

Quantification of Dopamine Transporter by ^{123}I -PE2I SPECT and the Noninvasive Logan Graphical Method in Parkinson's Disease

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(E)-N-(3-iodoprop-2-enyl)-2 β -carbomethoxy-3 β -(4'-methylphenyl) nortropane (PE2I), a cocaine analog, is a new, highly specific tracer for imaging dopamine transporter labeled with ^{123}I for in vivo SPECT. Its reversible binding on dopamine transporter and its rapid kinetics allow quantification of its binding potential according to a 3-compartment model. For quantification of distribution volume of reversible tracer, Logan developed a noninvasive and graphical method that allows accurate estimation of binding potential. In this study, we performed ^{123}I -PE2I SPECT on healthy volunteers and patients with Parkinson's disease (PD) to validate the Logan graphical method for quantification of ^{123}I -PE2I binding and to analyze the relationship between ^{123}I -PE2I SPECT and clinical features of this frequent degenerative disease. **Methods:** Eight PD patients (3 women, 5 men; mean age, 64 ± 7.9 y; disease duration range, 1–8 y, Hoehn and Yahr stage range, 1–2.5) and 8 age-matched healthy volunteers (4 women, 4 men; mean age, 61.5 ± 9.5 y) were included in 2 centers and studied with SPECT. Four sequential SPECT imaging sessions of 15-min duration were performed from 5 to 65 min after bolus injection of 140 ± 30 MBq of ^{123}I -PE2I.

Results: The kinetics of PE2I in healthy volunteers and PD patients were rapid, and the Logan graphical method allowed quantification of distribution volume ratio (DVR) in the caudate nucleus and putamen. ^{123}I -PE2I striatal specific binding was significantly reduced in PD patients, compared with healthy volunteers, in the caudate and putamen. The decrease of DVR in the putamen was significantly and inversely correlated to disease duration and Hoehn and Yahr stage. In asymmetric PD patients, ^{123}I -PE2I uptake was significantly more reduced in the putamen contralateral to the side with predominant clinical symptoms. However, ^{123}I -PE2I uptake was also significantly reduced in the ipsilateral putamen, compared with that in healthy volunteers, suggesting that ^{123}I -PE2I SPECT can detect nigrostriatal degeneration before the appearance of clinical symptoms. **Conclusion:** Our data indicate

that the Logan graphical method is accurate for noninvasive quantification of PE2I and that ^{123}I -PE2I SPECT is a useful quantitative method for accurate estimation of nigrostriatal dopaminergic nerve terminal degeneration. The close relationships between SPECT findings and clinical data suggest that this method is useful for objectively following the progression of PD and for assessing the effect of potential neuroprotective treatments. Finally, our findings suggest that ^{123}I -PE2I SPECT can be used for preclinical and early diagnosis of PD.

Key Words: Parkinson's disease; diagnosis; SPECT; ^{123}I -PE2I; Logan plot

J Nucl Med 2003; 44:663–670

Parkinson's disease (PD) is a progressive disabling neurodegenerative disorder observed in 1% of the population older than 55 y, the mean age at which the disease is first diagnosed (1). PD consists of a syndrome including tremor, rigidity, bradykinesia, and postural abnormalities. The 2 principal anatomopathologic characteristics of PD are the progressive loss of pigmented melanistic neurons of mesencephalon, particularly loss of dopaminergic neurons in the substantia nigra pars compacta (2), and a ventrocaudal gradient of degenerative lesion (3). In the past 2 decades, the strategy of symptomatic treatments has been improved and deep stimulation surgery has become an effective alternative for motor fluctuations and dyskinesia due to medical treatment (4). The issue for our new century will be the development of neuroprotective therapeutics aimed at slowing or stopping the degenerative process. This aim stresses the need for very early diagnosis of PD (5,6).

In recent years, PET and SPECT exploration of the dopamine system using specific ligands has evolved, thus showing the usefulness of pre- and postsynaptic transporters or receptors as objective markers of the integrity of this system (7,8). SPECT is widely available and offers an in

Received Aug. 2, 2002; revision accepted Jan. 13, 2003.

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vivo noninvasive diagnostic method to detect nigrostriatal nerve terminal lesions with specific ligands of the dopamine transporter (DAT) (9–11). A new high-affinity and selective ligand for imaging the DAT has recently been developed: (*E*)-*N*-(3-iodoprop-2-enyl)-2 β -carbomethoxy-3 β -(4'-methylphenyl) nortropane (PE2I) (12). In vitro studies have demonstrated that ^{125}I -PE2I has high affinity for DAT (dissociation constant [K_d] = 4 nmol/L) and very high selectivity for DAT versus serotonin (5HT) and noradrenaline transporters (12,13). PE2I has been labeled with ^{123}I and ^{11}C for in vivo SPECT and PET studies, which have shown a reversible and specific in vivo binding to the DAT (14,15). According to a 3-compartment model, 2 methods have been proposed to quantify in vivo binding of reversible tracer, that is, the specific (striatum)-to-nonspecific (occipital lobe or cerebellum) uptake ratio at pseudoequilibrium to determine binding potential (16), and the Logan graphical method to obtain distribution volume ratio (DVR) (17). Initially, quantification of PE2I was proposed using measurement of the striatum-to-cerebellum ratio (18), but Logan analysis was recently shown to be a more accurate method for quantification of striatal ^{123}I -PE2I binding because of the rapid kinetics of the tracer (19). Pinborg et al. (19) demonstrated that, compared with compartment kinetics analysis, the Logan graphical method was accurate for quantification of PE2I.

