



## Analytical Methods

Highly sensitive electrochemical impedance spectroscopy immunosensor for the detection of AFB<sub>1</sub> in olive oilLili Yu, Yang Zhang, Chenyi Hu, Hui Wu, Yayun Yang, Chusen Huang, Nengqin Jia<sup>\*</sup>

The Education Ministry Key Laboratory of Resource Chemistry and Shanghai Key Laboratory of Rare Earth Functional Materials, Department of Chemistry, Shanghai Normal University, Shanghai 200234, China

## ARTICLE INFO

## Article history:

Received 18 June 2013

Received in revised form 16 March 2014

Accepted 11 December 2014

Available online 18 December 2014

## Keywords:

Immunosensor

Carbon nanotube

Room temperature ionic liquids (RTILs)

Aflatoxin B<sub>1</sub> (AFB<sub>1</sub>)

Olive oil

Electrochemical impedance spectroscopy (EIS)

## ABSTRACT

Aflatoxin produced by *Aspergillus flavus* and *Aspergillus parasiticus* are commonly found in olive and its derivatives. Aflatoxin B<sub>1</sub> (AFB<sub>1</sub>) is a predominant toxin detected abundantly and has been implicated in the etiology of human hepatocellular carcinoma. This study proposes a sensitive and convenient electrochemical impedance spectroscopy (EIS) method for determining AFB<sub>1</sub> by MWCNTs/RTIL composite films-based immunosensor. The calibration curve for AFB<sub>1</sub> was linear in the range of 0.1–10 ng mL<sup>−1</sup> with the limit of detection (LOD) 0.03 ng mL<sup>−1</sup>. The presence of MWCNTs warrant fast electron transfer, and the ionic liquid provides a benign microenvironment for antibody. The experimental parameters, such as pH and incubating time, have been investigated and optimized. Furthermore, the detection of AFB<sub>1</sub> is presented to test this method after extracted from olive oils. It can be anticipated that this method would be used for the detection of AFB<sub>1</sub> in various agriculture products and vegetable oils.

© 2014 Elsevier Ltd. All rights reserved.

## 1. Introduction

Aflatoxins are a group of highly toxic secondary metabolites produced mainly by *Aspergillus flavus* and *Aspergillus parasiticus* on a variety of food products (Li et al., 2009). These toxins are known to be potent carcinogens, teratogens, mutagens, and immunosuppression and pose harmful threat to animal and human health. Naturally occurring aflatoxins are composed of B<sub>1</sub>, B<sub>2</sub>, G<sub>1</sub> and G<sub>2</sub>. Among them, aflatoxin B<sub>1</sub> (AFB<sub>1</sub>) is the most abundant and carcinogenic. The International Agency for Research on Cancer (IARC) has classified AFB<sub>1</sub> as a Group 1 carcinogenic to humans (Piermarini, Micheli, Ammida, Palleschi, & Moscone, 2007). The European Committee Regulations (ECR) has established the maximum permitted levels of 2 ng/g for aflatoxin B<sub>1</sub> and 4 ng/g for total aflatoxins (B<sub>1</sub>, B<sub>2</sub>, G<sub>1</sub> and G<sub>2</sub>) in various products (Gilbert & Anklam, 2002).

The olive (*Olea europaea* L.) and its derivatives, in particular olive oil, are significant products in the Mediterranean and Middle East regions (Cavaliere et al., 2007). Several survey studies have shown that olives are often stored for weeks in conditions that promote the mold growth, and the possible presence of aflatoxins would transfer into olive oil (Ghitakou, Koutras, Kanellou, &

Markaki, 2006). Since olive oils are widely consumed as diet in the Mediterranean, even low levels of contamination may cause severe health and safety problems.

Several methods and techniques for aflatoxin determination have been developed. High-performance liquid chromatography (HPLC) (Hu, Zheng, Zhang, & He, 2006), thin layer chromatography (TLC) (Lin, Zhang, Wang, Wang, & Chen, 1998), enzyme-linked immunosorbent assay (ELISA) (Rossi et al., 2012) and fluorescence methods have been used for the detection of aflatoxins. However, most of these techniques require well equipped laboratories, trained personnel, harmful solvents and are time-consuming. Thus, there is a need for developing a simple, rapid, and an effective analytical method for the determination of aflatoxins.

