxonyl-tris(2-methoxyisobutyl-isocyanide)) (11,12) have been validated as transport substrates for *MDR1* Pgp, enabling noninvasive imaging of Pgp-mediated transport activity in vivo. However, to exploit the greater sensitivity and quantification capabilities of PET, radiopharmaceuticals of short half-life ($t_{1/2}$) isotopes have been sought. Based on structures of known MDR cytotoxic drugs or classic modulators, several ^{11}C -labeled PET agents, including ^{11}C -colchicine, ^{11}C -verapamil, ^{11}C -daunomycin, and ^{11}C -paclitaxel have been reported (13–17). In addition, ^{18}F -paclitaxel has been synthesized and evaluated in nonhuman primates (18,19). While promising data have been generated, some PET agents suffer from modest radiochemical yields and others from complex pharmacokinetics in vivo mediated, at least in part, by rapid metabolism of the radiolabeled compounds. Earlier, we reported the synthesis and crystal structure of a candidate Ga(III) complex targeting Pgp (20). Herein, we report biochemical, pharmacologic, tissue biodistribution, and brain microPET analysis of this novel radiopharmaceutical with potential applications in both SPECT (^{67}Ga ; $t_{1/2}$ = 72 h) and PET (^{68}Ga ; $t_{1/2}$ = 68 min).

MATERIALS AND METHODS

Solutions and Reagents

All reagents, except as indicated, were obtained from Sigma-Aldrich Chemical Co. Stock solutions of LY335979 (gift of Eli Lilly and Co.), PSC 833 (gift of Mallinckrodt, Inc.), methotrexate, and cisplatin were prepared in dimethyl sulfoxide (DMSO). The

final concentration of DMSO in experimental buffers was <0.5%. Cyclosporin A was purchased as the Cremophor formulation and diluted in saline. The final concentration of Cremophor was <0.1%.

Control solution for transport experiments was a modified Earle's balanced salt solution (MEBSS) containing (mmol/L): 145 Na^+ , 5.4 K^+ , 1.2 Ca^{2+} , 0.8 Mg^{2+} , 152 Cl^- , 0.8 H_2PO_4^- , 0.8 SO_4^{2-} , 5.6 dextrose, 4.0 *N*-(2-hydroxyethyl)piperazine-*N'*-(2-ethanesulfonic acid), and 1% bovine calf serum (v/v), pH 7.4 \pm 0.05. Dulbecco's modified Eagle medium with 1% bovine calf serum was used as a control solution for transport experiments with incubation times of >90 min.

Cell Culture

Monolayers of drug-sensitive human epidermoid carcinoma KB3-1 cells and the colchicine-selected KB8-5 and KB8-5-11 MDR cell lines were grown as previously described (21,22). Growth conditions for stably transfected MCF-7 and MCF-7/*MDR1* cells, H69 and drug-selected H69AR cells, as well as stably transfected LLC/CMV and LLC/cMoat-1 cells, NIH3T3 and 3T3/MRP4 cells, and HEK293 and 293/MRP3, 293/MRP5 and 293/MRP6 cells have been described (22–31). Parental S1M1 and MCF-7 cells and their drug-selected derivative cells, S1M1-80 and MCF-7-AdVp3000, respectively (gift of Dr. Susan Bates), were maintained as described (5,27). ABC transporter status of all cell lines is summarized in Table 1.

TABLE 1
Summary of Cell Lines

Cell line	Cell species	Endogenous Pgp	Introduced human ABC transporter
KB3-1	Human	–	–
KB8-5	Human	–	Pgp +
KB8-5-11	Human	–	Pgp ++
MCF-7	Human	–	–
MCF-7/ <i>MDR1</i>	Human	–	Pgp +
H69	Human	–	–
H69AR	Human	–	MRP1 ++
LLC/CMV	Pig	Pgp +	–
LLC/cMoat-1	Pig	Pgp +	MRP2 +
HEK293	Human	Pgp +	–
293/MRP3	Human	Pgp +	MRP3 +
NIH3T3	Mouse	Pgp +	–
3T3/MRP4	Mouse	Pgp +	MRP4 +
HEK293	Human	Pgp +	–
293/MRP5	Human	Pgp +	MRP5 +
HEK293	Human	Pgp +	–
293/MRP6	Human	Pgp +	MRP6 +
S1M1	Human	Pgp +	–
S1M1-80	Human	Pgp +	BCRP/MXR +
MCF-7	Human	–	–
MCF-7-AdVp3000	Human	–	BCRP/MXR +

ABC transporter status of cell lines. Each cell line is listed by species of origin, endogenous Pgp expression levels, and identity of human ABC transporters introduced by drug selection or transfection into each respective cell line. Moderate levels of transporter expression are represented by +; high levels of expression are signified by ++.

Preparation of $[[3\text{-ethoxy-ENBDMPI}]\text{Ga}]^+ \text{ClO}_4^-$ (**1a**)

The synthesis of **1a** has been described earlier (20). Briefly, a heptadentate precursor ligand, 2-(2-hydroxy-3-ethoxyphenyl)-1,3-bis[4-aza-5-(2'-hydroxy-3'-ethoxyphenyl)-2'',2'''-dimethyl-but-4'-ene-1'-yl]-1,3-imidazolidine (0.14 g, 0.21 mmol), and gallium(III)acetylacetonate (0.08 g, 0.21 mmol) were reacted in methanol for 30 min, followed by addition of potassium perchlorate (0.03 g, 0.21 mmol) dissolved in 0.5 mL of hot water. Slow evaporation of methanol yielded pale yellow needles that were washed with methanol, then washed with ether, and dried to yield **1a** (0.10 g, 0.14 mmol, 67.6%).

Preparation of $^{67/68}\text{Ga(III)}$ complexes (**1b**)

Synthesis of the radiolabeled gallium(III) complex was described earlier (20). ^{67}Ga was obtained as the commercial citrate salt in water (Mallinckrodt Inc.), whereas ^{68}Ga was obtained as GaCl_3 after elution of a Ge/Ga generator (Dupont) with 6N HCl. Both were converted to the respective $^{67/68}\text{Ga}(\text{acetylacetonate})_3$ by reacting with acetylacetone using standard procedures (32). Radiolabeled ^{67}Ga - and ^{68}Ga -complexes were obtained through addition of ^{67}Ga - or ^{68}Ga -(acetylacetonate)₃ to heptadentate Schiff-base precursor ligand in ethanol at 80°C for 30 min. The contents were cooled, diluted with saline to 10% ethanol, and passed through a nylon syringe filter. The desired product was purified on a C₁₈ silica cartridge (Sep-Pak), eluted with saline:ethanol (90:10), assessed for radiopharmaceutical purity by radio-thin-layer chromatography (radio-TLC) on C₁₈ plates (Whatman) using an eluent mixture of methanol:saline (90:10; R_f: 0.47), and found to be ~100% pure.