The aim of this study was therefore to demonstrate that quantification of ^{123}I -PE2I DVR with the Logan graphical method without blood sampling allowed early diagnosis and follow-up of PD.

MATERIALS AND METHODS

Patients

Eight patients with idiopathic PD (3 women, 5 men; mean age, 64 ± 7.9 y) and 8 healthy volunteers (4 women, 4 men; mean age, 61.5 ± 9.5 y) were recruited at, respectively, the Department of Neurology, Bretonneau Hospital, Tours, France, and the Clinic Investigation Center, Purpan Hospital, Toulouse, France. The study was performed according to the standard ethical guidelines of the Hospital and University of Tours and was approved by the local ethical committee on April 27, 1998. All patients and healthy volunteers gave informed and written consent.

Seven of 8 patients had asymmetric disease and 1 had bilateral symmetric disease, all with bradykinesia and at least 1 of the other cardinal features of the disease: rigidity, rest tremor, or impaired postural reflexes. The diagnosis of PD was assessed according to the United Kingdom Parkinson's Disease Society Brain Bank criteria (20). None of the 8 patients had features suggestive of atypical parkinsonism or responded to the Quinn criteria for multiple-system atrophy (21) or the criteria for progressive supranuclear palsy of the National Institute of Neurological Disorders and Stroke and the Society for Progressive Supranuclear Palsy (22). No patient had relevant abnormalities on brain MRI or CT. No patient had mental deterioration or depression according to the criteria in the fourth edition of the *Diagnostic and Statistical Manual of Mental Disorders* (23) or according to the Mini-Mental State score (>25) (24). The clinical handicap state was determined by the modified version of the Hoehn and Yahr scale (1). Patients were

asked to stop dopaminergic treatment 8 d before the SPECT scan if they were taking anticholinergic molecules and dopamine agonists or 12 h before the SPECT scan if they were taking L-dopa. The 8 healthy volunteers had no relevant medical history, no hypertension, no diabetes, no cardiac disorders, and no history of cranial trauma or serious infectious disease. They were not receiving any medication. No healthy volunteer had relevant abnormalities found on brain MRI. They were recruited in the same age range as the parkinsonian patients. The characteristics of the 2 groups are presented in Table 1.

Radioiodine uptake by the thyroid gland was prevented by oral ingestion of 400 mg of potassium perchlorate 15 min before intravenous injection of ligand. A catheter was inserted into an antebachial vein, and an isotonic glucose solution was infused. A bolus of 140 ± 30 MBq ^{123}I -PE2I was injected through the catheter.

Preparation of PE2I

^{123}I -PE2I was prepared by iododestannylation of the tributyl tin precursor. To a vial containing 50 μg of the stannic precursor were added 50 μL of EtOH, 50 μL of HCl (0.1N), 740 MBq of ^{123}I -NaI (in 100 μL of NaOH, 0.1N, with a specific activity > 185 TBq/mmol; Cis Bio International), and 50 μL of 10 mg/mL chloramine T. The reaction was allowed to stand at room temperature for 30 min, quenched with 100 μL of $\text{Na}_2\text{S}_2\text{O}_5$ (300 mg/mL), basified with saturated NaHCO_3 , and extracted with ethyl acetate (3×1 mL). The combined ethyl acetate extracts were evaporated under a nitrogen stream, and the residue was dissolved in 200 μL of the high-performance liquid chromatography (HPLC) mobile phase. The radioiodinated solution was purified by HPLC using a reverse-phase C-18 column and a mixture of MeOH:H₂O:Et₃N (80:20:0.1) as the mobile phase (flow rate, 1 mL/min). The fraction eluted at the retention time of PE2I was collected and passed through a Sep-Pak C-18 column (Waters). The radioiodinated product was then eluted with 2×1 mL of EtOH and evaporated under a nitrogen stream. Structural identification and radiochemical purity were checked by HPLC using cold PE2I as a reference under the same conditions.

SPECT Protocol

SPECT data acquisition started 5 min after the intravenous injection. A double-head camera equipped with parallel collimators (Cardial Elscint; General Electric Medical Systems) was used for healthy volunteers, and a multislice brain-dedicated camera (Ceraspect; Digital Scintigraphics) was used for PD patients. Resolution was 8–9 mm and 7–8 mm in full width at half maximum for, respectively, the double-head and brain-dedicated cameras. In the healthy volunteers, four 15-min sequential acquisitions were obtained, followed by two 15-min acquisitions at 180 and 200 min after injection. In the patients, 4 sequential 15-min acquisitions using a $120 \times 3^\circ$ step rotation were obtained. Images were reconstructed from photopeak counts (159 ± 16 keV) using a filtered backprojection algorithm with a Butterworth filter (cutoff, 0.754 cm; order, 4; size, 7) for the double-head camera and a 2-dimensional Hanning filter (order, 0.5) for the Ceraspect camera. Images were displayed as a 128×128 matrix (pixel size, 1.67 mm²). SPECT data were reoriented according to a line passing through the inferior part of the frontal and occipital lobes parallel to the anterior–posterior commissure. We made no correction for the partial-volume effect or attenuation resulting in systematic errors; these were assumed to have a similar effect on data from both cameras. Cross calibration of the 2 cameras with phantoms