In comparison with abovementioned methods, the electrochemical impedance spectroscopy (EIS) technique is low-cost, sensitive and relatively easy to use (Ding, Du, Wu, & Ju, 2007). Impedance spectroscopy (EIS) is a non-destructive steady-state technique, and can be used as an ideal tool to detect the dynamics of bio-molecular interactions (Vig, Radoi, Muñoz-Berbel, Gyemant, & Marty, 2009).

In this work, a practical and sensitivity impedimetric immunosensor is proposed for the determination of aflatoxin-B<sub>1</sub> based on MWCNTs/RTIL/Ab-modified electrode. CNTs are highly electroconductive and characterized by a large surface area and excellent chemical and physical stabilities. Ionic liquids are ion conductive, and display a wide electrochemical potential window (Opallo &

<sup>\*</sup> Corresponding author. Tel.: +86 21 64321045; fax: +86 21 64321833.

E-mail address: [nqjia@shnu.edu.cn](mailto:nqjia@shnu.edu.cn) (N. Jia).

Lesniewski, 2011). Ionic liquids have also received much attention due to their unique structural and intermediate phase properties in nanometer-scale confinement (Chen et al., 2009). These properties are promising for electrode modifiers that are required to mediate electron-transfer reactions between electrodes and redox active species. The MWCNTs in the ILs exist as a three-dimensional (3D)-network structure of considerably untangled and much finer bundles, which are physically cross-linked due to cation- $\pi$  and  $\pi$ - $\pi$  interactions between the imidazolium cations and CNTs (Fujita, Murata, Masuda, Nakamura, & Ohno, 2012). The three-dimensional network will provide numerous conductive microcavities for the antibodies immobilization and small molecule hapten transfer (Li et al., 2012; Moghaddam, Løbersli, Gebhardt, Braunagel, & Marvik, 2001). The ionic liquid provides excellent biocompatible microenvironment to maintain activity of the antibody, and can be used as an excellent conductive binder to immobilize antibodies and MWCNTs onto the surface of electrode (Opallo & Lesniewski, 2011). Recombinant antibodies to low molecular weight haptens are of interest for diagnostic detection of food toxins, environmental pollutants and drugs of abuse. In present work, antibody against AFB<sub>1</sub> is used as probe for immunosensor construction. For practical application, the efficiency of the immunosensor has been evaluated by spiking blank olive oil with AFB<sub>1</sub>.

## 2. Materials and methods

### 2.1. Materials

The aflatoxin B<sub>1</sub> (AFB<sub>1</sub>) standard sample was obtained from Beijing Lianlixin BioTech Co., Ltd. Monoclonal antibody (Ab) was from Wuxi Jieshenglietang Bio-Tech Co., Ltd. Olive oil was purchased from a supermarket in Shanghai (China). Phosphate buffer solution (10 mM PBS, pH 7.5) contained 87 mM Na<sub>2</sub>HPO<sub>4</sub>, 14 mM KH<sub>2</sub>PO<sub>4</sub>, 137 mM NaCl, 2.7 mM KCl. Aqueous solutions of K<sub>3</sub>Fe(CN)<sub>6</sub>/K<sub>4</sub>Fe(CN)<sub>6</sub> (1.0 mM, 1:1) mixture with 0.1 M KCl (as the supporting electrolyte) were prepared as electrochemical probes. 1-Butyl-3-methylimidazolium hexafluorophosphate ([BMIM]PF<sub>6</sub>) was purchased from Hangzhou Kemer Chemical Co., Ltd. (China). Multi-wall carbon nanotubes (MWCNTs) (95% purity, diameter 10–20 nm, length 1–2  $\mu$ m) were purchased from Shenzhen Nanotech Port Co., Ltd. Hexane (AR), methanol (AR), and chloroform (AR) were purchased from Shanghai Chemical Reagent Ltd. (China). Ultra-pure water (18.2 MO) was used throughout the experiments.

### 2.2. Apparatus

All of the electrochemical experiments were carried out with a model CHI660B electrochemical workstation (Shanghai Chenhua Instruments, Shanghai, China). Electrochemical measurements were performed with a conventional three-electrode system

comprised of a platinum wire as the auxiliary electrode, saturated calomel electrode (SCE) as the reference and a modified GCE as the working electrode. All electrochemical measurements were carried out in PBS buffer (10 mM phosphate, pH 7.4) containing 1.0 mM K<sub>3</sub>Fe(CN)<sub>6</sub>/K<sub>4</sub>Fe(CN)<sub>6</sub> (1:1) and 0.1 M KCl as a redox couple. The electrochemical impedance spectra were recorded in the frequency range from 0.1 to 10<sup>5</sup> Hz, at the formal potential (0.20V versus SCE) of the redox couple and with a perturbation potential of 5 mV.