Cell Transport Studies

Coverslips with confluent cells were used for studies of cell transport and tracer kinetics as previously described (33). Cells on coverslips were removed from culture media and washed for 15–30 s in control solution, then immersed in 60-mm glass or plastic Petri dishes containing 4 mL of loading solution consisting of MEBSS control solution, drug, or vehicle, and ^{67}Ga -complex **1b** was diluted to the desired concentration (8–24 pmol/MBq; 37–74 kBq/mL) (<1% ethanol final). Coverslips with cells were removed after 90 min or at various times for kinetic studies, rinsed 3 times in 25 mL ice-cold control solution for 8 s each to clear extracellular spaces, and placed in 35-mm plastic Petri dishes. For washout studies, cells were first equilibrated in loading solution for 90 min, then washed 3 times in ice-cold control solution, and thereafter incubated in control solution (37°C) for various washout times. Subsequently, cells were again rinsed 3 times in ice-cold control solution and placed in 35-mm plastic Petri dishes. In both protocols, cells were then extracted in 1% sodium dodecyl sulfate with 10 mmol/L sodium borate before protein assay by the bicinchoninic acid analysis (Pierce Chemical Co.) method, using bovine serum albumin as the protein standard. Aliquots of the loading solution and ^{67}Ga -complex **1b** stock solutions also were obtained for standardizing cellular data with the extracellular concentration of **1b**. For cells in suspension culture, transport studies were performed as described (24,27). All cell extracts, ^{67}Ga -complex **1b** stock solutions, and loading solution samples were assayed for γ -activity in a well-type sodium iodide γ -counter (Cobra II; Packard). The absolute concentration of total Ga-complex **1b** in solution was determined from the activity of stock solutions and the specific activity of Ga based on the manufacturer's specifications for ^{67}Ga . Data are reported as fmol Ga-complex **1b** (mg protein)⁻¹ (nmol/L)⁻¹ as previously described (20), with (nmol/L) represent-

ing the total concentration of Ga-complex in the extracellular buffer.

Western Blots

Pgp was detected in crude, enriched membrane preparations from cell lines using Western blotting with monoclonal antibody (mAb) C219 (27). Immune complexes were identified with sheep antimouse antibody (1:2,000 dilution) coupled to horseradish peroxidase using the ECL Western blotting detection system (Amersham Life Sciences).

Biodistribution Studies

All animal procedures were approved by the Washington University Animal Studies Committee. Distribution of ^{67}Ga -complex **1b** in tissues of male 8-wk-old FVB wild-type (WT) and *mdr1a/1b*(-/-) gene-deleted (KO) mice (Taconic) was determined as previously described (22,34). For tumor xenografts, 7- to 8-wk-old male NCr athymic *nu/nu* mice (Taconic) were inoculated subcutaneously with 2×10^6 drug-sensitive KB3-1 cells in the left flank and drug-resistant KB8-5-11 cells in the right flank, and tumors were allowed to grow as described previously (21). ^{67}Ga -Complex dissolved in saline:ethanol (90:10) was diluted in saline for a final concentration of 740 kBq/mL. All mice were anesthetized by metofane inhalation and injected with 74 kBq of radio-tracer via bolus injection through a tail vein. Animals were sacrificed by cervical dislocation at 5, 15, 60, and 120 min after injection (*n* = 2 or 3 each). Blood samples were obtained by cardiac puncture, organs and tumors were then harvested rapidly, and all tissue samples were analyzed for γ -activity.

For analysis of metabolites, mouse tissues harvested 15 min after injection were minced in ethanol:saline (90:10), transferred to conical tubes, and centrifuged. Supernatants, containing the majority of the counts, were removed and analyzed through radio-TLC, revealing ~100% parental complex. Data are expressed as the percentage injected dose (%ID) per gram of tissue ([tissue kBq] [injected kBq]⁻¹ [g tissue]⁻¹ \times 100) or the percentage injected dose per organ ([tissue kBq] [injected kBq]⁻¹ \times 100). While the former are presented herein, please contact the corresponding author for the latter as supplemental tables.

Imaging Studies

Approximately 24-wk-old WT and KO mice were anesthetized with isoflurane inhalation. ^{68}Ga -Complex (7.4 MBq in 100 μL 10% ethanol/saline) was injected via a tail vein into mice positioned in a microPET R4 detector (Concorde Microsystems) and imaged (10-min acquisition time; 1 bed position; filtered-back-projection reconstruction; isotropic image resolution, 1.8 mm) (35). MicroPET images were corrected for decay, but not attenuation.

Analysis

All data points for transport assays were determined from preparations obtained from the same culture. EC₅₀ values (half-maximal effective concentration of drug) for modulators were estimated by a computer fit (σ -Plot; Jandel Scientific) of concentration–effect curves of Ga-complex transport inhibition as described (27,36). From biodistribution time–activity curves, the area under the curve (AUC) was calculated using trapezoidal integration (KaleidaGraph; Synergy Software) and reported as tissue kBq (injected kBq)⁻¹ (g tissue)⁻¹ \times 100 \times minute. Data are generally reported as mean \pm SEM. Pairs were compared by the Student *t* test. *P* values \leq 0.05 were considered significant.

RESULTS

Characterization of (Ga-[3-Ethoxy-ENBDMPI])⁺

Both ⁶⁷Ga, a single-photon radioisotope, and ⁶⁸Ga, a generator-produced positron-emitting radioisotope, were used for radiosynthesis of (^{67/68}Ga-[3-ethoxy-ENBDMPI])⁺ complex **1b** (Fig. 1). Both ⁶⁷Ga- and ⁶⁸Ga-complexes were obtained in 35% radiochemical yield and ~100% radiochemical purity. The total time required for reaction and work-up was compatible with that of short-lived isotopes. The longer-lived ⁶⁷Ga-complex **1b** was tested and found to be stable in human serum at 37°C for up to 24 h. Furthermore, radio-TLC analysis of tissue extracts 15 min after intravenous injection of ⁶⁷Ga-complex **1b** in mice, a time corresponding to initial imaging of tumors and the BBB, demonstrated the existence of only nonmetabolized parental compound in heart, liver, and kidney.