TABLE 1
Clinical Characteristics of Subjects at Time of ^{123}I -PE2I SPECT

Subject no.	Age (y)	Sex	Hoehn and Yahr score	Dominant side	Duration (y)
Healthy volunteers					
1	47	F			
2	49	M			
3	50	M			
4	58	M			
5	60	F			
6	65	F			
7	69	M			
8	73	F			
Mean \pm SD	61.5 \pm 9.5				
PD patients					
1	52	M	2	—	1.5
2	56	M	1	R	1
3	60	F	1.5	R	1.5
4	65	M	2	R	1.5
5	65	F	2.5	R	8
6	67	F	1.5	L	4
7	70	M	2.5	R	1.5
8	77	M	1.5	R	5
Mean \pm SD	64 \pm 7.9		1.88 \pm 0.6		3 \pm 2.5

showed that the use of 2 different cameras did not significantly affect the counting ratio measurement between the striatum and occipital regions. The 5 slices corresponding to the highest striatal uptake were digitally summed, yielding a final transverse slice 8.5 mm thick. Geometric standardized circular (caudate nucleus and occipital lobe) or elliptic (putamen) regions of interest (ROIs) were drawn on the striatum (S, specific binding) and the occipital cortex (O, free and nonspecific binding). The sizes of the ROIs were 74 mm² for the caudate nucleus (C), 140 mm² for the putamen (P), and 314 mm² for the occipital region. The mean activity was counted in the 6 different ROIs in counts per second per pixel; that is, C(T), P(T), S(T), and O(T), where T is time T.

Graphical Analysis

Average regional counts were used in calculations. Time-activity curves for each ROI were determined from 5 to 65 min after injection and were corrected for radioactivity decay of ^{123}I . Time-activity data were analyzed by the noninvasive linear graphical method developed by Logan et al. (17) for reversible ligands. This method assumed that the distribution volume of nondisplaceable tracer is the same in reference (occipital lobes) and striatal regions and that delivery of the tracer is similar for both regions. The integrated striatal ROI activity from time zero to T normalized to striatal activity at time T ($\int_0^T S(t)dt/S(T)$) was plotted against integrated occipital ROI activity from zero to T also normalized to striatal activity at time T ($\int_0^T O(t)dt/S(T)$).

$$\frac{\int_0^T \text{Str}(t)dt}{\text{Str}(T)} = \text{DVR} \frac{\int_0^T \text{Occ}(t)dt}{\text{Str}(T)} + C$$

with

$$C = \left[\frac{\text{DVR}}{k_2} \right] \frac{\text{Occ}(T)}{\text{Str}(T)} + \text{ct},$$

where Str = striatum, Occ = occipital lobe, and ct = constant.

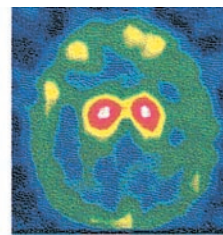
The Logan plot becomes linear when pseudoequilibrium is reached, that is, when the ratio Occ(T)/Str(T) becomes constant. The asymptotic slope equals DVR. DVR is defined as the ratio between distribution volume of specific binding of ^{123}I -PE2I to DAT (striatum) and distribution volume of nonspecific binding of the ligand in regions devoid of DAT (occipital lobes). DVR is related to the binding potential ($\text{DVR} = \text{binding potential} - 1$) (17), and binding potential is assimilated to the density of DAT (16). In a previous study with SPECT PE2I in a nonhuman primate, we demonstrated that 4 SPECT acquisitions done 5 min after injection during 1 h were sufficient to determine the Logan plot and DVR (25).

Statistical Analysis

Differences between patients and healthy volunteers for the DVR of the caudate, putamen, and striatum were assessed with a nonparametric Wilcoxon test. Associations between clinical parameters, that is, age, Hoehn and Yahr score, and evolution of the disease, were assessed with Spearman correlation coefficients. Differences between contralateral and ipsilateral putamen in hemiparkinsonism were assessed with a Wilcoxon matched pairs test.

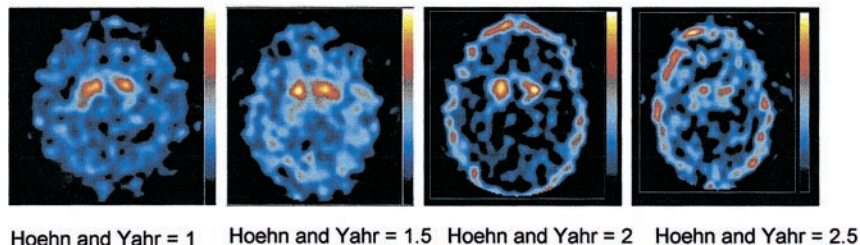
RESULTS

Table 1 summarizes demographic and clinical data of the 8 healthy volunteers and the 8 parkinsonian patients. Age range was similar between both populations. The sex distribution in PD was not significantly different from that in healthy volunteers. Four PD patients had a disease duration of less than 2 y, and 4 patients had more than 3 y of symptomatic clinical evolution. Four PD patients had a Hoehn and Yahr score of 1 or 1.5, reflecting unilateral extrapyramidal syndrome with or without impaired posture



Healthy volunteer

FIGURE 1. ^{123}I -PE2I SPECT (acquisition between 35 and 50 min after injection) of healthy volunteer and 4 PD patients according to 4 stages of Hoehn and Yahr clinical score. All PD patients are characterized by progressive reductions in dopamine nigrostriatal terminal density, first in putamen and then in caudate nucleus.



Hoehn and Yahr = 1

Hoehn and Yahr = 1.5

Hoehn and Yahr = 2

Hoehn and Yahr = 2.5

reflexes. Four PD had bilateral symptoms, 3 with asymmetric severity; the Hoehn and Yahr score was 2 or 2.5.