### 2.3. Functionalization of MWCNTs

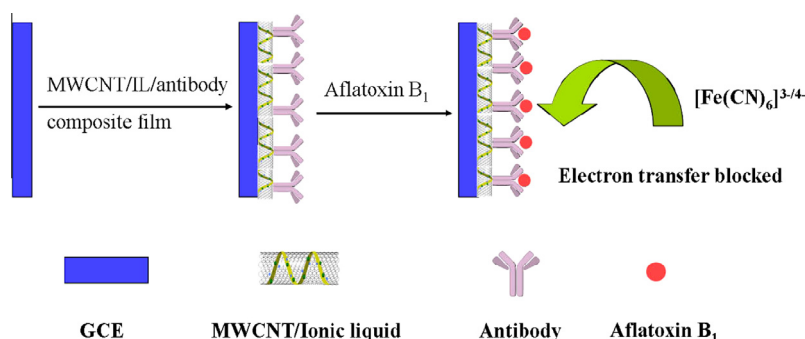
MWCNTs were suspended in a concentrated sulfuric acid/nitric acid mixture (3:1 v/v) and sonicated in a sonic bath for 16 h. After this treatment, the shortened carboxylate MWCNTs were obtained after filtration and were then thoroughly rinsed with water (Jia et al., 2010).

### 2.4. Electrodes preparation

Prior to modification, the glassy carbon electrodes (GCE, 3 mm in diameter) were polished with 0.3  $\mu$ m and 0.05  $\mu$ m alumina powder to form a mirror surface. The electrodes were successively sonicated in 1:1 (v/v) nitric acid/water solution, acetone and ultra-pure water, and then allowed to dry under a stream of nitrogen. Initially, a MWCNTs/ionic liquid mixture was prepared by adding 0.5 mg of the shortened carboxylate MWCNTs into 0.25 mL of the ionic liquid, and grinded them in an agate mortar for about 1 h. Then the suspensions were centrifuged at 15,000 rpm for about 30 min. The [bmim]PF<sub>6</sub>/MWCNTs was obtained by removing the supernatant with a pipette. Following that, for preparing MWCNTs/RTILs/Ab modified electrode, 0.25 mL of the Ab (1.64  $\mu$ g mL<sup>-1</sup>) solution was dropped into the MWCNTs/RTILs mixture, and slightly stirred for 0.5 h. Then 3  $\mu$ L of the above mixture was dropped on the electrode surface to fabricate electrochemical biosensing layers. The electrode was left in a fume cupboard to dry for 8 h at room temperature. Subsequently, for immunity of the sensor, the modified electrode was incubated in the 10 mL of PBS (pH 7.5) containing different concentrations of AFB<sub>1</sub> at 37 °C for 25 min. After this process, the MWCNTs/RTILs/Ab/AFB<sub>1</sub> electrode was rinsed with water and then with phosphate-buffered saline (pH 7.5) solution. As comparison, the MWCNTs/RTILs mixture modified electrodes were prepared in a similar way. The fabricated immunosensor was stored at 4 °C when not in use. The prepared process of MWCNTs/RTILs/Ab/AFB<sub>1</sub> immunosensor is schematically illustrated in Scheme 1.

### 2.5. Preparation of aflatoxin standards

Aflatoxin standard solutions were prepared as detailed in AOAC 971.22 (18th edition, 2005) (Horwitz & Jr., 2005). Using this



Scheme 1. Schematic representation of the fabrication of the immunosensor.

procedure, individual solutions of aflatoxins B<sub>1</sub> were prepared by dissolving approximately 0.1 mg of each aflatoxin with benzene/acetonitrile (98:2, v/v) in a 100 mL volumetric flask.

### 2.6. Spiking of olive oil samples

Oil samples were spiked with aflatoxins B<sub>1</sub> at 1, 10, 30, 50, 70, 100, 130, 150 ng mL<sup>-1</sup> levels in triplicate. These spike levels represent values above and below the maximum allowable regulatory limits of the European Committee Regulations (ECR), which is 2 µg/kg. Oil samples (2 g) were spiked in triplicate with 100 µL of aflatoxin standard solution for each of the three aflatoxin concentrations. A blank spiked with the solvent only and no aflatoxin was also prepared for each oil sample.