Cellular Transport Kinetics

KB8-5 cells express modest levels of Pgp as documented by Western blot analysis with mAb C219 (Fig. 2A); therefore, *MDR1* Pgp-mediated efflux transport would be expected to result in a decreased net cellular accumulation in KB8-5 cells compared with that of the parental KB3-1 cells. In KB3-1 cells, ⁶⁷Ga-complex **1b** approaches a plateau within 90 min (Fig. 2B). The steady-state value for the ⁶⁷Ga-complex was 292 ± 10 fmol (mg protein)⁻¹ (nmol/L)⁻¹. Given a typical cell water space of 4 μL (mg protein)⁻¹ (37), this indicated an intracellular-to-extracellular ratio of ~75, consistent with concentrative accumulation of the radiotracer within Pgp-negative cells. In contrast, in Pgp-positive KB8-5 cells, steady-state accumulation of the radiotracer was low, resulting in a KB3-1-to-KB8-5 uptake ratio of 104, a functional measure of high interaction of this compound with Pgp. In addition, cellular accumulation of ⁶⁷Ga-complex **1b** in KB3-1 cells at 4°C was minimal over 2 h (1.6 ± 0.2 fmol [mg protein]⁻¹ [nmol/L]⁻¹; $n = 4$), indicating a strong temperature-dependent process for permeation of the radiopharmaceutical. Furthermore, in KB8-5 cells, as expected, washout kinetics of the ⁶⁷Ga-complex at 37°C demonstrated a 10-fold faster rate ($k = 0.20$ min⁻¹) compared with that of KB3-1 cells ($k = 0.02$ min⁻¹) (Fig. 3). However, the overall clearance from KB3-1 cells was slower compared with that of other Pgp-targeted radiophar-

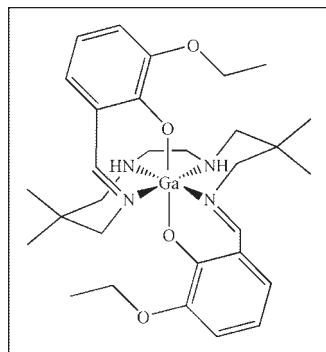


FIGURE 1. Structure of ([3-ethoxy-ENBDMPI]Ga)⁺ (**1a**), a *MDR1* Pgp-targeted gallium(III) Schiff-base complex. In the text, **1a** represents unlabeled Ga-complex and **1b** represents ⁶⁷Ga- or ⁶⁸Ga-complexes.

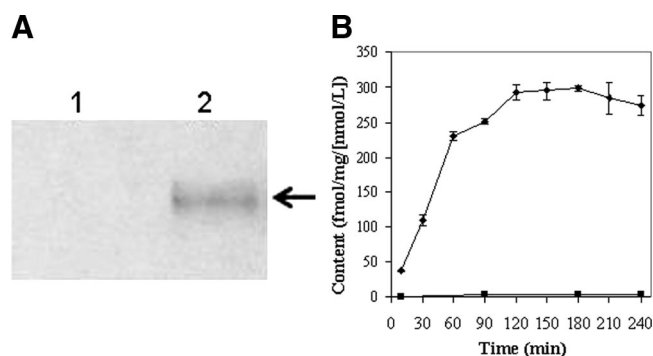


FIGURE 2. (A) Western blot (anti-Pgp mAb) of KB3-1 (lane 1) and KB8-5 (lane 2) cell membranes. Arrow demarcates Pgp. (B) Kinetics of ⁶⁷Ga-complex **1b** accumulation into drug-sensitive KB3-1 (◆) and Pgp-expressing KB8-5 (■) tumor cells. Cells were incubated in MEBSS loading buffer for the indicated times, then washed, and cell-associated activity was determined. Each point represents mean of 3 or 4 determinations; bars represent \pm SEM when larger than the symbol. Plot is representative of 2 independent experiments.

maceuticals such as ^{99m}Tc-sestamibi (27,33). Zero-trans washout was only ~85% complete by 2 h (Fig. 3), consistent with the modestly higher octanol:water partitioning coefficient for Ga-complex **1b** (log *P* = 1.7) versus Tc-sestamibi (log *P* = 1.1). Therefore, residual activity retained within intracellular compartments, even after 2 h, may be due to nonspecific interaction of **1b** with hydrophobic (i.e., membrane) compartments within cells in the absence of Pgp.

To further evaluate the mechanism(s) involved in intracellular accumulation of this tracer, KB3-1 cells were incubated with the ⁶⁷Ga-complex in buffer containing 130 mmol/L K⁺/20 mmol/L Cl⁻ and the potassium ionophore valinomycin (1 μg/mL). Under these conditions, electrical potentials of the mitochondrial membrane ($\Delta\Psi$) and plasma membrane (E_m) are depolarized to zero, thereby eliminating the inward driving force for hydrophobic cationic compounds such as **1b**. Thus, cellular accumulation is expected to decrease, and any net uptake (in-to-out ratio > 1) under these conditions is indicative of nonspecific membrane ab-

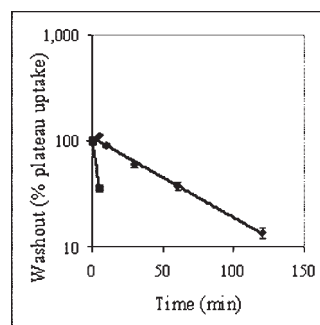


FIGURE 3. Washout kinetics of ⁶⁷Ga-complex **1b** from KB3-1 (◆) and KB8-5 (■) cells at 37°C. Cells were preequilibrated in MEBSS loading buffer (37°C) for 90 min and then transferred to isotope-free buffer. Cell-associated activity as a function of time in washout buffer is shown expressed as percentage of plateau uptake values. Each point represents mean of 3 or 4 determinations; bars represent \pm SEM when larger than the symbol. Note logarithmic scale for y-axis. Solid line represents a curve fit with a single exponential equation (◆, $k = 0.02$; ■, $k = 0.20$).

sorption. Under zero potential conditions, cell tracer accumulation decreased to 185 ± 5.0 fmol (mg protein) $^{-1}$ (nmol/L) $^{-1}$ compared with a control value of 372 ± 13 fmol (mg protein) $^{-1}$ (nmol/L) $^{-1}$ for this experiment, indicating a significant role for membrane potential in localization of the radiotracer as previously described at an earlier time point (20). However, the residual potential-independent retention was equivalent to an apparent in-to-out ratio of 46, indicating, in the absence of Pgp, a substantial level of nonspecific interactions with cellular constituents. Expression of Pgp in KB8-5 cells effectively countered both potential-independent as well as potential-dependent uptake components.