^{123}I -PE2I SPECT in Parkinsonian Patients Versus Healthy Volunteers

By visual analysis was observed a very high contrast between specific striatal uptake and nonspecific cortical binding in healthy volunteers and in PD patients. These data indicated a high concentration of the radiopharmaceutical in the striatum and minimal accumulation in other brain areas, in particular in the thalamus, hypothalamus, and midbrain, regions rich in 5HT and noradrenaline transporters. Figure 1 shows ^{123}I -PE2I uptake (summation of data acquired from 20 to 35 min after injection) in striatum in 1 healthy volunteer and 4 parkinsonian patients for each Hoehn and Yahr score. In unilateral or asymmetric PD, binding of ^{123}I -PE2I was markedly affected in contralateral putamen to the more affected side of the body but ipsilateral putamen was also affected. In addition, uptake of PE2I decreased when Hoehn and Yahr stage increased.

Figure 2 shows representative PE2I time-activity curves for the striatum and the occipital cortex of healthy volunteers and PD patients. These curves show rapid cerebral uptake and washout of PE2I. Striatal accumulation of PE2I after intravenous injection was rapid, reached a maximum at 15–20 min in healthy volunteers and at 10–15 min in PD

patients, and then decreased. In PD patients, striatal binding decreased more rapidly than in healthy volunteers, reaching nearly background level by 1 h. This type of kinetic is consistent with reversible binding.

Kinetic analysis by the Logan graphical method is illustrated in Figure 2 in a healthy volunteer and a patient with severe PD. The curves became linear soon after PE2I injection. The application of the Logan graphical method resulted in a linear relationship between integral $O(t)dt/S(T)$ and integral $S(t)dt/S(T)$, with a least squares correlation coefficient equal to 0.9995 ± 0.0005 in the healthy volunteers and 0.9953 ± 0.0066 in the patients. PE2I DVR values in the whole striatum, right and left striata, caudate, and putamen are shown in Table 2 for healthy volunteers and patients. A nonsignificant correlation was observed between striatal DVR and age in the healthy volunteers ($r = -0.461$, 95% confidence interval = $(-0.88; 0.36)$). No correlation between age and DVR was found for PD patients. The slopes of Logan plots were significantly less in parkinsonian patients than in healthy volunteers. In all regions, the DVR values were significantly lower in patients than in healthy volunteers ($P < 0.001$) (Fig. 3). When we compared all parkinsonian patients with healthy volunteers, mean DVR decreases were 48%, 44%, and 41% for caudate, putamen, and striatum, respectively. In the 4 patients with a Hoehn

FIGURE 2. Kinetics of ^{123}I -PE2I in striatum (caudate nucleus and putamen) and occipital lobe in healthy volunteer (A) and parkinsonian patient (B) according to 4 sequential SPECT acquisitions. (C) Quantification of distribution volume of ^{123}I -PE2I in striatum according to slope of Logan plot in healthy volunteers and parkinsonian patients.

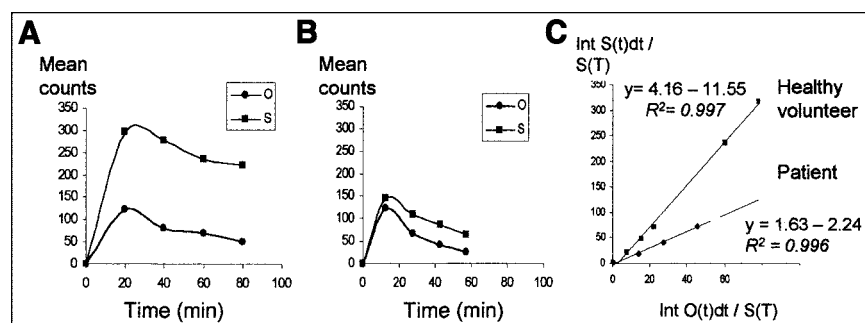


TABLE 2
¹²³I-PE2I Striatal DVRs

Subject no.	Caudate	Putamen	Right striatum	Left striatum	Striatum
Healthy volunteers					
1	5.60	3.39	3.85	3.70	3.77
2	8.12	5.15	5.58	5.63	5.61
3	6.56	4.20	4.51	4.49	4.50
4	7.65	4.27	5.26	4.65	4.96
5	5.44	2.87	3.74	3.32	3.53
6	6.48	3.70	4.46	3.86	4.16
7	6.18	3.58	4.25	4.09	4.17
8	5.49	3.19	3.77	3.66	3.72
Mean ± SD	6.44 ± 1.00	3.79 ± 0.72	4.43 ± 0.69	4.18 ± 0.73	4.30 ± 0.70
PD patients					
1	4.14	2.19	2.96	2.79	2.88
2	4.08	2.82	3.76	2.73	3.24
3	4.02	2.28	3.25	2.51	2.88
4	4.13	2.21	3.11	2.64	2.88
5	1.62	1.52	1.67	1.56	1.62
6	2.62	1.61	1.88	2.05	1.97
7	2.81	2.00	2.43	2.13	2.28
8	3.47	2.24	2.99	2.33	2.66
Mean ± SD	3.36 ± 0.9	2.11 ± 0.4	2.76 ± 0.7	2.34 ± 0.4	2.55 ± 0.5

and Yahr score lower than 2, mean reductions of DVR in caudate nuclei, putamen, and striatum were 39%, 41%, and 38%, respectively. In the 4 patients with a Hoehn and Yahr score of up to 2, mean decreases of DVR in caudate, putamen, and striatum were 57%, 48%, and 44%, respectively.

Correlation Between DAT Density and Clinical Impairment

In the 7 parkinsonian patients with lateralization of symptoms, DVR was significantly more decreased in the contralateral putamen than in the ipsilateral putamen ($P = 0.016$) (Table 3).