### 2.7. Extraction

Aflatoxins were extracted from oil samples by using the procedure developed by Daradimos et al. during which the final clean-up step using Sep-Pak cartridge was omitted (Daradimos, Marcaki, & Koupparis, 2000). Briefly, spiked oil samples (20 g) and hexane (80 mL) were transferred into a 250 mL separating funnel and extracted with 120 mL methanol/water extraction solvent (60/40 v/v) containing 4% NaCl. Then, AFB<sub>1</sub> was extracted from the obtained aqueous/methanolic by chloroform (26 mL).

## 3. Results and discussion

### 3.1. Cyclic voltammetry characterization

The changes of interface properties on the modified electrode after each assembly step could be efficiently detected by CV. Fig. 1A shows the cyclic voltammogram measurements based on the MWCNTs/RTILs/Ab-based immunosensor incubated in PBS (at pH 7.5) containing different concentrations of AFB<sub>1</sub> (0.0, 1.0, 5.0 ng mL<sup>-1</sup>) and 1.0 mmol L<sup>-1</sup> [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup>. A pair of well defined oxidation and reduction peaks is observed at the bare GCE (Fig. 1A, curve a) due to high electron-transfer between [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup> solution and the electrode. Immobilization of Ab-MWCNTs/RTILs on the GCE decreases the current of the redox couple (Fig. 1A, curve b). The reason is mainly attributed to the protein layer on the MWCNTs, which acts as an inert electron transfer blocking layer and hinders the diffusion of redox couple toward the electrode surface. After the binding of AFB<sub>1</sub> to the immobilized antibodies, the peak current of the redox couple was further reduced (Fig. 1A, curve c and d). It is reasonable that the Ab-AFB<sub>1</sub>

complex layer blocked the electron communication between the redox couple [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup> and the electrode.

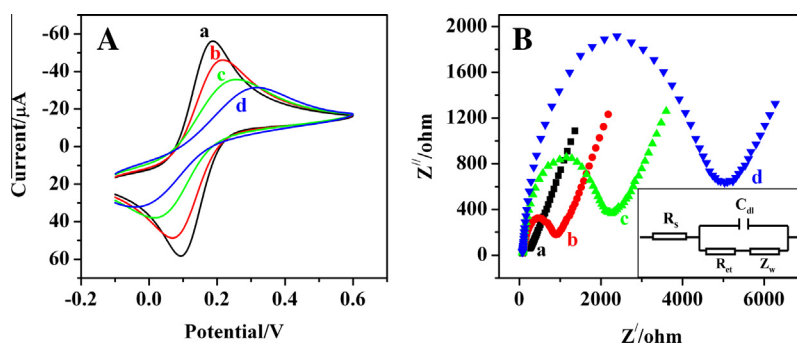
### 3.2. Impedance spectroscopy characterization

Electrochemical impedance spectroscopy is a highly effective technique to investigate the electron-transfer properties of the modified electrodes (Hu et al., 2012; Weng, Zhang, Sun, & Wang, 2011). The impedance spectra include a semicircle part at high frequencies and a linear part at lower frequencies. The semicircle portion corresponds to the electron transfer limited process and the linear portion results from the diffusion limiting step of the electrochemical process. The semicircle diameter in the impedance spectra infers the electron transfer resistance ( $R_{et}$ ) (Cui, Huang, Yin, Gao, & Zhu, 2008). An equivalent circuit model (inset in Fig. 1B) was used to fit the impedance data into  $R_{et}$  values. As shown in Fig. 1B, at a bare GCE, the redox process of the probe showed an electron-transfer resistance of about 151.9 Ω (Fig. 1B, curve a), while the MWCNTs/RTILs/Ab-modified electrode showed a higher resistance (605.6 Ω, Fig. 1B, curve b). When AFB<sub>1</sub> was immobilized on MWCNTs/RTILs/Ab-modified electrode, the  $R_{et}$  increased to 1865 Ω (Fig. 1B, curve c) and 4185 Ω (Fig. 1B, curve d), which is proportional to the amount of AFB<sub>1</sub> (1.0 ng mL<sup>-1</sup> and 5.0 ng mL<sup>-1</sup>, respectively). The increase of  $R_{et}$  is caused by electrically insulating bioconjugates produced from specific interaction of AFB<sub>1</sub> and Ab, which will block the electron-transfer process of the redox probe. Therefore, the results of electrochemical impedance spectroscopy (EIS) assays were in correspondence with those of the above CV measurements.