Effect of MDR1 Pgp Modulators on Tracer Accumulation in MDR Cells

Further validation of ^{67}Ga -complex **1b** as a substrate for *MDR1* Pgp was provided by monitoring tracer accumulation in KB8-5 cells in the presence of known Pgp inhibitors. Inhibition of Pgp-mediated transport of the ^{67}Ga -complex would be indicated by enhanced net accumulation of the radiotracer. The Pgp inhibitors cyclosporin A (a cyclic undecapeptide), LY335979 (a difluorocyclopropyl dibenzosuberane (38)), and PSC 833 (a cyclic analog of cyclosporin A (39)) enhanced plateau (90 min) tracer accumulation in KB8-5 cells (Fig. 4). LY335979 was most potent ($\text{EC}_{50} = 69$ nmol/L), cyclosporin was least potent ($\text{EC}_{50} = 3$ $\mu\text{mol/L}$), and PSC 833 demonstrated intermediate potency ($\text{EC}_{50} = 1$ $\mu\text{mol/L}$), consistent with the known potency rank order of these MDR inhibitors (27). Different maximal efficacies were observed at concentrations beyond the customary pharmacologic concentrations for the drugs. As expected, drugs such as methotrexate and cisplatin (100 $\mu\text{mol/L}$), not belonging to the MDR phenotype, did not enhance cell tracer accumulation (data not shown). Furthermore, in KB8-5 cells, the respiratory uncoupler carbonyl cyanide *m*-chlorophenylhydrazone (CCCP), a reagent known to depolarize mitochondrial membrane potential (33), abrogated the LY335979-induced enhancement of the ^{67}Ga -complex (control uptake, 3.8 ± 0.4 fmol [mg protein] $^{-1}$ [nmol/L] $^{-1}$; + CCCP [5 $\mu\text{mol/L}$], 2.9 ± 0.2 ; + LY335979 [1 $\mu\text{mol/L}$], 312.0 ± 8.2 ; + CCCP + LY335979, 50.2 ± 1.9), indicating that inhibition of Pgp with LY335979 allowed the radiopharmaceutical to concentrate in mitochondria in a potential-dependent manner.

Evaluation of ^{67}Ga -Complex **1b** in MCF-7 Cells Transfected with *MDR1* Pgp

Cell lines derived from stepwise selection with MDR drugs, such as KB8-5, may coexpress multiple mechanisms of drug resistance, thereby complicating interpretation of results (40). Thus, we used nondrug-selected MCF-7 cells stably transfected with *MDR1* (29) for confirmation of ^{67}Ga -complex transport. Control MCF-7 cells lack immunodetectable Pgp, whereas MCF-7/*MDR1* cells express readily detected Pgp by Western blotting analysis (29). Therefore, these matched cell lines provided a robust model system for analysis of *MDR1* Pgp without confounding effects of prior

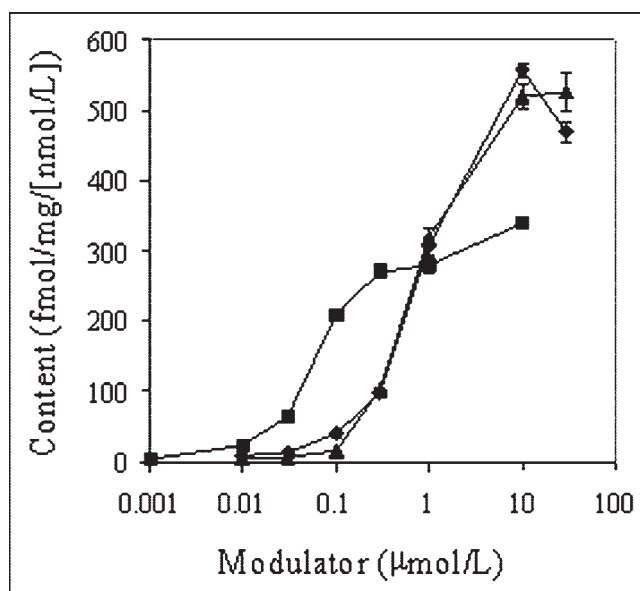


FIGURE 4. Concentration-effect curves of Pgp inhibitors LY335979 (■), cyclosporin A (▲), and PSC 833 (◆) on cellular accumulation of ^{67}Ga -complex **1b** in MDR KB8-5 cells. Cells were incubated for 90 min in loading buffer containing tracer and various concentrations of the indicated inhibitor. Each point represents mean of 4 determinations; bars represent $\pm\text{SEM}$ when larger than the symbol.

exposure to MDR drugs. Compared with parental cells, steady-state accumulation of ^{67}Ga -complex **1b** was almost 40-fold less in MCF-7/*MDR1* cells (155 ± 6.2 fmol [mg P] $^{-1}$ [nmol/L] $^{-1}$ vs. 3.8 ± 0.7 fmol [mg P] $^{-1}$ [nmol/L] $^{-1}$, respectively) (Fig. 5). LY335979 enhanced accumulation of the radiotracer in MCF-7/*MDR1* cells, consistent with blockade of Pgp-mediated efflux, whereas LY335979 showed a minimal effect in MCF-7 cells.

Cross-Reactivity of ^{67}Ga -Complex **1b** with Other Transporters

To further evaluate the sensitivity and selectivity of the ^{67}Ga -complex to report expression of *MDR1* Pgp and to monitor cross-reactivity with other ABC superfamily members, cell accumulation assays were performed in cell lines that express variable levels of *MDR1* Pgp and human multidrug resistance-associated proteins (MRP1–MRP6).

Cellular accumulation of radiotracer over 90 min in control H69 and H69AR cells was found to be 968 ± 57 and 103 ± 2.1 fmol (mg protein) $^{-1}$ (nmol/L) $^{-1}$, respectively (Fig. 6A), indicating a 9-fold decrease in accumulation of the tracer due to overexpression of *MRP1* in H69AR cells. In addition, in H69 cells, depolarization of membrane potential with 130 mmol/L K^+ /20 mmol/L Cl^- buffer plus valinomycin (1 $\mu\text{g/mL}$) decreased tracer content to 203 ± 7.0 fmol (mg protein) $^{-1}$ (nmol/L) $^{-1}$, indicating a substantial nonspecific in-to-out uptake ratio of 51, similar to that observed in KB cells. The Pgp inhibitor LY335979 showed no significant effect on cellular uptake of tracer in either control or H69AR cells. Furthermore, accumulation of the

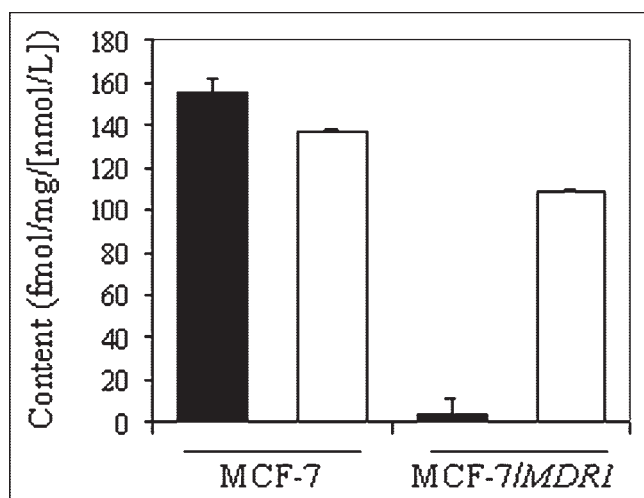


FIGURE 5. Cellular accumulation (90 min) of ^{67}Ga -complex **1b** in control MCF-7 and MCF-7/MDR1 cells in absence (solid bar) and presence (open bar) of MDR modulator LY335979 (1 $\mu\text{mol/L}$). Each bar represents mean of 4 determinations; small bars represent SEM.