Correlation was significant between putamen DVR and Hoehn and Yahr score ($r = -0.73$, $P = 0.04$) but not between striatum and caudate DVR. DVR in the putamen was 2.24 ± 0.49 for patients with a Hoehn and Yahr score

of 1 or 1.5 and 1.98 ± 0.32 for patients with a Hoehn and Yahr score of 2 or 2.5. The difference was not significant ($P = 0.148$) because of the small sample size.

In PD patients, DVR values in striatum, caudate, and putamen were significantly correlated with disease duration ($r = -0.84$, $P = 0.08$; $r = -0.70$, $P = 0.054$; $r = -0.65$, $P = 0.083$, respectively). The DVR values in the putamen, caudate, and striatum of patients with a disease duration of less than 2 y were 2.60 ± 0.55 , 3.84 ± 0.58 , and 2.83 ± 0.34 , respectively, and were significantly different from those of PD patients with a disease duration of 3–8 y (1.82 ± 0.36 , $P = 0.028$; 2.57 ± 0.93 , $P = 0.06$; and 2.08 ± 0.53 , $P = 0.057$, respectively).

DISCUSSION

Brain images after PE2I injection showed a high contrast between the background, that is, cortex and thalamus, and the striatum in healthy volunteers but also in parkinsonian patients. These data agree with previous ¹²⁵I-PE2I studies of postmortem human brain that documented intense binding in caudate and putamen and low binding in 5HT and norepinephrine-rich structures and in the cortex (26). These data are also concordant with PET studies using ¹¹C-PE2I (15). Our results showed rapid kinetics for PE2I, because it reached a striatal peak of uptake between 10 and 20 min and had rapid washout in healthy volunteers and in PD patients. Kinetics were even more rapid with evolution of nigrostriatal neuronal loss in PD.

Experience with SPECT imaging of DATs in healthy volunteers and in parkinsonian patients is steadily increasing. In recent years, a series of cocaine-derivative ¹²³I-labeled tracers have been developed that could be classified into 1 of 3 types according to their properties and kinetics.

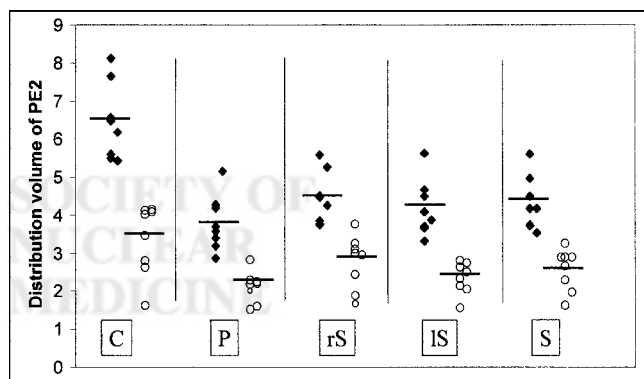


FIGURE 3. Distribution volume of ¹²³I-PE2I in caudate nucleus, putamen, right striatum (rS), left striatum (lS), and striatum in 8 healthy volunteers (◆) and 8 parkinsonian patients (○).

TABLE 3
¹²³I-PE2I DVRs in Putamen Contralateral and Ipsilateral to Side with Predominant Extrapyrarnidal Clinical Signs:
 Data for 7 Parkinsonian Patients

Subject no.	Dominant side	Hoehn and Yahr score	Contralateral DVR	Ipsilateral DVR
1	R	1	2.24	3.46
2	R	1.5	1.75	2.81
3	R	1.5	1.92	2.57
4	L	1.5	1.50	1.72
5	R	2	2.00	2.43
6	R	2.5	1.47	1.54
7	R	2.5	1.87	2.13
Mean ± SD			1.82 ± 0.3	2.38 ± 0.6
Wilcoxon matched-pairs test			0.016	

The first is the well-known ¹²³I-β-carbomethoxy-3-β-(4-iodophenyl)tropane (¹²³I-βCIT), which binds with high affinity to DAT (K_d = 0.2 nmol/L; inhibitory concentration of 50% [IC₅₀] = 1.6 nmol/L) but also to 5HT transporter (IC₅₀ = 3.78 nmol/L) (27). Its kinetics are slow, as shown by a striatal time–activity curve indicating a 12- to 18-h interval to highest uptake and a slow washout of less than 0.5% per hour (28). SPECT imaging must therefore be done 18–27 h after injection, when activity in brain compartments closely approximated equilibrium binding at the DAT. The binding potential of ¹²³I-βCIT can be simply quantified using the ratio between specific (striatum, caudate, putamen) and nonspecific (occipital lobe or cerebellum) activity during the plateau phase of tracer uptake (28). However, the prolonged wait for highest striatal uptake before SPECT can be performed is not easy to apply in clinical practice. Another difference between this tracer and PE2I is its high affinity for 5HT transporter in structures near the striatum, which can also be affected in PD, but it seemed that the kinetics of ¹²³I-βCIT in 5HT-rich regions are more rapid (9,29). The second type of DAT tracer is ¹²³I-FPCIT, a fluoroalkyl derivative of ¹²³I-βCIT. Compared with ¹²³I-βCIT, it binds with lower affinity to DAT (inhibition constant = 3.5 nmol/L) but with higher selectivity toward 5HT transporter (DAT/5HT = 2.8/1) (30). Sequential ¹²³I-FPCIT SPECT imaging of healthy volunteers and PD patients by Booij et al. showed that the time to peak striatal uptake after injection was 3 h and that washout rates were relatively slow (31). These findings suggested that binding potential could be quantified at steady-state binding, that is, 3–6 h after injection, using a simple ratio of specific activity to background activity (31). However, a recent study showed that significant washout occurred in striatum and occipital lobes 3–6 h after injection and resulted in a transient equilibrium state, which suggests that ¹²³I-FPCIT SPECT may not accurately quantify DAT density with the striatum-to-occipital lobe ratio (32). Finally, the third type of presynaptic tracers have a high affinity for DAT, a low affinity for 5HT and noradrenaline transporters, and rapid kinetics. Among them, 2 tracers are similar: ¹²³I-PE2I (K_d = 4 nmol/L, DAT/5HT = 29.4/1) (13) and ¹²³I-2β-