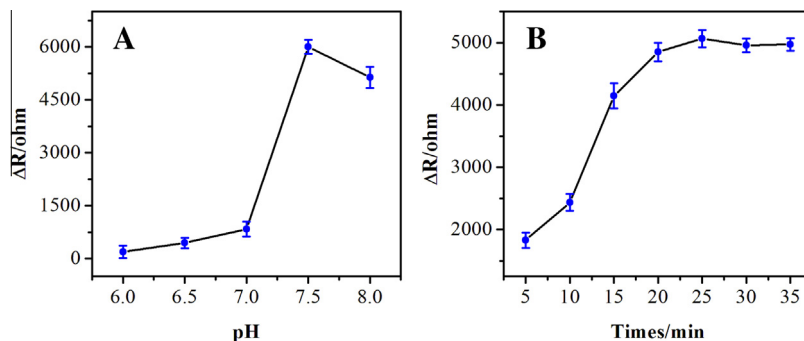
### 3.3. Optimization of experimental conditions

At the fabricated immunosensor, the electrochemical signal was related to the preparation process of the modified film, containing pH of the solution and incubation time of antigen. It is well known that protein activity is highly pH dependent and the optimum pH for anti-AFB<sub>1</sub> antibody activity could be determined experimentally. It can be seen from Fig. 2A that the  $\Delta R_{et}$  value increased with the increase of pH from 6.0 to 8.0. The immunosensor demonstrated the maximum response at pH 7.5. Consequently, an ideal pH of about 7.5 was selected for the test.

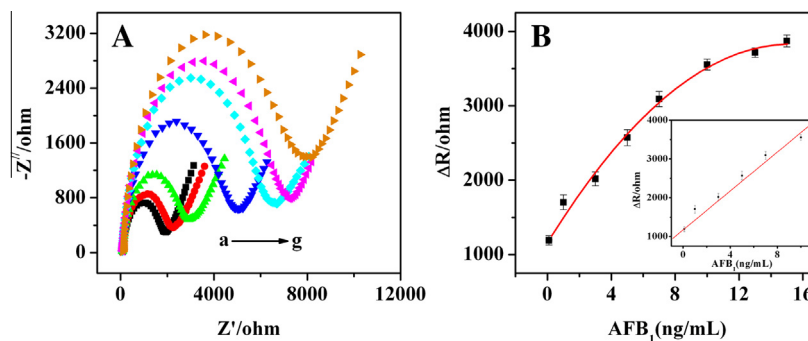
The incubation time was an important parameter for capturing AFB<sub>1</sub> antigens on the electrode surface. After increasing the incubation time with 7 ng mL<sup>-1</sup> AFB<sub>1</sub>, the impedance response at the MWCNTs/RTILs/Ab-modified electrode increased and tended to a steady value after 25 min (Fig. 2B), indicating that the bonding sites of anti-AFB<sub>1</sub> antibody tend to saturate. Longer incubation



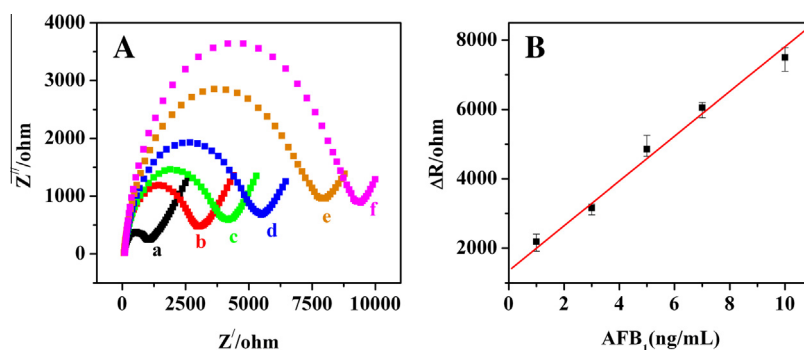
**Fig. 1.** Characterization of different electrodes by (A) cyclic voltammograms and (B) electrochemical impedance spectroscopy, (a) bare GCE and modified GCE fabricated based on the MWCNTs/RTIL composite films incubated in PBS (at pH 7.5) containing AFB<sub>1</sub> of (b) 0.0 ng mL<sup>-1</sup>, (c) 1.0 ng mL<sup>-1</sup> and (d) 5.0 ng mL<sup>-1</sup> for 25 min in 1.0 mol L<sup>-1</sup> [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup>. (Inset) An equivalent circuit representing the immunosensor-electrolyte solution interface.  $R_s$  is the solution-phase resistance;  $C_{dl}$  is the double-layer capacitance;  $R_{et}$  is the electron transfer resistance;  $Z_w$  is the Warburg impedance.