^{67}Ga -complex was monitored in cells stably transfected with human *MRP2*, *MRP3*, *MRP4*, *MRP5*, or *MRP6* to evaluate the cross-reactivity with these other MRP homologs. LY335979 enhanced uptake in all of the various control cells and their *MRP2*–*MRP6* transfectants (Fig. 6B), documenting the constitutive expression of endogenous Pgp in these cell lines. No further change in tracer content was observed by concurrent overexpression of human *MRP2*–*MRP5*, indicating a lack of cross-reactivity of the ^{67}Ga -complex with these transporters. Overexpression of human *MRP6* induced a slight increase in tracer content in the absence of LY335979 and an opposing 25% decrease in the

presence of LY335979 ($P < 0.02$), which together were interpreted as biochemically insignificant. Overall, these results indicated that the radiotracer cross-reacted with only MRP1, but to a modest degree (cell uptake ratio = 9) compared with Pgp (cell uptake ratio = 104).

Breast cancer resistance protein (BCRP/MXR) is an ABC half-transporter that is known to dimerize to form an active complex. Thus, to evaluate potential cross-reactivity with BCRP/MXR, ^{67}Ga -complex **1b** was evaluated in human breast carcinoma MCF-7 (control), MCF-7-AdVp3000 (+MXR), colon carcinoma S1M1 (control), and S1M1-80 (+MXR) cells (Fig. 6C). Uptake was found to be slightly lower in MCF-7/MXR cells and higher in S1M1/MXR cells compared with that of the paired parental cells. Furthermore, LY335979 (1 $\mu\text{mol/L}$) enhanced uptake of ^{67}Ga -complex **1b** in MCF-7/MXR cells and control S1M1 cells, whereas it reduced uptake in MCF-7 control cells and S1M1/MXR cells. The ≤ 2 -fold MXR-induced transport differences in opposing directions for each cell type were considered together to be biochemically insignificant. Thus, ^{67}Ga -complex **1b** is not transported significantly by BCRP/MXR.

Probing Pgp Transport Activity in Vivo

We used the biodistribution of ^{67}Ga -complex **1b** to probe Pgp function in a nude mouse tumor xenograft model. Bilateral tumors were produced in opposite flanks of *nu/nu* mice with drug-sensitive KB3-1 cells and multidrug-resistant KB8-5-11 cells (21). The Pgp-expressing KB8-5-11 tumor accumulated less ^{67}Ga -complex **1b** compared with that of the parental tumor in the opposite flank (Table 2), producing a readily detected 3-fold difference by 1 h after injection. Heart, an organ rich in mitochondria, but lacking Pgp, showed a tissue-to-blood ratio of >100 by 1 h after

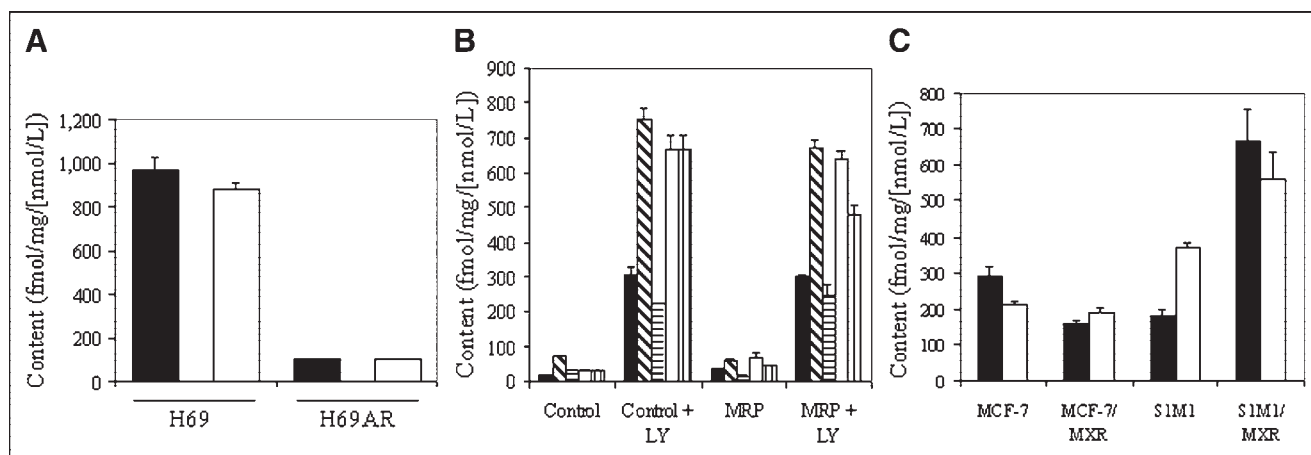


FIGURE 6. Effect of MRP family members on tracer uptake. (A) Cellular accumulation (90 min) of ^{67}Ga -complex **1b** in control H69 and MRP1-expressing H69AR cells in absence (solid bar) and presence (open bar) of MDR modulator LY335979 (1 $\mu\text{mol/L}$). (B) Cellular accumulation (90 min) of ^{67}Ga -complex **1b** in various parental control cells or matched cells expressing MRP2 (■), MRP3 (▨), MRP4 (▩), MRP5 (□), or MRP6 (▤) in absence or presence of MDR modulator LY335979 (1 $\mu\text{mol/L}$). (C) Cellular accumulation (90 min) of ^{67}Ga -complex **1b** in human breast carcinoma (MCF-7) and human colon carcinoma (S1M1) control cells compared with drug-selected cells expressing the half transporter BCRP/MXR in absence (solid bar) and presence (open bar) of MDR modulator LY335979 (1 $\mu\text{mol/L}$). Each bar represents mean of 3 or 4 determinations; small bars represent SEM.

TABLE 2
Biodistribution (%ID/g) of ^{67}Ga -Complex **1b** in Tumor-Bearing Nude Mice

5 min after injection				60 min after injection			
Organ	%ID/g		Tissue-to-blood ratio	Organ	%ID/g		Tissue-to-blood ratio
	Average	Range			Average	Range	
Blood	0.99	0.02		Blood	0.08	0.01	
Heart	6.44	0.00	6.5	Heart	8.33	0.30	105
KB3-1	0.31	0.05	0.3	KB3-1	0.35	0.02	4.4
KB8-5-11	0.21	0.02	0.2	KB8-5-11	0.10	0.02	1.28

Biodistribution of ^{67}Ga -complex **1b** in blood, heart, and tumors of nude mice with subcutaneous KB3-1 and KB8-5-11 xenografts. Mice were injected intravenously with 74 kBq (2 μCi) of ^{67}Ga -complex **1b** and sacrificed at 5 or 60 min after injection; tissues were harvested and counted. Data are expressed as %ID/g tissue at each time point. Values represent mean \pm range ($n = 2$). Also shown are tissue-to-blood ratios at each time point.

injection, as expected for unopposed membrane potential-driven influx of the tracer.