carbomethoxy-3β-(4-fluorophenyl)-n-(1-iodoprop-1-en-3-yl) nortropane (IACFT) (K_d = 4.96 nmol/L, DAT/5HT = 25/1) (33). The high selectivity of ¹²³I-PE2I for DAT is an important characteristic for future in vitro and in vivo studies of potential and selective neuroprotective or neurotrophic drugs on nigrostriatal neurons. Faster kinetics allow SPECT imaging within the first 2 h after injection, an interval that is convenient for clinical practice. The striatal time–activity curve showed a time to peak striatal uptake of less than 20 min, no plateau period, and rapid striatal washout after occipital washout. Logan (17) described a graphical method with or without blood sampling for quantification of the distribution volume of reversible tracer. Pinborg et al. (19) demonstrated recently that this method without blood sampling could accurately quantify the DVR of ¹²³I-PE2I for striatum, that is, the striatal ¹²³I-PE2I binding potential on DAT. Our data confirm that the Logan graphical method is appropriate for quantification of ¹²³I-PE2I in healthy volunteers and in PD patients, since Logan plots always became linear even with only 4 sequential SPECT imaging sessions from 5 to 65 min after injection. The slope of the Logan plot decreased according to the severity of nigrostriatal nerve terminal degeneration. In addition, Bonad et al. (34) compared 4 methods for quantification of ¹²³I-IACFT and validated the Logan graphical method as more appropriate for estimation of the binding potential of this tracer, which is similar to ¹²³I-PE2I. Moreover, in a previous study in a progressive model of PD induced with 1-methyl-4-phenyl-1,2,3,6-tetrahydropyridine (MPTP) in a nonhuman primate, we showed that ¹²³I-PE2I binding to DAT decreased even before clinical extrapyramidal signs were evident (25). Logan analysis is then confirmed as a useful method for accurate quantification of binding potential of reversible tracers, such as ¹²³I-PE2I. According to the Logan method, DVR is derived from the kinetics of ¹²³I-PE2I and the ratios of activity between 2 cerebral regions. This calculation reduces the variations due to counting yield differences between the 2 different cameras. Because multimodality imaging with an anatomic device was not available, we chose to define fixed geometric ROIs that demonstrated little inter- and intraindividual variability (35,36). Our data

showed that ^{123}I -PE2I is definitely an attractive tracer because of higher affinity to DAT; higher selectivity to DAT/5HT transporter, compared with that of ^{123}I -FPCIT; rapid kinetics, resulting in a shorter SPECT acquisition protocol; and easier quantification without blood sampling with the Logan graphical method.

Moreover, our findings confirmed that ^{123}I -PE2I is a useful tracer for studying DATs in patients with PD and thus identifying nigrostriatal degeneration. Our data demonstrated a significant decrease of PE2I binding in putamen but also in caudate nucleus in PD, whatever the clinical duration or clinical severity. In comparison, ^{18}F -F-dopa PET imaging showed an approximately 50%–60% decrease in putamen and 20%–30% decrease in caudate in parkinsonian patients (8,10). Differences between findings could be explained by the fact that PE2I and F-dopa measure different aspects of presynaptic dopaminergic neurons, which are differently affected in PD patients. ^{18}F -F-dopa uptake is dependent on dopamine metabolism of nigrostriatal nerve terminals, whereas ^{123}I -PE2I binding reflects nerve terminal integrity. In our 5 patients with a disease duration of less than 2 y, the mean decrease in DVR was 40%, 32%, and 34% for caudate, putamen, and striatum, respectively. These data agree with other SPECT studies of de novo patients with unilateral or asymmetric PD (37). In asymmetric PD, uptake of the tracer was significantly more reduced in the putamen contralateral to the side of the body showing initial and more severe extrapyramidal syndrome. In patients with unilateral extrapyramidal syndrome, the interval between the diagnosis of PD and the development of bilateral symptoms is often several years. Our data show that in those patients, PE2I binding was already decreased in the ipsilateral striatum. SPECT PE2I can therefore identify PD at its early onset but also in its presymptomatic period. A study demonstrated that SPECT imaging of DAT could identify preclinical PD in at-risk family members (38). We also recently demonstrated, in a progressive MPTP nonhuman primate model of PD, that ^{123}I -PE2I SPECT could identify lesions of dopaminergic nerve terminals before the development of extrapyramidal signs (25). These in vivo SPECT data are of prime importance because they demonstrate that SPECT can diagnose PD in the presymptomatic period. The implications of this concept are substantial, because it defines a period in which dopamine depletion progresses without symptoms. This presymptomatic period provides an opportunity for presymptomatic diagnosis and therapeutic intervention, ideally the administration of neuroprotective compounds. Our data demonstrate that putamen DVR is related to the severity of clinical symptoms and disease duration, a finding that corroborates previous SPECT studies of the DAT with other tracers such as ^{123}I -βCIT (9,29) and ^{123}I -FPCIT (7,31). The decrease in DVR, compared with Hoehn and Yahr score, was more important in caudate than in putamen, as agrees with other SPECT studies showing that the putamen-to-caudate ratio decreases with increasing Hoehn and Yahr stage (39). Our data demonstrate

that ^{123}I -PE2I SPECT is sensitive for longitudinal studies after progression of dopaminergic degeneration in PD. SPECT provides an opportunity for better understanding the pathophysiology of PD.