**Fig. 2.** Effect of (A) pH of PBS on the specific binding of AFB<sub>1</sub> and the Ab immobilized on the surface of the immunosensor. (B) Incubation time on the specific binding of AFB<sub>1</sub> and the antibody immobilized on the surface of the immunosensor.



**Fig. 3.** (A) Nyquist diagrams of MWCNTs/RTIL/Ab/AFB<sub>1</sub> modified GCE after incubation at 37 °C with (a) 0.1 ng mL<sup>-1</sup>, (b) 1 ng mL<sup>-1</sup>, (c) 3 ng mL<sup>-1</sup>, (d) 5 ng mL<sup>-1</sup>, (e) 7 ng mL<sup>-1</sup>, (f) 10 ng mL<sup>-1</sup>, (g) 13 ng mL<sup>-1</sup>, (h) 15 ng mL<sup>-1</sup> of aflatoxin B<sub>1</sub> in pH 7.5 PBS containing 1.0 mM of [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup>. (B) Linear relationship between electron transfer resistance and AFB<sub>1</sub> concentration in PBS.



**Fig. 4.** (A) Bare GCE electrode after modified with MWCNTs/IL/Ab, and adhered with different concentrations of AFB<sub>1</sub> in olive oil extraction solution: (a) background and after respective incubation with (b) 1 ng mL<sup>-1</sup>, (c) 3 ng mL<sup>-1</sup>, (d) 5 ng mL<sup>-1</sup>, (e) 7 ng mL<sup>-1</sup>, (f) 10 ng mL<sup>-1</sup>; (B) Linear regression of  $\Delta R_{et}$  versus concentration of AFB<sub>1</sub> in olive oil extraction solution (1–10 ng mL<sup>-1</sup>).

time would not enhance the response. Therefore, 25 min was chosen for the incubation of AFB<sub>1</sub>.

### 3.4. Analytical characteristics

The electrochemical impedimetric immunosensor response to various AFB<sub>1</sub> concentrations was studied. The modified electrode was immersed in different concentrations of AFB<sub>1</sub> and incubated at 37 °C for 25 min. After rinsed thoroughly with PBS buffer (pH 7.5) to remove nonspecifically bound conjugations, the immunosensor was used for electrochemical detection of AFB<sub>1</sub>. Measurements were carried out at conditions of frequency between 0.1 Hz to 10<sup>5</sup> Hz and an AC amplitude of 5 mV, and the representative Nyquist diagrams were shown in Fig. 3A, in which curve a–g represent the AFB<sub>1</sub> concentration of 0.1, 1, 3, 5, 7, 10, 13 and

15 ng mL<sup>-1</sup>, respectively. It can be seen that the electron-transfer resistance ( $R_{et}$ ) value increased obviously with the increasing concentration of AFB<sub>1</sub>. This result demonstrated that the more AFB<sub>1</sub> bound on the immunosensor surface, the higher was the electron-transfer resistance of the immunosensors.

The calibration curve was obtained by plotting the relative resistance versus AFB<sub>1</sub> concentration (Fig. 3B). The increased  $R_{et}$  value was proportional to the logarithm of the AFB<sub>1</sub> concentration in the range of 0.1–10 ng mL<sup>-1</sup>. The linear equation could be depicted as  $\Delta R_{et} (\Omega) = 268.4 C + 1217.6$  ( $R = 0.995$ ). The detection limit of 0.03 ng mL<sup>-1</sup> could be estimated from the signal-to-noise characteristics of these measurement data ( $S/N = 3$ ). The change of electron-transfer resistance tended to a relatively steady value when the concentration of AFB<sub>1</sub> exceeding 10 ng mL<sup>-1</sup>.



**Table 1**

The results of spiked olive oil samples using an electrochemical biosensor for AFB<sub>1</sub> determination.

Samples	AFB <sub>1</sub> added (ng mL <sup>-1</sup> )	AFB <sub>1</sub> found (ng mL <sup>-1</sup> )	RSD (%)	Recovery (%) <sup>a</sup>
1	2	2.3	5.7	116
2	4	4.14	2.3	104
3	7	6.75	3.1	96

<sup>a</sup> Averages of three different samples.