Drug-transporting Pgps (*MDR1* in humans; *mdr1a* in mice) are expressed on luminal surfaces of brain endothelial cells and limit entry of amphipathic compounds into the central nervous system (41). Therefore, these proteins constitute an important component of the BBB. To demonstrate application of the ^{67}Ga -complex as a functional marker of Pgp-mediated transport activity at the BBB, we determined the biodistribution of ^{67}Ga -complex **1b** in WT and *mdr1a*/*1b*($-/-$) (KO) mice. Relative to WT mice, KO mice showed 10-fold more ^{67}Ga -complex **1b** in brain parenchyma 5 min after injection of the complex (Tables 3 and 4). Additionally, the AUC_{5-120} of ^{67}Ga -complex **1b** in KO brain was 17-fold greater than that of WT mice ($P < 0.005$) (Table 5). By contrast, the AUC_{5-120} of the radiotracer in the blood of KO mice was only 1.2-fold that of WT control mice ($P > 0.5$). Because blood flow to the brain does not differ between *mdr1* KO mice and WT mice (42), differences in initial penetration and retention of radiotracer in the brain tissue of KO mice cannot be attributed to differences in cerebral perfusion and blood clearance.

In addition, the liver, a polarized tissue expressing Pgp, showed twice the retained activity (AUC_{5-120}) in KO mice compared with that in WT mice, whereas the heart, a Pgp-negative tissue, did not show any significant difference ($P > 0.5$). The heart-to-liver ratio in WT mice increased to 2.2 by 120 min, whereas in KO mice it was 0.4 (Tables 3 and 4), a low value reflecting the minimal non-Pgp-mediated clearance of ^{67}Ga -complex **1b** from livers of KO mice.

To further evaluate the potential utility of the Ga-complex as a PET radiotracer in vivo, ^{68}Ga -complex **1b** was obtained by reaction of ^{68}Ga -(acetylacetonate)₃ with precursor ligand, purified, and injected via tail vein into mice. Representative microPET images of brain tracer uptake at 5 min after injection in WT and KO mice are shown in Figure 7. Increased penetration and retention of the PET radiotracer were apparent in the brain of KO mice compared with that of WT mice, consistent with the biodistribution data.

DISCUSSION

Though well-characterized for contributing to drug resistance in cancer chemotherapy, *MDR1* Pgp also has emerged as a major contributor to the bioavailability, BBB penetration, and pharmacokinetics of a wide variety of drugs, including HIV protease inhibitors, antidepressants, antiarrhythmics, and new molecular therapeutics such as imatinib (Gleevec) (43,44). Therefore, agents that probe Pgp transport are desired to guide chemotherapeutic choices, drug regimens, and gene therapy strategies before treatment.

Various single-photon agents such as $^{99\text{m}}\text{Tc}$ -sestamibi and $^{99\text{m}}\text{Tc}$ -tetrofosmin, originally developed for myocardial perfusion imaging, have been shown to be robust substrates of *MDR1* Pgp. These agents have been shown to detect transport activity of Pgp in normal human tissues (45), in human tumors (46,47), and in patients treated with MDR modulators that inhibit transport activity of Pgp (1,45,48,49). They can predict chemotherapeutic failure in breast cancer, lung cancer, lymphoma, and osteosarcoma (50–54). However, nonmetabolized PET radiopharmaceuticals designed to interact with *MDR1* Pgp with high specificity would offer alternative probes with enhanced quantitative capacity for molecular imaging of Pgp activity in tissues in vivo.

In considering alternative radiolabels apart from conventional cyclotron-produced PET isotopes, generator-produced ^{68}Ga may offer practical radiopharmacy and distribution advantages. Among Ga-labeled compounds, selected monocationic, hydrophobic Ga(III) complexes with octahedral geometry arising from an N_4O_2 donor core can diffuse into intracellular compartments and, in the absence of Pgp, concentrate as a result of inwardly directed electrochemical driving forces (20). Hydrophobicity and pharmacologic activity can be controlled by variation of the substituents on the periphery of the molecule without impacting the N_4O_2 coordination core. Earlier, we reported the synthesis and structure of $(\text{Ga}[\text{3-ethoxy-ENBDMPI}])^+$ (**1b**) (20). In the present study, we now show that this radiotracer is recognized by *MDR1* Pgp as an efflux transport substrate with

TABLE 3
Biodistribution (%ID/g) of ^{67}Ga -Complex **1b** in FVB WT Mice

Time point (min)	Organ	%ID/g (mean \pm SEM)	Tissue-to-blood ratio
5	Blood	1.29 \pm 0.29	
	Lung	2.11 \pm 0.25	1.6
	Liver	25.58 \pm 0.36	19.8
	Spleen	2.02 \pm 0.12	1.6
	Kidneys	40.27 \pm 3.91	31.2
	Muscle	0.82 \pm 0.07	0.6
	Fat	0.17 \pm 0.05	0.1
	Heart	8.39 \pm 1.22	6.5
	Brain	0.06 \pm 0.01	0.0
	Bone	0.89 \pm 0.11	0.7
	Small intestine	10.71 \pm 1.57	8.3
	Large intestine	3.11 \pm 0.57	2.4
	Skin	0.45 \pm 0.07	0.3
15	Blood	0.43 \pm 0.12	
	Lung	1.72 \pm 0.19	4.0
	Liver	21.12 \pm 2.49	49.1
	Spleen	1.40 \pm 0.13	3.3
	Kidneys	36.15 \pm 0.83	84.1
	Muscle	0.79 \pm 0.14	1.8
	Fat	0.09 \pm 0.01	0.2
	Heart	7.01 \pm 0.54	16.3
	Brain	0.04 \pm 0.00	0.1
	Bone	0.82 \pm 0.06	1.9
	Small intestine	15.57 \pm 0.51	36.2
	Large intestine	2.61 \pm 0.18	6.1
	Skin	0.35 \pm 0.04	0.8
60	Blood	0.10 \pm 0.00	
	Lung	0.94 \pm 0.12	9.4
	Liver	7.58 \pm 0.35	75.8
	Spleen	0.60 \pm 0.09	6.0
	Kidneys	34.40 \pm 4.83	344
	Muscle	0.83 \pm 0.03	8.3
	Fat	0.07 \pm 0.02	0.7
	Heart	6.92 \pm 0.61	69.2
	Brain	0.03 \pm 0.00	0.3
	Bone	0.56 \pm 0.06	5.6
	Small intestine	29.41 \pm 2.21	294
	Large intestine	5.52 \pm 1.60	55.2
	Skin	0.30 \pm 0.04	3.0
120	Blood	0.03 \pm 0.00	
	Lung	0.81 \pm 0.04	27.0
	Liver	3.26 \pm 0.59	108
	Spleen	0.40 \pm 0.01	13.3
	Kidneys	30.66 \pm 2.19	1,022
	Muscle	0.89 \pm 0.06	29.7
	Fat	0.08 \pm 0.01	2.7
	Heart	7.31 \pm 0.47	243
	Brain	0.03 \pm 0.00	1.0
	Bone	0.41 \pm 0.04	13.7
	Small intestine	12.76 \pm 1.67	425
	Large intestine	42.35 \pm 4.55	1,411
	Skin	0.29 \pm 0.01	9.7