CONCLUSION

Our findings indicated that ^{123}I -PE2I SPECT with the Logan graphical method is useful for estimating nigrostriatal neuronal loss in patients with PD. One main advantage of ^{123}I -PE2I is its rapid kinetics, allowing SPECT acquisition 1 h after injection. We also observed a correlation between striatal ^{123}I -PE2I binding and disease duration and clinical features, suggesting that SPECT can be used to follow progression of the disease. One promising use of SPECT with ^{123}I -PE2I is the diagnosis of nigrostriatal degeneration in the presymptomatic period. This preclinical SPECT diagnosis of PD offers an opportunity for future early administration of neuroprotective therapeutics. Our findings suggest that quantitative PE2I SPECT can be a useful method to determine the neuroprotective potential of drugs.

ACKNOWLEDGMENTS

This study was supported by the EUREKA Program (Dopimag) and by a grant from Tours University Hospital.

REFERENCES

- Hoehn HM, Yahr MD. Parkinsonism: onset, progression and mortality. *Neurology*. 1967;17:427–442.
- Jellinger KA. Neurodegenerative disorders with extrapyramidal features: a neuropathological overview. *J Neural Transm*. 1995;46(suppl):33–57.
- Gibb WRG, Lees AJ. Anatomy, pigmentation, ventral and dorsal subpopulations of the substantia nigra, and differential cell death in Parkinson's disease. *J Neurol Neurosurg Psychiatry*. 1991;54:388–396.
- Pollack P, Fraix V, Krack P, et al. Treatment results: Parkinson's disease. *Mov Disord*. 2002;17(suppl 3):S75–S83.
- Riederer P, Sian J, Gerlach M. Is there neuroprotection in Parkinson syndrome? *J Neurol*. 2000;247(suppl 4):IV8–IV11.
- Riederer P, Brücke T, Müller T, Schwartz A, Storch A, Winner B. Workshop II: "Neuroprotection"—the Lugano consensus. *J Neurol*. 2000;247(suppl 4):IV36–IV37.
- Booij J, Tissingh G, Winogrodzka A, van Royen EA. Imaging of the dopaminergic neurotransmission system using single-photon emission tomography and positron emission tomography in patients with parkinsonism. *Eur J Nucl Med*. 1999;26:171–182.
- Thobois S, Guillouet S, Broussolle E. Contributions of PET and SPECT to the understanding of the pathophysiology of Parkinson's disease. *Neurophysiol Clin*. 2001;31:321–340.
- Seibyl JP, Marek KL, Quinlan D, et al. Decreased single-photon emission computed tomographic [^{123}I]β-CIT striatal uptake correlates with symptom severity in Parkinson's disease. *Ann Neurol*. 1995;38:589–598.
- Leenders KL, Salmon EP, Tyrrell P, et al. The nigrostriatal dopaminergic system assessed in vivo by positron emission tomography in healthy volunteer subjects and patients with Parkinson's disease. *Arch Neurol*. 1990;47:1290–1298.
- Sawle GV, Playford ED, Brooks DJ, Quinn N, Frackowiak SJ. Asymmetrical pre-synaptic and post-synaptic changes in the striatal dopamine projection in dopa naïve parkinsonism. *Brain*. 1993;116:853–867.
- Emond P, Garreau L, Chalon S, et al. Synthesis and ligand binding of nortropine derivatives: N-substituted 2b-carboxymethoxy-3b-(4'-iodophenyl) nortropine and N-(3-iodoprop-2E-enyl)-2b-carboxymethoxy-3b-(3',4'-disubstituted phenyl) nortropine: new high-affinity and selective compounds for the dopamine transporter. *J Med Chem*. 1997;40:1366–1372.
- Chalon S, Garreau L, Emond P, et al. Pharmacological characterization of (E)-N-(3-iodoprop-2-enyl)-2β-carboxymethoxy-3β-(4'-methylphenyl)nortropine as a selective and potent inhibitor of the neuronal dopamine transporter. *J Pharmacol Exp Ther*. 1999;291:648–654.