### 3.5. Stability and reproducibility of the AFB<sub>1</sub> immunosensor

The long-term stability and reproducibility of the EIS biosensor was also tested. After two months' storage (4 °C), the impedance response was retained at 87% value of the initial response. This indicated that the developed AFB<sub>1</sub> biosensor possessed good storage stability. The relative standard deviation (RSD) of intra-assay was investigated to be 4.3% and 2.7% by measuring the immunosensor response at the AFB<sub>1</sub> concentrations of 3 ng mL<sup>-1</sup> and 5 ng mL<sup>-1</sup>, showing an acceptable precision. For inter-assay reproducibility testing, a series of six measurements based on six immunosensors resulted in an RSD of 5.6% at 5 ng mL<sup>-1</sup> AFB<sub>1</sub>. The results indicated that the preparation of the immunosensor had acceptable inter-assay reproducibility.

### 3.6. Measurement of AFB<sub>1</sub> in olive oils

To demonstrate the applicability of the proposed method, the immunosensor-based EIS assay was then applied to the detection of the AFB<sub>1</sub> in olive oils. The olive oils samples were collected and the extraction procedure was performed as described in preparation Section. The MWCNTs/RTILs/Ab-based immunosensor was incubated in olive oil extraction solutions containing different concentrations of AFB<sub>1</sub> (1–10 ng mL<sup>-1</sup>) at 37 °C for 25 min, and then carried out a series of EIS measurements with [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup> as a redox probe (Fig. 4A). The corresponding calibration plot (Fig. 4B) of background-subtracted  $R_{et}$  value versus AFB<sub>1</sub> concentration was described by the follow equation:  $\Delta R_{et} (\Omega) = 600.56 C + 1651.9$ . Thus, the original concentration of AFB<sub>1</sub> in olive oil samples can be calculated from the calibration curve. For each concentration, five different samples were analyzed independently. Recovery studies were carried out with AFB<sub>1</sub> solution and AFB<sub>1</sub> spiked oil sample at different levels. Three olive oils samples were spiked to obtain final concentrations of AFB<sub>1</sub> equal to 2, 4 and 7 ng mL<sup>-1</sup>, respectively. The recovery was found to be in the range of 96–116%. For the replicate measurements, the accuracy was determined by calculating the relative standard deviation (RSD) and the values are summarized in Table 1. The obtained good recovery data demonstrated the suitability of the proposed method for the detection of AFB<sub>1</sub> in olive oil.

Furthermore, the results obtained by this immunosensor-based method was also compared to a standard fluorescence-based approach. As displayed in Table S1, the relative deviation was lower than 6.5%, confirming our developed immunosensor has a potential application in detection AFB<sub>1</sub> with a good accuracy and precision.

## 4. Conclusion

In summary, this study has successfully developed a simple, reliable method for the determination of aflatoxins B<sub>1</sub> in olive oils after the simple and rapid extraction procedure. Due to the ionic liquid offers mild microenvironment and good conductivity, experimental results indicated that the electrochemical immunoassay exhibited high sensitivity, acceptable reproducibility and stability. The simplicity of the method should make it suitable for use in the detection of many other agriculture products and vegetable oils (such as

cereals, nuts, peanuts, fruits, oilseeds and dried fruits). Our future study will use this method to prepare an electrochemical immunosensor for detecting aflatoxins in other products.

## Acknowledgments

This work was supported by Shanghai Sci. & Tech. Committee (12JC1407200), National Natural Science Foundation of China (21373138), Program for Changjiang Scholars and Innovative Research Team in University (IRT1269).

## Appendix A. Supplementary data

Supplementary data associated with this article can be found, in the online version, at <http://dx.doi.org/10.1016/j.foodchem.2014.12.030>.