Pharmacokinetics of ^{67}Ga -complex **1b** in FVB WT mice. Mice were injected intravenously with 74 kBq (2 μCi) of ^{67}Ga -complex **1b** and sacrificed at 5, 15, 60, or 120 min after injection; blood and tissues were harvested and counted. Data are expressed as %ID/g tissue at each time point. Values represent mean \pm SEM ($n = 3$). Also shown are tissue-to-blood ratios at each time point.

TABLE 4
Biodistribution (%ID/g) of ^{67}Ga -Complex **1b** in FVB *mdr1a/1b*($-/-$) Mice

Time point (min)	Organ	%ID/g (mean \pm range)	Tissue-to-blood ratio
5	Blood	0.65 \pm 0.00	
	Lung	4.30 \pm 0.93	6.6
	Liver	27.24 \pm 0.30	41.9
	Spleen	4.23 \pm 0.26	6.5
	Kidneys	37.02 \pm 3.35	57.0
	Muscle	0.87 \pm 0.05	1.3
	Fat	0.11 \pm 0.02	0.2
	Heart	8.62 \pm 1.27	13.3
	Brain	0.61 \pm 0.09	0.9
	Bone	1.17 \pm 0.15	1.8
	Small intestine	7.90 \pm 1.25	12.2
	Large intestine	2.48 \pm 0.39	3.8
	Skin	0.57 \pm 0.16	0.9
15	Blood	0.30 \pm 0.13	
	Lung	4.75 \pm 1.11	15.8
	Liver	21.69 \pm 3.47	72.3
	Spleen	4.93 \pm 1.27	16.4
	Kidneys	37.87 \pm 4.27	126
	Muscle	1.15 \pm 0.23	3.8
	Fat	0.24 \pm 0.05	0.8
	Heart	9.19 \pm 2.08	30.6
	Brain	0.64 \pm 0.26	2.1
	Bone	1.34 \pm 0.30	4.5
	Small intestine	8.73 \pm 1.46	29.1
	Large intestine	2.61 \pm 0.72	8.7
	Skin	0.67 \pm 0.25	2.2
60	Blood	0.26 \pm 0.06	
	Lung	2.96 \pm 0.18	11.4
	Liver	23.17 \pm 5.05	89.1
	Spleen	4.01 \pm 0.06	15.4
	Kidneys	38.51 \pm 1.11	148
	Muscle	0.91 \pm 0.02	3.5
	Fat	0.23 \pm 0.03	0.9
	Heart	8.68 \pm 0.28	33.4
	Brain	0.54 \pm 0.09	2.1
	Bone	0.97 \pm 0.05	3.7
	Small intestine	12.46 \pm 0.42	47.9
	Large intestine	2.95 \pm 0.14	11.3
	Skin	0.60 \pm 0.01	2.3
120	Blood	0.14 \pm 0.04	
	Lung	1.67 \pm 0.11	11.9
	Liver	17.22 \pm 0.70	123
	Spleen	1.86 \pm 0.05	13.3
	Kidneys	27.47 \pm 0.83	196
	Muscle	0.83 \pm 0.02	5.9
	Fat	0.09 \pm 0.01	0.6
	Heart	6.62 \pm 0.21	47.3
	Brain	0.44 \pm 0.01	3.1
	Bone	0.63 \pm 0.01	4.5
	Small intestine	15.71 \pm 0.43	112
	Large intestine	9.24 \pm 0.62	66.0
	Skin	0.40 \pm 0.03	2.9

Pharmacokinetics of ^{67}Ga -complex **1b** in FVB *mdr1a/1b*($-/-$) mice. Mice were injected intravenously with 74 kBq (2 μCi) of ^{67}Ga -complex **1b** and sacrificed at 5, 15, 60, or 120 min after injection; blood and tissues were harvested and counted. Data are expressed as %ID/g tissue at each time point. Values represent mean \pm range ($n = 2$). Also shown are tissue-to-blood ratios at each time point.

TABLE 5Biodistribution of ^{67}Ga -Complex **1b** in FVB WT and *mdr1a/1b*($-/-$) Mice (AUC_{5-120} ; %ID/g \times min)

Tissue	WT	<i>Mdr1a/1b</i> ($-/-$)
Blood	24.5 \pm 9.9	29.4 \pm 8.7
Heart	817.5 \pm 68.9	950.1 \pm 123.6
Liver	1,204.6 \pm 147.3	2,465.4 \pm 440.4
Kidney	3,921.3 \pm 410.4	4,072.6 \pm 271.8
Brain	3.7 \pm 0.3	62.5 \pm 16.1
Lung	131.8 \pm 15.8	357.5 \pm 67.8
Spleen	92.2 \pm 10.5	423.1 \pm 71.7
Muscle	96.2 \pm 9.0	109.0 \pm 13.0
Fat	9.8 \pm 2.0	22.0 \pm 3.6
Bone	68.4 \pm 6.5	112.5 \pm 17.7
Small intestine	2,408.4 \pm 203.8	1,404.9 \pm 96.4
Large intestine	1,647.4 \pm 295.2	516.4 \pm 56.4
Skin	36.8 \pm 4.0	65.1 \pm 14.7

Biodistribution of ^{67}Ga -complex **1b** in FVB mice (AUC_{5-120}). Biodistribution data for each tissue are presented as AUC_{5-120} values of ^{67}Ga -complex **1b** expressed as $\text{kBq (injected kBq)}^{-1} (\text{g tissue})^{-1} \times 100 \times \text{min} \pm \text{range or} \pm \text{SEM of 2 or 3 determinations, respectively.}$

high sensitivity. Indeed, the high steady-state nontarget-to-target cellular accumulation ratios compared with $^{99\text{m}}\text{Tc}$ -sestamibi and $^{99\text{m}}\text{Tc}$ -tetrofosmin (27) demonstrated the superior sensitivity of **1b** in detecting the outward transport activity of *MDR1* Pgp.