14. Guilloteau D, Emond P, Baulieu JL, et al. Exploration of the dopamine transporter: in vitro and in vivo characterization of a high-affinity and high-specificity iodinated tropane derivative (E)-N-(3-iodoprop-2-enyl)-2 β -carbomethoxy-3 β -(4'-methylphenyl) nortropane (PE2I). *Nucl Med Biol.* 1998;25:331–337.
15. Halldin C, Chou YH, Guilloteau D, et al. [¹¹C]PE2I: a selective radioligand for PET-examination of the dopamine transporters in human brain [abstract]. *Eur J Nucl Med.* 2000;27:928.
16. Farde L, Hall H, Ehrin E, et al. Quantitative analysis of D2 dopamine receptor binding in the living human brain by PET. *Science.* 1986;231:258–261.
17. Logan J, Fowler JS, Volkow ND, Wang GJ, Ding YS, Alexoff DL. Distribution volume ratios without blood sampling from graphical analysis of PET data. *J Cereb Blood Flow Metab.* 1996;16:834–840.
18. Kuikka JT, Baulieu JL, Hiltunen J, et al. Pharmacokinetics and dosimetry of iodine-123 labelled PE2I in humans, a radioligand for dopamine transporter imaging. *Eur J Nucl Med.* 1998;25:531–534.
19. Pinborg L, Videbaek C, Svarer C, Yndgaard S, Paulson O, Knudsen G. Quantification of (¹²³I) PE2I binding to dopamine transporters with SPET. *Eur J Nucl Med.* 2002;29:623–631.
20. Gibb WRG, Lees AJ. A comparison of clinical and pathological features of young- and old-onset Parkinson's disease. *Neurology.* 1988;38:1402–1406.
21. Quinn NP. Multiple system atrophy. In: Marsden CD, Fahn S, eds. *Movement Disorders 3*. Oxford, U.K.: Butterworth-Heinemann; 1994:262–281.
22. Litvan I, Mangone CA, McKee A, et al. Natural history of progressive supranuclear palsy (Steele-Richardson-Olszewski syndrome) and clinical predictors of survival: a clinicopathological study. *J Neurol Neurosurg Psychiatry.* 1996;61:615–623.
23. American Psychiatric Association. *Diagnostic and Statistical Manual of Mental Disorders: DSM IV*. 4th ed. Washington, DC: American Psychiatric Association; 1994.
24. Folstein MF, Folstein SE, McHugh PR. "Mini Mental Test": a practical method for grading the cognitive state of patients for the clinician. *J Psychiatr Res.* 1975;12:189–198.
25. Prunier C, Chalon S, Aesch B, et al. Binding potential evaluation of ¹²³I-PE2I a new specific dopamine transporter ligand, by kinetic approach in healthy and MPTP-treated monkeys [abstract]. *Eur J Nucl Med.* 2001;28:1010 (OS190).
26. Hall H, Halldin C, Guilloteau D, et al. Visualization of the dopamine transporter in the human brain post-mortem with the new selective ligand [¹²⁵I]PE2I. *Neuroimage.* 1999;9:108–116.
27. Neumeyer JL, Wang S, Milius RA, et al. Iodine-123- β -carbomethoxy-3- β -(4-iodophenyl)-tropane ([¹²³I] β -CIT): high affinity SPECT radiotracer of monoamine reuptake sites in brain. *J Med Chem.* 1991;34:3144–3146.
28. Laruelle M, Wallace E, Seibyl J, et al. Graphical, kinetic and equilibrium analyses of in vivo [¹²³I] β -CIT binding to dopamine transporters in healthy human subjects. *J Cereb Blood Flow Metab.* 1994;14:982–994.
29. Kim SE, Lee WY, Choe YS, Kim JH. SPECT measurement of iodine-123- β -CIT binding to dopamine and serotonin transporters in Parkinson's disease: correlation with symptom severity. *Neurol Res.* 1999;21:255–261.
30. Abi-Dargham A, Gandelman MS, Easquin G, et al. SPECT imaging of dopamine transporters in human brain with iodine-123-fluoroalkyl analogs of [¹²³I] β -CIT. *J Nucl Med.* 1996;37:1129–1133.
31. Booij J, Tissingh G, Boer GJ, et al. [¹²³I]FP-CIT SPECT shows a pronounced decline of striatal dopamine transporter labelling in early and advanced Parkinson's disease. *J Neurol Neurosurg Psychiatry.* 1997;62:133–140.
32. Seibyl JP, Marek K, Sheff K, et al. Iodine-123- β -CIT and iodine-123-FPCIT SPECT measurement of dopamine transporters in healthy subjects and Parkinson's disease. *J Nucl Med.* 1998;39:1500–1508.
33. Madras BK, Gracz LM, Fahey MA, et al. Altoprane, a SPECT or PET imaging probe for dopamine neurons: III. Human dopamine transporter in postmortem normal and Parkinson's diseased brain. *Synapse.* 1998;29:116–127.
34. Bonad AA, Fischman AJ, Alpert NM. Comparison of 4 methods for quantification of dopamine transporters by SPECT with [¹²³I]IACFT. *J Nucl Med.* 2000;41:1086–1092.
35. Verhoeff NP, Kapucu O, Sokole-Busemann E, van Royen EA, Janssen GM. Estimation of dopamine D2 receptor binding potential in the striatum with iodine-123-IBZM SPECT: technical and interobserver variability. *J Nucl Med.* 1993;34:2076–2084.
36. Baulieu JL, Ribeiro M, Levilion-Prunier C, et al. Effects of the method of drawing regions of interest on the differential diagnosis of extrapyramidal syndromes using ¹²³I-iodolisuride SPET. *Nucl Med Commun.* 1999;20:77–84.
37. Marek KL, Seibyl JP, Zoghbi SS, et al. [¹²³I] β -CIT/SPECT imaging demonstrates bilateral loss of dopamine transporters in hemi-Parkinson's disease. *Neurology.* 1996;46:231–237.
38. Maraganore DM, O'Connor MK, Bower JH, et al. Detection of preclinical Parkinson disease in at-risk family members with use of [¹²³I] β -CIT and SPECT: an exploratory study. *Mayo Clin Proc.* 1999;74:681–685.
39. Pirker W, Djamshidian S, Asenbaum S, et al. Progression of dopaminergic degeneration in Parkinson's disease and atypical parkinsonism: a longitudinal β -CIT SPECT study. *Mov Disord.* 2002;17:45–53.





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J Nucl Med. 2003;44:663-670.

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The Journal of Nuclear Medicine is published monthly.
SNMMI | Society of Nuclear Medicine and Molecular Imaging
1850 Samuel Morse Drive, Reston, VA 20190.
(Print ISSN: 0161-5505, Online ISSN: 2159-662X)

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