## References

- Cavaliere, C., Foglia, P., Guarino, C., Nazzari, M., Samperi, R., & Lagana, A. (2007). Determination of aflatoxins in olive oil by liquid chromatography–tandem mass spectrometry. *Analytica Chimica Acta*, 596, 141–148.
- Chen, S., Kobayashi, K., Miyata, Y., Imazu, N., Saito, T., Kitaura, R., et al. (2009). Morphology and melting behavior of ionic liquids inside single-walled carbon nanotubes. *Journal of the American Chemical Society*, 131, 14850–14856.
- Cui, R., Huang, H., Yin, Z., Gao, D., & Zhu, J. J. (2008). Horseradish peroxidase-functionalized gold nanoparticle label for amplified immunoanalysis based on gold nanoparticles/carbon nanotubes hybrids modified biosensor. *Biosensors & Bioelectronics*, 23, 1666–1673.
- Daradimos, E., Marcaki, P., & Koupparis, M. (2000). Evaluation and validation of two fluorometric HPLC methods for the determination of Aflatoxin B<sub>1</sub> in olive oil. *Food Additives & Contaminants*, 17, 65–73.
- Ding, L., Du, D., Wu, J., & Ju, H. (2007). A disposable impedance sensor for electrochemical study and monitoring of adhesion and proliferation of K562 leukaemia cells. *Electrochemistry Communications*, 9, 953–958.
- Fujita, K., Murata, K., Masuda, M., Nakamura, N., & Ohno, H. (2012). Ionic liquids designed for advanced applications in bioelectrochemistry. *RSC Advances*, 2, 4018–4030.
- Ghitakou, S., Koutras, K., Kanellou, E., & Markaki, P. (2006). Study of Aflatoxin B<sub>1</sub> and ochratoxin A production by natural microflora and *Aspergillus parasiticus* in black and green olives of Greek origin. *Food Microbiology*, 23, 612–621.
- Gilbert, J., & Ankam, E. (2002). Validation of analytical methods for determining mycotoxins in foodstuffs. *TrAC Trends in Analytical Chemistry*, 21, 468–486.
- Horwitz, W. L., & Jr., G. W. L. (2005). Official Methods of Analysis of AOAC International. *Official Method*, 971.22, 18th ed.
- Hu, C., Yang, D.-P., Xu, K., Cao, H., Wu, B., Cui, D., et al. (2012). Ag@BSA core/shell microspheres as an electrochemical interface for sensitive detection of urinary retinal-binding protein. *Analytical Chemistry*, 84, 10324–10331.
- Hu, Y.-Y., Zheng, P., Zhang, Z.-X., & He, Y.-Z. (2006). Determination of aflatoxins in high-pigment content samples by matrix solid-phase dispersion and high-performance liquid chromatography. *Journal of Agricultural and Food Chemistry*, 54, 4126–4130.
- Jia, N., Lian, Q., Tian, Z., Duan, X., Yin, M., Jing, L., et al. (2010). Decorating multi-walled carbon nanotubes with quantum dots for construction of multi-color fluorescent nanoprobe. *Nanotechnology*, 21, 045606.
- Li, P., Zhang, Q., Zhang, W., Zhang, J., Chen, X., Jiang, J., et al. (2009). Development of a class-specific monoclonal antibody-based ELISA for aflatoxins in peanut. *Food Chemistry*, 115, 313–317.
- Li, X., Li, P., Zhang, Q., Li, Y., Zhang, W., & Ding, X. (2012). Molecular characterization of monoclonal antibodies against aflatoxins: a possible explanation for the highest sensitivity. *Analytical Chemistry*, 84, 5229–5235.
- Lin, L., Zhang, J., Wang, P., Wang, Y., & Chen, J. (1998). Thin-layer chromatography of mycotoxins and comparison with other chromatographic methods. *Journal of Chromatography A*, 815, 3–20.
- Moghaddam, A., Løbersli, I., Gebhardt, K., Braunagel, M., & Marvik, O. J. (2001). Selection and characterisation of recombinant single-chain antibodies to the hapten aflatoxin-B<sub>1</sub> from naive recombinant antibody libraries. *Journal of Immunological Methods*, 254, 169–181.
- Opallo, M., & Lesniewski, A. (2011). A review on electrodes modified with ionic liquids. *Journal of Electroanalytical Chemistry*, 656, 2–16.
- Piermarini, S., Micheli, L., Ammida, N., Palleschi, G., & Moscone, D. (2007). Electrochemical immunosensor array using a 96-well screen-printed microplate for Aflatoxin B<sub>1</sub> detection. *Biosensors & Bioelectronics*, 22, 1434–1440.
- Rossi, C. N., Takabayashi, C. R., Ono, M. A., Saito, G. H., Itano, E. N., Kawamura, O., et al. (2012). Immunoassay based on monoclonal antibody for aflatoxin detection in poultry feed. *Food Chemistry*, 132, 2211–2216.
- Vig, A., Radoi, A., Muñoz-Berbel, X., Gyemant, G., & Marty, J.-L. (2009). Impedimetric aflatoxin M<sub>1</sub> immunosensor based on colloidal gold and silver electrodeposition. *Sensors and Actuators B: Chemical*, 138, 214–220.
- Weng, J., Zhang, Z., Sun, L., & Wang, J. A. (2011). High sensitive detection of cancer cell with a folic acid-based boron-doped diamond electrode using an AC impedimetric approach. *Biosensors & Bioelectronics*, 26, 1847–1852.