Selected MRP family members also may impact resistance to cytotoxic drugs. Within the MRP superfamily, MRP1, -2, -3, and -6 are organic anion transporters, whereas MRP4 has been shown to confer resistance to antiviral acyclic nucleotide analogs (55). Similarly, *MRP5* has been shown to act as an energy-dependent transporter of nucleotides (56). Drugs that are recognized by the MRP superfamily also include some neutral and cationic compounds (3). Ga-complex **1b** demonstrated a modest degree of cross-reactivity with MRP1, but the sensitivity for detection of transport activity was low compared with that of *MDR1* Pgp. By “modest,” we identified a 9-fold MRP1-dependent change in cell tracer content versus up to 100-fold for *MDR1* Pgp. The ratio of MRP1-dependent to *MDR1* Pgp-dependent transport is thus ~ 0.1 with Ga-complex **1b**, a ratio half that of $^{99\text{m}}\text{Tc}$ -sestamibi, another agent that also shows a modest cross-reactivity with MRP1 in cells in culture and a ratio of MRP1-dependent to Pgp-dependent transport of ~ 0.2 . However, in contrast to Pgp, an MRP1-dependent signal has not been observed with $^{99\text{m}}\text{Tc}$ -sestamibi in patients in several clinical trials attempting to define this. It would appear that the modest MRP1-dependent cross-reactivity observed in biochemical studies in cells in culture is buried in the background in living patients, whereas the 50-fold *MDR1* Pgp-dependent transport signals translate well to patients, as has been reported by many clinical trials with $^{99\text{m}}\text{Tc}$ -sestamibi. Furthermore, cellular accumulation in the presence of specific inhibitors of *MDR1*

Pgp, such as LY335979, readily differentiate transport mediated by *MDR1* Pgp versus MRP1 in vitro, and cells stably transfected with *MRP2-MRP6* did not show any clear trends. These observations were consistent with the postulation that Ga-complex **1b** will be a sensitive and reasonably selective probe for *MDR1* Pgp transport activity in vivo.

MDR1 Pgp is expressed in capillary endothelial cells in the brain and forms a major component of the BBB (41). Therefore, *mdr1a/1b*($-/-$) KO mice offer an interesting model to evaluate the utility of the reagent as a probe of Pgp transporter-mediated activity in vivo. Using the positron emissions of ^{68}Ga , we readily detected greater net uptake in the brain of KO mice, consistent with the quantitative biodistribution data obtained with the ^{67}Ga -complex. A drug-transporting protein, Pgp is also expressed along biliary canalicular surfaces of hepatocytes, poised to secrete substances into the bile. Biodistribution data in WT and KO mice demonstrated differences in accumulation of the radiotracer as expected for the presence or absence of drug-transporting Pgp in the liver.

PET agents exemplified by ^{11}C -verapamil (57,58) and ^{18}F -paclitaxel (18,19) have shown potential for noninvasive imaging of Pgp-mediated drug transport at the BBB. ^{11}C -Verapamil demonstrated 10-fold enhanced activity in the brain of KO mice compared with that of WT mice. However, this PET agent did not show any significant differences of activity in other tissues, including the liver (58). Another PET agent, ^{18}F -paclitaxel, also displayed pharmacokinetic profiles consistent with Pgp-mediated transport. The radiotracer showed enhanced accumulation in the brain of KO mice compared with that of WT mice with a differential uptake ratio ($\text{DUR} = \% \text{ID/g} \times \text{body weight}$) of 1,400 at 30 min after injection (18). However, the agent was similar to ^{11}C -verapamil in the livers of KO and WT mice, displaying a lack of significant differential uptake, in contrast to $^{99\text{m}}\text{Tc}$ -sestamibi or $^{67/68}\text{Ga}$ -complex **1b**. This lack of differential uptake in the livers of KO mice compared with WT mice for ^{11}C -verapamil and ^{18}F -paclitaxel may be attributed to the existence of metabolites or cross-reactivity with other transporters in the tissue. In contrast, ^{67}Ga -complex **1b** showed a DUR of 1,700 at 60 min after injection.

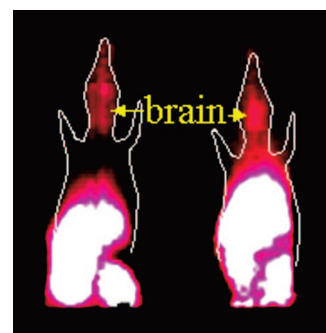


FIGURE 7. MicroPET image of ^{68}Ga -complex **1b** in brains of FVB WT and *mdr1a/1b*($-/-$) mice. After injection of mice with an intravenous bolus of radiopharmaceutical, images of abdomen, thorax, and head were obtained with microPET scanner. Representative coronal images of WT (left) and *mdr1a/1b*($-/-$) (right) mice obtained 5 min after injection are shown. A body outline is included for orientation.

tion in the brain and 205 in the liver. Furthermore, ^{67}Ga -complex **1b** showed 3- to 5-fold greater differences in brain AUC_{5-120} between KO and WT mice than $^{99\text{m}}\text{Tc}$ -sestamibi (59) and $^{99\text{m}}\text{Tc}$ -tetrafosmin (27), further documenting its potential superiority for imaging Pgp activity in vivo.

In addition, the liver showed twice the retained activity (AUC_{5-120}) of **1b** in KO mice compared with WT mice, whereas the heart, a Pgp-negative tissue, did not show any significant difference. Further analysis revealed that the heart-to-liver ratio in WT mice at 120 min increased to 2.2 compared with 0.4 in KO mice at the same time point. The observed lower heart-to-liver ratio in KO mice was consistent with a lack of cross-reacting non-Pgp-mediated clearance of **1b** in KO mice. Furthermore, the heart-to-liver ratio of 2.2 for ^{67}Ga -complex **1b** reported herein compared favorably with 1.1 for $^{99\text{m}}\text{Tc}$ -sestamibi (59). Thus, as an additional consequence of the differential tissue expression of Pgp, the superior heart-to-liver ratio of ^{67}Ga -complex **1b** versus $^{99\text{m}}\text{Tc}$ -sestamibi at 2 h would be beneficial in myocardial perfusion imaging.

CONCLUSION

While exploring structure-activity relationships of N_2O_2 gallium(III) complexes, we have identified a nonmetabolized cationic, hydrophobic $^{67/68}\text{Ga}$ -complex that is recognized by *MDR1* Pgp as an efficient transport substrate. We are cautiously optimistic that this radiopharmaceutical may enable both SPECT and PET monitoring of Pgp activity in tissues in vivo. Issues related to radiation dosimetry, automation, or remote synthesis will require additional experimentation. The potential for a ^{68}Ga generator-produced PET radiopharmaceutical for use within clinical environments, coupled with facile synthesis of the precursor ligand and a rapid radiolabeling procedure, enhances the promise of this approach for noninvasive assessment of Pgp at the BBB, in chemotherapy regimens, and during MDR gene therapy. Because of the mechanisms of cell localization and differential expression of Pgp in liver compared with heart, the agent also shows promise as a myocardial perfusion imaging agent.

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